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ABOUT COVER

Editorial board member of *World Journal of Stem Cells*, Dr. Elisa Oltra is Distinguished Professor at the Catholic University of Valencia (UCV), Spain. Having received her Bachelor's and Master's degrees in Biochemistry at UCV in 1988 and her PhD degree in Cell and Molecular Biology at the University of Miami, FL, United States in 1999, she returned to UCV in 2009, where she became Director of the first official European Master's degree program in Biobanking. Her current research interests include the identification of molecular biomarkers of fibromyalgia and myalgic encephalomyelitis/chronic fatigue syndrome (ME/CFS) and the study of immunomodulatory potential of mesenchymal stem cells. She has also served as Chair of the Biomarker subgroup ME/CFS Common Data Elements NINDS initiative at the National Institutes of Health (United States). (L-Editor: Filipodia)

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Dental stem cells: The role of biomaterials and scaffolds in developing novel therapeutic strategies

Cornelia Larissa Granz, Ali Gorji

ORCID number: Cornelia Larissa Granz [0000-0002-6284-0764](https://orcid.org/0000-0002-6284-0764); Ali Gorji [0000-0002-4557-3270](https://orcid.org/0000-0002-4557-3270).

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Cornelia Larissa Granz, Ali Gorji, Epilepsy Research Center, Westfälische Wilhelms-Universität Münster, Münster 48149, Germany

Ali Gorji, Department of Neurosurgery and Department of Neurology, Westfälische Wilhelms-Universität, Münster 48149, Germany

Ali Gorji, Shefa Neuroscience Research Center, Khatam Alanbia Hospital, Tehran 1996836111, Iran

Ali Gorji, Neuroscience Research Center, Mashhad University of Medical Sciences, Mashhad 9177948564, Iran

Corresponding author: Ali Gorji, MD, Full Professor, Epilepsy Research Center, Westfälische Wilhelms-Universität Münster, Domagkstr 11, Münster 48149, Germany. gorjial@uni-muenster.de

Abstract

Dental stem cells (DSCs) are self-renewable cells that can be obtained easily from dental tissues, and are a desirable source of autologous stem cells. The use of DSCs for stem cell transplantation therapeutic approaches is attractive due to their simple isolation, high plasticity, immunomodulatory properties, and multipotential abilities. Using appropriate scaffolds loaded with favorable biomolecules, such as growth factors, and cytokines, can improve the proliferation, differentiation, migration, and functional capacity of DSCs and can optimize the cellular morphology to build tissue constructs for specific purposes. An enormous variety of scaffolds have been used for tissue engineering with DSCs. Of these, the scaffolds that particularly mimic tissue-specific microenvironment and loaded with biomolecules favorably regulate angiogenesis, cell-matrix interactions, degradation of extracellular matrix, organized matrix formation, and the mineralization abilities of DSCs in both *in vitro* and *in vivo* conditions. DSCs represent a promising cell source for tissue engineering, especially for tooth, bone, and neural tissue restoration. The purpose of the present review is to summarize the current developments in the major scaffolding approaches as crucial guidelines for tissue engineering using DSCs and compare their effects in tissue and organ regeneration.

Key Words: Cell transplantation; Regenerative medicine; Tissue engineering; Neural crest; Angiogenesis; Biomolecules

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Core Tip: Dental stem cells have been used for different types of cell transplantation therapies, including teeth, bone, and neural tissue regeneration. In planning for successful tissue engineering toward organ-specific regeneration, choosing an appropriate scaffold that mimics the extracellular matrix in native tissue and loaded with suitable biomolecules to boost dental stem cell functions is of utmost importance.

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INTRODUCTION

Stem cells are undifferentiated cells with self-renewing and clonogenic capabilities, which can differentiate into various cell lineages. According to the basis of their origin, stem cells are categorized as embryonic, induced pluripotent stem cells (iPS), and adult (tissue-specific) stem cells^[1-3]. Based on their differentiation potential, stem cells can be classified as totipotent (the ability to give rise to all types of cells), pluripotent (the potential of the cells to produce any type of cells in the organism), multipotent (the potential to give rise to cells of their tissue of origin), oligopotent (the potential to differentiate into only a few cell types), and unipotent (the ability to produce one cell type)^[4]. Embryonic stem cells are pluripotent, whereas adult stem cells are limited to differentiating into various cell types of their original tissue (multipotent). iPS are pluripotent cells that originated from somatic differentiated cells after transduction. Adult stem cells exist in different tissues and organs, such as the bone marrow, blood vessels, peripheral blood, and skeletal muscles as well as the brain, heart, skin, intestine, liver, gonads, and teeth^[5-7].

Human mesenchymal stem cells (MSCs), which are multipotent non-hematopoietic progenitor cells, have been isolated from both adult and fetal tissues, such as the bone marrow, adipose tissue, endometrium, bone, muscle, umbilical cord, blood, Wharton's jelly, and amniotic fluid as well as nervous and dental tissues^[8]. Human MSCs have the potential to differentiate into both mesodermal (osteocytes, adipocytes, and chondrocytes) and non-mesodermal (endodermal and ectodermal) lineages (hepatocytes and neuronal cells)^[9] with both anti- and pro-tumorigenic properties^[10] as well as a limited risk of inflammatory reactions and uncontrolled growth^[11]. The source of MSCs has a crucial role in the outcomes of stem cell-based tissue engineering^[12]. Dental stem cells (DSCs) are neural crest-derived cells that can be obtained easily from dental tissues of both adults and children; therefore, they are a reliable, accessible source of autologous stem cells^[13,14]. DSCs are undifferentiated cells that have non-limited self-renewal, multipotent differentiation potential, and colony-forming capacity^[15]. DSCs can be isolated from the dental pulp of deciduous, natal, and permanent teeth, the periodontal ligament, the apical papilla, the dental follicle, and gingival tissue (Figure 1)^[16,17]. One of the unique characteristics of DSCs is their ability to differentiate into mesodermal, ectodermal, and endodermal cell lineages^[18]. DSCs from each source are capable of specifically differentiating into various distinct cells, including epithelial cells, odontoblasts, osteoblasts, chondroblasts, adipocytes, vascular cells, endotheliocytes, neuronal cells, glial cells, photoreceptor cells, and muscle cells^[19,20]. Although all stem cells obtained from various sources are named DSCs in this study, their phenotype, differentiation potential (both in *in vitro* and *in vivo* conditions) and functional properties (such as biological response during differentiation and tissue repair) are different^[21]. For instance, stem cells obtained from the apical papilla possess greater proliferation ability, express a higher variety of neural markers, and induce more uniform dentine-like tissues compared to dental pulp stem cells^[22-24]. Furthermore, DSCs isolated from exfoliated deciduous teeth exert a higher capacity for osteogenic regeneration and a greater proliferation rate compared to dental pulp stem cells^[25]. DSCs isolated from pulp tissues are the first and most frequent cells evaluated for their odontogenic, osteogenic, and neurogenic differentiation potentials^[26]. This heterogeneity of DSCs is effectively modulated by the function of their microenvironment^[27]. DSCs obtained from different sources exhibit

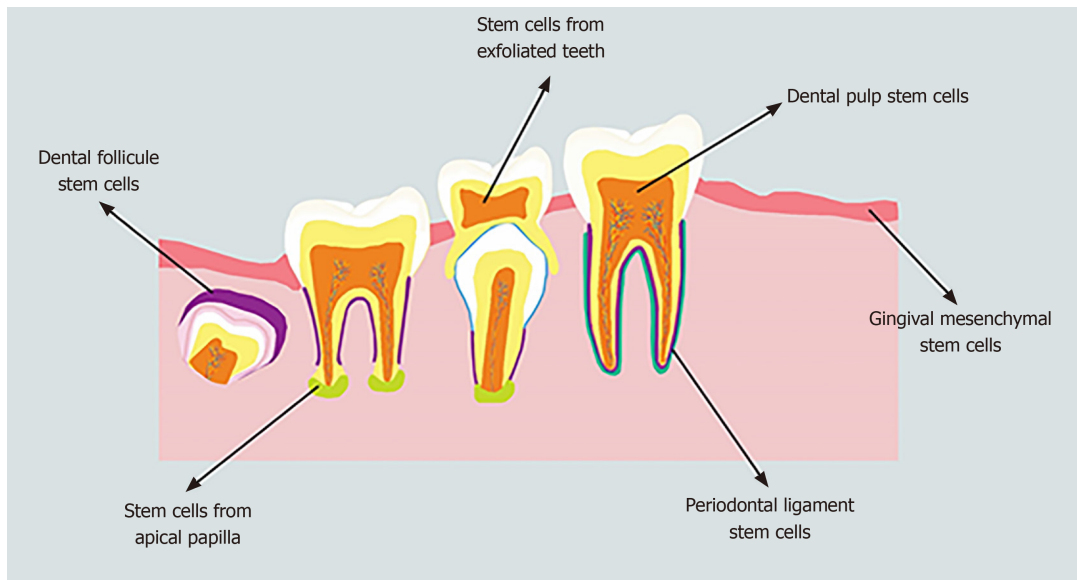


Figure 1 Schematic diagram of different sources where dental stem cells can be isolated. Various subpopulations of dental stem cells (DSCs) can be classified according to their tissue of origin. DSCs can be derived from the dental pulp stem cells, exfoliated deciduous teeth, periodontal ligament, dental follicle, apical papilla, and gingival tissue.

various patterns of cell surface markers (Table 1)^[28-31].

DSCs secrete numerous immunomodulatory mediators, such as interleukin (IL)-6, IL-10, IL-1 β , interferon- γ , and tumor necrosis factor- α as well as transforming growth factor-beta (TGF- β), hepatocyte growth factor, and vascular endothelial growth factor (VEGF)^[32], and do not express the major histocompatibility complex class II antigen^[33], which suggests their potential in the regulation of immune responses to promote tissue regeneration^[34]. DSCs from different sources may exert their immunomodulatory properties through the suppression of T-cell proliferation and lymphocyte activity as well as the activation of T-cell apoptosis^[34,35].

The fate of the stem cells (proliferation and differentiation) is regulated *via* a combination of *intrinsic* and *extrinsic* mechanisms. Intrinsic mechanisms consist of various transcription factors expressed by the cells. Extrinsic mechanisms are signals provided by the dynamic microenvironment (or “niche”), including the extracellular matrix (ECM), signaling molecules (such as growth factors and hormones), and neighboring cells^[36,37]. The microenvironment, which is a three-dimensional (3D) structure surrounded by specific cells and ECM, protects stem cells from inappropriate differentiation, cell damage, and apoptosis and governs tissue maintenance, regeneration, and repair^[38,39]. In addition to providing a physical microenvironment for cells, the ECM gives the tissue its mechanical properties (elasticity and rigidity), provides bioactive molecules and cues to residing cells, and establishes an environment to facilitate tissue remodeling in response to dynamic processes, such as wound healing^[40]. Furthermore, the ECM is produced and arranged by tissue-resident cells and secreted into the surrounding environment to provide support to the stem cells with its bioactive compounds^[41]. Stem cell behaviors are reciprocally regulated by the ECM and signals from the surrounding cells and molecules. Furthermore, inorganic ions, such as calcium and magnesium, as well as metabolic products, such as oxygen drive metabolites, and maintain stem cell fate^[42].

The nature of the stem cell microenvironment differs in various tissues. In teeth, a particular microenvironment exists at specific anatomic sites that regulates the behavior of DSCs^[39]. Two different stem cell microenvironments have been identified in teeth; (1) the pulp cell-rich zone; and (2) the perivascular and perineurium of the dental pulp. The pulp is composed of four distinct zones; an outermost layer containing the odontoblasts, a cell-free zone (zone of Weil) with no cells and rich in the ECM, the cell-rich zone contains stem/progenitor cells, and the pulp core. Dental pulp tissue is populated by odontoblasts, fibroblasts, dendritic cells, macrophages, and progenitor cells, whereas the pulp core contains dental pulp cells, vessels, nerves, and ECM^[43]. The induction of odontoblasts, the biological cells of neural crest origin that survive throughout life, occurs during tooth development. However, under appropriate conditions, DSCs can differentiate into pre-odontoblasts and later secretory odontoblasts, which actively participate in reactionary dentinogenesis^[44].

Table 1 Dental stem cells obtained from different sources exhibit various patterns of cell surface markers

| Markers | DPSCs | SCEDT | PLSCs | DFSCs | SCAP |
|----------|-------|-------|-------|-------|------|
| Nestin | + | + | + | + | |
| Vimentin | + | + | | | + |
| SOX2 | + | | + | + | + |
| SOX10 | + | | + | | |
| Stro-1 | + | + | + | + | + |
| Oct-4 | + | + | + | + | + |
| EphB | + | | | | |
| Nanog | + | + | + | | + |
| CD10 | | | + | + | |
| CD13 | + | + | + | + | + |
| CD14 | + | + | + | | |
| CD19 | + | | | | |
| CD24 | + | | | | + |
| CD25 | | | | + | |
| CD29 | + | + | + | + | + |
| CD34 | + | + | + | + | + |
| CD44 | + | + | + | + | + |
| CD45 | + | + | + | + | + |
| CD49 | | | | | + |
| CD53 | | | | + | |
| CD59 | + | | + | + | |
| CD73 | + | + | + | + | + |
| CD90 | + | + | + | + | + |
| CD105 | + | + | + | + | + |
| CD106 | | | | | + |
| CD117 | + | | | | |
| CD146 | + | + | | + | + |
| CD150 | | | | | + |
| CD166 | | + | | | + |
| CD271 | + | | + | | |
| SSEA-3 | | + | | | |
| SSEA-4 | | + | | | |
| TWIST-1 | + | | | | |
| c-myc | | + | | + | |
| Notch | | | | + | + |
| 3G5 | + | | | | |
| Klf-4 | | | + | | |
| FIK1 | + | + | | | |

DPSCs: Dental pulp stem cells; SCEDT: Stem cells obtained from exfoliated deciduous teeth; PLSCs: Periodontal ligament stem cells; DFSCs: Dental follicle stem cells; SCAP: Stem cells obtained from apical papilla.

Odontoblasts produce the main part of the ECM components of dentin and are involved in dentin mineralization^[45]. The dentin ECM consists of collagen (approximately 90%; Type I, III, and V), proteoglycans (such as chondroitin sulfate and heparan sulfate), growth factors [such as TGF- β and bone morphogenetic protein (BMP)], and enzymes (such as matrix metalloproteinase 1, 2, 3, 9, and 20)^[46]. In the dental pulp, DSCs also reside in perivascular and perineurium regions^[47], which can be identified by aldehyde dehydrogenase-1 expression^[48]. The EphB/ephrin-B signaling pathway reciprocally modulates the attachment and migration of DSCs originated from the perivascular niche *via* the mitogen-activated protein kinase pathway and phosphorylation of Src family tyrosine kinases^[49].

Pointing to the importance of ECM in maintaining homeostasis for proliferation and differentiation of DSCs, several studies have indicated that reconstruction of the appropriate microenvironment and boosting its interaction with stem cells are essential steps to successful cell therapy^[50]. The application of DSCs in stem cell therapeutic approaches is attractive due to their simple isolation and efficient administration^[51]. The multi-lineage capacity of DSCs differentiation to various tissues and organs suggests their greater ability than other adult stem cell populations for the treatment of different diseases^[52]. There is an enormous amount of evidence to indicate that DSCs have great potential for therapeutic cell approaches in various diseases, including liver disease, diabetes, myocardial infarction, ophthalmologic diseases, muscular dystrophy, Alzheimer's disease, Parkinson's disease, cerebral ischemia, and spinal cord injury^[53]. Furthermore, several studies have explored the potential of DSCs in the treatment of caries, periodontal disease, oral and maxillofacial defects, and alveolar bone atrophy^[54,55]. DSCs possess strong immunomodulatory abilities, which suggest that they are a favorable cell source for cell transplantation therapy in inflammatory disorders^[33]. It has been shown that DSCs are more beneficial for axonal regeneration than bone marrow stem cells due to their greater release of neurotrophic factors^[56]. Despite these extensive efforts, several essential parameters still need to be optimized for the clinical use of DSCs in cell transplantation therapy. One of the key challenges is the lack of an appropriate stem cell microenvironment, which leads to short-term survival of DSCs after implantation. To increase cell viability, transplanted cells require particular 3D structures with specific ECM components that protect DSCs from cell damage, maintain the stem cell homeostasis, and promote mutual biological information transfer between stem cells and the ECM^[50,57,58]. A large number of investigations have been carried out to reconstruct the stem cell microenvironment to strengthen the viability, proliferation, and appropriate differentiation of the transplanted cells for successful cell therapy^[59]. In this context, ECM scaffolds can form a desirable microenvironment for DSCs, which serve as a more favorable template for tissue repair and reconstruction^[60,61]. In this review, we provide a critical overview of the role of different biomaterials used to deliver DSCs to damaged tissue and their applications to improve, restore, and maintain tissue or organ reconstruction.

DIFFERENT TYPES OF SCAFFOLD FORMULATIONS

The general concept of tissue bioengineering involves three essential components; identification of suitable stem cells, development of appropriate scaffolds, and induction of potent signals to repair or regenerate human cells, tissues, or organs^[62]. Biomaterials are essential components for the construction of scaffolds. Tissue bioengineering combines scaffolds with various types of stem cells to reconstruct damaged tissues (Figure 2). The application of appropriate scaffolds could improve DSCs proliferation, differentiation, adhesion, and migration, which may promote their ability to repair the injured tissues and regenerate functional organs^[63]. Acellular tissues, as well as natural and synthetic biomaterials, can be used as the primary source for generating scaffolds^[64]. Acellular tissue matrices, such as an acellular adipose matrix, are derived from animal or human tissues with all cells eliminated during manufacture^[65]. In addition, the amniotic membrane has been suggested as a suitable biological scaffold for the proliferation and transplantation of DSCs^[66]. Natural biomaterials consist of proteins (collagen, gelatin, fibrin, and silk) and polysaccharides (agarose, alginate, hyaluronan, polylactic acid, and chitosan) which tend to be biocompatible due to their cellular adhesion sites, such as Arg-Gly-Asp binding sequences, and the ability to degrade without releasing toxic substances. However, due to the variability of materials, limited mechanical properties, the risk of transmitting pathogens, and provoking immune reactions, their formulations need to be promoted for stem cell culture^[67,68]. Synthetic biomaterials, including polymer-based

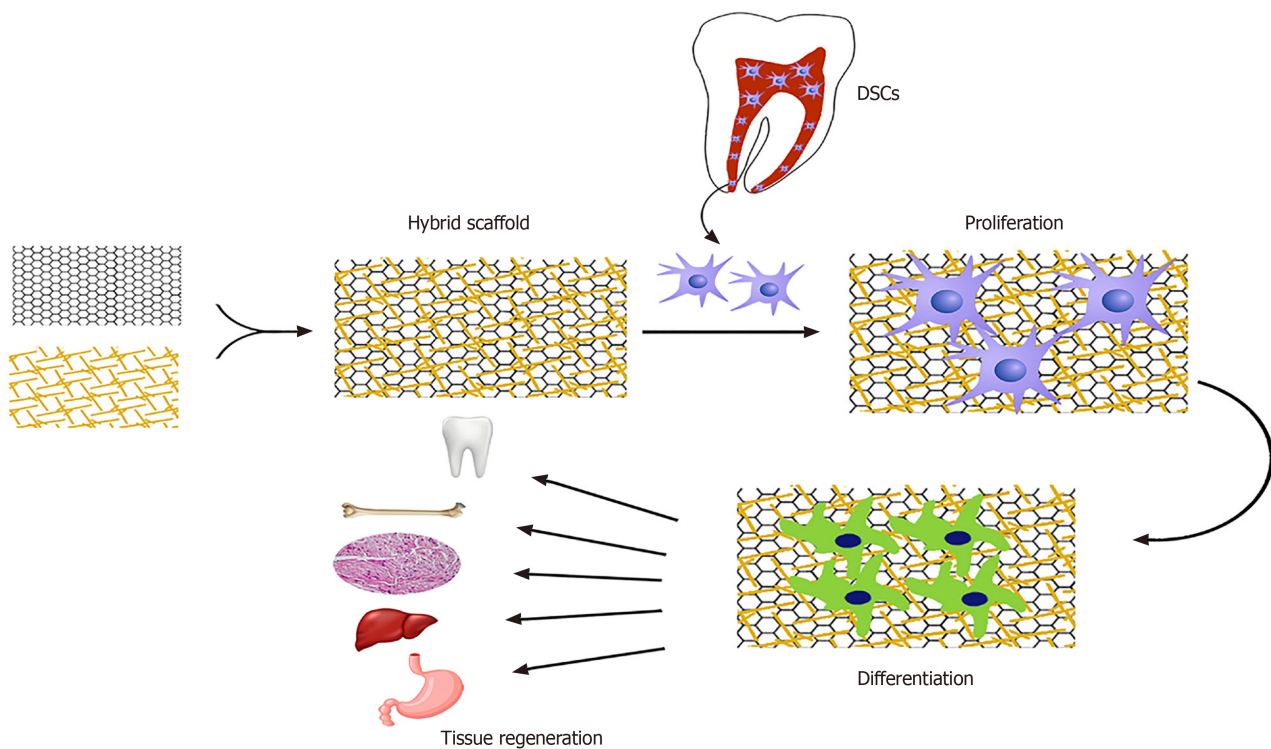


Figure 2 Schematic diagram of seeding dental stem cells on the hybrid scaffold, differentiation capability, and potential clinical applications for the regeneration of different tissues. DSCs: Dental stem cells.

biomaterials (such as polycaprolactone, polylactic acid, poly-lactic-co-glycolic acid, polyglycolide, poly-e-caprolactone, and poly-ethylene glycol) and ceramic-based biomaterials (such as hydroxyapatite, bioactive glass, and calcium phosphate) display a better mechanical property, reproducibility, and electrical conductivity as well as a lower degradation rate^[68-70]. Furthermore, synthetic biomaterials possess the possibility of optimizing the chemical and physical properties of a scaffold for a particular application^[71]. Hydrogels, which are networks of hydrophilic polymers, can be manufactured from natural biomaterials (such as collagen, fibrin, proteoglycans, and hyaluronic acid) or synthetic polymers (such as self-assembly peptide molecules or poly-ethylene glycol)^[37,72,73]. Hydrogels provide tissue-like microenvironments with particular cellular signals, desirable biocompatibility, semi-permeable membranes, and cell delivery vehicles^[74]. Furthermore, a wide range of nanocomposite biomaterials has been assembled by merging nanomaterials within the polymeric matrix to promote the efficiency of bioactive scaffolds^[75].

The desirable properties of a scaffold for stem cell transplantation are biocompatibility, biodegradability, mimic the 3D biological microenvironment, incorporation of different ECM, pore size, stability, electrical conductivity, porosity, non-immunogenicity, interconnectivity, safety (low or non-toxic) and alignment^[70,76,77]. Various fabrication techniques have been developed to produce different scaffolds, such as emulsion freeze-drying, electrospinning, thermally-induced phase separation, solvent casting/particular leaching, computer-aided design/computer-aided manufacturing, melt molding, rapid prototyping (3D printing, selective laser sintering, stereolithography, and fused deposition modeling), nanofiber self-assembly, and photolithography^[78,79]. The basic tissue engineering procedures consist of appropriate scaffold manufacture, hydrogel matrix support, and patterning design. The combination of these approaches promotes the development of the desired complex, both in tissue structure and function^[20,80].

Scaffold-based cultures are conventionally applied in two-dimensional (2D) systems. Although 2D systems are a valuable medium for the investigation of basic cell biology and preclinical drug testing, data generated in these systems are insufficient to translate into *in vivo* experimental studies^[81]. Furthermore, inappropriate cell-to-cell and cell-to-ECM contacts, reduction of polarization, and alteration of key signaling pathways modulate stem cell differentiation ability^[81,82]. Thus, several 3D scaffold-based cultures have been developed. Although existing 3D cultures are not without limitations, they enhance cell viability, growth, differentiation, and migration

and improve cellular communications^[82]. Combining DSCs with suitable scaffolds offers a promising strategy for cell delivery and transplantation. Two main approaches for this combination are cell-based and cell-free tissue engineering. In the cell-based approach, stem cells are seeded and cultured onto the scaffold *in vitro* to produce the desired tissue before transplantation^[83]. In the cell-free approach, a bioactive scaffold with growth and differentiation factors is embedded in the respective tissues, induces the homing of resident stem cells, and promotes their proliferation and differentiation^[84].

Furthermore, the environmental cues, such as various growth factors/morphogens, markedly affect the behavior of DSCs seeded in scaffolds and are vital to the success of regenerative therapies^[85,86]. Several proteins, such as BMP, sialoprotein, fibronectin, and osteopontin, are able to coat various types of biomaterials and promote the behaviors of DSCs^[87]. Pre-treatment of biomaterials with the abovementioned proteins could enhance adhesion, differentiation, proliferation, migration, and function of DSCs and improve the formation of new tissues^[87,88].

DSCS IN COMBINATION WITH SCAFFOLDS FOR TISSUE RESTORATION

DSCs represent an auspicious cell source for tissue engineering, particularly for tooth, bone, and neural tissue reconstruction. A vast number of these investigations point to the importance of various scaffolds to design effective tissue engineering approaches (Table 2).

TOOTH RECONSTRUCTION

The therapeutic role of DSCs in combination with various scaffolds has been extensively investigated in restoring tooth damage or loss due to caries, periodontal disease, trauma, or genetic disorders^[89]. The procedure of dentin formation consists of odontoblastic deposition, vascularization, and neuron formation^[20]. Among multiple approaches to promote dentin formation and teeth tissue regeneration, the application of DSCs with a synthetic pre-designed and optimized scaffold is the most accepted technique for tooth regeneration^[90]. The appropriate scaffold can be implemented with DSCs and growth factors to induce the generation of dental tissues, which can integrate with the adjacent tissues^[16]. Scaffolds developed from either synthetic or natural biomaterials have been used for tooth reconstruction. Natural materials, such as collagen^[91], chitosan/gelatin^[92], silk protein^[93], alginate^[94], hyaluronic acid^[95] as well as synthetic polymers, such as polyglycolate/poly-L-lactate^[96], polycaprolactone-poly glycolic acid^[97], polylactic acid-co-polyglycolic acid^[98], polycaprolactone /gelatin/nano- hydroxyapatite^[99], nano-hydroxyapatite/collagen/poly-L-lactide^[100] and poly-ethyl methacrylate-co-hydroxyethyl acrylate^[101] were used as scaffold materials for dental restoration and regeneration. Several investigations have indicated the regeneration of vascularized pulp-like tissue after subcutaneous implantation of tooth slices containing DSCs accompanied by an appropriate scaffold, particularly in the presence of growth factors such as dentin matrix protein^[102,103]. In several experiments, a combination of the abovementioned scaffolds was used to promote cell differentiation, vascularization, and safety as well as to reduce immunological and ectopic complications. The development of a vascularized dentin/pulp tissue in a subcutaneously transplanted human root canal containing a poly-lactic-co-glycolic acid scaffold seeded with DSCs has been reported^[104]. A scaffold consists of a pulp-specific ECM (an acellular ECM within the hydrogel) and an endothelial ECM (collagen-chitosan hydrogels) to promote odontogenic differentiation of DSCs and induce extensive vascularization in an *in vivo* model of a tooth root slice^[105]. Comparing collagen and gelatin with chitosan, it has been stated that chitosan exerts weaker support for human DSCs growth and differentiation^[106]. In addition, 3D nano-fibrous gelatin/silica bioactive glass hybrid scaffolds provide a suitable microenvironment that mimics the architecture and composition of a natural dental micromilieu and enhances the growth and differentiation of human DSCs^[107]. Furthermore, the administration of human DSCs associated with acellular dental pulp resulted in pulp-like tissue structures and the maintenance of ECM^[108]. DSCs seeded in 3D scaffold-free stem-cell sheet-derived pellets promote odontogenic differentiation^[109].

The application of combined DSCs with the ECM scaffold can be used for root canal therapy. It has been shown that DSCs are able to differentiate into functional odontoblasts with angiogenic potential^[110]. Implantation of a 3D scaffold by shaping

Table 2 A vast number of these investigations indicate the importance of various scaffolds to design effective tissue engineering approaches

| Scaffold | Growth factors/bioactive molecules | Experimental model | Target tissue | Ref. |
|---|------------------------------------|---|---------------|-------|
| Silicon | - | <i>In vitro</i> | Teeth | [168] |
| Collagen sponge | SCF | <i>In vitro</i> and <i>in vivo</i> (mice) | Teeth | [126] |
| Collagen type I and type III | SDF-1 | <i>In vivo</i> (dogs) | Teeth | [91] |
| Collagen type-I and N-acetic acid | SDF-1, bFGF, BMP-7 | <i>In vitro</i> and <i>in vivo</i> (rats) | Teeth | [120] |
| Collagen/chitosan | - | <i>In vitro</i> | - | [129] |
| Collagen-polyvinylpyrrolidone sponge | - | Case report | Teeth | [144] |
| Silk fibroin | SDF-1 | <i>In vitro</i> and <i>in vivo</i> (mice) | Teeth | [123] |
| Acellular dental pulp ECM | - | <i>In vivo</i> (mice) | Teeth | [108] |
| Intrafibrillar-silicified collagen | - | <i>In vitro</i> and <i>in vivo</i> (mice) | Teeth | [169] |
| Matrigel | bFGF-2, TGF- β 1 | <i>In vitro</i> | - | [121] |
| Peptide hydrogel | VEGF, TGF- β 1, FGF-1 | <i>In vivo</i> (mice) | Teeth | [118] |
| Gelatin methacrylate hydrogel | - | <i>In vivo</i> (rats) | Teeth | [133] |
| PuraMatrix™ | VEGF | <i>In vivo</i> (mice) | Teeth | [134] |
| Poly- ϵ -caprolactone and hydroxyapatite | SDF-1, BMP-7 | <i>In vitro</i> and <i>in vivo</i> (rats) | Teeth | [124] |
| Polycaprolactone-poly-glycolic acid | BMP-7 | <i>In vitro</i> and <i>in vivo</i> (mice) | Teeth | [97] |
| Thermoresponsive hydrogel | - | <i>In vitro</i> and <i>in vivo</i> (mice) | Teeth | [111] |
| DL-lactide/co-polymer of L-lactide /DL-lactide, and hydroxyapatite tricalcium phosphate | BMP-2 | <i>In vitro</i> and <i>in vivo</i> (mice) | Teeth | [132] |
| 3D hydroxyapatite scaffolds containing peptide hydrogels | - | <i>In vivo</i> (mice) | Teeth | [112] |
| Poly-lactic-co-glycolic acid | - | <i>In vitro</i> and <i>in vivo</i> (mice) | Teeth | [104] |
| Beta-tricalcium phosphate scaffold | BMP-2 | <i>In vitro</i> and <i>in vivo</i> (mice) | Teeth | [131] |
| Collagen sponge | - | Clinical trial | Bone | [153] |
| Collagen sponge | - | Clinical trial | Bone | [151] |
| Collagen sponge | - | Clinical trial | Bone | [152] |
| Chitosan/gelatin | BMP-2 | <i>In vitro</i> and <i>in vivo</i> (mice) | Bone | [92] |
| Arginine-glycine-aspartic acid | - | <i>In vitro</i> and <i>in vivo</i> (mice) | Bone | [141] |
| Granular 3D chitosan | - | <i>In vitro</i> | Neural tissue | [193] |
| Matrigel | BMP-9 | <i>In vitro</i> and <i>in vivo</i> (mice) | Bone | [180] |
| 3D nano-fibrous gelatin/silica bioactive glass hybrid | - | <i>In vitro</i> | Teeth | [107] |
| 3D gel collagen matrix | BMP-2 | <i>In vitro</i> and <i>in vivo</i> (rats) | Bone | [177] |
| Poly- ϵ -caprolactone biphasic calcium phosphate | - | <i>In vitro</i> and <i>in vivo</i> (rabbit) | Bone | [160] |
| Glass nanoparticles/chitosan-gelatin | - | <i>In vitro</i> and <i>in vivo</i> (rats) | Bone | [159] |
| 3D poly-lactide | Extracellular vesicles | <i>In vitro</i> and <i>in vivo</i> (rats) | Bone | [179] |
| 2D monolayer culture/3D poly lactic-co-glycolic | - | <i>In vitro</i> | Bone | [174] |
| Dense collagen gel or acellular | - | <i>In vivo</i> (rats) | Bone | [150] |
| Calcium phosphate cement functionalized with iron oxide nanoparticles | - | <i>In vitro</i> | Bone | [166] |
| Poly-lactic-co-glycolic acid | - | <i>In vitro</i> and <i>in vivo</i> (rats) | Bone | [164] |
| Hydroxyapatite-collagen sponge | - | Clinical trial | Bone | [146] |

| | | | | |
|--|--------------|---|-------------------|-------|
| 3D porous chitosan | bFGF | <i>In vitro</i> | Neural tissue | [201] |
| Fibrin and collagen | - | <i>In vivo</i> (rats) | Sciatic nerves | [9] |
| Collagen | Tetracycline | <i>In vivo</i> (mice) | Sciatic nerves | [206] |
| Collagen | - | <i>In vitro</i> and <i>in vivo</i> (rats) | Sciatic nerves | [210] |
| 3D alginate/hyaluronic acid | NGF | <i>In vitro</i> and <i>in vivo</i> (mice) | Peripheral nerves | [207] |
| Collagen sponge (DSCs condition medium) | - | <i>In vitro</i> and <i>in vivo</i> (rats) | Facial nerves | [211] |
| 3D bio-printing of scaffold-free nervous tissue | - | <i>In vitro</i> and <i>in vivo</i> (rats) | Facial nerves | [208] |
| Chitosan | - | <i>In vitro</i> and <i>in vivo</i> (rats) | Spinal cord | [198] |
| Aligned electrospun poly-ε-caprolactone/ poly-lactide-co-glycolic acid | - | <i>In vitro</i> and <i>in vivo</i> (rats) | Spinal cord | [202] |

bFGF: Basic fibroblast growth factor; BMP: Bone morphogenetic protein; NGF: Nerve growth factor; SDF: Stromal cell-derived factor; SCF: Stem cell factor; TGF-β: Transforming growth factor beta; VEGF: Vascular endothelial growth factor; DSCs: Dental stem cells; BMP: Bone morphogenetic protein; ECM: Extracellular matrix.

sheet-like aggregates of DSCs with a thermos-responsive hydrogel into the human tooth root canal generates pulp-like tissues with rich neovascularization without adding growth factors^[111]. Furthermore, transplantation of human DSCs with 3D hydroxyapatite scaffolds containing peptide hydrogels resulted in vascular ingrowth, osteodentin deposition, and pulp tissue formation in immunocompromised mice^[112]. Using bioengineered methods, it has been shown that it is possible to achieve functional teeth with entire roots^[113]. The nanofiber hydrogel PuraMatrix is a synthetic matrix that is used to create a biocompatible, biodegradable, and non-toxic 3D environment for a variety of cells^[114]. DSCs injected with PuraMatrix into full-length human root canals differentiate into functional odontoblasts; pointing to a novel strategy to facilitate root formation in damaged teeth^[115]. Several *in vitro* and *in vivo* studies revealed that the addition of various signaling molecules and growth factors [such as granulocyte colony-stimulating factor (G-CSF), stromal cell-derived factor (SDF), basic fibroblast growth factor (bFGF), and VEGF] to different scaffolds (both natural and synthetic) enhances the regeneration of intra-canal pulp-like tissues *via* the promotion of dentine formation, mineralization, neovascularization, and innervation^[116]. DSCs transplanted with SDF-1 or G-CSF on a collagen scaffold promote pulp reconstruction in an animal pulpitis model^[91,117]. Autologous DSCs transplanted into a root canal with collagen types I and III associated with SDF-1 after pulpectomy in dogs significantly increased the expression of angiogenic and neurotrophic factors, indicating the potent trophic effects of the combined scaffold and chemokine on neo-vascularization during pulp regeneration^[91]. In addition, DSCs seeded into peptide hydrogel loaded with FGF-1, TGF-β1, and VEGF differentiated into odontoblasts-like cells and formed a vascularized dental pulp-like tissue inside the dentin cylinder^[118]. Moreover, TGF-β2 increased the odontogenic differentiation of DSCs isolated from the apical papilla^[119]. DSCs isolated from adult human tooth pulp and seeded on the surfaces of 3D collagen gel cylinders exhibited significantly increased cellular recruitment when applied with SDF-1α, bFGF, or BMP-7^[120]. Encapsulating TGF-β1 and FGF-2 in a biodegradable polymer of lactide and glycolide microspheres provides the controlled release of growth factors to human pulp cells^[121]. Furthermore, scaffold composition plays a key role in determining whether the application of signaling molecules or growth factors is needed. Various growth factors, such as SDF, FGF, TGF-β1, VEGF, and BMP were loaded on different scaffolds, such as peptide hydrogel, collagen, gelatin hydrogel, and alginate hydrogel, to enhance endodontic regeneration of DSCs^[122]. In addition, a silk fibroin scaffold loaded with bFGF has been described as a promising scaffold for the proliferation and differentiation of DSCs *in vitro*^[123]. Implantation of DSCs with poly-ε-caprolactone and hydroxyapatite in association with SDF-1 and BMP-7 generated tooth-like structures (putative periodontal ligament and new bone formation) in the mandibular incisor extraction socket^[124]. In addition to SDF-1, stem cell factor (SCF), a potent chemokine, enhances the mobilization and trafficking of stem cells^[125]. SCF promoted neovascularization and new collagen fiber formation after subcutaneous implantation of DSCs with a collagen sponge scaffold in mice. Furthermore, SCF improved DSCs migration, proliferation, and chemotaxis *in vitro*, possibly *via* the upregulation of ERK and AKT phosphorylation^[126].

Sialoprotein is a dominant non-collagenous protein in dentin, which plays a role in the induction of dental pulp cell differentiation into odontoblast-like cells and is essential for dental pulp stem cell identity and fate^[127,128]. Subcutaneous implantation of DSCs seeded on a 3D scaffold containing an acellular ECM embedded in a collagen/chitosan scaffold led to the production of dental pulp-like tissue and the expression of dentin sialoprotein in nude mice^[129]. The application of DCSs combined with treated dentin matrix, a biological scaffold, has been suggested as a suitable therapeutic approach for the reconstruction of the tooth root^[130]. Immortalized DSCs exhibited potent odontogenic differentiation ability and secreted dentin sialophosphoprotein when seeded in a beta-tricalcium phosphate scaffold and BMP-2 in nude mice^[131]. Among three different scaffolds (DL-lactide, co-polymer of L-lactide and DL-lactide, and hydroxyapatite tricalcium phosphate), a copolymer of L-lactide and DL-lactide showed the highest odontogenic regenerative capacity after the addition of DSCs and BMP-2^[132].

A few studies have indicated that using a co-culture of DSCs with other stem cells improves neovascularization. The co-culture of DSCs and human umbilical vein endothelial cells with gelatin methacrylate xenogeneic hydrogel resulted in the neovascularization of mouse dental pulp^[133]. Transplantation of DSCs and human umbilical vein endothelial cells with VEGF seeded into PuraMatrix significantly enhanced vascularization and mineralization of mouse vascularized pulp-like tissue and osteodentin^[134]. In addition, using silk fibroin scaffolds promoted the ability of human DSCs in attracting vessels, which leads to the improvement of healing and regeneration of damaged tissues^[135]. Transplantation of DSCs with a tooth fragment/silk fibroin scaffold loaded with SDF-1 resulted in the generation of pulp-like tissues with vascularity, organized fibrous matrix formation, and dentin formation in nude mice^[136].

BONE RECONSTRUCTION

An enormous number of studies have been carried out to investigate the role of various scaffolds on the bone regeneration capacity of DSCs^[137]. The osteogenic differentiation ability of DSCs, mostly isolated from dental pulp or periodontal ligament, has been well demonstrated in both *in vivo* and *in vitro* studies^[138]. DSCs originating from dental pulp, dental follicle, gingival tissue, and periodontal ligament exert different osteogenic capacity^[139], which can be modulated by various types of biomaterial scaffolds^[140]. For instance, an *in vivo* investigation has shown that DSCs from the periodontal ligament encapsulated in an arginine-glycine-aspartic acid tripeptide scaffold exhibit a greater ability to repair bone defects by promoting the formation of mineralized tissue compared to gingival MSCs^[141]. In addition, DSCs derived from the dental pulp exhibit great neovascularization potential while differentiating into osteoblasts, which subsequently promote bone restoration^[142].

The most common scaffolds used to seed DSCs (particularly isolated from human dental pulp or exfoliated deciduous teeth) for bone tissue engineering in both experimental studies and clinical trials are collagen sponge membrane and hydroxyapatite/tri-calcium phosphate granules ceramic^[143]. DSCs seeded in collagen sponge scaffolds exhibit strong restoration ability in human mandible bone defects^[144]. The application of DSCs seeded onto a collagen-polyvinylpyrrolidone sponge scaffold in the left lower premolar region of a patient with periodontal disease increased bone density and decreased tooth mobility, periodontal pocket depth, and the bone defect area^[145]. Using DSCs with a hydroxyapatite-collagen sponge scaffold to fill the alveolar defect in 6 patients with cleft lip and palate resulted in satisfactory bone regeneration^[146]. A three-year clinical study revealed that the bone tissue regenerated following the application of human DSCs seeded on collagen scaffolds was uniformly vascularized and compact^[147]. However, this study revealed that the new bone developed at the implantation sites was compact and different from the normal spongy alveolar bone in the mandibles^[147]. In contrast, no ectopic bone formation was observed when DSCs were seeded on hydroxyapatite-tri-calcium phosphate scaffolds^[148]. Furthermore, it should be noted that for any successful cell transplantation approach, the optimal number of DSCs is essential. It has been demonstrated that dense culture conditions improve the mineralized nodule formation of DSCs and promote osteogenic-lineage commitment, possibly *via* the integrin signaling pathway^[149]. DSCs seeded in dense collagen gel scaffolds exert a higher beneficial effect on the craniofacial bone healing process compared to acellular scaffolds^[150].

DSCs isolated from the dental follicle and the periapical papilla have been considered for the regeneration of alveolar bone and were successfully assessed in a few preclinical pilot studies. The application of dissociative dental pulp with a collagen sponge scaffold in patients with deep intrabony defects due to chronic periodontitis led to the effective restoration of defects with significant stability of the gingival margin^[151]. In addition, the application of DSCs seeded onto collagen sponge in the deep intrabony defects of 29 patients suffering from chronic periodontitis significantly improved clinical outcomes of the periodontal regeneration process^[152]. Another clinical trial has shown that using DSCs in combination with the collagen sponge scaffold in 6 patients resulted in a well-differentiated bone with Haversian system formation in the tooth extraction site^[153].

Scaffold composition and surface properties play a key role in the osteogenic differentiation of DSCs and the process of bone tissue regeneration^[142,154]. Significantly greater mineralization occurred when DSCs were seeded into a collagen type I matrix^[155]. Furthermore, DSCs seeded on hyaluronic acid, fibrin, and polyesteramide type-C exhibit higher mineralization compared to standard tissue culture polystyrene^[156].

Ceramic scaffolds, such as tri-calcium phosphate, hydroxyapatite, bioactive glass biphasic calcium phosphate, and calcium silicate, have chemical and structural similarities to the native bone and are commonly used as scaffolds to enhance bone regeneration and restoration of DSCs^[157]. The addition of tricalcium phosphate to the composition of the other scaffolds enhances the differentiation of DSCs into osteoblast-like cells^[158]. Chitosan/gelatin scaffolds significantly increased DSCs viability and differentiation as well as the formation of hydroxyapatite-rich nanocrystalline calcium phosphate in immunocompromised mice, particularly when cells were pre-treated with recombinant human BMP-2^[92]. Potent bone formation was observed in the defect area of rat femoral bone after application of DSCs seeded in bioactive glass nanoparticles/chitosan-gelatin bionanocomposite compared to mesoporous bioactive glass nanospheres^[159]. A combination of poly- ϵ -caprolactone biphasic calcium phosphate with DSCs increased the newly formed bone regeneration of calvarial defects in rabbit models^[160]. Furthermore, a combination of poly-lactic-co-glycolic acid with ceramics is usually used to enhance biomimetic potential and promote bone regeneration^[161]. An *in vitro* study has revealed that human dental pulp SCs adhesion and proliferation, as well as their differentiation toward the osteogenic lineage, are significantly improved when seeded in hydroxyapatite (a member of the calcium phosphate-based bioceramics) and poly-lactide-co-glycolide^[162]. Implantation of human DSCs seeded in beta-tri-calcium phosphate scaffolds exerted an anti-inflammatory effect and restored periodontal hard tissue defects^[163]. Greater bone regeneration was also reported when human DSCs were seeded on poly-lactic-co-glycolic acid^[164] and α -calcium sulfate hemihydrate/amorphous calcium phosphate^[165] scaffolds. Calcium phosphate cement functionalized with iron oxide nanoparticles also exhibits a potent effect on the spreading, osteogenic differentiation, and bone mineral synthesis of DSCs, possibly *via* activation of the extracellular signal-related kinases WNT/ β -catenin pathway^[166].

Different forms of silicon, particularly the orthosilicic acid form, promote osteoblast proliferation and differentiation, the mineralization process, and collagen production through enhancement of the precipitation of apatite from calcium and phosphate-containing solutions^[167]. Semicarbazide-treated porous silicon exerted an appropriate scaffold for DSCs adhesion and *in vivo* cell therapy, whereas silanization with aminopropyltriethoxysilane-treated porous silicon has been suggested as a favorable scaffold for a long-term *in vitro* culture system for DSCs proliferation and differentiation^[168]. Intrafibrillar-silicified collagen scaffolds markedly improved the proliferation, osteogenic differentiation, and mineralization capacity of human DSCs compared to non-silicified collagen scaffolds^[169]. A novel biocompatible nano-engineered osteoinductive and elastomeric scaffold fabricated from a porous nanocomposite of poly-glycerol sebacate and nanosilicates enhanced the physical integrity and mechanical strength of the cellular microenvironment for *in vitro* osteogenic differentiation and bone regeneration without persistent scaffold-related inflammation *in vivo*^[170].

Hybrid composites are also used as promising biomaterials for bone regeneration. It has been suggested that four different scaffold materials, including porous hydroxyapatite alone or combined with three polymers polylactic-co-glycolic acid, alginate, and ethylene vinylacetate/ethylene vinylversatate, are suitable for DSCs osteogenic differentiation^[171]. Electrospun nano-ECM nanofibers with fluorapatite scaffolds enhance the growth, differentiation, and mineralization of DSCs^[172], possibly mediated *via* modulation of the FGF and VEGF signaling pathways^[173]. Comparing the

behavior of DSCs seeded on a 2D monolayer culture or 3D poly lactic-co-glycolic scaffold, it has been shown that DSCs exerted proper adherence and enhanced osteogenic differentiation on the 3D scaffold cultures^[174]. Furthermore, it has been suggested that DSCs seeded in hydrogel scaffolds have greater potential for odontogenic differentiation than cells embedded in collagen-I hydrogel scaffolds^[175]. Various layer-by-layer-modified gelatin sponge scaffolds increased the adhesion and proliferation of DSCs and enhanced their potential for bone tissue regeneration^[176].

Several differentiation factors, such as BMP, were used to potentiate DSCs bone formation capacity. A 3D gel-based heparin-conjugated collagen matrix combined with recombinant human BMP-2 improved DSCs differentiation and seeding efficiency *in vitro* and promoted the osteogenic differentiation of these stem cells to form ectopic bone formation in a rat model^[177]. Exfoliated human DSCs significantly increased the expression of BMP-2 and 7, bone and cartilage formation markers, when seeded in carbonate apatite scaffold in an *in vivo* alveolar bone remodeling model in rats^[178]. DSCs isolated from human gingival tissues seeded onto 3D poly-lactide scaffolds enriched with extracellular vesicles, small membrane vesicles containing various bioactive molecules, exhibited potent osteogenic inductivity *in vitro* and showed a marked improvement in bone healing of rat calvaria bone tissue *in vivo*^[179]. On the other hand, some biomaterial scaffolds may facilitate biomolecule-induced tissue formation. For instance, 3D matrigel scaffold enriched with DSCs led to enhanced BMP-9-induced osteogenesis and mineralization in ectopic bones in nude mice^[180].

Although the majority of studies rely on the application of DSCs alone, several studies have employed co-culture systems (DSCs in combination with other cells) intending to promote bone regeneration, particularly in 3D scaffolds^[181]. Human DSCs and amniotic fluid stem cells seeded onto fibroin scaffolds resulted in pronounced bone repair associated with neovascularization in critical-size rat cranial bone defects^[182]. The co-cultured constructs of DSCs and endothelial cells seeded in 3D polycaprolactone blended with poly-L/D-lactide revealed a significantly higher up-regulation of genes related to osteogenesis and angiogenesis^[183].

NEUROLOGICAL DISORDERS

DSCs derived from dental pulp and oral mucosa display high expression of various neural crest-related and developmental genes^[184]. DSCs can be differentiated into the neuron-, Schwann-, glia-, and oligodendrocyte-like cells^[185]. Due to the high proliferative capacity and propensity to differentiate into neural stem cells, DSCs are attractive candidates for developing a human neuronal lineage for the treatment of various disorders^[186]. The role of DSCs in cell transplantation therapy of traumatic and hypoxic-ischemic injuries of the central or peripheral nervous system as well as neurodegenerative diseases has been extensively investigated^[187]. DSCs are promising sources for cellular transplantation-based therapeutic strategies for neurological disorders^[188]. The seeding of DSCs into different scaffolds promotes cell viability and differentiation towards neuronal-like cells^[189,190]. Scaffolds can be designed to provide biological growth factors for neuronal tissues and to accurately adjust the diffusion rate of these essential biomolecules and enzymes^[187].

The application of combined DSCs with various scaffolds promotes the function of injured neural tissues and reduces the inflammatory responses. The most common scaffolds applied for neural tissue regeneration and repair include chitosan, heparin-polyoxamer, silicone tubes, poly-ε-caprolactone/poly-lactide-co-glycolic acid, and electrospun neuro-supportive scaffolds^[191]. Different scaffolds were used to enhance neural differentiation and promote their neuronal characteristics. DSCs can be seeded in the biodegradable electrospun neuro-supportive scaffold, which is amended by different 3D coatings, for enhanced *in vitro* and *in vivo* recovery of neuronal damage^[192]. The granular 3D chitosan scaffolds provide an appropriate microenvironment for attachment, proliferation, and neural differentiation of DSCs^[193]. Furthermore, a 3D floating sphere culture system has been shown to provide a suitable micromilieu for human DSCs to retain their neuronal characteristics compared to myogenic and osteogenic properties^[194]. Using an acellular ECM scaffold has been shown to promote DSCs to obtain a neuronal-like organization, including a central body associated with long cytoplasmic extensions that follow the underlying fibers, with high cell-matrix adhesion properties^[195]. Some scaffolds can support the neurotrophic release of DSCs for the subsequent survival and differentiation of neural stem cells as well as neural cells. For instance, DSCs promoted the survival and

differentiation of adult murine neural stem cells on ethyl acrylate and hydroxyethyl acrylate copolymer scaffold through the enhancement of neurotrophic factor secretion^[196].

Transplantation of DSCs with a chitosan scaffold markedly enhanced the recovery of motor function and suppressed inflammatory responses, possibly *via* the secretion of neurotrophic factors, such as glial cell-derived neurotrophic factor and brain-derived neurotrophic factor, in experimental models of spinal cord injury. Furthermore, the combination of DSCs with scaffolds inhibited cell injury and death through the reduction of caspase activity^[197]. A significant functional recovery of hind-limb locomotor activities has also been observed following the transplantation of DSCs seeded in chitosan scaffolds in a spinal cord injury animal model^[198]. Solubilized forms of acellular ECM from dentine, bone, and spinal cord have discrete structural, mechanical, and functional properties. Human DSCs exhibited a strong positive response to spinal cord ECM hydrogels by the greater expression of neural lineage markers. This ECM scaffold markedly enhanced the differentiation of DSCs to a neural lineage; indicating the importance of site-specific tissues in the promotion of stem cell behavior for constructive spinal cord regeneration^[24]. A combination of DSCs with heparin-polyoxamer, a desirable thermosensitive hydrogel for *in vivo* applications, loaded with various growth factors, such as bFGF and nerve growth factor (NGF), markedly promoted functional recovery, cellular regeneration, and tissue repair in a rat model of spinal cord injury^[187], possibly *via* modulation of the MAPK/ERK, PI3K/Akt and JAK/STAT3 signaling pathways^[199]. Indeed, both bFGF and NGF play an essential role in the neural differentiation of DSCs^[200]. Chitosan scaffolds in combination with bFGF exerted a synergistic facilitating effect on DSCs differentiation to neural cells, possibly *via* activation of the ERK signaling pathway^[201]. It has been shown that DSCs can proliferate efficiently on an aligned electrospun poly ϵ -caprolactone/poly lactide-co-glycolic acid scaffold and restore defects in rat spinal cord. Furthermore, these cells contribute to remyelination by the expression of oligodendrogenic lineage markers^[202].

Multiple studies have assessed the effects of DSCs with various scaffolds on various experimental models of peripheral nerve injury. DSCs seeded into a polylactic-glycolic acid scaffold significantly improved the regeneration of injured facial nerve and promoted functional recovery compared to autografts^[203]. Schwann-like cells derived from DSCs and grown in collagen scaffolds facilitated axonal outgrowth and myelination in both 2D and 3D *in vitro* models of peripheral nerve injury^[204,205]. Furthermore, oligodendrocyte progenitor cells induced by differentiation of human DSCs *via* gene transfection in combination with collagen or collagen and fibrin scaffolds improved axonal outgrowth and myelination in an animal sciatic nerve injury model^[9,206]. Human DSCs isolated from the periodontal ligament and gingival tissues and encapsulated in 3D alginate/hyaluronic acid scaffolds in the presence of NGF improved the proliferation and differentiation of DSCs toward the formation of neural tissues^[207]. DSCs seeded on poly-lactic-co-glycolic acid collagen enhanced the interconnections of injured axons in a model of facial nerve injury^[203]. When cultured under either 2D- or 3D-collagen scaffolds, human DSCs originating from gingival tissue have shown a greater capability of differentiating into neurons and Schwann-like cells in a 3D collagen scaffold compared to the 2D culture system. Furthermore, these cells with a 3D scaffold improved regeneration and functional recovery of neural tissues in rat facial nerve defects^[208]. It has been shown that collagen scaffolds in the presence of different growth factors, such as bFGF, exhibited favorable mechanical properties and improved facial nerve regeneration^[209]. Human DSCs expressing STRO-1, c-Kit, and CD34 markers and seeded in a collagen scaffold engrafted into rat sciatic nerve defects improved axonal regeneration from proximal to distal stumps^[210]. Interestingly, the administration of serum-free conditioned medium from DSCs plunged in a collagen sponge into the gap caused by rat facial nerve transection, induced axonal regrowth and restored the neurological deficits^[211].

THE IMPACT OF DIFFERENT SCAFFOLDS USED IN DSCS CELL THERAPY

Using an appropriate scaffold can promote the proliferation, differentiation, migration, and functional capacity of DSCs and can optimize and preserve the cellular morphology to build tissue constructs for a specific purpose^[63]. Although the application of DSCs alone could yield promising outcomes in cell replacement therapy in particular conditions^[212], an appropriate scaffold provides a viable

microenvironment to boost the development of DSCs towards new tissue formation, especially in tissues or organs with extensive defects^[213]. The optimal number of DSCs is essential to develop tissue and organ substitutes and to restore organ function^[149]. In addition to establishing definitive protocols for DSCs preparation, appropriate carrier scaffolds play a crucial role to increase the number of cells for implantation (Figure 3)^[214].

A crucial and challenging demand for an appropriate scaffold design is recapitulating the dynamic nature of the native tissue^[215]. Although each polymer scaffold has its pros and cons and favorable tissue engineering applications, collagen and fibrin, alone or by forming hybrid scaffolds, provide an adequate pulp connective tissue formation associated with marked vascularization, particularly when loaded with active biomolecules^[117,118,216]. Collagen is the main component of the ECM and is expressed widely in bone, teeth, and the brain. A collagen scaffold provides excellent biocompatibility and controllable biodegradability, particularly for bone tissue engineering^[217,218]. However, collagen has poor mechanical, chemical, and thermal stability and degrades fast at an uncontrolled rate. Fibrin is a non-toxic biomaterial scaffold that can attach various biological surfaces to regenerate tissues, such as bone and nervous tissues, with a low inflammatory response^[219]. However, low mechanical stiffness of fibrin scaffolds limits tissue diffusion and direct implantation of cells to the damaged tissues^[220,221]. Different bioceramic scaffolds exhibit excellent biocompatibility and osteoconductivity due to their chemical and structural similarity to native bone, which is characterized by high mechanical stiffness and low elasticity^[158,222]. Furthermore, bioceramic scaffolds improve stem cell differentiation and osteogenesis^[222]. The main disadvantages of bioceramic scaffolds are brittleness and slow biodegradation in the crystalline phase^[218]. Soft polymers with highly aqueous hydrogels, such as collagen, share a resemblance to neural tissues, play an important role as a possible internal filler for neural conduits and increase the quality of peripheral nerve regeneration^[223].

Furthermore, the scaffold should be porous and spongy to be able to deliver sufficient DSCs to injured tissues and to allow the stream of ECM and the formation of neovascularization^[165,166]. However, some of the currently available biomaterials do not fully imitate the essential functions of natural ECM and fail to provide an appropriate scaffold^[224]. Among the different biomaterials, the self-assembly of monodisperse cells into 2D or 3D complex structures that produce more extracellular matrix and promote intercellular communication possess the characteristics of the ideal approach^[225]. Although both 2D and 3D cell culture systems provide appropriate methods for stem cell replacement transplantation, 3D systems seem to be more effective at mimicking the ECM in native tissues^[226,227]. In general, 3D culture systems have been shown to be more beneficial in providing a template for the reconstruction of defects and cell-to-cell interactions as well as for improving cell adhesion, proliferation, ECM generation, maintenance of cell polarity, and restoration of various tissues^[228,229]. In addition, 3D scaffolds enhance the sensitivity of stem cells towards drugs and biomolecules^[230]. The optimization of 3D scaffold pore sizes may lead to better tissue regeneration through the enhancement of mechanical strength^[231]. The dimension of the defect is a key factor in selecting a scaffold for tissue or organ regeneration^[232]. For instance, in the reconstruction of cleft lip and palate, the amount of bone formation may not be enough to fill the bone defect^[233], a problem that may be solved by the application of 3D cell culture systems^[234]. In this regard, higher osteogenic differentiation of DSCs and MSCs has been observed in 3D than in 2D cell culture^[174,235].

In addition to an appropriate scaffold, using bioactive molecules, such as growth and angiogenic factors, has been suggested as a promising strategy for the improvement of DSCs transplantation. Bioactive molecules, such as VEGF, have a short half-life and need to be encapsulated in degradable materials to regulate their release and promote their effects^[236]. Scaffolds provide a purposeful approach for better incorporation between stem cells and biomolecules to improve tissue regeneration^[26]. The interpolation of active biomolecules with the scaffold is essential for their transport into the injured tissues and for their efficacy to promote the colonization of DSCs and their matrix deposition^[123]. DSCs and various scaffolds transplanted together with bioactive molecules, such as G-CSF, BMP, and bFGF, can fill the entire pulp or bone defect as well as develop new dentin or bone formation^[92,93,118]. Biomolecules, such as SDF-1, SCF, and G-CSF, help to summon DSCs and enhance the number of cells in the implantation site, and other factors, such as VEGF, can enhance the formation of new blood vessels in regenerative tissues^[26,237].

On the contrary, a few investigations have suggested that transplantation of DSCs without scaffold may have more beneficial effects on tissue regeneration. To prevent the inflammatory response, immune rejection, or infections, a few studies have

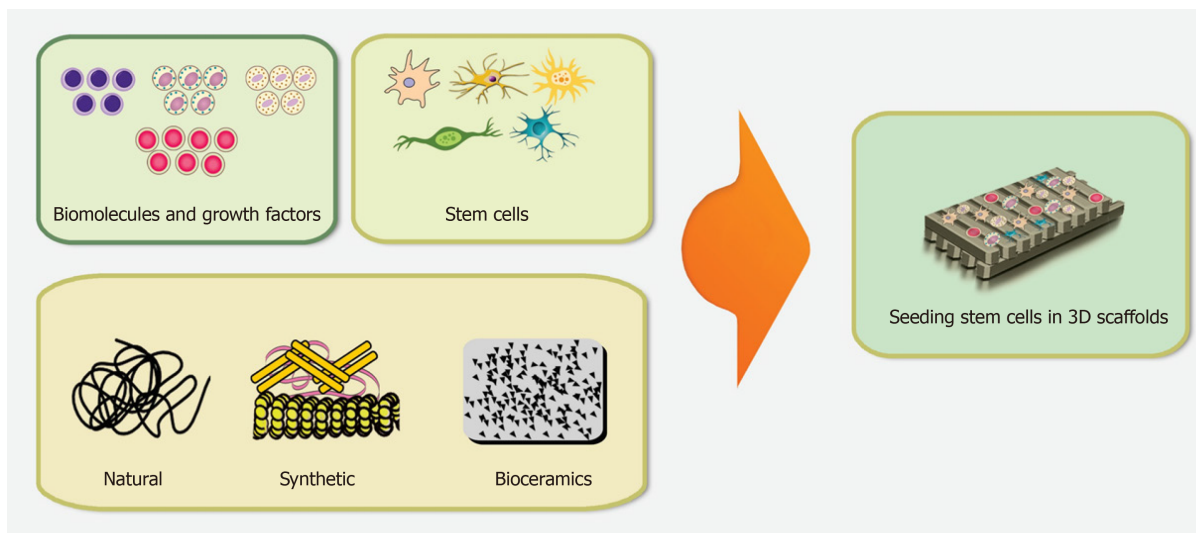


Figure 3 Schematic overview of the optimal biomimetic environment for application in tissue engineering. Stem cells require appropriate scaffold materials as well as biomolecules and growth factors to achieve optimal therapeutic effects.

indicated that transplantation of stem cells without scaffolds (such as 3D stem cell spheroids) may be an alternative option for DSCs transplantation^[238]. Transplantation of DSCs without a scaffold for injured tooth tissues in 26 patients led to the regeneration of 3D pulp tissue which contained blood vessels and sensory nerves 12 months after therapy^[239]. Despite these studies, it seems that the simple injection of competent DSCs inside organ defects is poorly regenerative^[123].

A few decades of intense basic studies and clinical trials on DSCs are essential to translate knowledge gained on these cells into the implementation of defined and reproducible therapeutic approaches to cure or alleviate diseases. In addition to the application of an ideal scaffold, the success of cell transplantation therapy using DSCs also relied greatly on designing methodologies for isolation and purification, a sufficient number of stem cells, and effective and safe differentiation into different lineages^[240,241]. The development of an accurate immunomodulatory strategy for injectable and implantable biomaterials is of particular importance to facilitate the grafting of DSCs at inflamed sites^[242,243].

CONCLUSION

This study describes the main scaffolds, both natural and synthetic, used in DSCs transplantation and evaluated the advantages and disadvantages of various types of scaffolds. Most of the existing studies concerning the development of novel therapeutic approaches for restoration of damaged tissues have been limited to *in vitro* and *in vivo* DSCs testing, with a small number of clinical trials. Although the co-application of biomolecules with an appropriate scaffold seems to be crucial for effective cell transplantation therapy with DSCs, there is still much to learn about the dynamics of these molecules as well as their interactions with the ECM and DSCs to allow planning of appropriate therapeutic approaches. Further advances in tissue engineering need to focus on innovative combinations of biopolymers and biomolecules to promote the capability of DSCs for novel and effective therapeutic approaches (Figure 3).

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Inflammatory niche: Mesenchymal stromal cell priming by soluble mediators

Aleksandra Jauković, Tamara Kukolj, Hristina Obradović, Ivana Okić-Đorđević, Slavko Mojsilović, Diana Bugarski

ORCID number: Aleksandra Jauković 0000-0003-2686-7481; Tamara Kukolj 0000-0002-3174-4358; Hristina Obradović 0000-0003-4626-7184; Ivana Okić-Đorđević 0000-0003-3552-1546; Slavko Mojsilović 0000-0002-4399-6720; Diana Bugarski 0000-0002-2629-5471.

Author contributions: Jauković A conceived of, designed, and wrote the manuscript; Kukolj T contributed to the article's conception and writing; Obradović H performed the literature review and writing; Okić-Đorđević I contributed to the literature review and article writing; Mojsilović S performed the literature analysis and article editing; Bugarski D made critical revisions to the manuscript; all authors read and approved the final version of the manuscript.

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Aleksandra Jauković, Tamara Kukolj, Hristina Obradović, Ivana Okić-Đorđević, Slavko Mojsilović, Diana Bugarski, Laboratory for Experimental Hematology and Stem Cells, Institute for Medical Research, University of Belgrade, Belgrade 11129, Serbia

Corresponding author: Aleksandra Jauković, PhD, Associate Professor, Laboratory for Experimental Hematology and Stem Cells, Institute for Medical Research, University of Belgrade, Dr. Subotića 4, PO BOX 102, Belgrade 11129, Serbia. aleksandra@imi.bg.ac.rs

Abstract

Mesenchymal stromal/stem cells (MSCs) are adult stem cells of stromal origin that possess self-renewal capacity and the ability to differentiate into multiple mesodermal cell lineages. They play a critical role in tissue homeostasis and wound healing, as well as in regulating the inflammatory microenvironment through interactions with immune cells. Hence, MSCs have garnered great attention as promising candidates for tissue regeneration and cell therapy. Because the inflammatory niche plays a key role in triggering the reparative and immunomodulatory functions of MSCs, priming of MSCs with bioactive molecules has been proposed as a way to foster the therapeutic potential of these cells. In this paper, we review how soluble mediators of the inflammatory niche (cytokines and alarmins) influence the regenerative and immunomodulatory capacity of MSCs, highlighting the major advantages and concerns regarding the therapeutic potential of these inflammatory primed MSCs. The data summarized in this review may provide a significant starting point for future research on priming MSCs and establishing standardized methods for the application of preconditioned MSCs in cell therapy.

Key Words: Mesenchymal stem cells; Pro-inflammatory cytokines; Alarmins; Priming; Boosting the therapeutic potential

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Core Tip: The inflammatory niche plays a key role in triggering the reparative and immunomodulatory functions of mesenchymal stromal/stem cells (MSCs). This paper summarizes the data on how soluble factors in the inflammatory microenvironment, including pro-inflammatory cytokines secreted by immune cells and alarmins released by

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damaged cells, affect MSCs' ability to regenerate tissue and modulate the inflammatory response. We also analyze data from *in vitro* and *in vivo* studies, which highlight the influence of these factors on the therapeutic potential of MSCs, thus providing an important background for the development of preconditioning strategies that might improve the outcomes of MSC-based cell therapies.

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INTRODUCTION

Inflammation is a localized immunologic response of the tissue elicited by harmful stimuli, including pathogens, irritants, or physical injury. This complex and protective response plays a fundamental role in the regulation of tissue repair, serving to eliminate harmful stimuli and begin the healing process^[1]. In fact, inflammation is considered an important initial phase, followed by cell proliferation and extracellular matrix remodeling. These phases overlap over time and each of them represents a sequence of dynamic cellular and biochemical events, contributing to tissue regeneration through the collaboration of many cell types and their soluble products^[2]. Immune cells, together with blood vessels, various stromal cells, extracellular matrix components, and a plethora of secreted soluble mediators, comprise an inflammatory microenvironment capable of inducing different responses of cells within injured tissue^[3].

Soluble mediators released from injured/necrotic cells or damaged microvasculature lead to enhanced endothelium permeability and infiltration of neutrophils and macrophages. Among these mediators are endogenous danger signals, known as alarmins, which are rapidly released by dying necrotic cells upon tissue damage and play an important role in promoting and enhancing the immune response^[4-6]. To date, the best-characterized alarmins are the interleukin (IL)-1 family of cytokines (IL-1 α and IL-33), high-mobility group protein B1 (HMGB1), S100 proteins, and heat shock proteins (Hsps)^[4,7]. In addition, during the inflammatory process, the phagocytosis of necrotic cells by resident/recruited neutrophils and macrophages induces the release of various inflammatory factors, such as tumor necrosis factor (TNF)- α , interferon (IFN)- γ , IL-1 β , IL-17, and chemokines^[8].

Aside from numerous soluble mediators, tissue injury mediated by immunity or infection involves an even greater number of various immune cells, including B cells, CD4⁺ and CD8⁺ T cells, and natural killer cells. While all immune cells play key roles in wound healing through the eradication of damaged tissue and invading pathogens, their excessive activation can actually aggravate the injury. Therefore, a comprehensive understanding of inflammatory niche elements might contribute to the development of novel therapeutic strategies for the treatment of inflammatory-associated diseases, as well as conditions of failed tissue regeneration.

One of the cellular compartments participating in the inflammatory niche represents mesenchymal stromal/stem cells (MSCs). MSCs are stem cells of stromal origin that possess self-renewal capacity and the ability to differentiate into three mesodermal cell lineages, including osteocytes, chondrocytes, and adipocytes^[9]. Considering their critical role in tissue homeostasis and wound healing, MSCs have garnered great attention as promising candidates for tissue regeneration. Although first isolated from the bone marrow (BM)^[10], MSCs may be obtained from various fetal and adult tissues, such as the umbilical cord (UC), peripheral blood, adipose tissue (AT), and skin and dental tissues^[11,12]. According to the minimum criteria proposed by the International Society for Cellular Therapy, MSCs originating from different tissues are evidenced by the property of plastic adherence *in vitro* and expression of various non-specific surface molecules, such as cluster of differentiation (CD)105, CD90, CD73, and CD29, in parallel with trilineage differentiation potential^[13]. However, the term MSC has recently been considered inappropriate, as it has become clear that MSCs from different tissues are not the same, especially with respect to their differentiation capacities^[14,15], whereas their multipotent differentiation potential has not been

confirmed in *in vivo* conditions. Therefore, Caplan^[17] recently proposed this term to stand for medicinal signaling cells^[16], indicating the correlation of the therapeutic benefits of MSCs with the secretion of various bioactive molecules.

Many studies have demonstrated that MSCs contribute to tissue repair by accumulating at sites of tissue damage and inflammation, where together with resident MSCs, they exert reparative effects in two ways. One way is to replace damaged cells through differentiation, and another is related to the ability of MSCs to strongly influence the microenvironment by releasing bioactive factors and interacting with multiple cell types^[18,19]. Indeed, poorly immunogenic MSCs that weakly express major histocompatibility complex (MHC) class I and lack MHC class II play a critical role in regulating the inflammatory microenvironment through interactions with immune cells such as T cells, B cells, natural killer cells, and dendritic cells^[20-22]. As a result of these interactions, MSCs suppress lymphocyte proliferation and maturation of monocytes into dendritic cells, while stimulating the generation of regulatory T cells (Tregs) and M2 macrophages^[23,24].

The major role in the crosstalk between MSCs and immune cells has been ascribed to soluble factors, which upon release by activated immune cells, significantly affect MSCs paracrine activity, conversely influencing immune cells. In particular, the immunosuppressive activity of MSCs has been related to the production of indoleamine-2,3-dioxygenase (IDO), nitric oxide (NO), prostaglandin-E2 (PGE2), IL-10, transforming growth factor (TGF)- β , and TNF α -stimulated gene-6^[25].

Inflammatory priming of MSCs

It is believed that the inflammatory niche plays a key role in triggering the reparative function of MSCs. Namely, studies have demonstrated that the immunosuppressive potential of MSCs is not inherently expressed but requires priming by inflammatory factors, including IFN- γ , TNF- α , or IL-1 β ^[18,26]. Moreover, it has been found that MSCs can polarize into MSC type 1 with a pro-inflammatory profile or MSC type 2 with an immunosuppressive phenotype, depending on the inflammatory condition^[23,27]. On the other hand, the inflammatory microenvironment influences the differentiation potential of resident and recruited MSCs, significantly impairing their regenerative capacity. In addition, several studies have shown that MSCs of different tissue origin may exert differential sensitivity to inflammatory conditions^[28,29]. These data point to the critical importance of interactions between MSCs and inflammatory factors for the outcome of wound healing.

Indeed, the regenerative potential of transplanted MSCs is affected by inflammatory conditions^[30], indicating the strong influence of the recipient's inflammatory status on the efficacy of MSC-based therapies. Interestingly, to reduce the heterogeneity of MSCs and generate more homogenous therapeutic products, MSC priming with cytokines has been proposed^[31]. The application of bioactive molecules in this context has been considered a supplemental molecular signal used to foster the therapeutic potential of MSCs and contribute to establishing a favorable microenvironment for tissue repair.

The complex cytokine network has been considered a critical part of the inflammatory microenvironment, where the pleiotropic properties of pro-inflammatory cytokines play a decisive role in the healing process and tissue regeneration. TNF- α , IFN- γ , IL-1, IL-17, and IL-6 are the most common inflammatory cytokines in this complex network^[32]. Moreover, another significant constituent of the inflammatory niche considers alarmins, such as IL-1 α and IL-33, HMGB1, S100 proteins, and Hsps, which can promote the immune response, thereby supporting host defense and tissue repair^[7]. Here, we review how these soluble mediators of the inflammatory niche influence the regenerative and immunomodulatory potential of MSCs, highlighting the major advantages and concerns regarding the therapeutic potential of inflammatory primed MSCs.

MSCs priming with pro-inflammatory cytokines

IFN- γ priming: One of the most studied inflammatory priming mediators is IFN- γ , which is a key player in cellular immunity regulation, heightening immune responses in infection and cancer. However, very little is known about the effects of IFN- γ on the regenerative potential of MSCs. Namely, Croitoru-Lamoury *et al.*^[33] demonstrated that IFN- γ exerts significant antiproliferative effects on mouse and human BM-MSCs (Figure 1) through IDO induction and production of downstream tryptophan metabolites, such as kynurenine, which can potentiate the suppressive effects on cell proliferation in an autocrine manner. This was the first study that linked IFN- γ -induced IDO with the control of MSC differentiation potential, as evidenced by the inhibition of both osteogenic and adipogenic marker expression in IFN- γ -primed BM-

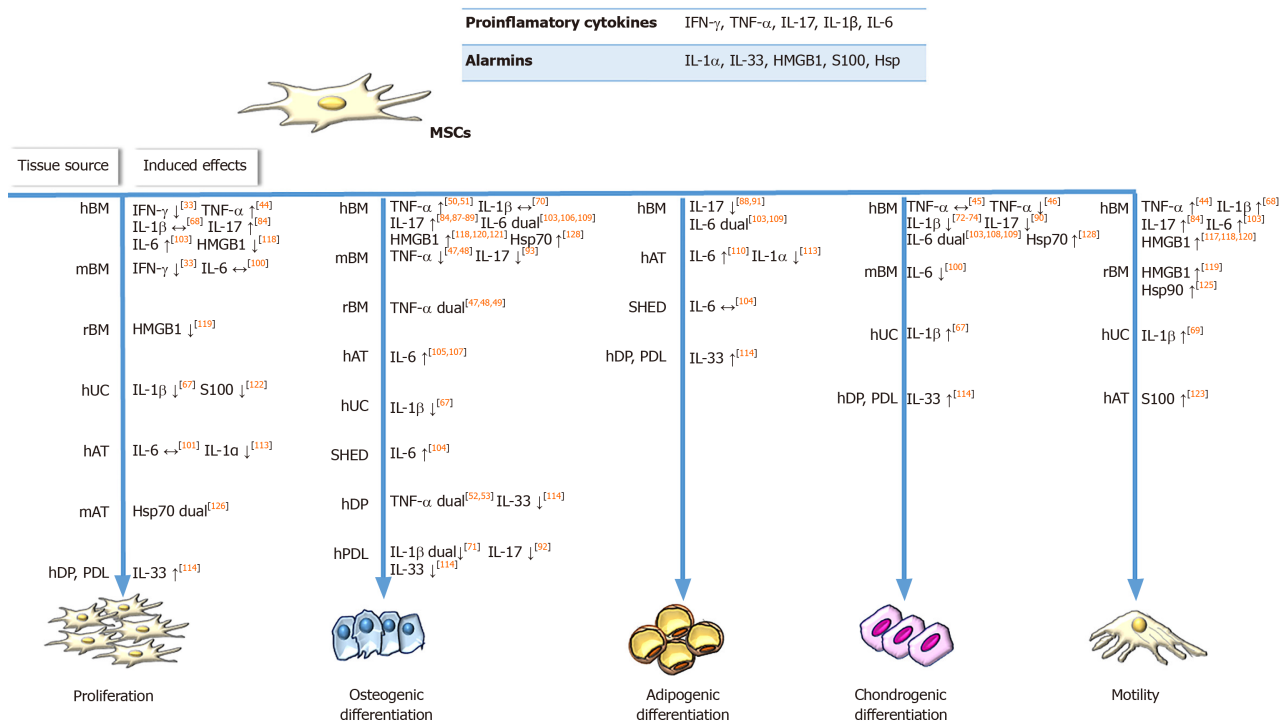


Figure 1 Influence of inflammatory priming on regenerative features of mesenchymal stromal/stem cells under *in vitro* conditions. Soluble factors in the inflammatory microenvironment, including pro-inflammatory cytokines secreted by immune cells and alarmins released by damaged cells, influence mesenchymal stromal/stem cells' (MSCs) ability to regenerate tissue by affecting their proliferation, migration and differentiation potential (osteogenic, chondrogenic, adipogenic). When applied *in vitro*, indicated inflammatory factors differently affect the regenerative properties of MSCs depending on the species or tissue origin of MSCs. Symbols: \uparrow and \downarrow represent stimulatory or inhibitory activity of priming factor, respectively; \leftrightarrow indicates no effects of priming factor. The term 'dual' indicates the data where priming factor dually affected MSCs function depending on applied concentration or MSCs donor age. The numbers in square brackets indicate the references. IFN- γ : Interferon gamma; TNF- α : Tumor Necrosis Factor alpha; IL: Interleukin; HMGB1: High mobility group box 1; Hsp: Heat shock proteins; MSCs: Mesenchymal stromal/stem cells; h: Human; WJ: Wharton jelly; BM: Bone marrow; r: Rat; UC: Umbilical cord; AT: Adipose tissue; DP: Dental pulp; PDL: Periodontal ligament; SHED: Exfoliated deciduous teeth.

MSCs upon induction of differentiation.

Numerous studies have demonstrated that the priming of MSCs with IFN- γ can enhance the immunosuppressive property of these cells by IDO stimulation^[34]. In addition, exposure to IFN- γ has been shown to induce UC Wharton's jelly (WJ)-MSCs to express other immunosuppressive factors, such as human leukocyte antigen G5, as well as C-X-C motif chemokine ligand (CXCL)9, CXCL10, and CXCL11^[35]. Even more, IFN- γ -primed WJ-MSCs secrete more IL-6 and IL-10 upon co-culture with activated lymphocytes, increasing the percentage of Tregs, while decreasing the frequency of T helper (Th)17 cells (Table 1).

Another mechanism underlying the inhibitory effects of IFN- γ -primed BM-MSCs on T-cell effector functions is the upregulation of programmed death-ligand 1 (referred to as PD-L1)^[36] (Table 1). However, in the context of potential MSCs' therapeutic use, the findings from several studies which have demonstrated that MSCs priming with IFN- γ led to upregulation of class I and class II human leukocyte antigen (referred to as HLA) molecules should be considered, as they indicated more immunogenic MSCs profile that is linked to a higher susceptibility to host immune cells recognition^[37,38]. Noteworthy, a recent study found that priming with IFN- γ did not increase HLA class II expression on senescent BM-MSCs but upregulated this molecule on early passage BM-MSCs, suggesting that IFN- γ priming effects can also be influenced by cell aging^[39].

Interestingly, *in vivo* experiments have demonstrated that IFN- γ affects the therapeutic efficacy of MSCs in a dose-dependent manner. Namely, when low concentrations of IFN- γ were used for murine BM-MSCs priming, the therapeutic effects of MSCs on experimental autoimmune encephalomyelitis in mice were completely inhibited, as demonstrated by the increased secretion of pro-inflammatory chemokine CCL2 and higher expression of MHC molecules class I and II^[38]. BM-MSCs primed with higher concentrations of IFN- γ prior to use in murine models of colitis reportedly increase MSC therapeutic efficacy, as demonstrated by the significantly attenuated development and/or reduced symptoms of colitis^[40]. These effects were

Table 1 Influence of inflammatory priming on immunomodulatory features of mesenchymal stromal/stem cells under *in vitro* conditions

| | Priming factor | MSCs source | Immunomodulatory effects of inflammatory priming | Suggested mechanism | Ref. |
|----------------------------|--|-------------|--|---|--|
| Pro-inflammatory cytokines | IFN- γ | hWJ-MSCs | ↓ Th1 and Th17 cells proliferation | ↑ CXCL9, CXCL10, CXCL11, ICAM-1, VCAM-1, IDO1 and HLA-G5 gene expression | Wang <i>et al</i> ^[35] , 2016 |
| | | | ↑ Th2 and Tregs (CD4+, CD25+, CD127dim/- cells) percentage | ↓ IFN γ , TNF α but ↑ IL-10 and IL-6 secretion in co-culture with PB-MNCs | |
| | | hBM-MSCs | ↓ T-cell effector functions and Th1 cytokine (IFN- γ , TNF- α , and IL-2) production | ↑ B7H1 and B7DC (ligands for PD1) expression | Chinnadurai <i>et al</i> ^[36] , 2014 |
| | IFN- γ and TNF- α | hBM-MSCs | ↓ T cell proliferation | ↑ IDO activity | François <i>et al</i> ^[55] , 2012 |
| | | | ↑ Monocyte differentiation into M2 (IL-10-secreting CD206+) immunosuppressive macrophages | | |
| | | | ↓ CD3/CD28-induced T-cell proliferation | ↓ Potency to trigger increased IFN- γ and IL-2 synthesis by activated T cells | Cuerquis <i>et al</i> ^[59] , 2014 |
| | TNF- α /IFN- γ and IL- β | rBM-MSCs | ↓ Proliferation of syngeneic lymphocytes | ↑ NO production | Murphy <i>et al</i> ^[80] , 2019 |
| | IL-17 | hBM-MSCs | ↓ PHA-stimulated T-cell proliferation | ↑ IL-6 gene expression | Sivanathan <i>et al</i> ^[94] , 2015 |
| | | | ↓ Expression of CD25 on CD4+ effector T cells | Treg-mediated IL-2 deprivation | |
| | | | ↓ T cell effector function and Th1 cytokines (IFN- γ , TNF- α , IL-2) secretion | | |
| Alarmins | | | ↑ Formation of Tregs (CD4+ CD25 high CD127 low FoxP3+) | Cell-contacts and ↑ PGE2 and TGF- β expression | |
| | IFN- γ , TNF- α and IL-17 | mBM-MSC | ↓ T-cell proliferation | ↑ iNOS expression | Han <i>et al</i> ^[95] , 2014 |
| | IFN- γ , TNF- α and IL-6 | hAT-MSC | ↓ Proliferation of PHA or MLR activated PB-MNCs | ↑ IDO expression | Crop <i>et al</i> ^[111] , 2010 |
| | IL-1 α | hBM-MSCs | ↓ IL-6, TNF- α and ↑ IL-10 secretion in LPS-activated mouse microglial BV2 cells | ↑ G-CSF secretion | Redondo-Castro <i>et al</i> ^[78] , 2017 |
| | | | | | |
| | HMGB1 | hBM-MSC | Unaffected inhibition of Con A-induced lymphocyte proliferation | / | Meng <i>et al</i> ^[118] , 2008 |
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Symbols: ↑ and ↓ represent stimulatory or inhibitory activity of priming factor, respectively. IFN- γ : Interferon gamma; TNF- α : Tumor Necrosis Factor alpha; IL: Interleukin; HMGB1: High mobility group box 1; MSCs: Mesenchymal stromal/stem cells; h: Human; WJ: Warthon jelly's; BM: Bone marrow; r:rat; AT: Adipose tissue; Th: T helper; PHA: Phytohaemagglutinin; MLR: Mixed lymphocyte reaction; LPS: Lipopolysaccharide; Con A: Concanavalin A; CXCL: C-X-C motif chemokine ligand; ICAM-1: Intercellular adhesion molecule-1; VCAM-1: Vascular cell adhesion molecule 1; IDO: Indoleamine-pyrrole 2,3-dioxygenase; HLA-G5: Human leukocyte antigen-G molecules; PB-MNCs: Peripheral blood mononuclear cells; B7H1: B7 homolog 1; PD1: Programmed cell death protein 1; NO: Nitric oxide; PGE2: Prostaglandin E₂; TGF- β : Transforming growth factor beta; iNOS: Inducible NO synthase; G-CSF: Granulocyte - colony stimulating factor.

found to be related to the increased migration of IFN- γ -primed MSCs along with their enhanced capacity to inhibit Th1 inflammatory responses, all of which contributed to decreased mucosal damage. In addition, Polchert *et al*^[41] showed that IFN- γ -primed mouse BM-MSCs suppress graft *vs* host disease more efficiently than non-primed MSCs depending on the magnitude of IFN- γ exposure (Figure 2). By contrast, a recent study showed that infusion of thawed IFN- γ -primed human MSCs failed to improve retinal damage in a murine model of retinal disease^[42].

TNF- α priming: TNF- α is a pleiotropic cytokine involved in systemic inflammation, which also affects the metabolism, growth, and differentiation potential of various cell types. Regarding the regenerative potential of TNF- α -treated MSCs, it has been

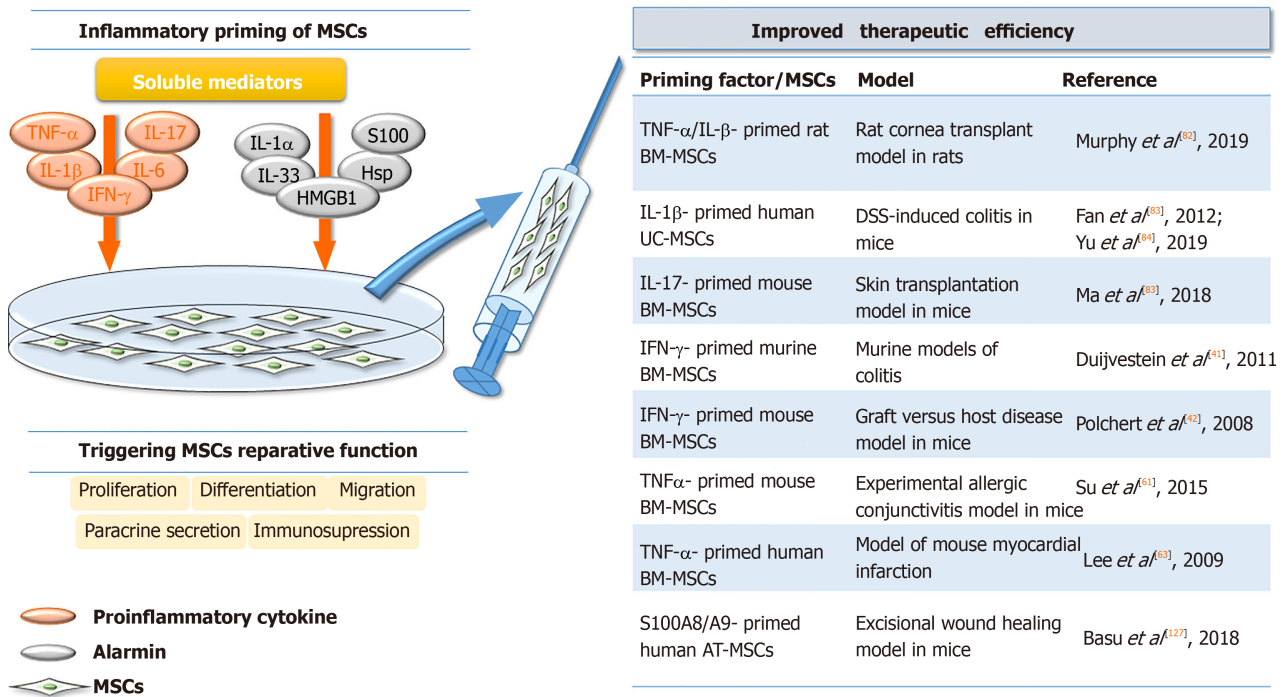


Figure 2 Improved *in vivo* therapeutic potential of inflammatory primed mesenchymal stromal/stem cells. The inflammatory niche mediators, including proinflammatory cytokines and alarmins, play a key role in triggering the reparative functions of mesenchymal stromal/stem cells, influencing their paracrine secretion, proliferation, differentiation, migration and immunomodulatory potential. When applied *in vivo*, the improved therapeutic efficiency of inflammatory primed MSCs has been detected in various experimental models. The numbers in square brackets indicate the references. TNF- α : Tumor Necrosis Factor alpha; IL: Interleukin; IFN- γ : Interferon gamma; HMGB1: High mobility group box 1; Hsp: Heat shock proteins; BM: Bone marrow; MSCs: Mesenchymal stromal/stem cells; UC: Umbilical cord; AT: Adipose tissue; DSS: Dextran sulfate sodium.

determined that this cytokine promotes the proliferation of human synovial MSCs and BM-MSCs^[43,44], while not affecting their clonogenic potential. Moreover, the involvement of the nuclear factor-kappa B (NF- κ B) signaling pathway is implicated in TNF- α -stimulated invasion and proliferation of BM-MSCs^[44] (Figure 1). Furthermore, the preconditioning of MSCs with TNF- α differentially regulates their chondrogenic differentiation depending on the tissue source and donor age (Figure 1). Namely, while TNF- α does not affect the chondrogenic capacity of human synovial MSCs and BM-MSCs^[43,45], Wheiling *et al.*^[46] revealed that it inhibited the chondrogenesis of human BM-MSCs isolated from elderly donors. In addition, several studies have indicated that TNF- α alters the osteogenic differentiation of MSCs in dose-, tissue source-, and species-specific manners (Figure 1). Regarding rodent MSCs, several studies have found that TNF- α inhibits the osteogenic differentiation of MSCs^[47,48], while continuous delivery of TNF- α stimulates the osteogenic differentiation of rat BM-MSCs seeded onto three-dimensional biodegradable scaffolds^[49]. The enhanced osteogenic potential has also been evidenced for human BM-MSCs treated with TNF- α ^[50,51]. However, it dually affects dental pulp stem cells, promoting their osteogenic differentiation through the Wnt/ β -catenin signaling pathway, while suppressing the osteogenesis of these cells at high concentrations^[52,53].

In the context of the stronger immunomodulatory capacity of TNF- α -primed MSCs, studies have demonstrated increased secretion of the immunosuppressive molecules PGE2 and IDO, chemokine IL-8, CXCL5, CXCL6, and certain growth factors such as hepatocyte growth factor, insulin-like growth factor 1, and vascular endothelial growth factor (VEGF)^[54-57] (Table 1). Moreover, it has been revealed that TNF- α priming of rat UC-MSCs suppresses the inflammatory milieu by increasing TGF- β and IL-10 expression^[58]. Because the immunosuppressive effects of TNF- α are less pronounced compared to IFN- γ priming in WJ-MSCs^[28], several studies have investigated the combined effects of TNF- α and IFN- γ on the immunomodulatory potential of MSCs. Indeed, when human BM-MSCs were subjected to combined pretreatment with TNF- α plus IFN- γ , more effective inhibition of CD3/CD28-induced T-cell proliferation was observed compared to non-primed MSCs^[59] (Table 1). Also, combined TNF- α and IFN- γ preconditioning was shown to increase IDO activity in BM-MSCs, resulting in monocyte differentiation into M2 immunosuppressive

macrophages, which further inhibited T-cell proliferation *via* IL-10 secretion^[55].

Regarding the beneficial effects of MSC preconditioning with TNF- α , an *in vivo* study performed by Su *et al*^[60] showed that the culture medium of TNF α -primed mouse BM-MSCs reduced experimental allergic conjunctivitis through multiple cyclooxygenase-2-dependent antiallergic mechanisms. In addition, the culture medium of TNF-primed human AT-MSCs has been shown to accelerate cutaneous wound closure, angiogenesis, and infiltration of immune cells in a rat excisional wound model *via* IL-6 and IL-8 secretion^[61]. Also, in a model of mouse myocardial infarction, improved cardiac function related to decreased inflammatory responses and reduced infarct size has been documented in animals receiving TNF- α -primed human BM-MSCs^[62]. By contrast, TNF priming reverses the immunosuppressive effects of mouse MSCs on T-cell proliferation, resulting in the failure of MSC treatment of murine collagen-induced arthritis^[63].

IL-1 β priming: IL-1 β is the key mediator of inflammatory responses, which contributes to the host-defense response facilitating activation of innate immune cells^[64]. Regarding the effects of IL-1 β priming on MSCs proliferation and differentiation, heterogeneous results have been reported (Figure 1). Namely, while IL-1 β preconditioning increases equine AT-MSCs and human synovium-derived MSCs proliferation^[65,66], exposure of UC-MSCs to IL-1 β results in suppressed proliferation^[67]. Moreover, functional analyses of human BM-MSCs have revealed that treatment with IL-1 β does not affect the proliferation of these cells, and promotes their migration and adhesion to extracellular matrix components^[68]. Also, a study by Guo *et al*^[69] demonstrated that IL-1 β promoted UC-MSCs transendothelial migration through the CXCR3-CXCL9 axis, indicating the beneficial effects on MSC homing to target sites.

Many studies have described the modulatory effects of IL-1 β stimulation on the osteogenic differentiation of MSCs, with conflicting results depending on the MSC tissue origin as well as IL-1 β concentration (Figure 1). Sonomoto *et al*^[70] demonstrated the ability of IL-1 β to induce the osteogenic differentiation of human BM-MSCs *via* the Wnt pathway. Increased osteogenesis has also been found for equine AT-MSCs and human UC-MSCs treated with IL-1 β ^[65,67]. On the other hand, depending on the concentration, IL-1 β exerts dual effects on the osteogenesis of periodontal ligament-MSCs, since low doses of IL-1 β promote osteogenesis by activating the bone morphogenetic protein (referred to as BMP)/Smad signaling pathway, while higher doses of the cytokine impede osteogenesis^[71]. IL-1 β treatment also inhibits the chondrogenesis of MSCs from the femoral intramedullary canal in a dose-dependent manner *via* NF- κ B activation^[46]. In accordance with these findings, decreased chondrogenic differentiation has been reported for BM-MSCs and synovial fluid-MSCs treated with IL-1 β ^[72-75]. However, Hingert *et al*^[76] showed that pretreatment of BM-MSCs with IL-1 β followed by BMP-3 stimulation in a three-dimensional *in vitro* hydrogel model resulted in high proteoglycan accumulation and SRY-box transcription factor 9 expression, suggesting that IL-1 β may be the causative factor.

Several studies have indicated changes in the secretory profile of MSCs primed with IL-1 β , as well as the significance of IL-1 β priming in combination with other factors. Regarding gingival-MSCs, IL-1 β preconditioning induces the expression of TGF- β and matrix metalloproteinase agonists^[77], while in human BM-MSCs, IL-1 β increases granulocyte colony-stimulating factor (referred to as G-CSF)^[78], IL-6, VEGF, CXCL1, and CCL2 chemokines^[79]. The immunosuppressive activities of rat BM-MSCs were shown to be significantly promoted after preconditioning with TNF- α or IFN- γ in combination with IL- β , as the decreased proliferation of syngeneic lymphocytes *in vitro* was demonstrated^[80] (Table 1). These effects were confirmed by *in vivo* experiments in a rat cornea transplant model, where after transplantation of syngeneic MSCs primed with TNF- α /IL- β enhanced graft survival (up to 70%) was observed compared to unprimed MSCs (up to 50%). In addition, the increased number of Tregs and reduced expression of pro-inflammatory cytokines in the draining lymph node of these animals were found, whereas there was an increased number of regulatory monocyte/macrophage cells and Tregs in the lungs and spleen^[80].

Administration of IL- β -primed human UC-MSCs in mice with dextran sulfate sodium-induced colitis also increases the number of Tregs and Th2 cells, while reducing Th1 and Th17 cells in the spleen and mesenteric lymph nodes^[81]. A recent study by Yu *et al*^[82] emphasized the role of PGE2 and IDO induction in the observed immunosuppressive effects of umbilical cord blood-MSCs primed with IL-1 β and IFN- γ in the same disease model. Moreover, another recent study showed that the culture medium of IL-1 β -primed AT-MSCs increased the phagocytic capacity of neutrophils, which may contribute to inflammation resolution, removal of tissue debris, and support of tissue repair in joint pathology^[83]. Overall, the results indicating the

immunosuppressive phenotype of IL-1 β -primed MSCs strongly suggest that this cytokine might promote the therapeutic efficacy of MSCs in disorders related to an exaggerated immune response (Figure 2).

IL-17 priming: IL-17 is another pro-inflammatory cytokine that plays a pivotal role in linking the immune and hematopoietic systems, while also contributing to the pathogenesis of numerous autoimmune and inflammatory diseases. However, the effects that this cytokine exerts on MSCs are still not fully understood. To date, it has been shown that IL-17 stimulates the proliferation of mouse and human BM-MSCs, as well as the migration of human BM-MSCs and trans-endothelial migration of peripheral blood MSCs^[84-86] (Figure 1). Regarding the differentiation potential, published results have shown that IL-17 priming enhances osteogenic^[84,87-89], but inhibits chondrogenic^[90] and adipogenic^[88,91] differentiation in human BM-MSCs. Moreover, IL-17 can decrease the osteogenic differentiation of periodontal ligament-MSCs through extracellular signal-regulated protein kinases 1 and 2 (referred to as ERK1/2), and c-Jun N-terminal kinase mitogen-activated protein kinases^[92]. Research related to the effects of IL-17 on the differentiation potential of mouse BM-MSCs has led to conflicting results, as one study found that IL-17 did not affect the differentiation potential of MSCs towards osteoblasts^[85], whereas another showed suppressed osteogenic differentiation of these cells mediated by I κ B kinase and NF- κ B^[93].

Regarding the immunomodulatory activity of MSCs, IL-17 priming enhances the immunosuppressive features of MSCs. While IL-17 has no impact on MSC markers and the low immunogenic phenotype of human BM-MSCs, IL-17-primed MSCs suppress T-cell proliferation and inhibit CD25 expression and expression of Th1 cytokines, including IFN- γ , TNF- α , and IL-2^[94]. Moreover, a study showed that mouse MSCs pretreated with IFN- γ and TNF- α in combination with IL-17 significantly reduced T-cell proliferation *via* the inducible nitric oxide synthase (referred to as iNOS) pathway^[95] (Table 1). The same study confirmed the immunosuppressive activity of BM-MSCs primed with IL-17 *in vivo* in a mouse model of concanavalin A-induced liver injury. However, another study showed that IL-17 significantly reduced the suppressive capacity of olfactory ecto-MSCs on CD4+ T cells, mainly through the downregulation of suppressive factors (PD-L1, iNOS, IL-10, and TGF- β)^[96]. The positive effect of IL-17 on the immunomodulatory features of MSCs has been confirmed in *in vivo* studies with different animal models. Namely, in a study in which mouse BM-MSCs were treated with IL-17 prior to their use in ischemia-reperfusion acute kidney injury, a significant decrease in IL-6, TNF- α , and IFN- γ levels and higher spleen and kidney Treg levels were shown compared to mice that received non-primed MSCs^[97]. In another work, IL-17-primed mouse BM-MSCs used in a skin transplantation model were found to increase the Treg subpopulation as well as IL-10 and TGF- β levels, significantly prolonging graft survival^[98].

IL-6 priming: Pleiotropic effects on immune regulation, hematopoiesis, and tissue regeneration are exerted by another inflammatory cytokine, IL-6^[99]. Preconditioning MSCs with IL-6 has been shown to influence their behaviors in different manners depending on the tissue origin of the MSCs (Figure 1). Namely, a few studies have reported conflicting data showing that IL-6 has no effect on the proliferation of human AT-MSCs and mouse BM-MSCs^[100,101], whereas in other studies, IL-6 increased the proliferation of human placenta-derived MSCs and BM-MSCs^[102,103]. Moreover, the stimulating effect of IL-6 on BM-MSCs growth and *in vitro* wound healing is mediated by ERK1/2 activation^[103]. It has also been reported that IL-6 differentially influences stem cell differentiation (Figure 1). Priming with IL-6 under osteogenic induction conditions has been shown to enhance mineralization and alkaline phosphatase expression in human BM-MSCs, AT-MSCs, and stem cells from human exfoliated deciduous teeth (called SHEDs)^[104-107]. However, studies using lower concentrations of IL-6 have shown no effect on osteogenic differentiation potency of human BM-MSCs^[103]. Although IL-6 inhibits the chondrogenic differentiation of human BM-MSCs when added during differentiation induction^[103], concomitant supplementation with IL-6 and soluble IL-6 receptor contributes to the enhanced chondrogenesis of this type of MSC^[108]. Treatment with IL-6 during or prior to adipogenic differentiation induction reduces the adipogenesis capacity of human BM-MSCs^[103], while other studies have reported no or positive effects of IL-6 on the adipogenic ability of human BM-MSCs, AT-MSCs, and SHEDs^[104,109,110].

Even less is known about the immunomodulatory potential of IL-6-preconditioned MSCs. In this context, few studies have analyzed IL-6 effects in combination with other pro-inflammatory cytokines. Namely, altered immunological status has been reported

for AT-MSCs primed with a combination of IFN- γ , TNF- α , and IL-6 (Table 1), as shown by the upregulated expression of HLA class I and class II, as well as CD40^[111], indicating a potentially more immunogenic phenotype. In addition, although the same priming conditions have no effect on AT-MSCs differentiation capacity, they enhance their immunosuppressive activity mainly through increased IDO expression. Another study demonstrated that human AT-MSCs and BM-MSCs primed with another combination of pro-inflammatory cytokines, IL-1, IL-6, and IL-23, exerted increased differentiation potential towards osteogenic and adipogenic lineages, while their morphology, immunophenotype (except upregulated CD45), and costimulatory molecule expression were similar to non-primed cells. Also, primed MSCs showed increased TGF- β and decreased IL-4 production, while their suppressive effect on T-cell proliferation was comparable to controls^[112]. Although these findings suggest that priming with IL-6 might promote the therapeutic efficacy of MSCs in the treatment of various inflammatory and autoimmune disorders, no study investigating the *in vivo* therapeutic potential of MSCs preconditioned with IL-6 (alone or combined with other cytokines) has been performed to date.

MSCs priming with alarmins

Alarmins are constitutively expressed inside cells and exert various functions under physiological conditions. Upon tissue damage induced by pathogens or physical/chemical injuries, dying necrotic cells passively and rapidly release alarmins outside of cells to promote the immune response and support tissue repair^[4,5,6]. In addition to these activities, alarmins are involved in many other processes, such as cellular homeostasis, wound healing, and tumor development^[6,7]. The best-characterized alarmins, such as IL-1 α , IL-33, HMGB1, S100 proteins, and Hsps, will be discussed here in the context of their effects on MSC biology and potential role in tissue repair.

IL-1 α and IL-33 are both dual-function cytokines that are localized in the nucleus under homeostatic conditions, where they function as transcription factors. Data on their extracellular effects on MSCs are very elusive. It has been demonstrated that IL-1 α stimulates the expression of trophic factor G-CSF *via* IL-1 receptor type 1 signaling in human BM-MSCs. In addition, the conditioned medium of IL-1 α -primed BM-MSCs was shown to inhibit the secretion of inflammatory and apoptotic markers in lipopolysaccharide-activated mouse microglial BV2 cells and increase secretion of the anti-inflammatory IL-10 cytokine^[78], suggesting that MSCs priming with IL-1 α favors their immunosuppressive activities (Table 1). Another recent study showed that IL-1 α decreased the proliferative and adipogenic differentiation capacity of AT-MSCs, whereby adipogenesis was inhibited predominantly during the early phase of differentiation *via* NF- κ B and ERK1/2 pathways with subsequent stimulation of pro-inflammatory cytokines, such as IL-8, IL-6, CCL2, and IL-1 β , during adipogenic differentiation of AT-MSCs^[113] (Figure 1). Since the effects of IL-1 α are conspicuous at the beginning of the differentiation process, it is important to further examine IL-1 α priming in the context of MSC differentiation. It was recently demonstrated that without changing MSC marker expression^[114,115], IL-33 treatment has the potential to modify the regenerative^[114] and immunomodulatory characteristics of MSCs^[115]. Our recent study demonstrated that IL-33 treatment reduced periodontal ligament-MSCs and dental pulp MSCs osteogenesis but supported their proliferation, clonogenicity, and stemness (Figure 1). Both MSC types primed with IL-33 maintained their differentiation capacity, while increased alkaline phosphatase activity was also observed, indicating that IL-33 may contribute to the preservation of the dental stem cell pool^[114]. Research conducted by Terraza *et al.*^[115] demonstrated that IL-33 with IFN- γ stimulated the high expression of IL-6, TGF- β , and iNOS in mouse BM-MSCs. Despite the scarce data on IL-1 α and IL-33 priming of MSCs, overall data indicate that preconditioning with these molecules should be additionally explored as an MSC priming strategy.

Another nuclear alarmin is HMGB1, a non-histone DNA-binding protein involved in the maintenance of the chromatin structure and gene expression regulation^[116]. The knowledge on the effects of released HMGB1 on MSCs functions is still contradictory, as its stimulatory^[117] as well as inhibitory^[118,119] actions on MSCs proliferation have been reported. The promoted migratory capacity of MSCs primed with HMGB1 has also been demonstrated^[117-119], indicating its beneficial effects for MSC functional adjustment in therapeutic use. In the presence of HMGB1, the osteogenic differentiation of MSCs is also induced^[118,120,121] (Figure 1). Moreover, HMGB1 stimulates the secretion of various cytokines by MSCs including macrophage CSF, eotaxin-3, epidermal growth factor receptor, VEGF, angiopoietin-2, CCL-5, urokinase plasminogen activator receptor, and macrophage migration inhibitory factor, which

may be associated with the induced osteogenic differentiation under HMGB1 influence^[121]. Furthermore, in rat BM-MSCs, along with promoted MSC migration, HMGB1 stimulates VEGF-induced differentiation to endothelial cells but decreases their proliferation and platelet-derived growth factor-induced differentiation to smooth muscle cells^[119]. These findings indicate that HMGB1 priming could be a significant factor in tissue engineering for MSC-guided differentiation. Regarding immunomodulatory functions, it has been reported that HMGB1 priming has no effect on BM-MSCs ability to inhibit the proliferation of concanavalin A-stimulated lymphocytes *in vitro*^[118] (Table 1), but additional research is needed to confirm these functions.

Unlike IL-1 α , IL-33 and HMGB1 alarmins, S100 proteins, and Hsps are located in the cytoplasm during homeostasis^[4]. The effect of extracellular S100A6 has been investigated on MSCs derived from WJ of the UC, and the results have shown the ability of this molecule to increase cellular adhesion and reduce their proliferation capacity by interacting with integrin β 1^[122] (Figure 1). Regardless, pretreatment of human AT-MSCs with S100A8/A9 and their subsequent application to wounds induced in C57BL/6 mice significantly improve wound healing due to transcriptome expression profile changes related to the enhanced protective MSCs phenotype^[123]. Regarding the Hsp protein family, it has been demonstrated that Hsp90 increases viability and protects rat BM-MSCs against apoptosis, simultaneously increasing the paracrine effect of MSCs^[124]. Another study showed that Hsp90 α promotes rat MSCs migration, possibly mediated by the increased secretion of MMPs, SDF-1/CXCR4, and vascular cell adhesion protein 1^[125] (Figure 1). Interestingly, the dual effects of Hsp70 have been demonstrated depending on the age of the MSCs. Namely, in a study by Andreeva *et al*^[126], Hsp70 increased the growth of aged but not young mouse AT-MSCs (Figure 1), suggesting the potential beneficial effects of Hsp70 priming. Moreover, the important role of Hsp70 in the osteogenesis of human MSCs is demonstrated by increased alkaline phosphatase activity and MSC mineralization^[127,128].

CONCLUSION

As MSCs are crucial cellular components for tissue repair, it is essential to understand how the inflammatory microenvironment modulates the functionality of these cells. The beneficial effects of MSCs have been demonstrated, but due to the large heterogeneity detected within MSC populations, the success of their application in clinical trials has been limited. Moreover, it is believed that the inflammatory niche is indispensable for triggering MSC activity in an appropriate manner. Therefore, preconditioning methods have been applied to enhance and/or adjust MSCs functionality, including their regenerative and immunomodulatory status. To date, studies of the MSCs response to soluble factors featuring the inflammatory niche have been mostly focused on the effects provoked during their presence, pointing to the necessity of further exploring the durability of these changes. In this work, we collected data on the therapeutic potential of MSCs treated with pro-inflammatory cytokines (TNF- α , IFN- γ , IL-1 β , IL-17 and IL-6) and alarmins (IL-1 α , IL-33, HMGB1, S100 proteins, and Hsps) that are predominantly released at the site of the damaged tissue.

The reviewed data strongly indicate that all aforementioned factors possess the ability to modify the regenerative and immunomodulatory activities of MSCs, and the effects of these factors depend on the MSC tissue and species origin, as well as on donor age and cellular aging (senescence) status. In addition, different effects have been reported depending on the priming factor concentration and their selected combinations, as well as on the disease model, indicating that all of these aspects together should be carefully considered in relation to specific application requirements. Importantly, the effects of primed MSCs have been demonstrated in various animal wound and disease models, suggesting the validity of priming approaches for MSC therapy. Indeed, priming MSCs with certain inflammatory factors, such as TNF- α , IL- β , IFN- γ or S100A8/A9, contribute to the suppression of graft *vs* host disease and colitis, as well as to improved corneal and skin graft survival, mediated by their dominant immunosuppressive activity (Figure 2). Together, the data summarized in this paper provide a significant starting point for future research on priming MSCs and set future directions for establishing standardized methods for the application of preconditioned MSCs in cell therapy.

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Role of the CXCR4-SDF1-HMGB1 pathway in the directional migration of cells and regeneration of affected organs

Nazmul Haque, Ismail M Fareez, Liew Fong Fong, Chanchal Mandal, Noor Hayaty Abu Kasim, Kranthi Raja Kacharaju, Pratiwi Soesilawati

ORCID number: Nazmul Haque 0000-0002-8191-8993; Ismail M Fareez 0000-0001-6993-5339; Liew Fong Fong 0000-0001-9165-2343; Chanchal Mandal 0000-0003-2865-2847; Noor Hayaty Abu Kasim 0000-0002-8889-842X; Kranthi Raja Kacharaju 0000-0002-2057-9473; Pratiwi Soesilawati 0000-0002-1141-5645.

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Nazmul Haque, Ismail M Fareez, Liew Fong Fong, Department of Oral Biology and Biomedical Sciences, Faculty of Dentistry, MAHSA University, Selangor 42610, Malaysia

Chanchal Mandal, Biotechnology and Genetic Engineering Discipline, Life Science, Khulna University, Khulna 9208, Bangladesh

Noor Hayaty Abu Kasim, Faculty of Dentistry, University Kebangsaan Malaysia, Kuala Lumpur 50300, Malaysia

Noor Hayaty Abu Kasim, Faculty of Dental Medicine, Universitas Airlangga, Surabaya 411007, Indonesia

Kranthi Raja Kacharaju, Department of Conservative Dentistry, Faculty of Dentistry MAHSA University, Selangor 42610, Malaysia

Pratiwi Soesilawati, Department of Oral Biology, Faculty of Dental Medicine, Universitas Airlangga, Surabaya 60115, Indonesia

Corresponding author: Nazmul Haque, PhD, Senior Lecturer, Department of Oral Biology and Biomedical Sciences, Faculty of Dentistry, MAHSA University, Jalan SP 2, Bandar Saujana Putra, Selangor 42610, Malaysia. nazmul@mahsa.edu.my; tanna.bge@gmail.com

Abstract

In recent years, several studies have reported positive outcomes of cell-based therapies despite insufficient engraftment of transplanted cells. These findings have created a huge interest in the regenerative potential of paracrine factors released from transplanted stem or progenitor cells. Interestingly, this notion has also led scientists to question the role of proteins in the secretome produced by cells, tissues or organisms under certain conditions or at a particular time of regenerative therapy. Further studies have revealed that the secretomes derived from different cell types contain paracrine factors that could help to prevent apoptosis and induce proliferation of cells residing within the tissues of affected organs. This could also facilitate the migration of immune, progenitor and stem cells within the body to the site of inflammation. Of these different paracrine factors present within the secretome, researchers have given proper consideration to stromal cell-derived factor-1 (SDF1) that plays a vital role in tissue-specific migration of the cells needed for regeneration. Recently researchers recognized that SDF1 could facilitate site-specific migration of cells by regulating SDF1-

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CXCR4 and/or HMGB1-SDF1-CXCR4 pathways which is vital for tissue regeneration. Hence in this study, we have attempted to describe the role of different types of cells within the body in facilitating regeneration while emphasizing the HMGB1-SDF1-CXCR4 pathway that orchestrates the migration of cells to the site where regeneration is needed.

Key Words: C-X-C motif chemokine 12; Mesenchymal stem cells; Monocytes; Neutrophils; Peripheral blood mononuclear cells; Receptor for advanced glycation end products

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Core tip: In the last few decades, cell-based regenerative therapy has received considerable attention for the treatment of degenerative diseases or the regeneration of injured organs. However, poor cell retention is considered a major drawback associated with the short-term regenerative benefits. Furthermore, the short-term regenerative benefits are linked to paracrine factors secreted by the transplanted stem cells. To improve regenerative outcomes, researchers have identified the role of stromal cell-derived factor-1 (SDF1) as a key chemotactic factor that can facilitate site-specific migration and retention of transplanted cells, and stem or progenitor cells within the body by activating the SDF1-CXCR4 or HMGB1-SDF1-CXCR4 pathways.

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INTRODUCTION

Over the past decades, non-communicable diseases, especially degenerative diseases are becoming more prevalent worldwide, which also contributes to major morbidity. During the past two decades, stem cell-based regenerative therapy has been considered hopeful in addressing the unmet needs of treating degenerative diseases^[1].

Among the different tools of regenerative medicine “stem cells” are considered the most promising due to their self-renewal capability and multi-differentiation potential. However, recent studies have shown that the positive outcomes of different types of stem cell-based regenerative therapies are not directly correlated to the engraftment of transplanted cells^[2,3]. These findings have created a huge interest in the regenerative potential of paracrine factors and have led scientists to reveal the regenerative potential of proteins in the secretomes. Further studies have revealed the mitogenic, angiogenic, anti-apoptotic, anti-scarring and chemoattractant features of secretomes or cell culture supernatants that make them a potential tool for regenerative therapy^[1,4]. Furthermore, the regenerative potential of the secretome from adult stem cells^[5], freshly isolated healthy peripheral blood mononuclear cells (PBMC)^[6] and apoptosis-induced PBMC^[7,8] has been acknowledged by several researchers. Secretomes from stem and progenitor cells have been found to be favorable for regenerating tissues or treating several disorders including neuronal disorders^[9], vascular diseases^[10] and cutaneous wounds^[11]. The growing evidence on the role of paracrine factors (cytokines, chemokines and growth factors) in the regeneration of affected organs has led to the introduction of cell culture supernatants or secretomes as a new therapeutic tool of regenerative medicine.

Regeneration is a complex process and several types of cells namely lymphocytes, monocytes, neutrophils, endothelial progenitor cells (EPCs), hematopoietic stem cells (HSCs), mesenchymal stem cells (MSCs), and tissue resident stem cells are involved in the process of regeneration. Recent studies reported that stromal cell-derived factor-1α (SDF1α) present in the secretome increases proliferation, viability, migration and homing of stem and progenitor cells; helps lymphoid tissue development and differentiation; and inhibits apoptosis of cells^[4,12]. All these features are highly important for regeneration of damaged organs^[13]. Furthermore, SDF1 and C-X-C-X-C

chemokine receptor type 4 (CXCR-4) play a vital role in the high mobility group box 1 (HMGB1)-mediated inflammatory cell recruitment to the site of damaged tissue which is also vital for tissue repair and regeneration^[14]. Hence, in this review we have attempted to describe the role of different types of cells in regeneration while emphasizing activation of the HMGB1-SDF1-CXCR4 pathway which is considered a key pathway that regulates the directional migration of all cells and facilitates the process of regeneration.

PBMC IN REGENERATION

PBMC are widely used in preclinical research and applications in vaccine trials, source of biomarkers in various infectious and chronic diseases, and are a useful tool in studying various aspects of pathology and biology *in vitro*^[15]. In addition, PBMC are an easily accessible source of different types of adult stem and progenitor cells, such as HSCs, MSCs, osteoclast precursor cells, and EPCs^[16]. Due to the content of different types of adult stem cells, in a favorable microenvironment the potential to differentiate into several tissue specific cells including mature blood cells, endothelial cells, hepatocytes, cardiomyocytes, smooth muscle cells, epithelial cells, neural cells, osteoblasts, osteoclasts, and myofibroblasts has been shown^[16-18]. Furthermore, compared to bone marrow (BM) or other multipotent cells sources, the isolation of PBMC is less invasive. However, a series of standard procedures for PBMC collection, isolation, cryopreservation and preparation are crucial for their use in cell-based regenerative therapy^[15]. PBMC contain terminally differentiated immune cells, namely monocytes and lymphocytes that also play a vital role in tissue remodeling and regeneration^[19-21].

Monocytes

Monocytes that contribute approximately 4%-10% of leukocytes in our bloodstream are highly plastic in nature^[22]. Monocytes and macrophages are the largest types of white blood cells and are involved in inflammation and elimination of harmful foreign substances^[23,24]. As part of the innate immunity they are involved in tissue homeostasis and facilitate wound healing by removing apoptotic and necrotic cells^[24].

In regenerative tissues, macrophages are highly plastic and play a decisive role in tissue repair and regeneration^[25]. In response to injury and subsequent healing, macrophages are capable of polarization towards a spectrum of phenotypes. Based on the environmental cues and molecular mediators, these cells will differentiate into either pro-inflammatory type I macrophage (M1) or anti-inflammatory type II macrophage (M2) phenotypes^[25-27].

Studies have reported that M1 macrophages infiltrate tissues at the earlier stages of acute injury to promote the clearance of necrotic cells or tissue debris. Moreover, following activation M1 macrophages secrete a wide range of pro-inflammatory cytokines such as interleukin (IL)-1, IL-6, IL-8, IL-12, IL-18, IL-23, tumor necrosis factor (TNF)- α , monocyte chemoattractant protein (MCP)-1 and macrophage inflammatory protein (MIP)-1^[28]. Whereas, M2 macrophages appear within the injured tissue at later stages and release high amounts of anti-inflammatory paracrine factors such as IL-10 and transforming growth factor- β (TGF- β)^[25,29]. They are also capable of secreting extracellular matrix (ECM) remodeling components such as fibronectin, osteopontin, fibrin cross-linker transglutaminase and promote tissue healing^[30,31]. Although there are controversies regarding the sequential presence of the two different macrophages within tissues, this is because of the dynamic shift in macrophage polarization or the recruitment of new monocytes which do not invalidate the role of macrophages in tissue regeneration.

Lymphocytes

Among the different types of lymphocytes, the regulatory T-cells (Treg) are involved in the repair and regeneration of affected tissues and organ systems. Following injury, Treg are recruited to the site to regulate inflammation and modulate the process of regeneration^[32]. Following the initiation of inflammation, Treg inhibit recruitment of neutrophils by secreting IL-10 which in turn helps to minimize the secretion of inflammatory cytokines namely IL-1 β , IL-6, interferon (IFN)- γ , and TNF- α . Moreover, Treg induce apoptosis of neutrophils and clear debris by activation of M1 macrophages. In addition, they play a vital role in macrophage polarization towards the M2 phenotype by secreting anti-inflammatory cytokines such as IL-4, IL-10, and IL-13 which eventually support tissue repair and regeneration^[32,33]. However, the

regenerative function of Treg follows a tissue specific manner. For instance, in skeletal muscle, Treg infiltrate the tissues in response to IL-33 following activation of the M1 population and removal of necrotic tissues by these cells. Following infiltration, Treg inhibit M1-mediated inflammation and shift the polarization of macrophages towards the M2 population^[32]. Whereas, in heart tissues, recruitment of the higher number of Treg induces polarization of macrophages towards the M2 phenotype that help to inhibit inflammation, excessive matrix degradation, and adverse remodeling which eventually reduce ventricular ruptures and increases the rate of survival^[34].

PERIPHERAL BLOOD POLYMORPHONUCLEAR CELLS IN REGENERATION

Neutrophils are the most abundantly found white blood cells in the human peripheral circulation and contribute approximately 50%-70% to all circulatory white blood cells. They are the first leukocyte population recruited to the site of injury and regulate the process of tissue regeneration positively or negatively^[32]. However, the role of neutrophils in the process of regeneration is microenvironment-dependent and context-specific.

For example, in the case of skeletal muscle injury, neutrophils impair the restoration and function of muscles by releasing hypochlorous acid, nicotinamide adenine dinucleotide phosphate oxidase, and other cytokines^[32,35,36]. Downregulation of lung regeneration following ischemia-reperfusion by neutrophils has also been reported^[37]. It is noteworthy that neutrophils have also shown positive effects on the repair of lung epithelium and nerve cells^[38,39].

MESENCHYMAL AND OTHER TISSUE-SPECIFIC STEM CELLS IN REGENERATION

Apart from HSCs, other adult stem cells or tissue-specific progenitor cells such as MSCs, EPCs, mammary stem cells, intestinal stem cells, and neural stem cells are found in adult tissues^[40]. Tissue-specific stem cells maintain tissue homeostasis, while MSCs can differentiate into a variety of cell types. MSCs, in particular, have promising cell sources, as they can be harvested from various sources, such as BM, umbilical cord (UC), adipose tissue, and dental tissues^[41-43]. Unlike embryonic stem cells (ES cells or ESCs), which are pluripotent, MSCs are multipotent cells which possess limited differentiation potential. Nevertheless, their potential to differentiate into osteoblasts and osteocytes is very well known. There is also accumulating evidence regarding their robust potential in tissue healing and regenerative medicine, in both preclinical and clinical studies^[44-46]. According to a recent PubMed search conducted on November 2019, there were 110 MSC-based human clinical trials exploring the safety and efficacy of stem cells for tissue healing and the treatment of degenerative diseases. However, most of these trials were phase I and phase II, or a mixture of phase I/II studies. Whereas, phase III or phase II/III trials which investigate the long-term safety of MSC-based therapies prior to full establishment of MSCs in clinical practice are poorly documented. Thus, BM-derived MSCs (BMSCs) have been the most studied stem cells in cell therapy and tissue repair for the last 5 years, due to their multi-lineage differentiation potential^[47].

However, it is worthwhile noting that different MSC populations exhibit tissue-specific characteristics such as the expression of specific cell surface markers and transcription factors. In response to injury signals, these MSCs can potentially migrate from their niche to reach target tissues through vessel walls in the peripheral circulation^[48]. Many studies have been conducted to investigate both the chemical and mechanical factors that influence the homing mechanism and engraftment of MSCs into local areas of damaged sites. The chemical factors that affect the trafficking process are the presence of a variety of chemokines, growth factors and cytokines, whereas the mechanical factors involved in the process include ECM stiffness, vascular cyclic stretching and hemodynamic forces or shear stress on the vessel walls^[49]. These factors make up the vital characteristics of MSCs and result in their promising effect in tissue healing and differentiation.

The first characteristic of MSCs is their multi-lineage differentiation potential. MSCs are capable of differentiating into several mesoderm lineages, including adipogenic, osteogenic, chondrogenic and myogenic lineages, depending on the multitude of

stimuli and inhibitors present in the tissue microenvironment^[50]. The microenvironment plays an important role in the activation or downregulation of transcription factors that regulate the expression of genes responsible for the induction and progression of tissue-specific differentiation^[51]. MSCs can also generate neural cells in the ectodermal layer, and hepatic cells and pancreatic cells in the endodermal layer^[52]. The study by Chen *et al*^[53] was among the first to explore the ability of MSCs to differentiate into functional islet-like cells that might play an important role in the future treatment of diabetes. MSCs cultured in stiff scaffolds can easily differentiate into osteoblasts, and showed the potential for myogenic, adipogenic and neurogenic differentiation, respectively, but with a decrease in elasticity. Recently, Jung *et al*^[54] demonstrated that ECM proteins in 3D composites were able to trigger differentiation of BMSCs into mesodermal lineages with enhanced adipogenic differentiation and IL-6 expression compared to that in 2D ECM proteins.

Secondly, MSCs are capable of dynamic interactions with their microenvironment and secrete a wide variety of paracrine factors that are required for tissue recovery or wound healing. Several studies refuted the hypothesis that direct trans-differentiation or cell fusion of MSCs was the principal mechanism underlying their therapeutic action in tissue regeneration^[55]. Indeed, MSCs transplantation regulated released factors in experimental models of tissue injury, which was largely associated with suppression of immune and inflammatory reactions, inhibition of apoptosis, and enhancement of cell proliferation and angiogenesis, thereby promoting regeneration of the tissue^[56]. Apart of MSCs-mediated secretion of these paracrine and autocrine factors, extracellular vesicles such as exosomes and microvesicles may also regulate these functional roles^[57,58]. The MSC-mediated factors released at high levels include the following: (1) Growth factors and their receptors [*i.e.*, granulocyte-macrophage colony-stimulating factor (GM-CSF), basic fibroblast growth factor (bFGF), vascular endothelial growth factor (VEGF), insulin-like growth factor-binding proteins (IGFBP3, IGFBP4, IGFBP7) and bone morphogenetic protein 2 (BMP-2)]; (2) Extracellular matrix remodelers/mediators [*i.e.*, periostin, fibronectin, collagen, TIMP metalloproteinase inhibitor 2 (TIMP-2), metalloproteinase inhibitors, and decorin]; and (3) Immune system signaling regulatory proteins (*i.e.*, TGF- β , MCP-1, IL-6, and IL-8)^[49,59]. Various studies have demonstrated that the released pro-inflammatory cytokines up-regulate the efficacy of MSC-mediated immunomodulation and functional improvement in microvascular injury^[60], inflammatory liver disease^[61], osteoarthritis^[62], spinal cord injury^[63], brain cancer^[64], ischemic limb regeneration^[65], and asthmatic^[66] models. Taken together, it is well accepted that the combination of MSCs with these trophic factors can modulate their behavior during inflammation and tissue injury. Research should now focus on the strategies to manipulate and modulate the secretion of these molecules in the infused or implanted MSCs microenvironment to enhance their functional role^[1].

Finally, MSCs exhibit immunomodulatory properties^[67-69]. The immunomodulatory properties of MSCs proved effective in treating various immune disorders in both *in vivo* and human studies. MSCs modulate the functions of almost all cells of both the innate and adaptive immune systems and induce an anti-inflammatory phenotype^[59]. MSCs interact with a variety of immune cells and have the capacity to inhibit the excessive response of B cells, T cells, macrophages, dendritic cells, and natural killer cells^[68]. Nevertheless, the underlying molecular and cellular mechanisms behind MSC-mediated immunomodulation have not been fully elucidated. MSCs have been shown to modulate the immune response by secreting soluble factors [*e.g.*, IL-6, M-CSF, IL-10, TGF- β , HGF, and prostaglandin E2 (PGE2)] in the presence of adhesion molecules [*i.e.*, vascular cell adhesion molecule (VCAM)-1, intercellular adhesion molecule (ICAM)-1, and lymphocyte function-associated antigen (LFA)-3]^[70-72]. Through a synergy of cell contact-dependent mechanisms and these soluble factors, MSCs are able to initiate the T-cell interactions that play a prominent role in their immunomodulatory potential^[71,73]. Furthermore, anti-inflammatory monocytes/macrophages and Tregs are also important in MSC-mediated immunosuppression^[69,74]. Studies also linked the low immunogenic properties of MSCs to the lower level of expression of major histocompatibility complex (MHC) class I antigens, and lack of MHC class II and co-stimulatory molecules such as CD80, CD86, and CD40^[75,76]. Although the immunomodulatory effect of MSCs is hypothesized to be *via* MSC-secreted cytokines in many studies, most studies documented that MSCs act differently depending on the local microenvironment and the presence of inflammatory cytokines during the pre-treatment of MSCs. An understanding of the immune suppressive role of MSCs would enhance prospective clinical applications of these cells.

Thus, the fate of MSCs is vastly influenced by their environment which includes mechanical or physical stimulation, growth factors, cell density, and cell-cell

attachment or interactions. However, this multipotency of MSCs could also be due to another reason which has been widely discussed. In fact, a debate is currently ongoing regarding the 'stem cell' status of MSCs^[77]. It is postulated that MSCs are purely specific adult stem cells, which contradicts findings that MSCs are a diverse mixture of many specific lineage progenitor cells. However, these shortcomings provide a good reason for the continuous research on MSCs in stem-cell based therapy.

CELL MIGRATION IS ESSENTIAL FOR TISSUE REGENERATION

Progenitors and MSCs migrate and initiate the homing mechanism in response to inflammatory signaling molecules and corresponding receptors around the injured tissue. MSCs are therapeutically capable of reaching and homing to sites of inflammation by various routes such as intravenous (IV), intra-arterial (IA), intraparenchymal, intracoronary (IC) local administration and into the subarachnoid and epidural spaces^[48]. From the systemic circulation, MSCs migrate specifically to damaged tissue sites and exert their functional effects locally under a variety of pathologic conditions. Luger *et al.*^[78] demonstrated that intravenously administered fluorescent and radiolabeled MSCs homed to regions of myocardial injury to suppress the progressive deterioration in left ventricular function and adverse remodeling in mice, and it is thought to be a feasible and effective therapeutic strategy for the treatment of patients with large infarcts and ischemic cardiomyopathy. MSCs homing involves various chemokines and their receptors (*i.e.*, SDF1, CCL5, CXCR4, CXCR5, CXCR6, CCR2, CCR3, and CCR4), matrix metalloproteinases (MMPs) [MMP-2 and membrane type 1 MMP (MT1-MMP)], receptor tyrosine kinase dependent growth factors [*e.g.*, hepatocyte growth factor-Mesenchymal Epithelial Transition Factor (c-Met) proto-oncogene/receptor tyrosine kinase (HGF/c-Met) axes, platelet-derived growth factor (PDGF) and insulin-like growth factor 1 (IGF-1)] and some other adhesion molecules (*i.e.*, integrin β 1, integrin α 4, and VCAM)^[79-82]. These homing signals are released by injured cells and/or respondent immune cells. Besides these homing signals, other molecules are implicated in different steps of the homing process such as PGE2 and hematopoietic cell E-/L-selectin ligand (HCELL) that are functionally involved in cell migration to the injured tissue^[83]. These factors could be a feasible strategy to facilitate therapeutic delivery of MSCs to targeted injured tissue.

Of the different chemokines and chemokine-mediated pathways, the SDF1-CXCR4 and HMGB1-SDF1-CXCR4 axis have received considerable attention due to their potential in-site specific directional migration of stem and progenitor cells. The role of HMGB1-SDF1-CXCR4 in regeneration of injured tissues or organs is discussed further below.

HMGB1-SDF1-CXCR4 AXIS IN FACILITATING TISSUE-SPECIFIC MIGRATION

HMGB1 in orchestrating the process of migration and regeneration

HMGB1 protein is a highly conserved non-histone nuclear protein that binds to DNA and regulates the expression of genes and the chromosomal architecture^[84]. Extracellular HMGB1 is actively secreted from activated or stressed immune cells, while passively secreted from necrotic tissues^[85,86]. Following secretion into the extracellular space, HMGB1 exerts chemotactic activity or acts as a damage-associated molecular pattern molecule^[87]. Indeed, the overall signaling mechanism by HMGB1 interacting with target cells needs to be elucidated for future therapeutic intervention^[88].

Wound healing is a complex process that involves the ECM, cytokines, growth factors and several types of cells. The steps involved in the process of wound healing include hemostasis, inflammation, cell migration and proliferation, wound contraction, and remodeling^[89,90]. During the inflammatory phase, vasodilation followed by early vasoconstriction which is mediated by histamine, leukotrienes, and prostaglandins, increases capillary permeability and cell migration into the wound site^[91]. Neutrophils are the first among the infiltrated cells to the site of injury followed by monocytes and lymphocytes. Initiation of leukocyte migration is mediated by several autocrine and paracrine factors. In addition, proteases are involved in the elimination of denatured ECM components. Following infiltration into the site of injury, monocytes transform into macrophages and clear debris from the area, release

cytokines and growth factors, such as FGF, TGF- β , PDGF, and EGF that help to initiate the formation of granulation tissue^[92]. HMGB1 also acts as an important chemotactic factor that regulates the directional migration of monocytes and neutrophils^[93]. Following injury or inflammation, HMGB1 is released into the extracellular space and triggers the secretion of TNF, IL-1 α , IL-6, and IL-8 from monocytes, macrophages and neutrophils^[94-96].

Upon interaction of HMGB1 with the advanced glycation products (RAGE), toll-like receptor (TLR) 2, TLR4, and TLR9, activate pro-inflammatory responses thereby facilitating cell migration and the release of pro-inflammatory cytokines (Figure 1)^[97-99]. In 2018, Xue *et al*^[100] showed that the HMGB1/RAGE axis mediated migration of neural stem cells (NSCs) by the formation of filopodia which was further linked to the activation of RAGE/Rac and CDC42 or the RAGE/MAPK signaling cascade.

SDF1 in upregulation of the HMGB1-SDF1-CXCR4 axis

SDF1 α , known as C-X-C motif chemokine 12 (CXCL12), is a chemotactic factor encoded by the CXCL12 gene on chromosome 10^[101]. Studies have reported the therapeutic potential of the SDF1-CXCR4 axis in tissue regeneration. SDF1 is capable of activation, mobilization, homing and retention of HSCs, MSCs and several progenitor cells^[80,102-104]. SDF1 is able to bind to CXCR4 and CXCR7. However, the SDF1-CXCR4 axis induces the homing process by regulating the cellular secretion and cell adhesion molecules, while SDF1-CXCR7 is involved in angiogenesis and tumor development^[105].

Principally, the binding of chemokine SDF1 to the chemokine receptor CXCR4 plays an important role in homeostatic regulation of leukocyte trafficking, hematopoiesis, organogenesis, cell differentiation and tissue regeneration in response to other molecules that are involved in triggering inflammation^[14,106]. The mechanism of MSCs mobilization mediated by HMGB1 is analogous to the recruitment of inflammatory cells to injured tissues for leukocyte trafficking and homing (Figure 1). As mentioned above, HMGB1 acts as a damage-associated molecular pattern which is released either from necrotic cells or by secretion from activated immune cells, hepatocytes, enterocytes, and possibly several other types of cells under distress^[107]. Stress conditions that promote HMGB1 secretion include hypoxia^[108], lethal irradiation^[109], treatment with specific antitumor drugs^[110] or through regulation of autophagy^[111]. HMGB1-induced cell migration requires both I κ B kinase (IKK)- β and IKK α -dependent nuclear factor- κ B (NF- κ B) activation. IKK β -mediated activation of NF- κ B maintains expression of RAGE, while continuous production of SDF1 is ensured by IKK α -dependent NF- κ B activation^[112,113]. Moreover, HMGB1 induces both physical and functional interactions between molecules that prevent the degradation of SDF1^[114].

In 2012, Kew *et al*^[115] proposed that the SDF1-CXCR4 axis works as a co-receptor signal for RAGE receptor-dependent HMGB1 migration responses. Furthermore, SDF1 binding to CXCR4 can also induce CXCR4-TCR heterodimerization, which in turn can enhance gene transcription, cytokine production, increased calcium ion concentrations, and could facilitate cell migration. However, it is possible that the SDF1-CXCR4 axis might have other indirect effects on the regulation of cell migration such as enhancing HMGB1 binding to RAGE, which require further investigation.

TLR and RAGE dependent or independent activation of the HMGB1-SDF1-CXCR4 axis

There is ample evidence of the capability of stem cells to regulate numerous growth factors, cytokines and chemokines. Chemokines, specifically, regulate cell locomotion and integrin function by binding to seven transmembrane domain receptors coupled to G-protein-coupled receptors (GPCR)s, which are heterotrimeric GTP-binding proteins, that are differentially expressed in various cell types^[48,107]. In addition, there is always a need to assess the consequences of the combined activity of these chemokines and other inflammatory molecules to control appropriate tissue distribution of distinct leukocyte subsets under normal and pathological conditions. One of the interesting insights in stem cell research is the effect of such paracrine factors in the HMGB1-SDF1-CXCR4 signaling pathway during tissue regeneration.

Extracellular HMGB1 can interact with different molecules to dictate their biologic effects. The role of HMGB1 as a chemokine or cytokine is determined by its oxidative state (Figure 1). The role of extracellular HMGB1 to promote cell migration was first reported in smooth muscle cells in 2010^[116]. Similar involvement was also reported in different cell types in the same year by Rauvala and Rouhiainen^[117]. Studies showed that HMGB1-induced cell migration requires the formation of a heterocomplex with

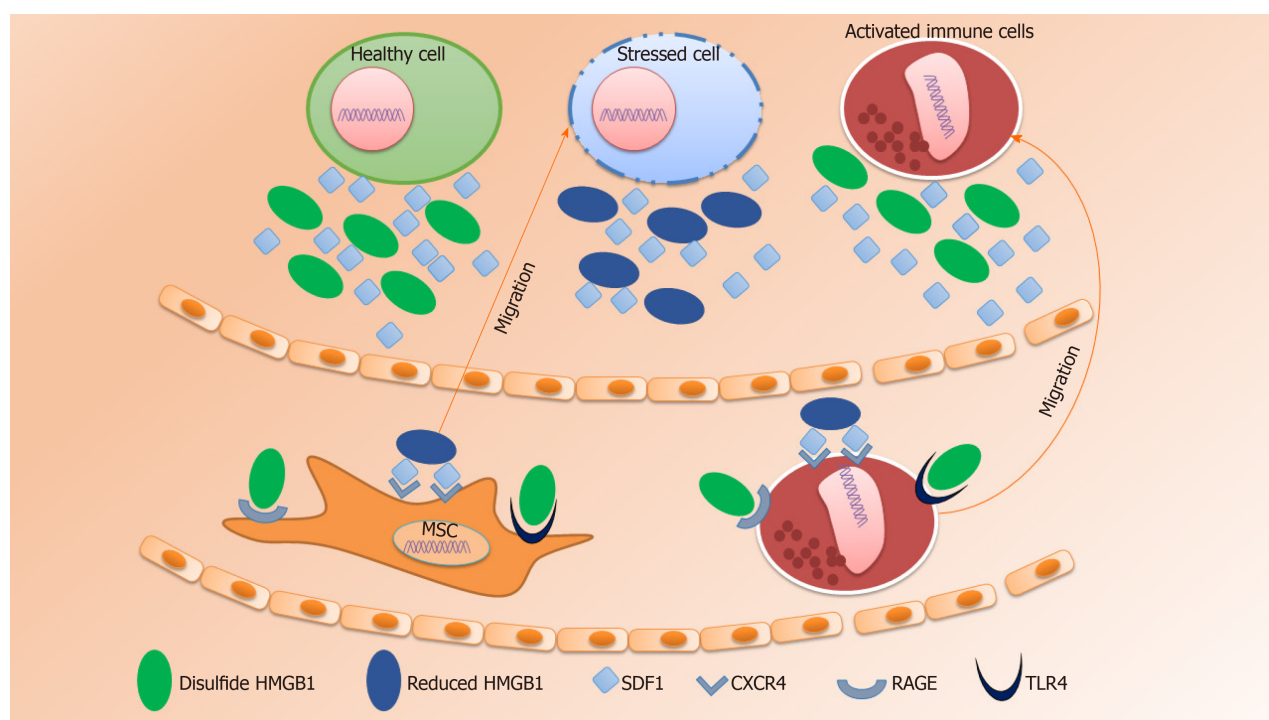


Figure 1 Schematic diagram of the dynamic HMGB1–CXCL12–SDF1 axis for accelerated tissue regeneration. Disulfide (oxidized) HMGB1 usually binds to RAGE and TLR and regulates the expression of genes with pro- or anti-inflammatory properties and partial chemotactic properties. Whereas, fully reduced HMGB1 released from necrotic or stressed cells forms a heterocomplex with SDF1 secreted from activated immune cells or from cells within the injured tissues. Later, this heterocomplex binds to the CXCR4 receptors on the cells and facilitates site-specific migration^[123-125]. MSC: Mesenchymal stem cells.

SDF1 and further binding with CXCR4, and not with RAGE, TLR2, or TLR4. Furthermore, it was also reported that HMGB1 does not affect migration by other chemokines such as CXCL8, CCL2, CCL7, CCL19, and CCL21^[14].

The bonding chemistry between SDF1 and HMGB1 was analyzed by NMR chemical shift mapping and revealed that most of the amino acids present in SDF1 have the ability to bind HMGB1 or its individual HMG boxes^[14]. Each HMGB1 molecule has two HMG boxes and thereby can attach two SDF1 molecules at a time. Interestingly, the first few N-terminal residues of the SDF1 molecule do not attach to the HMGB1 molecule and remain free. These free residues can access deep inside the CXCR4 transmembrane domain to initiate signaling cascades^[118]. As the HMGB1-SDF1 heterocomplex can present two SDF1 ligand molecules to dimers of the CXCR4 receptor, this heterocomplex would be more efficient than SDF1 alone in inducing cellular migration^[119]. Alternatively, the HMGB1-SDF1 heterocomplex may help to unlock the CXCR4 binding site to promote SDF1 binding, or help lock in SDF1 into the CXCR4 transmembrane domain by providing direct HMGB1-CXCR4 contacts.

HMGB1 induces changes in SDF1 residues that are responsible for the activation of CXCR4, the SDF1 receptor. An analysis using fluorescence resonance energy transfer (FRET) demonstrated that there are different conformational rearrangements of CXCR4 homodimers triggered by SDF1 alone or in complex with HMGB1^[14]. It has also been hypothesized that the formation of a heterocomplex between HMGB1 and SDF1 acts through CXCR4 which promotes the recruitment of monocytes to the injury site^[14]. The interaction of locally produced SDF1 and its receptor CXCR4 expressed on the surface of MSCs plays an important role in the homing of transplanted cells. The binding of SDF1 to both CXCR4 and CXCR7 is also responsible for the production of paracrine mediators, including VEGF, IGF-1, β -FGF and HGF that exert mitogenic, pro-angiogenic, anti-apoptotic, and anti-inflammatory effects^[120]. Hypoxia has been shown to enhance the expression of both SDF1 receptors, CXCR4 and CXCR7, in MSCs. Liu *et al.*^[121] demonstrated that SDF1 α is upregulated in ischemic kidneys during reduced oxygen tension. Hypoxia induces expression of CXCR4 and CXCR7 while promoting the role of both SDF1 receptors for enhanced migration, adhesion and survival of hypoxia preconditioned (HP)-MSCs and thus improves homing of systemically delivered MSCs to the ischemic kidney. In addition, in normal culture-expanded MSCs, CXCR4 expression will alleviate progressively and thus could affect its ability to migrate toward the SDF1 gradient in the ischemic tissue.

The intracellular signaling cascades have not yet been clearly demonstrated. In the case of SDF1-CXCR4 bonding, activation and coordination of focal adhesion kinase (FAK) and phosphoinositide 3-kinase (PI3K) were reported in the migration of human dental pulp stem cells^[122]. Subsequently, increased β -catenin expression by phosphorylation of protein kinase B (Akt) at ser473 that inhibits the activation of glycogen synthase kinase 3 beta (GSK3 β) was also reported. All these results indicate that the SDF1-CXCR4 axis activates the FAK/PI3K/Akt and GSK3 β / β -catenin pathways that could facilitate the migration of human dental pulp stem cells. Whereas in the HMGB1-SDF1-CXCR4 axis, elevated extracellular signal-regulated kinase (ERK) phosphorylation and Ca²⁺ release from stores were reported^[14]. Elevated ERK phosphorylation was observed in the presence of the SDF1-HMGB1 heterocomplex but not observed in the presence of SDF1 and HMGB1 alone. In the presence of HMGB1 a suboptimal SDF1 concentration was reported with a rapid increase in intracellular Ca²⁺.

CONCLUSION

Until now, the migration and retention of transplanted cells have been considered a major drawback of cell-based regenerative therapy. SDF1 and its receptor CXCR4 play an important role in maintaining homeostasis by facilitating the homing of progenitor or other adult multipotent stem cells in the BM and regulating their mobilization into peripheral tissues during injury or stress. Studies have shown the potential of the SDF1-CXCR4 axis and/or HMGB1-SDF1-CXCR4 signaling pathways in regulating the process of directional migration followed by retention which are vital for the regeneration of injured tissues or organs. In addition, these pathways could play a major role in regulating the inflammatory conditions at the site of injury. Further studies concentrating on these pathways could make cell-based regenerative therapy more efficient and fruitful.

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Mechanotransduction of stem cells for tendon repair

Hao-Nan Wang, Yong-Can Huang, Guo-Xin Ni

ORCID number: Hao-Nan Wang 0000-0003-3590-7633; Yong-Can Huang 0000-0001-8548-8233; Guo-Xin Ni 0000-0001-9181-8155.

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Hao-Nan Wang, Guo-Xin Ni, School of Sport Medicine and Rehabilitation, Beijing Sport University, Beijing 100084, China

Yong-Can Huang, Shenzhen Engineering Laboratory of Orthopaedic Regenerative Technologies, Department of Spine Surgery, Peking University Shenzhen Hospital, Shenzhen 518036, Guangdong Province, China

Yong-Can Huang, National and Local Joint Engineering Research Center of Orthopaedic Biomaterials, Peking University Shenzhen Hospital, Shenzhen 518036, Guangdong Province, China

Corresponding author: Guo-Xin Ni, PhD, Professor, School of Sport Medicine and Rehabilitation, Beijing Sport University, No. 48 Xinxu Road, Haidian District, Beijing 100084, China. niguoxin@bsu.edu.cn

Abstract

Tendon is a mechanosensitive tissue that transmits force from muscle to bone. Physiological loading contributes to maintaining the homeostasis and adaptation of tendon, but aberrant loading may lead to injury or failed repair. It is shown that stem cells respond to mechanical loading and play an essential role in both acute and chronic injuries, as well as in tendon repair. In the process of mechanotransduction, mechanical loading is detected by mechanosensors that regulate cell differentiation and proliferation *via* several signaling pathways. In order to better understand the stem-cell response to mechanical stimulation and the potential mechanism of the tendon repair process, in this review, we summarize the source and role of endogenous and exogenous stem cells active in tendon repair, describe the mechanical response of stem cells, and finally, highlight the mechanotransduction process and underlying signaling pathways.

Key Words: Stem cells; Mechanical loading; Tendon repair; Mechanotransduction

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Core Tip: Stem cells and mechanical loading are crucial to tendon injuries. In this review, we summarize the sources and roles of endogenous and exogenous stem cells for tendon repair, describe the mechanical response of stem cells, and finally highlight the mechanotransduction process and underlying signaling pathways. The deeper understanding of interactions between stem cells and mechanical loading offers great

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potential for the development of new therapeutic strategies for tendon repair.

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INTRODUCTION

Tendon is a unique form of connective tissue that links muscle to bone. It is the anatomical structure that transmits muscle-contraction force to the skeleton in order to maintain posture or produce motion. Tendons are composed of triple-helical collagen I molecules assembled into fibrils that, in turn, form fibers, fascicles, and ultimately, tendon^[1-3]. This mechanosensitive tissue has specific mechanical properties that enable it to respond and adapt to the loading transmitted by muscles; the collagen fibrils, considered to be the fundamental force-transmitting unit of the tendon, are densely arranged within the extracellular matrix (ECM), oriented parallel to the bone-muscle axis. A multitude of ECM molecules, including collagens, elastin, proteoglycans, and glycoproteins, are involved in tendon-specific collagen I. Tenocytes, the main type of cell located inside the collagen fibers, produce collagen I and ECM molecules^[2]. Additionally, tendon stem/progenitor cells (TSPCs), also commonly termed as tendon-derived stem cells (TDSCs) or tendon stem cells (TSCs), located in the fascicular matrix, are responsible for replenishing tendon cells through differentiation and proliferation^[4]. Under certain conditions, such as aberrant loading, TSPCs have multidifferentiation potential, namely, TSPCs can differentiate into tenocytes, chondrocytes, osteocytes, and adipocytes^[4,5].

Tendon injuries range from chronic to acute, with partial or complete tendon rupture^[2,6]. Chronic tendon injury mainly refers to tendinopathy, which is the most common tendon overuse injury and is characterized by pain and impaired function and performance^[7]. The pathogenesis of tendinopathy is far from well understood and has been interchangeably defined as a degenerative condition or a failure of the healing process. Moreover, increased expression of inflammatory cytokines, such as COX-2 and interleukin (IL)-6, has been observed in overuse tendinopathy^[8]; currently, the production of inflammatory cytokines is not considered to be a classic inflammatory response, but rather, the production expressed by resident tenocytes under overload^[9,10]. Histologically, disorganization of collagen, increased noncollagenous ECM, hypercellularity, and neovascularization can be seen^[11,12]. The exact relationship between tendinopathy and tendon rupture remains unknown, but it has been reported that tendinopathy increases the risk of tendon rupture^[13]. Acute partial or complete tendon rupture interrupts tendon continuity, leading to bleeding, clotting, and the release of PDGF, TGF- β , ATP, and ADP from platelets and of epinephrine and norepinephrine from blood vessels at the wound site^[9], resulting in a decrease or even loss of function and, potentially, in the loss of mobility. After injury, tendon undergoes a natural healing process involving successive steps— inflammation and formation of new cells, as well as ECM formation and remodeling^[14]. Currently, the treatment for tendon injuries differs from that for other chronic and acute injuries. Conservative treatments include therapeutic exercise^[15,16], shockwave^[17], and injection therapy^[18], which are helpful for reducing pain and improving function in tendinopathy, but pain during treatment, slow recovery, and risk of failure remain. A surgical procedure is usually the first choice for total tendon rupture, but patients may still face postoperative issues, such as proliferation of scar tissue, decreased mobility, and risk of second rupture.

To this end, stem-cell-based therapy has been introduced to clinical practice, and it may have broader future applications with the advantages of offering regeneration and repair. TSPCs, which tend to differentiate into tenocytes and are able to replace the loss of normal tenocytes, have been found to reside in tendon tissue. Thus, they have great potential to become the ideal cell source for stem-cell-based therapy^[19,20].

Mechanical loading plays a crucial role in the biology of TSPCs^[21]. In particular, proper loading aids in promoting the proliferation and tenogenic differentiation of TSPCs, which is beneficial for tendon repair, whereas aberrant loading might lead to nontenocyte differentiation, which could hinder tendon healing. In order to further

understand the response and mechanism of stem cells to mechanical loading, related to tendon injury and repair, this paper summarizes the sources of stem cells and describes the mechanical response of TSPCs for tendon repair, and it further discusses the underlying signaling pathways of TSPCs responding to mechanical stimuli.

ENDOGENOUS AND EXOGENOUS STEM CELLS/PROGENITORS FOR TENDON REPAIR

Several types of endogenous and exogenous stem cells have proven effective for tendon repair. TSPCs are fibroblast-like cells^[22], which have been identified in mice, rabbits, and humans, with typical stem-cell makers^[4,22,23]. Nevertheless, the exact source location of TSPCs remains unclear. TSPCs have been isolated and differentiated from tendon^[4], peritenon^[24], and perivascular sources^[25,26]. A recent study reported that a PDGFRA⁺ cell population expressing tubulin polymerization-promoting protein family member 3 (TPPP3⁺), which is located in peritenon, has stem-cell characteristics, such that it may generate new tenocytes and self-renew upon injury^[27]. TSPCs share some common markers with tenocytes, such as collagen I, collagen III, tenascin C, and tenomodulin (TNMD), but they express still more markers, like Oct-4, SSEA-1/4, and nucleostemin^[4,5]. Both TSPCs isolated from the tendon and peritenon regions of mouse Achilles tendons have the Sca1, CD90, and CD44 markers^[26], but progenitor cells from the tendon and peritenon regions can be distinguished with genes such as *Scx*, *Mkx*, *Thbs4*, and *Wnt10a*^[24]. Moreover, perivascular stem cells isolated and cultured from human supraspinatus tendon biopsies express both tendon-like and stem/precursor-cell-like markers, including musashi-1, nestin, prominin-1/CD133, CD29, CD44, *Scx*, and *Smad8*^[25]. TSPCs from the tendon proper lack CD133 markers, however, which may help distinguish TSPCs from tendon proper and perivascular sources. TSPCs have shown a high capacity for proliferation and multipotential differentiation into tenocytes, osteoblasts, chondrocytes, and adipocytes^[4,28]. Although TSPCs show multipotential differentiation, they also show spontaneous tenogenic differentiation, which can be beneficial for tendon repair^[20]. In a tendon-window-wound study, TSPCs participated in tendon repair by proliferation and activation of tenogenesis^[29]. The therapeutic effect of TSPCs has also been confirmed by using animal models. It has been reported that TSPCs promote tendon repair by improving cell and collagen-fiber alignment, collagen birefringence, and Young's modulus typical of tendon, as well as by increasing ultimate stress capacity^[30]. Similarly, ultimate failure load and the expression of collagen I and collagen III in the ruptured Achilles tendon have been much improved by TSPC transplantation^[31]. Nevertheless, the abnormal differentiation of TSPCs into nontendon cells has a negative effect on tendon development, homeostasis, and repair. For instance, tendon progenitor cells of injured tendon have strong chondrogenic potential, which may cause endochondral ossification as a result of ectopic mineralization^[32]. To date, very scant clinical research has been performed using TSPCs for tendon-related diseases.

As shown in Table 1, stem cells/progenitors derived from other tissues, such as bone marrow-derived mesenchymal stem cell (BMSCs) and adipose-derived stem cells (ASCs), are much easier to acquire than TSPCs^[33,34], and they have been proven efficient for tendon repair^[14,19]. BMSCs are spindle-shaped^[35] and have the potential of tenogenic differentiation^[36,37] and high proliferation^[4,38]. Several mechanisms may contribute to tendon repair with exogenic BMSCs. First, BMSCs can differentiate into certain new cells (tenocytes) to replace lost normal cells^[19,39]; second, BMSCs can secrete various cytokines and growth factors to promote the proliferation of cells in injured tissue^[40]; and third, BMSCs can increase the deposition of collagenous proteins^[41]. BMSC-based therapy has been found to improve histological and biomechanical properties and to increase the expression of collagen in animal injury^[42,43]. But the application of BMSCs may also carry the risk of nontendon differentiation and of forming ectopic bone during tendon repair^[44]. The clinical application of BMSCs was started very early, and four clinical trials (NCT03688308, NCT01788683, NCT02484950, and NCT01687777) using BMSCs for rotator-cuff repair are at the stage of recruiting, and the results have not yet been released. ASCs are spindle-shaped^[45] with stem-cell marks^[23,35,46]; these cells commonly being isolated from subcutaneous adipose tissue^[34] and liposuction aspirates^[47], have shown the multipotential ability of differentiation including tenogenic cells^[48-50] and high proliferation^[23,38,51]. ASC transplantation could enhance the secretion of collagen I and tenascin-C during healing and improve the mechanical strength of tendon^[52,53], as well as improve the pathological changes of tendinopathy and the normalization of collagen ratios within the affected tendon^[54].

Table 1 Difference among tendon stem/progenitor cells, bone marrow-derived mesenchymal stem cells, and adipose-derived stem cells for tendon repair

| | TSPCs | BM-MSCs | ASCs |
|--|---|---|--|
| Morphology | Fibroblast-like shape ^[22] | Spindle-shaped ^[35] | Spindle-shaped ^[45] |
| Phenotypes | Positive: CD13, C29, CD44, CD54, CD73, CD90, CD105, CD146 and CD166 Negative: CD2, CD3, CD11b, CD14, CD15, CD16, CD18, CD19, CD31, CD34, CD45, CD56, CD71, CD106, CD117, CD123, and CD235a ^[4,22,23] | Positive: CD13, CD29, CD44, CD73, CD90, and CD105 Negative: CD14, CD19, CD34, CD45 ^[35,37] | Positive: CD13, C29, CD44, CD49d, CD54, CD73, CD90, CD105, and CD166 Negative: CD14, CD19, CD31, CD34, CD45 and CD71 ^[23,35,46] |
| Proliferation | TSPCs = BM-MSCs ^[4] ; TSPCs ≤ ASCs ^[23] | BM-MSCs = TSPCs ^[4] ; BM-MSCs < ASCs ^[38] | ASCs > BM-MSCs ^[38] ; ASCs ≥ TSPCs ^[23] |
| Tenogenic differentiation | Spontaneous differentiation ^[20] , or promoted by growth factors ^[120] and mechanical loading ^[75] | Induced by growth factors ^[36] and mechanical loading ^[39] | Induced by growth factor supplements ^[48,49] and extracorporeal shockwave ^[50] |
| Evidence for tendon repair <i>in vitro</i> | Tenogenic differentiation ^[20,75,120] and high proliferation potential ^[4,28] | Tenogenic differentiation and high proliferation potential ^[4] ; enhanced secretion of bioactive factors ^[40] and the deposition of ECM ^[41] | Tenogenic differentiation and high proliferation rate ^[51] |
| Evidence for tendon repair <i>in vivo</i> | High proliferation and activation of tenogenesis ^[29] ; improved collagen alignment and biomechanical properties ^[30,31] | Improved histological and biomechanical properties; increased expression of collagen ^[42,43] | Modulation of microenvironment ^[55] ; enhancing the secretion of collagen and mechanical strength of tendon ^[52,53] |
| Evidence for tendon repair in clinics | None | Four registered trials, but the results are not available | Reduction of pain, tendon defect areas post intervention ^[56] |
| Advantages | Spontaneous tenogenic differentiation ^[20] ; higher proliferation and therapeutic effectiveness ^[31] | Easier acquirement ^[33] ; enhanced secretion of bioactive factors ^[40] ; increased the deposition of collagenous proteins ^[41] | Easier acquirement ^[34] ; inhibition of osteogenic differentiation ^[55] ; confirmed clinical outcome ^[56] |
| Limitations | Limited number obtained from isolation ^[63] | High potential of osteogenic differentiation ^[44] ; lower therapeutic effectiveness than TSPCs ^[31] | Risk of fibrotic tissue formation, scarring ^[57] , and forming adipocytes ^[58] |

TSPCs: Tendon stem/progenitor cells; BMSCs: Bone marrow-derived mesenchymal stem cells; ASCs: Adipose-derived stem cells; ECM: Extracellular matrix.

Recently, a study indicated that ASCs improved tendon repair in tendinopathy by inhibiting inflammation and inducing neovascularization at the early stage of tendon healing, and ASCs are also effective for the inhibition of ectopic ossification *in vivo*^[55]. Additionally, the clinical safety and efficacy of ASCs therapy have been reported. After allogeneic ASC treatment, patients with lateral elbow epicondylitis self-reported outcomes with reduced pain and improved function, without safety issues, as well as demonstrated decreased tendon defect areas in ultrasound images at 52 wk post-injection^[56]. However, the application of ASCs may give rise to fibrotic tissue formation and scarring^[57] as well as forming adipocytes^[58] during tendon repair. In addition, induced pluripotent stem cells (iPSCs) can be reprogrammed from adult somatic cells. It has been found that human iPSC-derived neural crest stem cells (iPSC-NCSCs) can differentiate into mesenchymal-lineage tenocytes, which accelerate the process of tendon repair^[59]. In a rat patellar-tendon window-defect trial, iPSC-NCSCs promoted healing by improving matrix synthesis and mechanical properties and by increasing fetal tendon-related matrix proteins, stem-cell recruitment factors, and the tenogenic

differentiation factor^[60].

Compared with exogenic stem cells/progenitors, TSPCs possess higher regenerative potential for tendon repair. For instance, during treatment of rat Achilles tendon injury, TSPCs have a greater positive effect on morphological and histological alteration and biomechanical strength when compared to BMSC transplantation^[31]. This distinction may be because TSPCs proliferate more rapidly and have a greater capacity for colony formation^[41,61,62]; additionally, TSPCs undergo spontaneous tenogenic differentiation, whereas BMSCs do not^[20]. It has been demonstrated that mouse TSPCs express higher levels of tenogenic markers, such as Scx, Comp, Sox9, and Runx2, than mouse BMSCs; similarly, human TSPCs express more TNMD than BMSCs^[4]. Thus, TSPCs more rapidly differentiate to functional tenocytes. Moreover, the expression of collagen I and collagen III is higher in TSPCs, which results in greater biomechanical strength at the early stage of repair^[31]. However, the limited number of resident TSPCs hinders the large-scale clinical application^[63]. Hence, both endogenous and exogenous stem cells have therapeutic potential. According to current evidence, TSPCs possess some advantages for tendon repair, but the efficacy of endogenic and exogenic stem cells requires further investigation.

MECHANICAL RESPONSE OF STEM CELLS/PROGENITORS FOR TENDON REPAIR

A number of factors influence the homeostasis of tendon, in which mechanical loading plays a critical role^[64]. Under normal or physiological loading, the magnitude of loading is much less than the ultimate tensile strength (UTS). Typically, tendon could return to its original length when the strain is less than 4% of elongation; but tendon will have macroscopic tearing and eventually rupture when the strain is beyond 8%-10% of elongation^[65]. Researchers usually use 4% cyclic uniaxial stretching to mimic this loading condition *in vitro*, and to moderate treadmill running model of rats (13 m/min, 15 min/d, and 5 d/wk in the first week; 13 m/min, 50 min/d, and 5 d/wk for another 3 wk) *in vivo*^[21]. In normal or physiological loading, tendon can maintain homeostasis and respond to loading through cellular anabolic adaptation^[3,21]. By contrast, abnormal loading may be different from normal mechanical loading in magnitude, frequency, duration, and/or direction; typically, abnormal loading of tendon can be unload, overload, or high repetitive low load^[66]. Compared with explants tensioned with constant 4% strain, nontensioned rabbit patellar tendon decreased linear stiffness, elongation to failure, and maximum failure force after 20 h^[67]; undergoing cyclic loading at approximately 35% of the UTS led to tendon rupture in 15 min^[68]; also, cyclic loading under 5% of UTS (around 1% strain) resulted in rupture within 15 h^[69]. *In vitro*, researchers usually use 8% cyclic uniaxial stretching to mimic the overloading condition, as well as intensive treadmill running (13 m/min, 15 min/d, and 5 d/wk in the first week; 13 m/min, 3 h/d, 4 h/d, and 5 h/d in the second, third, and fourth weeks for 5 d)^[21]. Abnormal loading can lead to failed repair or pathological changes by causing anabolic changes in tendon^[14,21,70]. After high-intensity repetitive-exercise-induced injury, the expression level of IL-1 β increases in mouse tendon^[71]. Moreover, a greater production of inflammatory mediators induced by IL-1 β , including COX-2, MMP-1, and PGE-2, has been reported for human tendon fibroblasts with excessive stretch loading than with moderate stretching or without stretch loading *in vitro*^[72]. Similarly, the level of PGE-2 significantly increases in mouse patellar and Achilles tendons after rigorous treadmill running compared to caged control groups *in vivo*^[73], indicating that overloading tendon may lead to a higher production of PGE-2. These inflammatory mediators may, in turn, promote the degradation of tendon, such as through neutrophil infiltration and decreased collagen production, thereby negatively impacting the repair of injured tendon.

TSPCs undergo similar mechanical loading as tenocytes. Mechanical loading, no matter what level, can increase TSC proliferation, which is indeed necessary for healing injured tendon^[21]. Patellar and Achilles TSCs isolated from mice after moderate treadmill running have nearly double proliferation rates compared to the TSCs isolated from less active mice *in vitro*^[21]; also, compared to inactive mice, cellular production of collagen increases by 70% and 200% for patellar and Achilles TSCs, respectively, for mice completing moderate treadmill running *in vivo*^[74]. Currently, few studies have found that the magnitude of stretching could lead to different cell fate. In particular, a higher magnitude of stretching may cause aberrant differentiation compared to a lower magnitude of stretching *in vitro*. It was reported that 4% stretching promoted the differentiation of TSCs into tenocytes with increased gene

expression of collagen I; 8% stretching, however, promoted the differentiation of TSCs into nontenocytes, including adipocytes, chondrocytes, and osteocytes, aside from differentiation into tenocytes, as evidenced by higher expression levels of genes such as *PPAR γ* , *collagen II*, *Sox-9*, and *Runx2* *in vitro*^[75]. Similarly, increased differentiation into adipocytes, chondrocytes, osteocytes, and tenocytes with high gene expression of *LPL*, *Sox-9*, *Runx2*, *Osterix*, *collagen I*, and *TNMD* was found in mice after intensive treadmill running *in vivo*^[76]. Also, mechanical loading can influence both TSC proliferation and differentiation due to an inflammatory mediator. In response to rigorous treadmill running, mouse patellar and Achilles tendons increase the production of PGE-2, which can decrease cell proliferation and induce both adipogenesis and osteogenesis of TSCs, as well as promote the production of fatty and calcified tissues within tendon^[73]. These findings are consistent with the clinical understanding that complete rest without loading will decrease tendon strength and induce pathologic change in tendon, such that total rest is relatively contraindicated for tendinopathy^[77,78]. In short, mechanical loading is necessary for TSC proliferation and collagen production, but excessive loading may cause abnormal differentiation of TSCs into nontenocytes, leading to tendon injury or failed tendon repair.

TSPCs would not be able to respond to mechanical loading without mechanotransduction, which converts mechanical signals from the environment into biochemical signals^[79] (Figure 1). As a mechanical signal is transmitted to the microenvironment, it causes the physical perturbation of cells and deformation of the extracellular matrix^[80,81]. Both TSPCs and tenocytes reside in the pericellular matrix, such that TSPCs experience a force similar to tenocytes. In tendon, tissue probably undergoes various types of force, including tensile loading, shear, and even compression force^[81,82]. As tendon has the function of transmitting force from muscle to bone, tendon is exposed to high-tensile force, whereas the tendon-bone junction area commonly experiences compression force^[83]. Further, the midportion of a tendon can potentially be exposed to both shear and compression forces due to the different forces to which the posterior and anterior areas of the tendon are exposed^[84]. It has been reported that cyclic tensile loading on tendon may cause interstitial fluid flow, leading to shear force and perhaps hydrostatic force.

Moreover, effector-cell mechanosensors detect mechanical signals and induce an intercellular response *via* various downstream signaling pathways to regulate stem-cell differentiation and proliferation^[85,86]. Typically, effector cells can sense mechanical signaling from groups of transmembrane mechanosensitive proteins, namely, mechanosensors such as ion channels, integrins, G-protein coupled receptors (GPCRs), growth factor receptor (GFR), and primary cilium^[85]. Ion channels play an essential role in cellular mechanotransduction. Cystic fibrosis transmembrane conductance regulator (CFTR) is a stretch-mediated activation channel that aids in passing chloride and water in and out of cells^[87,88]. Recently, a study reported that CFTR regulates tenogenic differentiation through inhibiting the Wnt/ β -catenin/ERK1/2 signaling pathway in TSPCs^[89]. Also, Ca^{2+} is a greatly powerful second messenger regulating cell migration and influencing the differentiation of stem cells^[90,91]. Several studies have shown that transient receptor potential melastatin 7 (TRPM7) works as a calcium channel conducting calcium influx^[90,92], which, in turn, activates transcription factor NFATc1, which then induces osteogenesis in mesenchymal stem cells (MSCs)^[93,94]. Interestingly, integrins become involved in the intracellular concentration of calcium by interaction with ion channels^[95]. In addition to interaction with ion channels, accumulating evidence indicates that integrin systems can detect mechanical signals and then transduce them to nuclear signaling^[96,97]. Once integrin receptors bind their ligands in the ECM, they move laterally in the plane of the membrane to form focal adhesions, which play a central role in cell motility and cytoskeletal dynamics, as well as in regulating cell proliferation, differentiation, and gene expression^[98]. GPCRs have the ability to sense mechanical loading and regulate molecular mechanisms downstream *via* binding protein ligand. For instance, Wnt binds frizzled receptors, which span the plasma membrane and constitute a distinct family of GPCRs that regulate osteogenic differentiation in MSCs^[99]. Studies have found that, when a stretching force is applied to TSPCs, Wnt5a activates a co-receptor, receptor tyrosine kinase-like orphan receptor 2 (ROR2), and regulates Wnt5a/JNK and Wnt5a/RhoA signaling pathways downstream for osteogenic differentiation in TSPCs^[100,101]. Additionally, growth factors bind their GFRs and regulate signaling pathways downstream—in TSPCs, GFRs mediate bone morphogenetic protein (BMP) signaling pathways involved in biomechanical loading-induced differentiation^[102,103]. Further, primary cilium, an extraordinary organelle that exists on nearly all somatic cells, also plays a role in the detection of mechanical signaling. Currently, research specifically focused on the primary cilium of TSPCs is rare, but it can be hypothesized that the

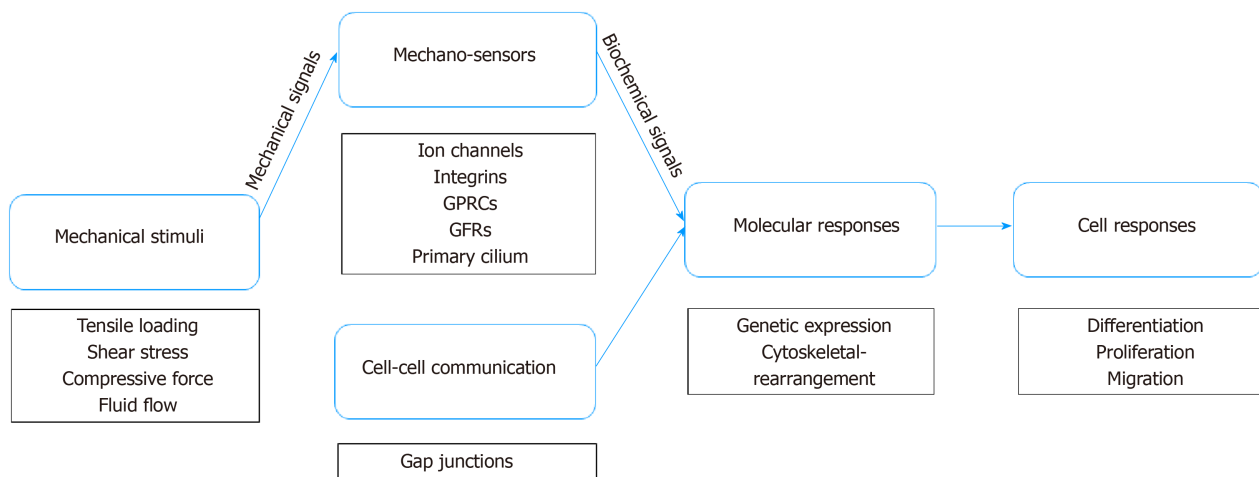


Figure 1 Process of mechanotransduction in stem cells for tendon repair. This figure describes various ways by which mechanical loading stimulates mechanosensors to emit mechanical signals that convert into biochemical signals, which, in turn, activate the rearrangement of cytoskeleton and activate genetic expression via various signaling pathways. Cell-cell communication transduces signals from one cell to another cell via gap junctions. GPRC: G protein-coupled receptor; GFR: Growth factor receptor.

principle might be similar to tenocytes and MSCs. In tenocytes, the length of primary cilium immediately and significantly increases in a stress-deprived environment and can be reversed by cyclic tensile loading^[104]. In MSCs, frizzled receptors are thought to localize cilium membranes, such that primary cilium is involved in controlling differentiation by tuning Wnt signaling pathways in MSCs^[105,106].

In addition, even if a cell is not to receive mechanical stimulation, the cell can still respond via a process known as cell-cell communication, whereby it can communicate with a distant cell receiving mechanical stimulation^[107,108]. To date, limited research has investigated the mechanism of cell-cell communication in TSPCs. Because TSPCs are stem cells/progenitors of tendon, however, they may have similar communication characteristics as tenocytes and MSCs. Connexins form gap junctions between the cytoplasm of adjacent cells allow for the direct intercellular exchange of ions and molecules^[109]. Gap junctions are immunohistochemically detected among tenocytes, and connexins 32 and 43 form a three-dimensional network to respond to mechanical stimulation together^[110]—connexin 32 has a stimulatory function, whereas connexin 43 is inhibitory^[109]. Additionally, cell-cell communication can be altered to some degree by stretching; specifically, communication increases under low-level stretching (4%) and decreases under high-level stretching (8%)^[111]. Moreover, a recent study has shown that connexin 43 plays an impactful role in protecting MSCs from premature senescence, which results in the failure to properly differentiate *in vitro*^[112]. Connexin 43 may contribute to early tenogenesis in MSCs, but the mechanism in mechanotransduction is still not clear^[113].

UNDERLYING SIGNALING PATHWAYS OF STEM CELLS/PROGENITORS RESPONDING TO MECHANICAL STIMULI

As the important role of mechanotransduction in TSPCs responding to mechanical loading has been realized, it has been demonstrated that various underlying signaling pathways transmit biomechanical signals to nuclei (Figure 2). With the noncanonical Wnts signaling pathway, Wnts binds co-receptor ROR2 and regulates signaling pathways downstream, in turn influencing osteogenic differentiation in TSPCs^[114]. Mechanical tension promotes osteogenic differentiation of rat TSPCs via the Wnt5a/Wnt5b/JNK signaling pathway. Under 8% elongation uniaxial mechanical tension (UMT) stimulation, TSPCs exhibit increased protein levels of Wnt5a, Wnt5b, and P-JNK, as well as increased cytoskeletal rearrangement^[100]. The mRNA expression of osteogenic genes, such as *Runx2*, *Dlx5*, *Alpl*, and *collagen 1a1*, also increases^[100]. Additionally, UMT induces the appearance of osteogenic differentiation in rat TSCs through the Wnt5a/RhoA signaling pathway. RhoA and its effector protein, ROCK, play an important role in osteogenetic differentiation of MSCs^[115], as they show increased mRNA expression of the osteogenic genes *Runx2*, *Alpl*, and *collagen 1a1*,

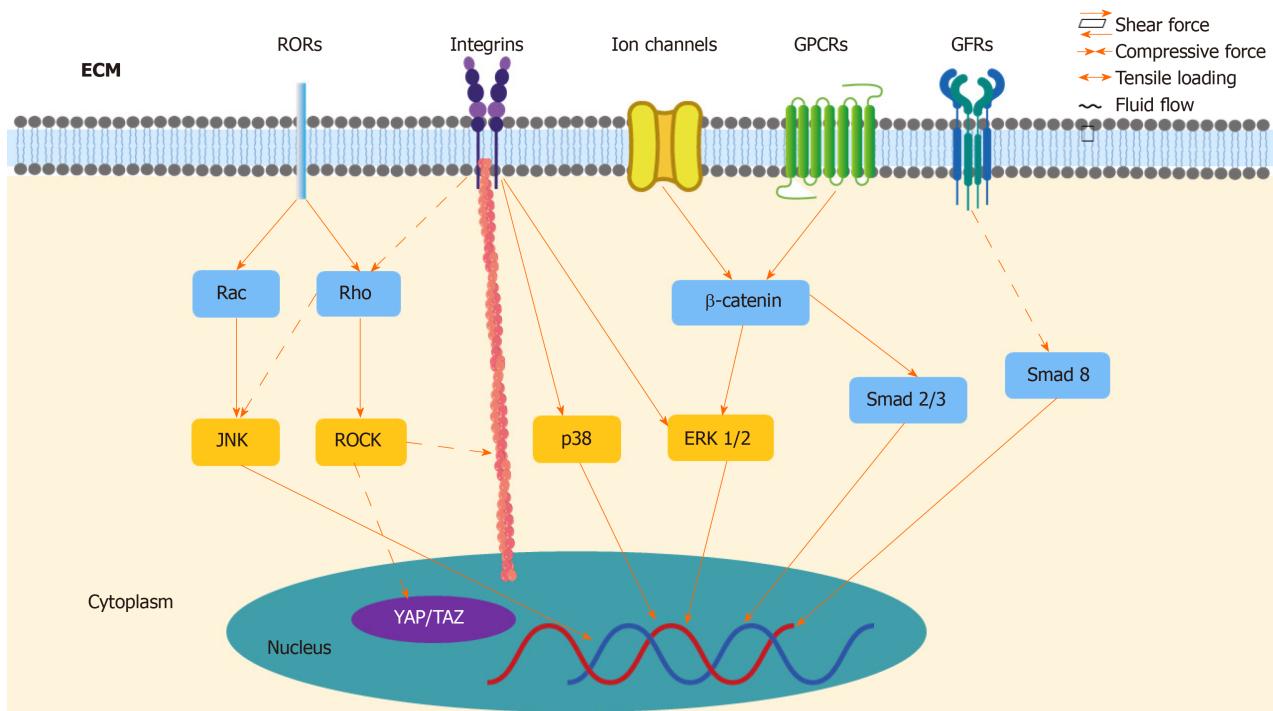


Figure 2 Signaling pathways responding to mechanical stimuli applied to a cell. This figure describes how mechanosensors, such as G-protein coupled receptors, integrins, ion channels, and growth factor receptor, sense mechanical loading and activate a series of signaling pathways downstream, in turn promoting gene expression and/or cytoskeleton rearrangement in tendon repair. ECM: Extracellular matrix; ROR: Receptor tyrosine kinase-like orphan receptor; GPCRs: G-protein coupled receptors; GFRs: Growth factor receptor; JNK: c-Jun N-terminal kinase; ROCK: Rho-associated protein kinase; ERK: Extracellular signal-regulated kinase; YAP: Yes-associated protein; TAZ: PDZ-binding motif.

along with ALP activity, as well as ALP cytochemical staining and Runx2 protein expression after 2% elongation mechanical tension^[101]. Only the expression of Wnt5a increased under UMT, not the other noncanonical Wnts, such as Wnt5b, Wnt7a, and Wnt11, but it can be inferred that the difference in Wnt protein levels might be due to varying magnitude of loading^[101]. To date, the interaction between Wnt5a/JNK and Wnt5a/RhoA remains to be further investigated, insofar as whether Wnt5a/JNK regulates cells independent of or depending on the RhoA pathway^[116].

In addition to noncanonical Wnts signaling pathways, the Wnt/ β -catenin signaling pathway also contributes to differentiation in TSPCs. Wnt commonly binds frizzled receptors and downregulates β -catenin in the canonical Wnt/ β -catenin signaling pathway^[114]. In a rat tendinopathy model and a human tendon with tendinopathy, increased expression of Wnt3 and β -catenin has been observed. Wnt3a can increase ALP activity, calcium nodule formation, and the expression of osteogenic markers in TSPCs^[117]. Similarly, strain loading promotes osteogenic differentiation and inhibits adipogenesis *via* β -catenin^[99]. A recent study reported that CFTR, a stretch-mediated activation channel, can regulate TSPCs during tenogenic differentiation under mechanical stretching. Mice with dysfunctional CFTR showed reduced levels of tendon markers, including *Scx*, *TNMD*, collagen Ia1 chain, and decorin, as well as abnormally active Wnt/ β -catenin signaling, which, in turn, further activated the ERK1/2 signaling pathway^[89]. Inhibiting ERK1/2 signaling can promote tenogenic differentiation in TSPCs, both *in vitro* and *in vivo*, however, and increase matrix formation and mechanical properties, which is helpful in the tendon healing process^[89]. Moreover, activation of Wnt/ β -catenin signaling suppressed the expression of tenogenic genes *Scx*, *Mkx*, and *Tnmd* in TSPCs by reducing the amount of Smad2 and Smad3, which are intracellular mediators for TGF- β signaling^[118].

In rat TSPCs, both 4% and 8% stretching can increase the amount of BMP-2, and 4% stretching upregulates BMP-2 genetic expression, when compared to unstretching, which does not obviously promote the expression of BMP-2^[119]. Studies have proven that BMP-2 causes aberrant proliferation and differentiation in TSPCs, in other words, the addition of BMP-2 to human TSPC cultures reduces the proliferation of cells and promotes osteogenic differentiation *in vitro*^[120]. BMP-2 promotes osteogenic differentiation through ALP cytochemical staining, ALP activity, and calcium nodule formation. Additionally, BMP-2 inhibits tenogenic marker expression, but promotes osteogenic, adipogenic, and chondrogenic differentiation in TSPCs^[103]. After BMP-2

stimulation, TSPCs show increased glycosaminoglycan (GAG) production and mRNA expression of aggrecan (*Acan*), along with decreased mRNA expression of decorin (*Dcn*), biglycan (*Bgn*), and fibromodulin (*Fmod*)^[103]. To date, it remains to be determined whether the BMP-2 downstream molecular signaling pathways induce differentiation of TSPCs. Smad8 might play a role, as activated Smad8 promotes MSC tenogenic differentiation *via* inhibiting the BMP-2 induced osteogenic pathway^[121].

ECM deformation initiates integrin signaling at focal adhesion sites where the ECM binds integrin, which activates downstream proteins, such as ERK1/2, p38, and JNK^[98]. Higher matrix stiffness increases TDSC proliferation and forms more stress fibers, as well as inhibits the differentiation of TDSCs into tenogenic, chondrogenic, and osteogenic lineages *via* focal adhesion kinase (FAK) or ERK1/2 signaling pathways^[122]. Similarly, another study found that ERK/MAPK signaling pathways increase the tenogenic expression level in mouse MSCs^[123]. In addition to ERK, p38 kinases also affect integrin-induced signaling pathways in TSPCs, as it was reported that 8% mechanical stretching caused an upregulated response in ERK1/2 and p38 kinases, as well as altered expression of matrix proteins, integrins, and matrix metalloproteinases^[124]. Interestingly, mechanical loading might precisely regulate ERK signaling, as the level of ERK1/2 phosphorylation induced by cyclic uniaxial mechanical stretching is related to stretching time *in vitro*^[125]. Furthermore, RhoA/ROCK and the cytoskeleton may also contribute to integrin signaling. This demonstrates that FAK has the ability to regulate mechanical stretch-induced tenogenic differentiation by mediating RhoA/ROCK downstream and interacting with the cytoskeleton in human MSCs^[126].

Recent studies have identified two important transcriptional coactivators – Yes-associated protein (YAP) and transcriptional coactivator with PDZ-binding motif (TAZ) in the Hippo signaling pathway^[127]. Mechanical loading has the ability to influence YAP/TAZ activities through stretching, geometry, and substrate rigidity, which, in turn, regulates stem-cell fate and behavior^[128]. In human MSCs, YAP/TAZ knockdown promotes adipogenic differentiation on rigid substrates, which commonly happens on soft substrates^[127]. Also, shear stress can induce human MSC osteogenic and fibrochondrogenic differentiation and promote TAZ nuclear translocation *via* the RhoA/ROCK signaling pathway and YAP/TAZ^[129,130]. In addition, another study suggests that YAP/TAZ may be a downstream effector of the noncanonical Wnts signaling pathway, which plays a crucial role in TSPC differentiation. Thus, YAP/TAZ might mediate gene expression, osteogenesis, and cell migration of TSPCs^[131]. To date, limited research has been conducted into the deep mechanism of Hippo and YAP/TAZ signaling pathways in tenocytes and TSPCs, but the potential value of this area is certain. In short, several signaling pathways have been demonstrated to participate in the mechanotransduction of TSPCs, such as noncanonical Wnts, Wnt/ β -catenin, BMP-2, and integrin, as well as YAP/TAZ.

CONCLUSION

This review summarizes the sources and roles of the endogenous and exogenous stem cells that can be used for tendon repair, describes the mechanical response of stem cells in tendon repair, and finally, highlights the mechanotransduction process and its underlying signaling pathways. Mechanical loading plays a crucial role in both tendon injury and repair. When mechanical loading is applied, the stimulation is detected by mechanosensors, such as ion channels, integrin, GPCRs, GFR, and primary cilium, which then transmute the mechanical signal into a biological signal, and in turn, regulate various downstream signaling pathways. Suitable mechanical loading is helpful for promoting both the proliferation and differentiation of TSPCs, which are crucial for tendon repair. These findings promise a bright future with new therapeutic strategies for tendon repair. Further studies are necessary to identify mechanosensors and deeply understand the signaling pathways of stem cells.

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Senescent mesenchymal stem/stromal cells and restoring their cellular functions

Qing-Shu Meng, Jing Liu, Lu Wei, Hui-Min Fan, Xiao-Hui Zhou, Xiao-Ting Liang

ORCID number: Qing-Shu Meng 0000-0002-9879-3138; Jing Liu 0000-0003-2126-0146; Lu Wei 0000-0002-7976-5203; Hui-Min Fan 0000-0002-9776-3180; Xiao-Hui Zhou 0000-0002-2965-6914; Xiao-Ting Liang 0000-0003-3262-1858.

Author contributions: Meng QS and Liu J contributed equally to this work; Liang XT and Meng QS defined the study topic; Liu J, Wei L, and Fan HM collected the references; Meng QS wrote the paper; Liu J made the tables; Liang XT and Zhou XH revised the manuscript and resolved all disagreements in discussion with Meng QS and Liu J.

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Qing-Shu Meng, Jing Liu, Lu Wei, Hui-Min Fan, Xiao-Hui Zhou, Xiao-Ting Liang, Shanghai Heart Failure Research Center, Shanghai East Hospital, Tongji University School of Medicine, Shanghai 200120, China

Qing-Shu Meng, Jing Liu, Lu Wei, Hui-Min Fan, Xiao-Hui Zhou, Xiao-Ting Liang, Research Center for Translational Medicine, Shanghai East Hospital, Tongji University School of Medicine, Shanghai 200120, China

Qing-Shu Meng, Jing Liu, Lu Wei, Hui-Min Fan, Xiao-Hui Zhou, Xiao-Ting Liang, Institute of Integrated Traditional Chinese and Western Medicine for Cardiovascular Chronic Diseases, Tongji University School of Medicine, Shanghai 200120, China

Hui-Min Fan, Department of Heart Failure, Shanghai East Hospital, Tongji University School of Medicine, Shanghai 200120, China

Xiao-Ting Liang, Institute for Regenerative Medicine, Shanghai East Hospital, School of Life Sciences and Technology, Tongji University, Shanghai 200120, China

Corresponding author: Xiao-Ting Liang, MD, PhD, Research Fellow, Institute for Regenerative Medicine, Shanghai East Hospital, School of Life Sciences and Technology, Tongji University, No. 150, Jimo Road, Shanghai 200120, China. liangxt@tongji.edu.cn

Abstract

Mesenchymal stem/stromal cells (MSCs) have various properties that make them promising candidates for stem cell-based therapies in clinical settings. These include self-renewal, multilineage differentiation, and immunoregulation. However, recent studies have confirmed that aging is a vital factor that limits their function and therapeutic properties as standardized clinical products. Understanding the features of senescence and exploration of cell rejuvenation methods are necessary to develop effective strategies that can overcome the shortage and instability of MSCs. This review will summarize the current knowledge on characteristics and functional changes of aged MSCs. Additionally, it will highlight cell rejuvenation strategies such as molecular regulation, non-coding RNA modifications, and microenvironment controls that may enhance the therapeutic potential of MSCs in clinical settings.

Key Words: Mesenchymal stem cells; Senescence; Features; Function; Rejuvenation strategy

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Core Tip: Mesenchymal stem cell (MSC) administration is a promising therapeutic strategy for various human diseases. However, cell aging limits MSC function and therapeutic properties via reducing their activities. We review the morphological changes, molecular expression alterations, and functional degeneration of aged MSCs, and the effects of aged MSCs on immune cells and other target cells. Additionally, we summarize the strategies to rejuvenate aged MSCs to enhance their clinical potential.

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INTRODUCTION

Mesenchymal stem/stromal cells (MSCs) are multipotent progenitor cells that can retain postnatal capacity for both self-renewal and multilineage differentiation. The minimal criteria for MSCs as defined by the International Society for Cellular Therapy in 2006 are adherence to plastic under culture conditions; positivity for cell surface markers CD44, CD90, CD105, and CD73; negativity for hematopoietic markers CD45, CD34, CD14, CD11b, CD79α, CD19, and human leukocyte antigen-DR; and multi-differentiation potential of osteogenesis, chondrogenesis, and adipogenesis^[1]. They are a heterogeneous population of cells isolated from a variety of mesodermal tissues. These cells are involved in a wide range of physiological and pathological processes, such as bone development, adipogenesis, fibrosis, and inflammatory regulation^[2]. Over the past few decades, the amount of MSC-focused research has grown exponentially. These studies include both preclinical and clinical trials of either autologous or allogeneic MSCs. Infusion of MSCs has been performed to evaluate their safety and therapeutic efficacy in diseases of the immune^[3], hematological^[4], cardiovascular^[5,6], nervous^[7,8], respiratory^[9], digestive^[10], skeletal^[11], endocrine^[12], and reproductive^[13] systems^[14]. To date, more than 1000 MSC-based clinical trials have been registered in the United States National Institute of Health database^[15,16]. It is well recognized that MSC administration is a safe and effective strategy in the treatment of a variety of diseases.

Emerging evidence has demonstrated that multiple factors, including cell species, tissue source, isolation method, culture conditions, and cellular status, may explain the inconsistency in the features and characteristics of MSCs in some preclinical and clinical trials. A recent study showed that aging is an important factor affecting MSC properties and functions^[17]. Age-dependent decline in MSC number and function was found in old individuals^[18]. Additionally, MSCs from young donors may also become senescent because of excessive cell passage, oxidative stress, and other injuries^[19,20]. The senescent cells manifest a sequence of progressive changes in cellular morphology, biological function, and molecular expression^[21,22], as well as weakened efficacy in cell-based therapies^[23]. Therefore, appropriate quality controls or cellular rejuvenation processes are required to obtain clinical-grade MSCs. In this review, we will focus on investigations that have assessed the molecular features and functional changes of aged MSCs and highlight rejuvenation strategies that will enable more effective clinical translation.

CHARACTERISTICS AND FUNCTIONAL CHANGES OF AGED MSCS

Aging MSCs exhibit morphological changes and undergo a progressive decline in homeostasis, which contributes to the age-dependent deterioration of MSC function^[24]. These changes in senescent MSCs include a general decrease in their regenerative capacity, a switch in differentiation potency, and weakened regulatory functions (such as immunosuppressive effects)^[25]. A full understanding of these characteristics is fundamental for the development of strategies to delay or even prevent MSC

senescence. In view of this, the phenotypes and functional characteristics of senescent MSCs will be summarized in this section.

Morphological changes in aged MSCs

The most noticeable changes in aged MSCs are morphological. *In vitro* imaging analysis demonstrated that MSCs from early passages (P1-P3) were remarkably uniform in size^[24]. At P5, they exhibited a flattened and enlarged morphology compared with those at P1. Additionally, gradual telomere shortening is a typical characteristic of aging in MSCs^[26]. Moreover, these changes in morphology represented the heterogeneous response to the cellular microenvironment *in vitro* and *in vivo*.

Alterations of activity

In aged MSCs, the balance of homeostasis is disrupted, the proliferative ability declines, and mitochondrial dysfunction increases. In addition, both the DNA repair and retrogression of anti-oxidative capacity are reduced^[18,27]. Senescent MSCs display delayed self-cloning as well as restricted differentiation potency^[28]. Additionally, they exhibit a shift in differentiation potency from osteoblasts to adipocytes^[29-33]. Genetic stability, another biological index affecting MSCs activity, is involved in biosafety issues and therapeutic efficacy of these cells^[34]. Mounting evidence suggested that long-term cultured MSCs acquired genetic alterations, with the promotion of cell senescence and potential increased risks of transformation. However, the relevance of increased genomic instability with culture passages is still being debated^[35-38]. Roselli *et al.*^[39] reported that MSCs were genetically stable in long-term cultures at least up to passage 10, and abnormal MSC clones showed neither growth advantage nor senescence resistance. Some authors suggested that senescent cells are unlikely to undergo malignant transformation, even if the presence of few tumorigenic cells can not be excluded^[40]. The inconsistencies may be caused by tissue sources, culture conditions, culture times, and culture passages^[41]. Nevertheless, it is of critical importance to evaluate MSC genetic stability before clinical application.

Biomarkers for aged MSCs

Several methods may be used to identify MSC senescence. The most widely used measures include increased senescence-associated (SA) beta-galactosidase activity (SA-beta-gal), cell cycle arrest, and persistent DNA damage response signaling^[22]. Furthermore, specific markers for senescent MSCs have been discovered. Analysis of the MSC compartment revealed that MSC subpopulations differ between developmental and aged stages. CD271(-)CD146(+) cells only appeared in fetal bone marrow (BM)-containing colony-forming-unit-fibroblasts. The dominant MSC subset in pediatric and fetal samples was the CD271(bright)CD146(+) population, whereas the main cell type in adult samples was CD271(bright)CD146(-)^[42]. The proportion of CD11b+, CD3+, Gr-1+, or F4/80+ cells is upregulated in BM from aged mice, while the percentage of B220+ cells was significantly decreased compared with those from young mice BM^[43].

Recently, novel specific biomarkers were found to demonstrate the senescent state of MSCs^[21]. MSC-derived microvesicles (MVs) are one such biomarker^[44], and senescent late passage MSCs displayed a smaller MSC-MV size compared with early passage MSCs. Additionally, when comparing late and early passage MSC-MVs, there was a lower ratio of CD105+ cells and decreased osteogenesis in late passage MSC-MVs^[45]. When the percentage of CD264+ cells was greater than 35%, CD264 expression was inversely correlated with the regenerative potential of MSCs. Above the 75% threshold, MSCs were enlarged and showed a decreased proliferation and differentiation potency.

CyBC9, a senescence-specific fluorescent probe, is a promising tool used to rapidly identify both early and late senescent phenotypes in clinically relevant MSCs^[46], and it can be applied to live cells as a nontoxic probe. The mitochondrial *Cox1* gene containing the differentially methylated CpG island 4 was upregulated in MSCs from human fetal heart tissues. This demonstrated that CpG hypo-methylation in mitochondria might serve as a biomarker for senescence of human fetal heart MSCs induced by chronic oxidative stress^[20].

Portraits of expression profiles

Recent studies have demonstrated significant changes in the expression profiles (including transcriptomic, proteomic, epigenetic, and non-coding RNAs) of senescent MSCs. Transcriptome drift even preceded replicative exhaustion and other aging metrics^[47]. Utilizing a microarray assay, transcriptome analyses were performed using

various types of aged MSCs (Table 1).

Transcriptomics: Assays for gene expression profiles have been performed on multiple types of aging MSCs. These MSCs were obtained from various species and tissues, and subjected to different treatments. Benisch *et al*^[48] investigated the transcriptional profiles of human BM-MSCs from five elderly patients (79-94 years old) who had osteoporosis (hMSC-OP), the age-matched control group (hMSC-old; donor age 79-89 years), middle-aged donors (hMSC-C; donor age 42-67 years), and healthy middle-aged donors (42-64 years old) until they entered senescence (hMSC-senescent). By using hMSC-C as control cells, they found a small overlap of gene expression in the hMSC-old, hMSC-senescent, and hMSC-OP groups. By comparing the gene expression profiles of hMSC-OP, hMSC-old, and hMSC-senescent with hMSC-C, special transcriptomic features in each group were obtained. The differentially expressed genes in the three groups are mainly involved in proliferation, differentiation, osteoclastogenesis, and DNA repair^[48]. Wu *et al*^[49] identified six hub genes and eleven transcription factors related to adherens junctions, DNA damage induced by oxidative stress, attribution of telomeres, differentiation, and epigenetic modulation by comparing the gene alterations between hMSC-C and hMSC-old. Yoo *et al*^[50] revealed that 19 genes were downregulated and 43 upregulated in senescent human BM-MSCs relative to young MSCs. And these genes were mainly involved in metabolic functions and cell adhesion. Additionally, 394, 1073, and 2077 genes were significantly up-regulated in BM-MSCs from pesticide exposed, P14 MSCs, and MSCs from aged donor, compared with control MSCs (P3), respectively^[51]. And 218, 1077, and 1571 genes were down-regulated in BM-MSCs from pesticide exposed, P14 MSCs, and MSCs from aged donor, compared with P3 MSCs, respectively. Insulin-like growth factor-1 (*Igf-1*), *prolactin*, *leptin*, and *Cox-2* were identified as key genes of the predicted protein-protein interactions^[51]. In murine BM-MSCs that were freshly sorted by fluorescence-activated cell sorting, 927 differentially expressed genes were obtained in aged BM-MSCs. These genes contained cytokine receptors, chemokines, markers of cell senescence, and other groups, which were seen in the gene expression omnibus^[52].

Human umbilical cord (hUC)-derived MSCs, cultured in chemically defined xeno- and serum-free medium, displayed comparable growth trajectories up to passage (P) 9 and variably approached senescence after P10. However, significant changes in the transcription profiles occurred earlier. Microarray analysis of 14500 human genes in aged hUC-MSCs revealed that a nonlinear evolution of aging MSCs appeared after P5 and accumulated rapidly after P9^[47]. As for hUC vein-MSCs, young (P9) and senescent (P18) cells were used for transcriptome analysis assays. This study identified 73 differentially expressed genes in senescent cells, compared with young MSCs^[49]. Among these, 18 upregulated genes were screened out as characteristic molecular signatures of senescence when comparing senescent and young hMSCs derived from donors with normal or constitutional chromosome inversion karyotype. Among them, 11 novel candidate markers for senescence were identified.

In response to IL-2 priming, human adipose-derived MSCs (ADSCs) showed increased expression of genes encoding potent growth factors, cytokines, angiogenic, and anti-apoptotic promoting factors, and they were defined as novel transcriptional signatures closely associated with senescence^[53]. In CD45-CD31-CD34+ ADSCs from murine inguinal fat pads, aging has been shown to affect cellular signaling and function as well^[54]. Single-cell transcriptional profiles of ADSCs isolated from both young and aged mice were analyzed by utilizing a microfluidic-based single-cell gene expression platform. About 70 gene targets related to stemness, vasculogenesis, and tissue remodeling were evaluated and used to define ADSC clusters in each group. Ingenuity Pathway Analysis of a subset of this heterogeneous cell collection was performed. This analysis suggested that deficiency of a putatively vasculogenic subpopulation of ADSCs was a potential risk for age-related impairments in ADSCs function (particularly with regard to wound healing)^[54].

Proteomics: Proteomics is an efficient and accessible tool used to determine protein expression profiles. An SA secretome, also known as SA secretory phenotype (SASP), usually contains the expression of growth factors, cytokines, and extracellular proteases that modulate the microenvironmental phenotypes caused by senescent cells^[55]. The SASP is useful for the development of biological markers and rejuvenation strategies in aged MSCs^[22]. Secretome analyses for secretory protein profiles in senescent MSCs are summarized in Table 2. For example, elderly MSCs exhibited increased levels of pro-inflammatory factors, including interleukin-6 (IL-6), IL-8 (IL-8/CXCL8), and monocyte chemoattractant protein-1 (MCP-1/CCL2). Neutralization of these factors improved their immunomodulatory function^[56]. In the conditioned

Table 1 Summary of various transcriptomics analyses studies of senescent mesenchymal stem cells

| Ref. | Species | Tissue sources | Classification | Cells | Groups | Database | Differentially expressed genes (DEGs) | Identification of targets |
|--|---------|------------------------------|---|--|---|---|---|--|
| Benisch <i>et al</i> ^[48] , 2012 | Human | Bone marrow of femoral heads | Affymetrix Gene Chip | Cultured in DMEM/Ham's F-12 (1:1) medium supplemented with 10% fetal calf serum (FCS), 1 U/mL penicillin, 100 µg/mL streptomycin, and 50 µg/mL L-ascorbic acid 2-phosphate. Used after 1 to 2 passages | hMSC-C: Middle-aged donors (42-67 yr old); hMSC-old: The age-matched control group (79-89 yr old); hMSC-OP: Patients (79-94 yr old) who had primary osteoporosis; hMSC-senescent: Healthy donors of middle-age (42-64 yr old) until they entered senescence | GEO accession numbers: GSE35955; GSE35956; GSE35957; GSE35958; GSE35959 | One gene was upregulated and seven downregulated in all three groups, compared with the hMSC-C group; 38 genes with enhanced and 36 genes with reduced expression in hMSC-OP and hMSC-old groups, compared with hMSC-C; 2477 genes with higher and 1222 genes with lower expression in hMSC-OP, in comparison with hMSC-old | The reliable or promising candidates for osteoporosis, including susceptibility genes: <i>Lrp5</i> , <i>Spp1</i> (Osteopontin), <i>Col1a1</i> , <i>Sost</i> , and <i>Mab211l</i> |
| Yoo <i>et al</i> ^[50] , 2013 | Human | Bone marrow-derived MSCs | SSH analysis | Purchased from Cambrex Bio Science | Young human MSCs (Y-hMSCs): Approximately 10 population doubling levels (PDL); senescent MSCs (S-hMSCs): Until approximately 30 PDL, at least 80% of the cells were positive for SA-β-Gal staining | NA | Nineteen genes were down-regulated and 43 upregulated in S-hMSCs | Gradually downregulated mRNA in S-hMSCs: <i>Pdia3</i> , <i>Wdr1</i> , <i>Fstl1</i> , <i>Copg1</i> , <i>Lman1</i> , and <i>Pdia6</i> ; significantly upregulated genes: <i>Hsp90b1</i> , <i>Eid1</i> , <i>Atp2b4</i> , <i>Ddah1</i> , <i>Prnp</i> , <i>Rab1a</i> , <i>Psq5</i> , <i>Tm4sf1</i> , and <i>Ssr3</i> |
| Bustos <i>et al</i> ^[52] , 2014 | Mouse | Bone marrow | Affymetrix Gene Chip | Sorted by fluorescence-activated cell sorting (FACS) | BM-MSCs from young (3-mo-old) and aged (24-mo-old) mice; young donor BM-MSCs <i>vs</i> aged ones | GEO accession number: GSE44403 | 927 genes were differentially expressed | Confirmed by qPCR: Cytokine receptors (15 genes), chemokines (<i>Ccr7</i> , <i>Cxc3cr1</i> , <i>Cxcr5</i>), markers of cell senescence (<i>CDK</i> , <i>p21</i> , <i>p27</i> , and <i>p53</i>), <i>Marcks</i> , <i>Mmp9</i> , and <i>Timp2</i> |
| Duscher <i>et al</i> ^[54] , 2014 | Mouse | Inguinal fat pads | Microfluidic-based single-cell gene expression platform | CD45-/CD31-/CD34+ cells were sorted | Adipose-derived mesenchymal stem cells (ADSCs) from young (3 mo) and aged (21 mo) mice | NA | Differences in transcriptional profiles of genes related to cell stemness, remodeling, and vasculogenesis: <i>Adam10</i> , <i>Angpt1</i> , <i>Angpt2</i> , <i>Hif1a</i> , <i>Mef2c</i> , and <i>Sod2</i> | Age-related depletion of a subpopulation of MSCs characterized by a pro-vascular transcriptional profile, such as <i>Angpt1</i> , <i>Vegfa</i> , and <i>Sod3</i> |
| Medeiros <i>et al</i> ^[19] , 2017 | Human | Umbilical cord veins | The GeneChip Human Genome U133 Plus 2.0 array | The surface markers including CD105, CD73, CD90, CD14, CD34, and CD45 were analyzed by flow cytometry; differentiation capacity toward three lineages was assessed | hMSCs in the 9 th (Y-hMSCs) and 18 th passages (S-hMSCs) were used for assays, hMSCs/n from the donor with normal karyotype, and hMSCs/inv from the donor with a constitutional inversion of chromosome 3; the comparisons were as follows: (1) Y-hMSCs/n & S-hMSC/n; (2) Y-hMSCs/inv & S-hMSCs/inv; (3) Y-hMSCs/n & Y-hMSCs/inv; and (4) S-hMSCs/n & S-hMSCs/inv | GEO accession number: GSE56530 | 73 DEGs in S-hMSCs/n compared with Y-hMSCs/n and 279 DEGs in S-hMSCs/inv compared with Y-hMSCs/inv; 93 DEGs in Y-hMSCs/inv compared with Y-hMSCs/n; 425 DEGs in S-hMSCs/inv compared with S-hMSCs/n. The candidates for senescent markers: <i>Dio2</i> , <i>Foxe1</i> , <i>Galnt5</i> , <i>Has3</i> , <i>Krt19</i> , <i>Krt34</i> , <i>Krtap1-55</i> , <i>Oc730755</i> , <i>Mrv1</i> , <i>Plcb4</i> , and <i>Scube3</i> | Confirmed by qPCR: <i>Ankrd1</i> and <i>Mmp1</i> in S-hMSC/n <i>vs</i> Y-hMSC/n; <i>Sfrp1</i> , <i>Ankrd1</i> , <i>G0s2</i> , and <i>Ndn</i> in S-hMSC/inv <i>vs</i> Y-hMSC/inv; <i>Adora2b</i> , <i>Sfrp1</i> , <i>Kynu</i> , <i>G0s2</i> , <i>Aldh1a1</i> , and <i>Mab211l</i> in Y-hMSC/inv <i>vs</i> Y-hMSC/inv; and <i>Adora2b</i> , <i>Ccl7</i> , <i>Sfrp1</i> , <i>Kynu</i> , <i>Ankrd1</i> , <i>Mmp1</i> , <i>Lamc2</i> , <i>G0s2</i> , <i>Mab211l</i> , and <i>Ndn</i> in S-hMSC/inv <i>vs</i> S-hMSC/n |
| Wu <i>et al</i> ^[49] , 2019 | Human | Bone marrow of femoral heads | Affymetrix Gene Chip | Cultured in DMEM/Ham's F-12 (1:1) medium supplemented with 10% FCS, 1 U/mL penicillin, 100 µg/mL streptomycin, and 50 µg/mL L-ascorbic acid 2-phosphate. used after 1 to 2 | Middle-aged group <i>vs</i> elderly group | GEO accession number: GSE35955 | 156 up-regulated and 343 down-regulated differentially expressed genes (DEGs) | Six hub genes identified by PPI network analysis: <i>Ctnnb1</i> , <i>Ppp2r1a</i> , <i>Fyn</i> , <i>Mapk1</i> , <i>Pik3c2a</i> and <i>Ep300</i> . 11 TFs identified by TFs screening: <i>Creb1</i> , <i>Cux1</i> , <i>Egr1</i> , <i>Ep300</i> , <i>Foxc1</i> , <i>Hsf2</i> , <i>Mef2a</i> , <i>Plau</i> , <i>Sp1</i> , <i>Stat1</i> and |

| | | | | passages | | | | Usf1 |
|---|-------|---|--------------------------------------|--|--|---|---|---|
| Wiese <i>et al</i> ^[47] , 2019 | Human | The perivascular region of Wharton's jelly from umbilical cords | Affymetrix GeneChip U133A 2.0 arrays | Provided by Tissue Regeneration Therapeutics, Inc. Positive for the cell surface markers CD73, CD90, CD105, CD10, CD140b, CD146 (40%-60%), CD166, and MHC-I; negative for the cell surface markers CD45, CD31, CD34, and HLA-DR. Exhibit trilineage potential in directed differentiation assays | Human umbilical cord perivascular cells (HUCPVCs) from early passages (P2–P5), mid-passages (P6–P9), and pre-senescent passages (P10–P12) | GEO accession number: GSE119987 | The transcriptome of HUCPVCs was stable through P5. A single significantly DE gene was identified at P6 and P7 compared with P2, whereas 5 DE genes were detected at P8 and 27 at P9. The number of significantly DE probe sets increased from 27 (P9) to 301 (P10), then to 1094 (P12) | Significant transcriptome drift occurred only after P5 |
| Leveque <i>et al</i> ^[51] , 2019 | Human | Bone marrow aspirates from the iliac crest of healthy donors (21 to 26 years old) | RNAseq Analysis | The surface markers including CD34, CD45, CD73, CD90, and CD105 were analyzed by flow cytometry; differentiation capacity toward three lineages was assessed | Four groups: Control MSCs (P3); 21 d pesticide mixture exposed MSCs (P4); long-term cultivated MSCs (P14); and MSCs from aging donor (72 yr old) | The SRA database under accession number PRJNA510912 | 394, 1073, and 2077 EST were significantly increased from pesticide exposed, P14 MSCs, and MSC from aged donor; 218, 1077, and 1571 ESTs were down-regulated | Confirmed by QPCR: <i>Igf-1</i> , <i>Prolactin</i> , <i>Leptin</i> , and <i>Cox-2</i> |

GEO: Gene expression omnibus; DEGs: Differentially expressed genes; hMSC: Human mesenchymal stem cells; MSC: Mesenchymal stem cells; HUCPVCs: Human umbilical cord perivascular cells; FCS: Fetal calf serum; ADSCs: Adipose-derived mesenchymal stem cells; PDL: Population doubling levels; DMEM: Dulbecco's Modified Eagle's medium; FACS: Fluorescence-activated cell sorting; BM: Bone marrow.

medium (CM) from senescent MSCs induced by the HIV protease inhibitor tipranavir, the soluble proteins were evaluated to find dysregulated secreted factors using antibody arrays and liquid chromatography-mass spectrometry (LC-MS)^[57]. Semi-quantitative antibody arrays and LC-MS analysis identified altered secretion of 86 proteins related to the extracellular matrix, cell adhesion, angiogenesis, and wound healing. Among the identified secreted factors in the proteomic analysis, a series of TGF- β targets were significantly upregulated. Further investigation revealed that insulin-like growth factor-binding protein 7 (IGFBP7), one of the targets of TGF- β , is independent of any additional factors that induce osteogenesis in hMSCs. IGFBP7 is also essential for the viability of hMSCs during osteogenesis^[57].

In the ADSCs from one-year-old male C57BL/6 mice, the anti-senescent protein, telomerase reverse transcriptase (TERT), and the anti-apoptotic transcription factor myocardin were overexpressed to restore their functions. The secretomes in CM and exosome-enriched fractions from the transgenic cells were analyzed using a proteomic approach. This approach involved combining two-dimensional gel electrophoresis with matrix-assisted laser desorption/ionization time-of-flight mass spectrometry^[58]. The comparative targeted proteomic analysis revealed that both matrix metalloproteinase-2 (MMP-2) and its inhibitor metalloproteinase inhibitor 2 (TIMP2) levels are increased by two-fold in the CM compared with those in mock-transduced cells.

Epigenetics: Epigenetic profiles of aged human BM-MSCs have been reported, and briefly reviewed by Cakouros and Gronthos^[59]. Using the human methylation bead

Table 2 Summary of secretome alteration analysis studies of senescent mesenchymal stem cells

| Ref. | Species | Tissue sources | Classification | Cells | Groups | Differentially expressed proteins | Identification of targets |
|---|---------|---|--|---|--|---|---|
| Kizilay <i>et al</i> ^[56] , 2017 | Human | Subcutaneous and pericardial adipose tissue | R&D Systems Human Cytokine Array; multipot electrochemiluminescence immunoassay V-Plex Pro inflammatory Panel | CD44, CD73, CD105, and CD90 expression was more than 95%; CD45, CD34, CD19, CD14, and HLA-DR expression was less than 5%; differentiation capacity toward three lineages was assessed | E-MSCs: MSCs from elderly ATH patients (> 65 yr old); A-MSCs: MSCs from adult ATH patients (< 65 yr old) | The expression of IL-6, IL-8/CXCL8, MCP-1/CCL2, MIF, IFN- γ , IL12p70, IL-13, IL-2, and IL-4 was elevated in E-MSCs relative to A-MSCs | Neutralization of IL-6, IL-8/CXCL8, and MCP-1/CCL2 significantly improved the E-MSCs' immunomodulatory function |
| Infante <i>et al</i> ^[57] , 2018 | Human | Bone marrow | Semi-quantitative antibody arrays; liquid chromatography-mass spectrometry (LC-MS): Version 4.0.4265.42984, Nonlinear Dynamics | Obtained from Lonza commercially; passages 3-4 | Ctrl-hMSCs: Incubated with dimethyl sulfoxide alone; PreA-hMSCs: Treated with the HIV protease inhibitor (tipranavir) every other day until passage 11 | A dysregulation in the secretion levels of 42 proteins was detected by antibody arrays; 44 were detected by LS-MS in preA-hMSCs; most of them were overexpressed in preA-hMSCs, in comparison with ctrl-hMSCs | IGFBP7 is essential for hMSCs viability during early osteogenic differentiation |
| Madonna <i>et al</i> ^[58] , 2019 | Mouse | Peri-epididymal visceral adipose tissue from 1-yr-old male C57BL/6 mice | Two-dimensional gel electrophoresis (2DE); matrix-assisted laser desorption/ionization time-of-flight mass spectrometry | The expression of CD45, CD34, CD133, ASMA, Desmin, CD105, CD73, CD90, CD79, and CD160 was analyzed by flow cytometry | Mock AT-MSCs: Mock-transduced AT-MSCs; rTMAT-MSCs: Rejuvenated by TERT and the anti-apoptotic transcription factor myocardin overexpression | 113 protein spots were picked up and identified from the whole CM and exosome-enriched fraction in rTMAT-MSCs | Two novel candidates supporting angiogenesis in the whole CM of rTMAT-MSCs: MMP2 and its inhibitor TIMP2 |

hMSC: Human mesenchymal stem cells; MSC: Mesenchymal stem cells; TERT: Telomerase reverse transcriptase; MMP2: Matrix metalloproteinase-2; CM: Conditioned medium; LC-MS: Liquid chromatography-mass spectrometry.

ChIP array, researchers identified a series of hypomethylated, hypermethylated, and hydroxymethylated CpG sites in MSCs from aged subjects^[60-62]. However, differentially methylated CpG sites are a robust age-related DNA methylation signature, illustrating similar DNA changes independently of disease state, sex, tissue, and cell type^[59,63]. Additionally, aged human BM-MSCs from long-term culture exhibited consistent epigenetic changes *in vitro* when the methylation profile of human BM-MSCs at early and late passages was assessed^[64]. Following the application of enhanced reduced representation bisulfite sequencing, the global DNA methylation profiling demonstrated a greater breadth than previously reported. The genome-wide analyses using whole-genome bisulfite sequencing provided a better understanding of how the epigenetic modifications alter gene expression and regulate the biological characteristics^[65].

Non-coding RNAs: It has been previously reported that some non-coding RNAs are associated with cellular senescence in different cell types^[66-70]. MicroRNAs (miRNAs) are small non-coding RNAs that have highly conserved sequences and regulate target genes in cellular functions of metabolism, proliferation, apoptosis, and senescence^[71,72]. In senescent MSCs, 43 miRNAs were identified and characterized using a miScript miRNA assay^[73]. Among them, the expression of 24 miRNAs was closely related to

cellular senescence as referred to previous studies. As for the rest, fourteen miRNAs (miR-10, miR-27b, miR-30b, miR-30d, miR-103a, miR-103a-2, miR-136, miR-140-5p, miR-323-3p, miR-330-5p, miR-361-5p, miR-409-3p, miR-424, and miR-455-3p) were upregulated, and five miRNAs (miR-16-2, miR-29b, miR-199b-5p, miR-454, and miR-618) were downregulated in response to cellular aging. Additionally, miR-29b and miR-199b-5p modulated cellular senescence *via* LAMC networks^[73].

In MSCs cultured under hypoxic conditions, miRNA expression profiles of MSCs from young (≤ 30 years old) and aged (≥ 60 years old) donors were analyzed using an Agilent Technologies Bioanalyzer high sensitivity DNA chip^[74]. Principal component analysis demonstrated differentially expressed miRNAs in normal and hypoxic groups. There was > 2 -fold upregulation of nine miRNAs in young MSCs and two miRNAs in aged MSCs after culturing under hypoxic conditions. Also, the hypoxia induced downregulation of four miRNAs in young MSCs and thirty-one miRNAs in aged MSCs, respectively. MiR-543 and miR-590-3p were identified as regulators of cellular aging in hMSCs through direct binding to the aminoacyl tRNA synthetase-interacting multifunctional protein-3/p18 transcripts and decreasing the protein expression levels^[75].

Long non-coding RNAs (lncRNAs) are non-coding transcripts, longer than 200 nucleotides, that play critical roles in the regulation of MSCs senescence. They are not only involved in age-related lineage fate switching but also in the reprogramming of old cells^[76,77]. LncRNA microarray analysis of young and aged Sca-1+CD29+CD45-CD11b- murine BM-MSCs has demonstrated that 92 lncRNAs showed altered expression^[76]. Among them, 83 lncRNAs were downregulated, and 9 were upregulated in cells isolated from aged mice. Further investigation demonstrated that the candidate BM stem cell-related lncRNA (BMNCR) was highly expressed in the BM-MSCs of young mice, and significantly decreased during aging. Moreover, the BMNCR levels in human BM-MSCs were negatively correlated with age. The effects of BMNCR were evidenced by Bmn-cr-KO and Bmn-cr-Tg mice simultaneously^[76].

Functional degeneration of aged MSCs

The senescent MSCs exhibit significant impairments in paracrine functions^[78], resistance to oxidative stress, hypoxia, or serum deprivation-induced apoptosis^[79-81]. The age-dependent decrease in cytokines, chemokines, and growth factors released by MSCs will impact cellular functions such as apoptosis, migration, osteogenesis, angiogenesis, cell adhesion, and immunomodulation^[52,54,82]. Finally, the aged MSCs delay wound healing and exacerbate tissue injuries^[54]. In summary, the functional regression of senescent MSCs limits their application in tissue engineering and regenerative medicine.

Age-related effects of MSCs on target cells

Bidirectional signaling exists between MSCs and their target cells^[83,84]. The interaction between MSCs and target cells has been shown to occasionally follow a time-dependent model of regulation and feedback^[85]. MSC senescence decreases the functions of a large variety of immune cells, hematopoietic stem and progenitor cells (HSPCs), oligodendrocytes, senescent chondrocytes, and other target cells through either direct or indirect cross-talk (Figure 1)^[78,84,86].

Immune cells: Previous studies have demonstrated that MSC senescence retards immunosuppression in various types of immune cells. Replicative senescence of MSCs derived from BM or adipose tissue showed decreased ability to suppress T-cell, but not natural killer and B-cell proliferation^[87,88]. Long-term expansion of MSCs reduced the capacity to inhibit CD4+ and CD8+ T cell proliferation. This phenomenon was observed by co-culturing MSCs with alphaCD3CD28-activated peripheral blood mononuclear cells. The inhibitory effect on T-cell proliferation significantly decreased along with increased passage number of hBM-MSCs, and the effect in hUC-MSCs was even more substantial^[88]. ADSCs derived from elderly subjects also displayed a diminished capacity to suppress the proliferation of activated T cells. Similar results were observed in MSCs isolated in parallel from Lewis and Brown Norway rats of young (less than 4 wk old) and aged (older than 15 mo) groups^[89]. Aside from proliferation, the senescent MSCs impair the suppressive effects of the activation-antigen expression and cytokine production in phytohemagglutinin-stimulated T cells^[79]. Soluble factors and direct cell-cell contact partially mediate the decreased suppressive effect of aged MSCs on T cells^[56].

In addition to lymphocytes, MSC senescence affects the phenotypes and functions of macrophages and dendritic cells^[29,90]. When co-cultured with BM-MSCs from young

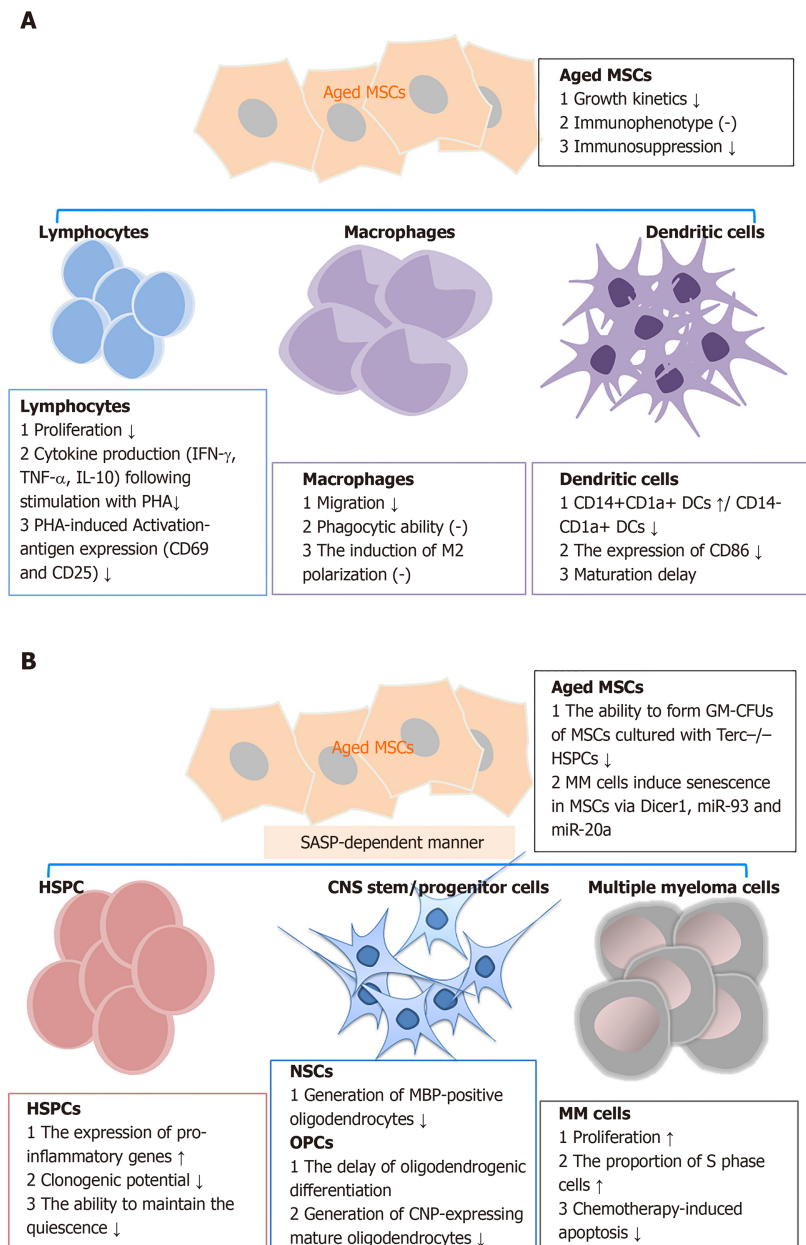


Figure 1 Effects of senescent mesenchymal stem cells on target cells. A: Effects of aged mesenchymal stem cells (MSCs) on immune cells; B: Effects of aged MSCs on other target cells, including hematopoietic stem and progenitor cells, neural stem cells, and multiple myeloma cells. DCs: Dendritic cells; HSPCs: Hematopoietic stem and progenitor cells; NSCs: Neural stem cells; OPCs: Oligodendrocyte progenitor cells; MM cells: Multiple myeloma cells; MSCs: Mesenchymal stem cells; PHA: Phytohemagglutinin; GM-CFUs: Granulocyte macrophage-clone formation units; MBP: Myelin basic protein; CNP: 2',3'-cyclic-nucleotide 3'-phosphodiesterase.

mice, a macrophage cell line (RAW264.7 cells) exhibited higher migration rates, although they displayed similar phagocytic ability and induction of macrophage M2 polarization^[29]. In dendritic cells, cellular maturation was inhibited when cultured with expanded marrow stromal cells relative to the parental MSCs^[91].

Other target cells: Apart from immune cells, senescent MSCs show impaired activity against multiple target cells. Senescent MSCs enhanced the expression of pro-inflammatory SASP factors in HSPCs and inhibited their clonogenic potentials^[92]. These cells also have a reduced capacity to maintain CD34+CD38- HSPCs quiescence, as a result of increased IL-6 secretion^[93]. In a study on telomere dysfunction in MSCs, using Terc-/- mice, Ju *et al*^[94] found that aged Terc-/- BM-MSCs depressed the functions of HSPCs and early hematopoietic progenitors. Aging MSCs had a reduced ability to induce oligodendrogenic differentiation in neural stem cells. Additionally, the production of 2',3'-cyclic-nucleotide 3'-phosphodiesterase-positive oligodendrocytes in oligodendrocyte progenitor cells was reduced. The impaired differentiation suppressed the generation of myelin-like sheaths during central

nervous system remyelination^[95]. Also, in the peri-infarct cortex of rats subjected to transient middle cerebral artery occlusion, aged MSC administration resulted in more microglia and reduced pericyte infiltration compared with that for young MSCs. The changes in cellular components probably correlated with reduced expression of brain-derived neurotrophic factor and MCP-1^[96]. In a myocardial infarction (MI) model, the infusion of old MSCs resulted in a switch of the cellular profile in the infarct region. This was characterized by fewer endothelial cells, vascular smooth muscle cells, and macrophages, and more fibroblasts compared with young MSCs^[97]. Similarly, senescent MSCs facilitated the growth of multiple myeloma (MM) cells, which aggravated disease progression^[98]. In turn, MM cells (such as NCI-H929, OPM-2, KMS-12-BM, and primary CD138+ tumors cells) induced senescence in MSCs derived from healthy controls with decreased expression of Dicer1, miR-93, and miR-20a.

CELLULAR REJUVENATION STRATEGIES

Simple isolation, standardized culture methods, and potential autologous application make MSCs a superior cell source for the treatment of various diseases and injuries^[13]. Therefore, optimizing the viability and function of MSCs for infusion is of great significance. With an increased understanding of the characteristics of MSC senescence, further investigations are ongoing to resolve challenges linked to the clinical application of cellular therapies. To date, the rejuvenation strategies have demonstrated therapeutic potential including molecular regulation, non-coding RNA modification, and control of the microenvironment.

Molecular regulation

Multiple molecules have been confirmed to restore the proliferative ability and biological function of MSCs *via* gene modification, or the administration of recombinant proteins, agonists, or inhibitors.

Sirtuins: The sirtuins (SIRT), which include seven sirtuin homologs, are wellknown for their ability to delay cellular senescence and extend the lifespan of organisms ranging from yeast to humans^[99]. SIRT1 overexpression in aged MSCs ameliorated the senescence phenotype, recapitulated angiogenesis, and protected cells from oxidative stress. Infusion of SIRT1-modified aged MSCs promoted the expression of pro-angiogenic factors, such as angiopoietin 1, and basic fibroblast growth factor (bFGF). Additionally, SIRT1-modified aged MSCs increased Bcl-2/Bax ratio at the protein level, promoted cellular survival, inhibited fibrosis, upregulated vascular density, and improved heart function in an MI model, compared with vector-aged MSCs^[100]. SIRT1 pathway activators, including nicotinamide mononucleotide^[101], nicotinamide phosphoribosyl transferase^[102], cell-deposited decellularized extracellular matrix^[103], and SIRT1720^[104] have been applied in aged human MSCs. They improve cell viability and osteogenesis while inhibiting apoptosis and adipogenesis in aged MSCs. Pretreatment of aged MSCs with SIRT1720 enhanced therapeutic efficacy by promoting angiogenesis and repressing fibrosis following rat MI^[104].

Likewise, the overexpression of SIRT3 improves the antioxidant capacity and promotes the survival of old human MSCs through activating forkhead box O3a in the nucleus, manganese-superoxide dismutase, and catalase. In an MI model, the application of old human MSCs overexpressing SIRT3 enhanced cardiac function and decreased infarct size^[105]. SIRT6 maintains hMSC homeostasis by co-activating the antioxidant nuclear factor erythroid 2-related factor 2 pathway, RNA polymerase II, and heme oxygenase 1^[106].

Growth factors: Growth factors are a superfamily of proteins that promote cell survival, expansion, migration, and differentiation, as well as prevent disruption of homeostasis *in vitro* and *in vivo*^[107]. Through stimulation of the FGFR1/2 pathway, LY294002 (a PI3K inhibitor) rescued MSCs from senescence^[108]. Acadesine activates adenosine 5'-monophosphate-activated protein kinase (AMPK), a downstream signal of FGF21, and abrogates the depletion of FGF21-induced senescence by inhibiting mitochondrial fusion^[109]. Silencing mitofusin-2 has been found to inhibit MSC senescence induced by the abrogation of FGF21 as well. Knockdown of insulin-like growth factor binding protein 4 restored the osteogenic potency of aged MSCs *via* the activation of Erk and Smad signals^[110]. Pretreatment of aged MSCs with macrophage migration inhibitory factor (MIF) enhanced the secretion of vascular endothelial growth factor (VEGF), bFGF, hepatocyte growth factor, and insulin-like growth factor,

which promoted their growth, paracrine function, and survival^[80]. MIF-rejuvenated MSCs release growth factors through interactions with CD74 and subsequent activation of AMPK-FOXO3a signaling, which protects cells from doxorubicin-induced senescence by modulating the PI3K-Akt signaling pathway^[111].

Additional potential regulators: The AKT pathway plays an important role in the rejuvenation of features and functions of aged MSCs. This pathway can act *via* ERBB4/PI3K/AKT^[112], lactoferrin/AKT^[113], Vc/AKT/mTOR^[114], and fucoidan/FAK-Akt-TWIST axes^[115]. Administration of rapamycin, an inhibitor of the mTOR signaling pathway, raised the expression level of NANOG, postponed replicative arrest, and enhanced the lifespan increment of BM-MSCs^[116]. NANOG, an embryonic transcription factor, is a pluripotency marker that facilitates myogenic differentiation and restores the contractile function of senescent MSCs^[117]. Additionally, a high number of potential regulators involved in senescent MSC rejuvenation have been screened and investigated *in vitro*. For example, both L-carnitine^[118] and curcumin^[119] affect the methylation status of the *TERT* promoter, increase the telomerase activity, and consequently alleviate the aging-related features of ADSCs. In human BM-MSCs, the addition of L-carnitine during expansion also elevates cell production^[120].

Many *in vivo* experiments using various disease models have been conducted to confirm the efficacy of the rescue strategies to rejuvenate aged MSCs. It is reported that melatonin can protect MSCs from senescence *via* prion protein (PrPc)-dependent enhancement of mitochondrial function^[121]. Implantation of genetically-modified old human MSCs with tissue inhibitor of matrix metalloproteinase-3 or VEGF promotes angiogenesis, prevents adverse remodeling, and preserves cardiac function to a similar extent compared with young hMSCs^[122]. Stem cell antigen 1 (Sca-1)+ MSCs resident in the heart increase angiogenesis, and activate cell proliferation in the infarcted heart, which improves cardiac function after MI^[123,124]. Overexpression of neuron-derived neurotrophic factor rejuvenates human ADSCs and BM-MSCs from the elderly, reduces the ischemic area, and repairs cardiac function after MI by improving angiogenesis and decreasing apoptosis^[125,126]. Ethyl pyruvate, a HMGB1 inhibitor, restores the senescent phenotype of BM-MSCs, alleviates clinical signs of lupus nephritis, and prolongs survival of MRL/Mp-lpr/lpr mice *via* TLR4-NF-kappaB signaling^[127]. These candidates (both *in vitro* and *in vivo*) may be valuable for the identification of suitable targets with utility in the production of clinical-grade MSCs.

Non-coding RNA modification

Non-coding RNAs are novel genetic regulators involved in regenerative medicine. With respect to aging, transfection of the miR-195 inhibitor restores the expression of anti-aging factors, including TERT and SIRT1, as well as phosphorylation of AKT and FOXO1. The miR-195 inhibitor reduced the expression of SA-beta-gal, which significantly induced telomere relengthening and restored the proliferative abilities of old MSCs. Administration of aged MSCs with miR-195 knockout alleviated infarction size and improved left ventricular function^[128]. Additionally, miR-10a, miR-29c-3p, and miR-130b have been reported to rejuvenate MSC senescence by targeting different downstream pathways^[128-131]. The overexpression of miR-10a in aged hBM-MSCs stimulates angiogenesis by inducing the expression of angiogenic factors *via* activated Akt. These cells then enhance implanted stem cell survival and improve cardiac function after MI^[129]. The miR-29b-3p derived from BM-MSCs regulates aging-associated insulin resistance^[132]. In multiple myeloma-MSCs, Dicer1 overexpression and upregulation of miR-93/miR-20a could reverse the effects on differentiation and reduce cellular senescence^[98]. The lncRNA Bmncr regulates the age-related lineage switch between osteogenic and adipogenic differentiation in BM-MSCs. Overexpression of Bmncr (Bmncr-Tg) reduced bone loss and fat accumulation by maintaining extracellular matrix protein fibromodulin and activating the bone morphogenetic protein 2 pathway^[76].

Microenvironment modulation

A conducive microenvironment is essential for maintaining MSC activity^[133]. When BM-MSCs were treated with BM supernatant from systemic lupus erythematosus (SLE) patients, they demonstrated characteristics of senescence. An inflammatory microenvironment is considered to play a primary role in the senescence of SLE BM-MSCs^[127]. In unbalanced microenvironments caused by aging, the survival, proliferation, colony formation, migration, and appropriate differentiation of grafted BM-MSCs were significantly suppressed^[43,84]. In addition, the BM pCO₂ and HCO₃⁻ levels displayed a close correlation with MSC differentiation and proliferation^[134].

Therefore, microenvironment regulation is a promising strategy to reverse the decline of aged MSCs and promote the clinical efficacy^[135,136].

Rejuvenating the senescent MSCs is more effective in hypoxic conditions compared with that in normal conditions. The neuroprotective effects of CM from aged human BM-MSCs against cerebral ischemia were enhanced by hypoxia conditioning *in vitro*^[137,138]. Stem cell-deposited decellularized extracellular matrix can rescue hUC-MSCs from oxidative stress-induced premature senescence and facilitate their clinical application in regenerative medicine^[103]. The co-culture system is a convenient means of modulating the cellular microenvironment. BM-MSCs co-cultured with young (P3) human umbilical vein endothelial cells demonstrated a higher proliferative ability and decreased pro-inflammatory (cytokines and miRNA) phenotype, compared with the old cells (P13)^[139]. In conclusion, the enhancement of the microenvironment has a significant effect on the prevention of MSC senescence.

Other factors influencing rejuvenation

Besides restoring the activities of aged autologous MSCs, some researchers have attempted to find an accessible source for the replenishment of autologous MSCs. In the past few decades, the differentiation of pluripotent stem cells into MSC-like cells has been explored to address the problems of viability and scarcity of autologous MSCs derived from old individuals^[140-142]. Induced pluripotent stem cells (iPSCs) and embryonic stem cells (ESCs), which acquire a rejuvenation gene signature, are the alternative sources of MSCs^[141,143]. However, the production protocols used to derive MSCs from iPSCs and ESCs require optimization. The introduction of new technologies, such as 3D culture and gene engineering, might make them more valuable for further clinical application^[142].

Biomaterials and various cellular components are potential carriers used for the modification of aged MSCs. MVs carrying mRNAs, miRNAs, non-coding RNAs, proteins, and DNA are a novel and promising tool used to reverse aging in cells by mediating intercellular communication^[44,108]. For instance, exosomes containing miR-17 and miR-34a from young MSCs rejuvenate aged murine hematopoietic stem cells *via* AKT/autophagy-related mRNAs^[144]. Extracellular vesicles from human iPSCs can reduce cellular reactive oxygen species levels and alleviate aged phenotypes of senescent MSCs by partially delivering intracellular peroxiredoxin antioxidant enzymes^[145]. Media supplied with human platelet lysate from younger donors were able to facilitate MSC expansion and osteogenic differentiation^[146]. Additionally, many bioactive hydrogels^[147], biomimetic scaffolds^[148], and other biomaterials^[149,150] have been tested to assess whether they can modify aged MSCs. Removal of senescent cells in a high-throughput manner is another strategy that can be used to address the challenge of senescence^[151]; this strategy, which has been explored in clinical trials, involves the isolation and enumeration of senescent MSCs from undiluted human whole blood.

Some chemical compounds and foods rejuvenate senescent MSCs. Zinc sulfate significantly reduced the doubling time and increased *TERT* gene expression of rat ADSCs under extremely low-frequency-electromagnetic field^[152]. It also enhanced telomere length extension in human ADSCs by regulating telomerase and methylation of the *TERT* gene promoter CpG island^[153]. Besides zinc sulfate, resveratrol mimics the effects of dietary restriction, improves osteogenic function, and promotes mitochondrial activities of senescent MSCs through the regulation of mitofilin^[154]. NT-020, a dietary supplement containing blueberry, green tea, vitamin D3, and carnosine, rescued the reduced proliferation of MSCs in serum from aged rats^[155]. Additionally, *Undaria pinnatifida* and its ethanol extracts improve replication ability and ameliorate functional decline in senescent hBM-MSCs (P17)^[156].

The rejuvenation methods mentioned above have potentials to optimize the functional status of aged MSCs. However, most of them were *in vitro* or rodent model studies. Further research is needed to evaluate their long-term safety and efficacy before it can be clinically useful.

CURRENT CHALLENGES AND FUTURE PERSPECTIVES

Senescence is an inevitable biological process for MSCs obtained from old individuals or long-term cultures. Although recent studies have revealed the characteristics and mechanisms of MSC senescence and attempted to rejuvenate aged MSCs, many issues remain unresolved. First, in studies of age-correlated phenotypic alterations, the expression of CD90 and CD73 in intervertebral disc cells was reduced in older individuals, while CD146 expression was increased^[157]. However, the expression of

these factors (MSC markers) is rarely compared between young and aged MSCs. The comparison of these two types of cells provides a better understanding of senescent MSCs. Second, the effects of cellular rejuvenation for aged MSCs need to be determined *in vivo*, especially in the context of the multidirectional functions of regulators^[158]. For example, hypoxia not only promotes the expansion of MSCs^[159,160], but also influences the activity of MSCs during osteogenic differentiation^[161]. Future work *in vivo* can provide more information about clinical efficacy. Additionally, MSCs isolated from specific tissues usually maintain lineage differentiation towards a specific cell type, and this plays a crucial role in regenerative therapy^[161]. Therefore, the directional differentiation capacities in aged MSCs must be clarified following the increase in available tissue sources. Finally, many newly developing technologies, such as MVs, three-dimensional spheroid culture, and nanobiotechnology, will aid in improving aged MSC function in clinical therapies. Additionally, the functional discrepancies in various rejuvenation factors reported in different studies should be evaluated. For example, although a decline of osteogenesis capacity in aged MSCs was reported, other studies suggested that bone formation capacity was not affected in aged MSCs^[162]. The function of pigment epithelium-derived factor (PEDF) responding to the senescence is unanticipated to demonstrate the different results in different research teams^[97,163]. Liang *et al*^[97] showed that increased PEDF secretion resulted in the impaired therapeutic ability of aged MSCs. However, Cao *et al*^[163] showed that PEDF delayed cellular senescence and allowed a greater expansion of MSCs by suppressing oxidative stress and preserving differentiation potentials, compared with that in the control group. The different PEDF functions are possibly attributable to MSC heterogeneity, varying research objectives, and the specific experimental models used.

CONCLUSION

The rejuvenation of aged MSCs holds great promise for the accelerated translation of cell-based approaches (especially autologous cell administration) into clinically relevant therapies.

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Mechanisms of action of neuropeptide Y on stem cells and its potential applications in orthopaedic disorders

Jian-Qun Wu, Nan Jiang, Bin Yu

ORCID number: Jian-Qun Wu 0000-0002-6805-7746; Nan Jiang 0000-0003-2416-1653; Bin Yu 0000-0002-3109-2062.

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Jian-Qun Wu, Department of Orthopedics and Traumatology, Huadu District People's Hospital, Guangzhou 510800, Guangdong Province, China

Nan Jiang, Bin Yu, Division of Orthopaedics and Traumatology, Department of Orthopedics, Nanfang Hospital, Southern Medical University, Guangzhou 510515, Guangdong Province, China

Nan Jiang, Bin Yu, Guangdong Provincial Key Laboratory of Bone and Cartilage Regenerative Medicine, Nanfang Hospital, Southern Medical University, Guangzhou 510515, Guangdong Province, China

Corresponding author: Bin Yu, MD, PhD, Professor, Surgeon, Department of Orthopedics, Nanfang Hospital, Southern Medical University, No. 1838 North Guangzhou Avenue, Baiyun District, Guangzhou 510515, Guangdong Province, China. yubin@smu.edu.cn

Abstract

Musculoskeletal disorders are the leading causes of disability and result in reduced quality of life. The neuro-osteogenic network is one of the most promising fields in orthopaedic research. Neuropeptide Y (NPY) system has been reported to be involved in the regulations of bone metabolism and homeostasis, which also provide feedback to the central NPY system *via* NPY receptors. Currently, potential roles of peripheral NPY in bone metabolism remain unclear. Growing evidence suggests that NPY can regulate biological actions of bone marrow mesenchymal stem cells, hematopoietic stem cells, endothelial cells, and chondrocytes *via* a local autocrine or paracrine manner by different NPY receptors. The regulative activities of NPY may be achieved through the plasticity of NPY receptors, and interactions among the targeted cells as well. In general, NPY can influence proliferation, apoptosis, differentiation, migration, mobilization, and cytokine secretion of different types of cells, and play crucial roles in the development of bone delayed/non-union, osteoporosis, and osteoarthritis. Further basic research should clarify detailed mechanisms of action of NPY on stem cells, and clinical investigations are also necessary to comprehensively evaluate potential applications of NPY and its receptor-targeted drugs in management of musculoskeletal disorders.

Key Words: Neuropeptide Y; Bone marrow mesenchymal stem cells; Hematopoietic stem cells; Fracture; Osteoporosis; Osteoarthritis

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Core tip: Neuropeptide Y (NPY) system is crucial for bone metabolism and homeostasis. NPY can regulate biological effects of different types of cells through central and peripheral nervous systems. Here, we summarize recent findings regarding the roles of NPY and its receptors in bone metabolism and homeostasis, and discuss the biological actions and underlying mechanisms of NPY on bone marrow mesenchymal stem cells, hematopoietic stem cells, endothelial cells, and chondrocytes. We also review the potential applications and efficacy of NPY and NPY receptor-targeted drugs in the treatment of fracture healing, osteoporosis, and osteoarthritis.

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INTRODUCTION

As a substantial portion of the whole body, skeletal muscles are integral for locomotion and metabolic health^[1]. Musculoskeletal disorders, such as fracture, delayed/non-union, osteoporosis, and osteoarthritis, are the primary causes of disability and lead to reduced life quality. Skeletal metabolism and homeostasis are accurately regulated by neural signal networks between nervous systems and bone cells.

Recently, neuropeptide Y (NPY) has emerged as one of the major regulators of bone metabolism and homeostasis. NPY, a 36-amino-acid peptide first isolated from the porcine brain by Tatemoto^[2] in 1982, is widely distributed in the central nervous system (CNS) and peripheral nervous system^[3]. It is produced by nerve endings, and acts as a critical molecule in the interactions between nerves and the osseous system through central- and peripheral-mediated pathways^[4,5]. NPY can maintain the homeostases of bone, blood vessels, and immune system *via* different NPY receptors^[6,7]. Previous studies have indicated that NPY can stimulate proliferation, promote osteoblastic differentiation, and prevent apoptosis of bone marrow mesenchymal stem cells (BMSCs) through Y1R^[8]. In addition, NPY is also able to facilitate neuroprotection, restore bone marrow dysfunction, and thus mediate bone marrow microenvironment^[9]. Aside from BMSCs, treatment with NPY caused a decreased number of osteoclasts by promoting mobilization of hematopoietic stem cells (HSCs) *via* Y2R and Y5R. Furthermore, NPY can accelerate endothelial cell (EC) proliferation and capillary tube formation through Y1R, Y2R, and Y5R^[9,10]. As NPY possesses capacities of regulating different types of cells, it determines the relative rates of bone formation and resorption process, which is critical for prevention against bone structure damage and bone metabolic disorders^[11].

In recent years, stem cell therapy is a burgeoning field in regeneration and restoration of the impaired musculoskeletal tissues^[12]. Enrichment and differentiation of stem cells have been confirmed for the benefits in bone regeneration and maintenance of bone homeostasis. As both experiments and clinical investigations have revealed definite efficacy of stem cells in treatment of fractures, osteoporosis, cartilage, and ligament injuries^[13-15], it has become an attractive avenue of research for therapeutic applications in musculoskeletal disorders.

This article reviews the current knowledge of NPY, potential roles of NPY receptors, and interactions among NPY, NPY receptors, and stem cells, primarily BMSCs and HSCs. In addition, the potential influences of NPY on biological functions of ECs and chondrocytes, which are also involved in the development of many orthopaedic disorders, are also discussed. Furthermore, the potential applications and efficacy of NPY and its receptor-targeted drugs in the treatment of fracture, osteoporosis, and osteoarthritis are also summarized.

NPY AND RECEPTORS

Recent studies have shown that NPY participates in many physiological and psychological processes, such as inhibition of vascular smooth muscle contraction and alleviation of anxiety and depression^[16,17]. Till now, five primary NPY receptors (Y1R, Y2R, Y4R, Y5R, and y6R) have been found in mammals, and all of them belong to the superfamily of G protein-coupled receptors^[18]. Different receptors are distributed differently in the human body, play different biological functions, and have different affinities for NPY (Y2R > Y1R > Y5R, Y4R = y6R)^[19]. Y1R and Y2R are reported to be involved in bone homeostasis. Y4R is distributed in both brain and peripheral tissues^[20]. Y5R, predominant in the CNS, consistently co-localizes with Y1R^[21]. y6R, also observed in rat genome, seems to be non-functional in humans^[22].

Current evidence indicates that hypothalamic secreted NPY inhibits bone formation. Previous *in vivo* studies found that an increase of NPY in the hypothalamus led to a decreased volume of cancellous bone and inhibition of the osteoblasts activity^[23,24]. These results are similar to the finding of another study that overexpression of hypothalamus-specific NPY in the wild-type (WT) mice displayed anti-osteogenic effects^[25]. Likewise, both deficiency of NPY [NPY (-/-)] in mice and inhibition of central NPY signaling pathway can induce bone gain^[5,26]. As targeted deletion of the *NPY* gene in the hypothalamus has not been realized yet, current research of the potential effects of hypothalamus-specific NPY on peripheral stem cells may be conducted *via* the approach of isolating BMSCs or other stem cells from mice deficient in hypothalamus-specific NPY.

It is known that both Y1R and Y2R are distributed abundantly in the CNS. As an auto-receptor, Y2R is primarily located presynaptically, and inhibits NPY expression and release^[27,28]. Both hypothalamus and germline deletions of Y2R produce an identically promotive bone anabolic phenotype, implying that hypothalamic Y2R may modulate bone formation *via* CNS mechanism, and also protect against central NPY-induced bone loss^[26,29]. A previous study showed that the osteoblastic activity of the mice with double knockout of Y4R and Y2R in the hypothalamus was more obvious than those with only knockout of Y2R, demonstrating the probably synergistic role of Y4R in hypothalamic control of the bone mass^[30]. Nonetheless, targeted deletion of Y1R in the hypothalamus failed to recapitulate this increased bone mass phenotype, which had been observed in systematic deficiency of Y1R [Y1R (-/-)] mice. This implies that Y1R may participate in the regulation of bone regulation by non-hypothalamic pathways^[31]. Interestingly, double deletions of global Y1R and Y2R in mice did not result in any additive effects on bone phenotype, suggesting that Y1R and Y2R may share a common pathway in regulation of bone homeostasis^[31]. As for y6R, its mRNA is only expressed in the hypothalamus but not in bone components, such as BMSCs, osteoblasts, or osteoclasts. Compared to the WT controls, significantly decreased bone density and volumes of cortical and cancellous bone were found in the mice with y6R(-/-) in the hypothalamus, which is primarily attributed to the increasing number of osteoclast precursors in y6R(-/-) mice^[22].

Peripheral NPY acts directly in a paracrine fashion to maintain the bone homeostasis. Growing evidence shows that NPY is expressed in non-neuronal cells in the bone marrow microenvironment, such as osteoblasts^[32], osteocytes^[33], BMSCs^[8,34], and ECs^[35]. *In vitro* studies have indicated that NPY has direct effects on osteoblast lineage by inhibiting differentiation of mesenchymal progenitors and mineralization of mature osteoblasts^[33,36]. Overexpression of osteoblasts-specific NPY (Col2.3NPY) resulted in decreases in bone trabecular number, thickness, and volume^[37], whereas changes of serological NPY levels did not reveal such effects^[37]. These results imply that overexpression of local NPY may cause changes of bone phenotypes. Outcomes of clinical studies have revealed that patients with craniocerebral injury had accelerated fracture healing and higher serological NPY levels, the latter of which showed a positive correlation with the severity of craniocerebral injury^[38]. Gu *et al*^[38] inferred that serum NPY may originate from cerebrospinal fluid, as the NPY level in the serum was almost equal to that in the cerebrospinal fluid among the patients with craniocerebral injury, and severe craniocerebral injury may cause leakage of cerebrospinal fluid^[38,39].

It is definite that Y1R is expressed in osseous tissue, including adipocytes, osteoblasts, and bone marrow cells^[8,33,40-42]; however, whether Y2R is expressed in the bone or not remains in debate. Some studies reported that Y2R can be found in MC3T3 and BMSCs^[41,42], but not in osteoblasts^[43]. It is speculated that such differences may be explained by two reasons. The first reason is that Y2R exists in the bone, but may be expressed under specific conditions, and thus, it cannot always be detected. Second, potential limitations of the current techniques may also affect the detection rate. As for Y1R, both *in vitro* and *in vivo* studies have shown that the mice with knockout of

osteoblast-specific *Y1R* recapitulate the bone phenotype of germline *Y1R* deficient mice^[5,36]. These findings confirm the role of *Y1R* in inhibiting bone formation, as well as in enlarging the negative effects of NPY on osteocytes. Although the selective deletion of *Y1R* from osteoblasts did not hinder the process of fracture healing, lack of systemic *Y1R* caused delays of endochondral fracture repair^[44]. Considering that *Y1R* plays important roles in many physiological functions, aside from the above-mentioned issues, other underlying mechanisms may also account for the effects of global *Y1R* deletion on bone healing process (Figure 1).

MECHANISMS OF ACTIONS OF NPY ON BMSCs AND HSCs

NPY and BMSCs

BMSCs, isolated from bone marrow, are termed as a “fibroblast-like” osteogenic cell population. With plastic-adherent culture characteristics, BMSCs express specific surface antigens CD105 and CD90 (> 95%) but not CD45 or CD34 (< 2%)^[45], and are capable of differentiating into osteoblasts, chondrocytes, and adipocytes^[19,46]. As BMSCs play a vital role in repairing musculoskeletal tissues, fracture healing and spinal injury regeneration can be accelerated following application of BMSCs^[47]. Local injection of BMSCs has also yielded promising results in the treatment of bone nonunion and bone defect^[48].

Currently, conflicting results still exist regarding the potential role of NPY in proliferation of BMSCs^[8,36,42]. Our previous study revealed that NPY can enhance proliferation and prevent apoptosis of BMSCs in a concentration-dependent manner by activating the Wnt/ β -catenin signaling pathway. Such NPY-induced activities were partially blocked by PD160170, a *Y1R* antagonist^[8], implying that NPY-induced proliferative and anti-apoptotic effects of BMSCs may be partially achieved through *Y1R*. Another study also found that NPY is able to stimulate proliferation of BMSCs derived from rats of different ages, and this capacity was blocked by *Y5R* antagonist, demonstrating an inhibitory role of *Y5R* in the proliferation of rat BMSCs. In addition, Igura *et al.*^[42] found that NPY increased the proliferation of BMSCs of transgenic overexpression of *Y5R* in the elder rats by activating extracellular signal-regulated kinase 1/2 (Erk1/2) pathways. Aside from BMSCs, NPY can also promote the proliferation of human embryonic stem cells, which was achieved *via* NPY/*Y1R*/*Y5R* by activation of ERK1/2 pathways^[49]. However, one study failed to find a promotive role of NPY on BMSC proliferation. Lee *et al.*^[36] reported that BMSCs isolated from *Y1R* (-/-) mice formed a greater number and larger size of colonies than the WT controls, implying that NPY may inhibit BMSC proliferation.

Apart from its potential influences on BMSC proliferation, NPY can also facilitate the migration of BMSCs by upregulated expression of CXC chemokine receptor 4^[50], which is in accordance with the finding of our study that NPY therapy significantly increased the total migration distance and speed of BMSCs^[51].

In addition to the controversy regarding the effect of NPY on the proliferation of BMSCs, the potential activities of NPY on osteogenic differentiation of BMSCs and the underlying mechanisms are also in debate. Some studies found that NPY stimulated the differentiation of BMSCs into osteoblasts, which was supported by upregulating the expression of alkaline phosphatase (ALP), collagen type I (COL-I), osteocalcin (OCN), and runt-related transcription factor 2 (Runx2) through the Wnt signaling pathway^[51,52]. Other studies reported that NPY inhibited osteogenic differentiation of BMSCs, evidenced by the findings of decreased ALP and OCN expression, and reduced mineralization of BMSCs as well^[41]. Besides, another study also found the inhibitory effect of NPY on isoprenaline-induced differentiation into osteoblasts from BMSCs^[40]. Interestingly, BMSCs isolated from NPY (-/-) mice display an increased ability in osteogenic differentiation, which was confirmed by increases in ALP activity, OCN gene expression, and mineralization^[52]. These diverse outcomes can be explained by the fact that NPY-induced osteogenic differentiation of BMSCs may be achieved *via* auto-regulation mechanisms.

Growing evidence has revealed that auto-regulation mechanisms of NPY may correlate to the plasticity of its receptors. It has been noted that NPY led to upregulated expression of *Y1R* throughout BMSC osteogenic differentiation^[36,38,41]. In a recent study, Wee *et al.*^[52] found that during osteogenic differentiation of BMSCs in the WT mice, the expression of *Y1R* was increased while NPY was decreased. However, as in NPY (-/-) mice, *Y1R* expression level did not alter during differentiation, demonstrating that increased *Y1R* expression during BMSC differentiation may be assisted or induced by NPY. Outcomes of NPY or its receptor gene knockout animal

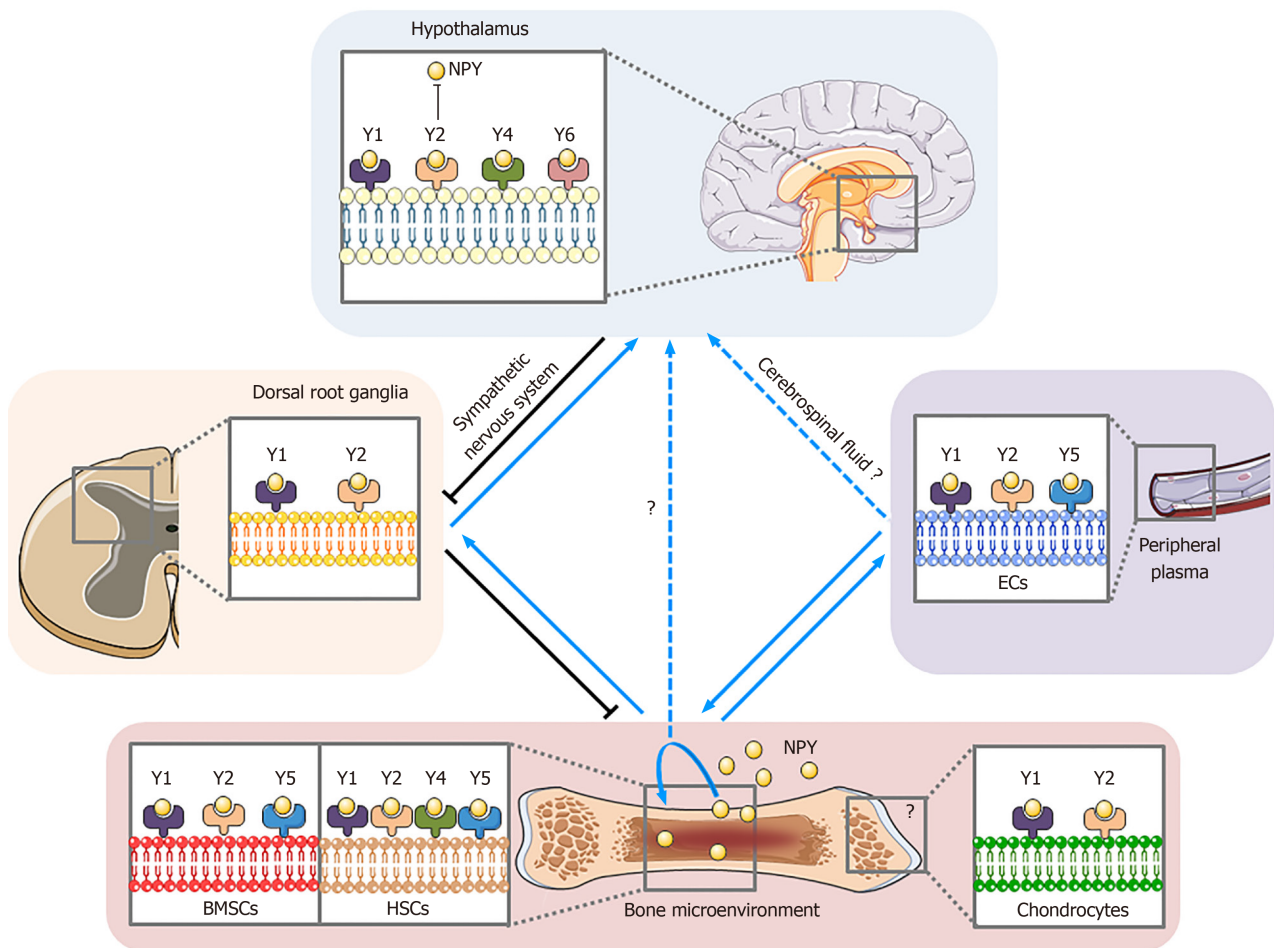


Figure 1 Neuropeptide Y is involved in the regulation of bone microenvironment through central- and peripheral-mediated pathways via different neuropeptide Y receptors. NPY: Neuropeptide Y; BMSCs: Bone marrow mesenchymal stem cells; HSCs: Hematopoietic stem cells; ECs: Endothelial cells.

models revealed that the presence of functional Y1R directly hindered the osteogenesis of BMSCs or bone cells, as evidenced by the finding that BMSCs isolated from Y1R (-/-) mice displayed an increased capacity of osteogenic differentiation^[36]. An *in vitro* experiment showed that blockade of Y1R by PD160170 facilitated osteogenic differentiation of BMSCs^[53]. On the contrary, Dong *et al*^[34] reported that melatonin can upregulate the expression of NPY and Y1R, and promote MSC osteoblastic differentiation. Apart from BMSCs, lack of Y1R also promoted differentiation of mesenchymal progenitor cells and activated mature osteoblasts^[36]. Yahara *et al*^[54] also noticed that inhibition of Y1R increased the ALP activity and mineralization in mouse pre-osteoblast MC3T3-E1 cells.

Aside Y1R, Y2R may also participate in osteogenic differentiation of BMSCs, which is supported by the finding that BMSCs, treated with either NPY1-36 (universal Y2R agonist) or PYY3-36 (Y2R preferring agonist), revealed significantly elevated levels of ALP activity and OCN expression. Such effects of NPY1-36 were blocked by a Y2R antagonist, BII0246, and a marked decrease of Y1R protein level was also found following treatment with exogenous PYY3-36 or NPY1-36^[41].

During osteogenic differentiation of BMSCs, potential interactions may exist between Y1R and Y2R^[42,43]. By detecting the NPY ligand-receptor system in BMSCs derived from rats of different ages, Igura *et al*^[42] found that, although NPY expression increased with age, Y1R protein was upregulated whereas Y2R protein was downregulated with an increase in age. In addition, Lundberg *et al*^[43] found that the lack of Y2R signaling mediated downregulation of Y1R in BMSCs, which was proved by the finding of decreased expression of Y1R in BMSCs from Y2R (-/-) mice. They inferred that downregulation of Y1R is possibly due to the lack of feedback inhibition of NPY release and resulted in elevated levels of NPY, which in turn caused subsequent overstimulation of Y1R, following desensitization and downregulation of the Y1R population^[43]. Moreover, alternation of Y1R expression may have different

effects on NPY. The precursor osteogenic cells (*e.g.*, BMSCs and osteoblast precursor cells), which are able to inhibit osteogenic differentiation through Y1R, have low expression levels of Y1R. However, in osteogenic conditions (*e.g.*, osteogenic induction medium), Y1R expression in these cells is increased, with Y2R expression decreased.

In addition to Y1R and Y2R, y6R may also be involved in the regulation of BMSC differentiation into osteoblasts. BMSCs isolated from y6R (-/-) mice showed significant reductions of ALP, osterix, and mineralizing surface, implying possibly opposite roles of Y6R to those of Y1R and Y2R in BMSC differentiation and activities^[22].

Currently, some studies also reported potential mechanisms of NPY in mediation of BMSC osteogenic differentiation from another perspectives. Gu *et al*^[38] indicated that NPY can directly promote the osteogenic differentiation of MSCs by upregulating Runx2. Ma *et al*^[55] reported that the anabolic activity of osteoblasts treated with NPY may also enhance the gap junction intercellular communication (GJIC). Tang *et al*^[56] noticed that the levels of NPY and p-ERK1/2 in fracture model rats were significantly higher than those in the controls. They also found that use of BIBP3226, a Y1R antagonist, inhibited the fracture healing process by downregulating the p-ERK expression in the fracture site, indicating that the ERK pathway may participate in the NPY-induced effects on fracture healing. Additionally, Sharma *et al*^[57] also observed that activation of ERK could facilitate osteogenic differentiation of human MSCs.

In summary, considering the still existing controversies regarding the role of NPY in BMSCs and still not-well-understood mechanisms, future more studies are warranted to provide more definitive evidence regarding the links between NPY/NPY receptors and BMSCs.

NPY and HSCs

HSCs, or hematopoietic stem/progenitor cells, responsible for regeneration and repopulation of all blood cell lineages, contact osteoblasts in endosteal microenvironments or sinusoidal endothelium^[58]. NPY receptors Y1, Y2, Y4, and Y5 were found to be highly expressed in HSCs, and NPY plays a crucial role in the proliferation and mobilization of HSCs^[59,60].

Growing evidence has suggested that NPY acts directly or indirectly in the regulation of HSC proliferation. NPY can directly inhibit the proliferation of HSCs in cell cultures, as confirmed by an increased number of HSCs in G0 phase, with decreased numbers of cells in S and G2/M phases^[60]. Besides, the number of HSCs in NPY (-/-) mice is decreased, suggesting that NPY may protect HSCs in the bone marrow microenvironment^[9,61].

In addition to potential influences on HSC proliferation, NPY and its receptors are also involved in regulating the survival and mobilization of HSCs. It was reported that NPY/Y1R can improve the survival and apoptosis of HSCs, which maintains the survival of nestin⁺ cells, and thus be linked to retention of HSCs^[9]. NPY-induced biological effects on HSCs, osteoblasts, and osteoclasts play an important role in the process of fracture healing. Nonetheless, detailed mechanisms of such effects remain largely unclear. Several studies explored the underlying mechanisms from different perspectives. Park *et al*^[61] indicated that the effect of NPY on HSC mobilization might be achieved by increasing the expression levels of matrix metalloproteinase 9 (MMP-9) in osteoblasts *via* Y1R, which was strengthened by the finding that NPY failed to display a positive activity on HSC mobilization in mice with Y1R (-/-) in osteoblasts. Singh *et al*^[59] reported that NPY3-36, a agonist of Y2R and Y5R, facilitated the mobilization of HSCs to the peripheral blood, whereas selective Y2R and Y5R antagonists hindered such activity. It has been noted that NPY can be also secreted by HSCs, indicating that HSCs may exert regulatory feedback on itself by releasing NPY^[9]. In ovariectomized mice, NPY therapy could help reduce the bone loss due to HSC mobilization, and result in an increased number of osteoblasts and a decreased number of osteoclasts^[61]. Using an ovariectomy-induced osteoporosis mouse model, Park *et al*^[62] also found that NPY-based recombinant peptides could relieve ovariectomy-induced bone loss and may be used for osteoporosis treatment.

In summary, current evidence suggests that NPY is able to induce the rapid mobilization of HSCs into the peripheral blood, and increase the number of osteoblasts. Therefore, it is reasonable to believe that a comprehensive understanding of the role of NPY in HSCs may pave the way for its future clinical applications^[63].

MECHANISMS OF ACTIONS OF NPY ON ECs AND CHONDROCYTES

NPY and ECs

NPY-positive fibers predominantly localize alongside blood vessels in bone tissue and bone marrow, and associate with EC migration, capillary tube formation, and self-renewal^[10,64,65]. ECs express Y1R and Y2R and can produce, store, and respond to NPY, suggesting an autocrine regulatory mechanism of NPY in the endothelium (Figure 2)^[10,35,66].

In vitro studies have revealed that NPY can promote the migration and capillary tube formation of human ECs *via* Y1R, Y2R, and Y5R^[10,65]. Previous studies also indicated that NPY-induced angiogenic effect on ECs was achieved primarily through Y2R^[65,67]. Furthermore, NPY can regulate the angiogenic process by influencing the proliferation of ECs, which was achieved mainly *via* Y5R^[10]. NPY3-36, an agonist of Y2R and Y5R, was found to be able to reduce EC contact and increase vascular permeability, and selective Y2R and Y5R antagonists restored the vascular integrity^[59]. Interactions may exist among BMSCs, HSCs, and ECs *via* NPY. It has been observed that NPY originating from platelet lysate caused an decreased angiogenic activity of human adipose stromal cells, which may be linked to reduced expression of vascular endothelial growth factor (VEGF) and a lower intracellular calcium level^[68]. As a ubiquitous and potent peptide, VEGF is involved in many angiogenic cascades. Increased levels of VEGF facilitate angiogenesis and osteoblastic differentiation of BMSCs^[69], and the level of VEGF secreted by BMSCs is elevated following treatment with NPY^[51]. Wang *et al*^[50] found that NPY promoted endothelial differentiation and tube formation of BMSCs, the latter of which is involved in all the stages of EC angiogenesis, including survival and proliferation, migration, tube formation, and maturation of blood vessels^[70].

NPY and chondrocytes

Although chondroblasts and osteoblasts share the same progenitor reservoir (BMSCs), specific effects of NPY on chondrocytes have not been clarified. However, anatomical studies have indicated that NPY-positive sympathetic nerve fibers are located in cartilage, and chondrocytes can also secrete NPY^[32].

NPY can promote the proliferation of both chondrocytes and articular cartilage, and the effect of NPY on chondrogenesis may be achieved through autocrine mechanisms *via* Y1R^[32]. A new study found that intra-articular injection of NPY caused more severe osteoarthritis phenotypes, which was evidenced by more severe cartilage degradation and fibrillation, whereas a combination of NPY with BIIE0246 (Y2R antagonist) but not BIBO3304 (Y1R antagonist) significantly alleviated the above negative effects, indicating that Y2R may play an important role in NPY-induced chondrocyte hypertrophy and cartilage matrix degradation^[71]. In addition, NPY-induced chondrocyte hypertrophy was also marked by increased levels of col10a1 (a biomarker indicating hypertrophy of chondrocytes), MMP-13, and ADAMTS-5 through activation of mTORC1 in a Y2R-dependent manner^[71]. Chen *et al*^[72] found that NPY markedly augmented the expression of Col2a1 (a biomarker indicating proliferation of chondrocytes), Col10a1, and OCN in the murine chondrogenic cell line ATDC5. And inhibition of Y1R partly hindered the capability of NPY, demonstrating that Y1R may participate in NPY-induced activities (proliferation, chondrogenesis, and mineralization) in ATDC5 cells^[72]. It is known that Runx2 and Osterix are biomarkers for chondrocyte differentiation and cartilage mineralization. In the Y1R (-/-) mice, the expression levels of Runx2 and Osterix increased in the long bones^[36], both of which facilitated the formation of cartilage callus. Based on current findings, potential strategies to solve NPY-related hypertrophy of chondrocytes and cartilage degradation may be a research hotspot in the future.

APPLICATIONS OF NPY IN ORTHOPAEDIC DISORDERS

Fracture

Fracture healing process can be divided into inflammatory, reparative, and remodeling stages. During the initial phase, BMSCs are recruited to the fracture site and differentiate into chondrocytes simultaneously, and the level of NPY in the peripheral blood is increased^[56]. NPY- and Y1R-positive BMSCs and osteoblasts can be found in the new osseous tissue^[64]. Innervation of NPY occurs in a spatio-temporal dependent manner in the inflammatory and remodeling stages^[73], demonstrating

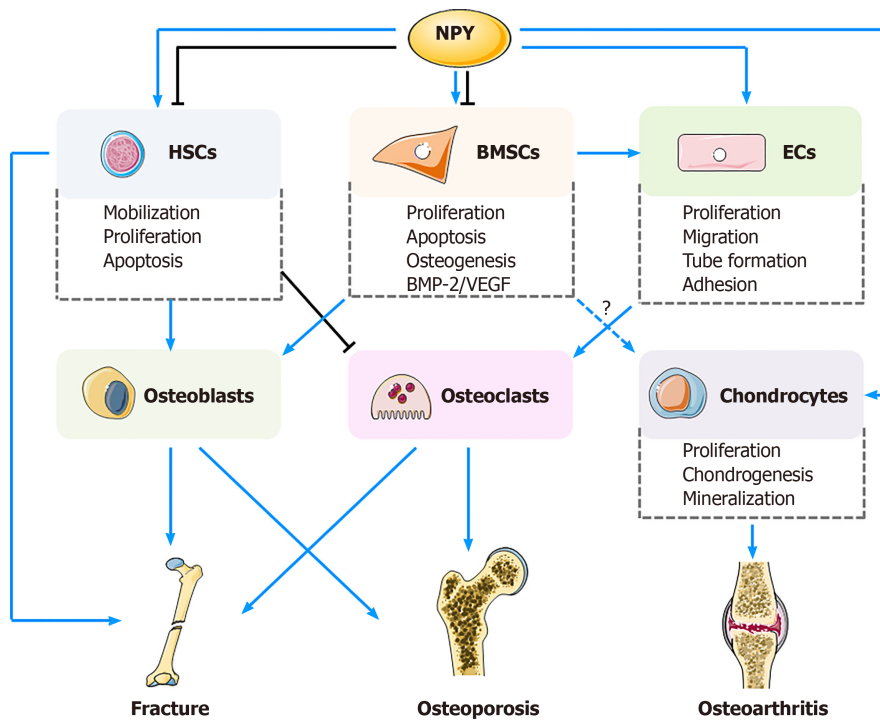


Figure 2 Neuropeptide Y exerts potential regulatory effects on biological functions of bone marrow mesenchymal stem cells, hematopoietic stem cells, endothelial cells, and chondrocytes, and their potential applications in management of fracture healing, osteoporosis, and osteoarthritis. NPY: Neuropeptide Y; BMSCs: Bone marrow mesenchymal stem cells; HSCs: Hematopoietic stem cells; ECs: Endothelial cells; BMP-2: Bone morphogenetic protein 2; VEGF: Vascular endothelial growth factor.

different functions of NPY among different fracture stages. Previous studies found that the volumes of cortical and cancellous bones in NPY-deficient mice were significantly increased, which may result from elevated osteoblast activities and upregulated expression of Runx2 and Osterix^[23,24]. Lundberg *et al*^[49] reported that, compared with the WT controls, Y2R (-/-) mice presented with greater bone mass, which may correlate with the reinforced abilities of BMSCs, thus being able to produce more mineralized extracellular matrix as well as increased expression of ALP and OCN. As mentioned previously, NPY can directly increase the number and viability of BMSCs by promoting their proliferation and inhibiting apoptosis^[8], together with increased osteogenic differentiation and BMP-2 expression^[51]. Aside from *in vitro* and *in vivo* experiments, clinical observations also confirmed the role of NPY in fracture healing process. Gu *et al*^[38] reported that, compared with those with a single fracture, patients with a fracture and accompanying traumatic brain injury had higher serological levels of NPY and accelerated fracture healing process. This finding can be explained by the fact that NPY can directly promote osteogenic differentiation of MSCs^[38]. Besides, Y1R antagonist play a direct role in regulation of BMSCs. Liu *et al*^[53] noted that treatment with PD160170, a Y1R antagonist, promoted osteogenic differentiation of BMSCs, with higher expression of COL-I, OCN, and Runx2. The *in vivo* outcomes also showed increases in bone volume/total volume (BV/TV), bone mineral density, and bone trabeculae number after PD160170 intervention^[53]. However, considering the still limited evidence from clinical investigations, more studies are necessary. In short, NPY can induce proliferation and angiogenic and osteogenic differentiation of BMSCs, facilitating bone regeneration.

VEGF is one of the most important components in angiogenesis, which is regarded as an essential factor that directly influences the fracture healing process^[74]. BMSCs can promote vessel sprouting and vascularization, which is considered to be important for bone formation, whilst ECs can accelerate bone repair by facilitating the recruitment of osteoclast precursors and stimulating the osteoclastogenic process^[75]. NPY can also facilitate vessel sprouting, adhesion, migration, proliferation, and capillary tube formation in ECs^[10,59,65]. Also, during the process of angiogenesis, NPY receptors are indispensable. For example, Lee *et al*^[67] observed that NPY-induced aortic sprouting and *in vivo* matrigel capillary formation were decreased by 50% after deleting Y2R gene or using its antagonists, implying the vital role of Y2R in angiogenesis. During the angiogenesis process, continuous nutrients and cytokines are transported to the

fracture site, providing synergistic effects in fracture healing.

Osteoporosis

Osteoporosis, a disorder characterized by progressive bone loss and thus an increased risk of fracture, often results from menopausal loss of estrogen in women^[76]. Currently, the primary methods to investigate the effects of NPY system on osteoporosis include examining bone phenotypes in gene knockout models and using NPY receptor antagonists.

Increasing number of studies indicated that Y2R is essential in mediating bone gain and loss. For example, mice lacking Y2R globally or specifically in the hypothalamus are characterized by greater bone loss compared to the WT controls, indicating that Y2R is critical in protection against bone loss^[77,78]. In addition, ovariectomized mice injected with JNJ-31020028, a Y2R antagonist, showed increases in the whole-body bone mineral density, vertebral trabecular bone volume, and trabecular thickness^[79] (Table 1). NPY3-36, an agonist of Y2R and Y5R, strongly lowered the expression level of receptor activator of Nfkb ligand (RANKL) and upregulated the basal levels of osteoprotegerin (OPG) in BMSCs, suggesting that Y2R may induce bone formation by affecting the expression of RANKL and OPG in BMSCs^[40,41]. These results also hint that selective pharmacological manipulation of Y2R may be a potential strategy for anabolic treatment of osteoporosis.

Aside from Y2R, Y1R may be also involved in regulation of bone homeostasis. Sousa *et al*^[80] found that in mice, oral administration of BIBO3304, a Y1R antagonist, led to increased rates of mineral deposition in both cortical and cancellous bones, which may result from an increased number of osteoblasts following direct actions of NPY/Y1R on osteoclasts^[80] (Table 1). Although there is still a lack of enough evidence to support the belief that NPY can improve the status of osteoporosis *via* direct regulations of BMSCs, based on the potential role of Y1R in osteogenic differentiation of BMSCs, it can be speculated that inhibition of Y1R may be a potential anabolic strategy for prevention of bone loss.

Nonetheless, other studies displayed different outcomes. Tang *et al*^[56] reported that, compared with the controls, the rats treated with the Y1R antagonist BIBP3226 showed remarkable reductions in volumes of callus bone and tissue, and BV/TV as well. This demonstrates a potential negative effect of Y1R antagonist on bone healing (Table 1). Similarly, Sousa *et al*^[44] also observed a lower rate of bone healing in Y1R (-/-) mice, with a decreased volume of bone callus and a weaker bone strength. Osteoclasts of hematopoietic origin also express high levels of NPY and Y1R^[33]. Since osteoclasts are differentiated from HSCs, NPY can effectively alleviate ovariectomy-induced bone loss by decreasing the number of osteoclasts in bone marrow microenvironment through HSC mobilization, and increasing the number of osteoblasts as well^[61]. These findings imply that NPY may act as a potential indicator of HSC mobilization, and supplementation of NPY may provide a therapeutic effect for bone loss.

Osteoarthritis

Stem cells can provide preventive and regenerative effects in early stages of osteoarthritis^[81]. Neurotransmitters, such as substance P (SP) and calcitonin gene-related peptide (CGRP), modulate osteo-chondrogenic differentiation of mesenchymal progenitor cells during endochondral ossification in limb development^[82]. Guo *et al*^[83] found that fracture-related pain in a rat model was partially relieved by an NK1 (substance P receptor) antagonist LY303870. In a rat knee model evaluating SP coupled with self-assembled peptide hydrogels, Kim *et al*^[84] observed that cartilage regeneration and regenerative properties were markedly improved by recruiting MSCs. However, to date, few studies have addressed the role of NPY and its receptors in chondrocytes and their potential applications in osteoarthritis therapy.

One of the most frequent symptoms of osteoarthritis is pain of the affected joint, which associates with irritation of sensory nerve endings following pathological changes in the subchondral bone and synovial lining, with neuropeptide-containing nerves in the joint tissue as an important regulatory element^[85,86]. NPY is able to bind to free nerve endings in accessory ligaments, synovium, subchondral bone, menisci, articular cartilage, and periosteum^[87], and changes afferent sensitivity^[88]. The visual analog scale (VAS) score, used to rate pain, was negatively correlated with the mean optical density values for NPY by immunohistochemical analysis in all patients with osteoarthritis, implying that NPY may be involved in the generation of pain^[89]. Similarly, the mean level of CGRP in the synovial tissue of patients with severe osteoarthritis-related pain (VAS > 6) was significantly higher than that of patients with moderate to lower pain (VAS < 6)^[90]. In another study, higher levels of CGRP were detected in the infrapatellar fat pad in patients with knee osteoarthritis, which is

Table 1 Effects of neuropeptide Y receptor-targeted drugs on bone metabolism

| Antagonist | Bone phenotype | Administration and subjects |
|---|---|--|
| Y1R antagonist BIBP3226 ^[56] | Callus tissue volume ↓, callus bone volume and callus ↓, BV/TV ↓ | Intraperitoneal injection Sprague-Dawley rats |
| Y2R antagonist JNJ-31020028 ^[79] | Vertebral trabecular bone volume ↑, bone mineral density ↑, trabecular thickness ↑; P1NP and CTX biomarkers ↓ | Intraperitoneal injection Ovariectomized Mice |
| Y1R antagonist BIBO3304 ^[80] | Osteoblast activity ↑, cortical and cancellous bone volumes ↑; no adverse effects | Oral administration Mice |

P1NP: Procollagen type 1 N-terminal pro-peptide; CTX: Collagen type I C-telopeptide; BV/TV: Bone volume/total volume.

implicated as a possible cause of osteoarthritis development and related pain^[91].

Traditionally, the rationale application of MSCs for management of osteoarthritis stems from their ability to differentiate into chondrogenic lineage rather than osteoblasts, which can help improve degeneration of the cartilage, and alleviate joint damage and related pain^[92]. A decrease in the subchondral bone lesions may help reduce joint pain, which may be a future treatment target in relief of osteoarthritis-related pain^[93]. Besides, NPY can increase the VEGF expression and promote osteoblastic differentiation and angiogenesis of BMSCs^[38,51,55]. As cartilage does not contain blood vessels, it may be considered a hostile environment for spreading of vascular channels^[82]. VEGF, a crucial regulator of angiogenesis, can induce tube formation activity into cartilage channels, likely resulting in calcification and stiffness of subchondral bone, accompanied by increased innervation and subsequent increases in nociceptors^[94]. Therefore, blocking NPY could be of interest in pain treatment and osteoarthritis prevention.

Inflammation plays a crucial role in the pathogenesis of osteoarthritis. Prostaglandins are the key mediators of inflammation and pain in osteoarthritis^[87]. NPY is considered to have pro-inflammatory effects. In a clinical study, Hernanz *et al*^[95] found that the level of NPY in the synovial fluid of the knee joint in patients with rheumatoid arthritis was higher than the healthy controls, and NPY stimulated the expression of interleukin-1 β (IL-1 β), IL-6, and tumor necrosis factor- α (TNF- α). In a murine chondrogenic cell line, NPY was found to be able to promote proliferation and increase viable cell count of ATDC5 cells. Besides, the chondrogenic differentiation of ATDC5 can be enhanced by NPY *via* upregulating Runx2 and Col10a1. In the tissue engineering field, stem cell-scaffold-NPY combinations may be used to repair cartilage and tissues.

NPY receptor-targeted drugs

As mentioned previously, Y1R and Y2R antagonists have been applied to minimize the bone loss caused by different musculoskeletal disorders. Y1R and Y2R have been identified as novel therapeutic targets for the treatment of obesity and cancer^[96,97]. Recently, a group of Y1R antagonists have been commercially available. Among these, BIBO3304, a Y1R antagonist, is the most potent^[98]. However, the effect and efficacy of BIBO3304 have been only evaluated in animals, and clinical trials are required to confirm its role^[56,79,80] (Table 1).

CONCLUSION

This review introduces NPY and NPY receptors, and the potential mechanisms of actions of NPY on BMSCs, HSCs, ECs, and chondrocytes. NPY exerts different biological effects in different types of cells, including proliferation, apoptosis, differentiation, migration, mobilization, and cytokine secretion. NPY and its receptors play important roles in promoting bone union and anti-osteoporosis by regulating relative cell functions. Currently, limited studies have investigated the role of NPY in chondrocytes and its efficacy in controlling pain and inflammation in osteoarthritis. Improved clinical investigations addressing the role of NPY and its receptors in orthopaedic disorders may provide new insights into the stem cell research and

therapy.

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Stem cell treatments for oropharyngeal dysphagia: Rationale, benefits, and challenges

Eric K Tran, Kevin O Juarez, Jennifer L Long

ORCID number: Eric K Tran 0000-0003-4506-9266; Kevin O Juarez 0000-0002-5104-6047; Jennifer L Long 0000-0002-4185-2328.

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Eric K Tran, David Geffen School of Medicine, University of California-Los Angeles, Los Angeles, CA 90095, United States

Kevin O Juarez, Department of Otolaryngology, Yale School of Medicine, New Haven, CT 06511, United States

Jennifer L Long, Department of Head and Neck Surgery, David Geffen School of Medicine, University of California-Los Angeles, Los Angeles, CA 90095, United States

Jennifer L Long, Greater Los Angeles VA Healthcare System, Los Angeles, CA 90073, United States

Corresponding author: Jennifer L Long, MD, PhD, Associate Professor, Department of Head and Neck Surgery, David Geffen School of Medicine, University of California-Los Angeles, 650 Charles Young Dr, CHS Room 62-150, Los Angeles, CA 90095, United States. jlong@mednet.ucla.edu

Abstract

Dysphagia, defined as difficulty swallowing, is a common symptom negatively impacting millions of adults annually. Estimated prevalence ranges from 14 to 33 percent in those over age 65 to over 70 percent in a nursing home setting. The elderly, those with neurodegenerative diseases, head and neck cancer patients, and those with autoimmune conditions such as Sjögren's syndrome are disproportionately affected. Oropharyngeal dysphagia refers specifically to difficulty in initiating a swallow due to dysfunction at or above the upper esophageal sphincter, and represents a large proportion of dysphagia cases. Current treatments are limited and are often ineffective. Stem cell therapy is a new and novel advancement that may fill a much-needed role in our treatment regimen. Here, we review the current literature regarding stem cell treatments for oropharyngeal dysphagia. Topics discussed include tissue regeneration advancements as a whole and translation of these principles into research surrounding tongue dysfunction, xerostomia, cricopharyngeal dysfunction, and finally an overview of the challenges and future directions for investigation. Although this field of study remains in its early stages, initial promising results show potential for the use of stem cell-based therapies to treat oropharyngeal dysphagia and warrant further research.

Key Words: Dysphagia; Xerostomia; Hemiglossectomy; Stem cells; Myoblasts;

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Mesenchymal stem cells

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Core Tip: Oropharyngeal dysphagia, despite its widespread prevalence, is a difficult condition to treat, particularly in those who have undergone irradiation or resection in the head and neck. This challenge stems from the lack of native functional tissue upon which current therapies such as physical rehabilitation rely. There have been several studies examining the use of stem cell therapy as a potential new treatment option for these patients. Our objective is to review and consolidate the current literature regarding this topic and discuss the recent advancements, challenges, and future directions for research in this field.

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INTRODUCTION

Dysphagia is an extremely common yet morbid condition affecting over 9 million or over 1 in 25 adults in the United States annually^[1]. Of those reporting swallowing problems, 32% report their condition to be moderate while 25% perceive it as a large problem greatly impacting their quality of life. Stroke is the most common etiology followed by other neurologic diseases such as Parkinson's disease, amyotrophic lateral sclerosis, and muscular dystrophy^[2]. Head and neck cancer and its associated treatments, including resection and irradiation, often cause oropharyngeal dysphagia as well.

Given the oropharyngeal structures' location and vital function in promoting a patent airway, speech articulation, and deglutition, damage to these structures and resulting dysphagia leads to significantly increased risk for malnutrition, aspiration pneumonia, and death. Despite the significant morbidity associated with this condition however, there exists few reliable treatments that have proven to dramatically improve outcomes. Current therapies are limited and often heavily rely on physical rehabilitation of oral cavity and oropharynx swallowing function. These include isometric and resistance lingual strengthening exercises in cases of impaired tongue functioning or muscles intended to strengthen oral cavity and pharyngeal muscles^[3,4]. A study conducted by Robbins *et al*^[5] showed that among ten stroke patients who underwent isometric lingual exercise program, all subjects showed significantly increased isometric and swallowing pressures, reduction in airway invasion, and even increased lingual volume. Still, although improvement has been found in young and older healthy adults and those suffering from stroke, this success has not reliably translated toward head and neck cancer patients, who may have had extensive resection or irradiation in tumor removal. In these patients, the lack of normal oropharyngeal tissue impedes the efficacy and feasibility of swallowing rehabilitation exercises. Thus, these patients may benefit from newer, more innovative therapies.

Stem cell therapy has, in recent years, generated much interest in regards to its therapeutic potential to replace damaged tissue, guide wound healing, and restore function. Current research on this topic is extremely limited and primarily in investigational stages of study, although a few have advanced to clinical trials^[6]. We aim to describe the current literature regarding the promising results of stem cell administration to restore swallowing function.

PHYSIOLOGY OF SWALLOWING

To understand dysphagia, we must first appreciate the mechanisms and anatomy underlying normal physiologic swallowing (Figure 1). Typically, swallowing consists of three stages: An oral stage, pharyngeal stage, and esophageal stage. The oral stage is

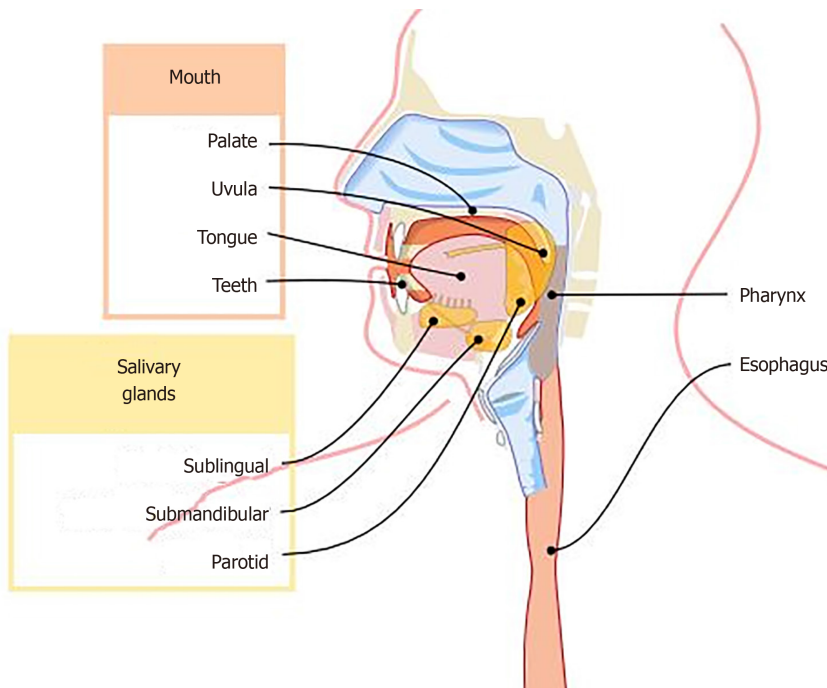


Figure 1 Anatomy of upper gastrointestinal tract. Depiction of upper gastrointestinal tract which clearly delineates the anatomically correlated oral, pharyngeal, and esophageal stages of swallowing. Complex interactions between numerous components facilitates this process and dysfunction in any may lead to dysphagia. This depiction also illustrates potential target areas for stem cell intervention.

further subdivided into an oral preparatory stage where a bolus of food or liquid is taken into the mouth and held in the anterior portion of the oral cavity, and an oral propulsive stage where this bolus is propelled posteriorly by the tongue into the oropharynx. Variations exist between swallowing liquids and solids. Solid food swallowing requires mastication and allows food to reside in the posterior oral cavity during bolus preparation. Liquids transit much more rapidly and are more difficult to control. Following the oral phase, the pharyngeal phase consists of two vital functions: Propulsion of the food downwards and through the upper esophageal sphincter (UES), and protection of the airway to prevent aspiration. First, the soft palate elevates and forms a seal with the posterior pharynx, preventing food from traveling upwards into the nasopharynx. The pharyngeal constrictor muscles then contract rhythmically, squeezing the bolus downwards towards the UES. Opening of the UES to allow passage into the esophagus is dependent on relaxation of the cricopharyngeus muscle, pressure from the bolus to expand the sphincter, and mechanical forces exerted by the thyrohyoid and suprahyoid muscles which lift the larynx and pull open the UES. Concurrently, the vocal folds close to seal the glottis and as the entire larynx is lifted by the thyrohyoid and suprahyoid muscles, the epiglottis is pressed against the laryngeal inlet and the oblique interarytenoid muscles contract to complete the seal. This serves to protect the airway. Finally in the esophageal stage, the bolus is propelled downwards *via* a peristaltic wave. The upper 1/3 of the esophagus is comprised primarily of skeletal muscle while the lower 2/3 is largely smooth muscle. The lower esophageal sphincter opens to allow passage into the stomach^[7,8]. The entire process requires precise timing to transfer from one phase to the next. Given the enormous complexity and coordination required in swallowing, it is unsurprising that dysfunction of involved structures along any of these steps can result in dysphagia. Stem cell-based replacement therapy, thus, attempts to restore normal tissue or function in each of these structures.

STEM CELL THERAPIES FOR LARYNGEAL MUSCLE

Within the field of skeletal muscle regeneration, laryngeal muscles are of particular interest with regards to dysphagia given the function of the larynx in protecting the airway during deglutition. Vocal fold adduction is an important mechanism in preventing aspiration and facilitating coughing should particles enter the airway, as may often occur among patients suffering from dysphagia^[9]. Denervation models of

the laryngeal muscles mimic iatrogenic injuries to the recurrent laryngeal nerves or neurodegenerative diseases that commonly cause problems with swallowing. Additionally, findings regarding regeneration of bulbar muscle (innervated by cranial nerves) may differ from somatic skeletal muscles, and thus be more directly applicable to the bulbar muscles of swallowing.

Halum *et al*^[10] described a denervation model of vocal fold paralysis with subsequent autologous muscle-derived stem cell (MDSC) injection. 16 male rats underwent unilateral denervation of the recurrent laryngeal nerve (RLN). Myoblasts were isolated from sternocleidomastoid muscle biopsy and cultured at subconfluency to avoid myotube formation. One month post injury, autologous MDSCs labeled with a fluorescent marker were injected into the laryngeal thyroarytenoid (TA) muscle of half the animals while the remaining half received saline alone. MDSC persistence was found at both two weeks and two months post-treatment, with evidence of fusion with native muscle fibers at two months. TA muscle volume was increased in the myoblast injection group at both time points, and muscle fiber diameter increased within the myoblast injection group by two months. Upon laryngoscopy visualization, two animals achieved weak adductor motion of the vocal folds at two months, while no adduction was observed among the control group. Researchers did not find significant differences in reinnervation between the groups indicating that the improvements were due to muscle enhancements rather than neurologic signals^[10]. As a follow up, the same group studied the use of trophic factors to enhance MDSC survival following injection. They found co-administration with insulin-like growth factor (IGF-1) and ciliary neurotrophic factor (CNTF) significantly increased survival, and cell persistence correlated with decreased myofiber atrophy^[11]. Furthermore, CNTF was found to enhance neuron outgrowth and branching within vagus nerve motor neuron cultures *in vitro*^[12]. When these findings were translated to a larger model utilizing canines, increased laryngeal adductor force was observed in a small group of MDSC-injected larynges. Three dogs underwent RLN injury and were separated into non-injection control, MDSC injection, and MDSC-enhanced injection as defined by use of acetylcholine chloride to increase motor end plate conduction. Compared to pre-injury, the non-injected control demonstrated adduction force measurements 60% of baseline, while the MDSC-injected group and MDSC-enhanced injection group demonstrated 98% and 128% adductor force measurements respectively^[13]. While swallowing function was not directly measured in any of these studies, clinical experience links laryngeal adductor function with prevention of aspiration during swallowing in a subset of patients.

STEM CELL THERAPIES FOR TONGUE DYSFUNCTION

Several groups have attempted stem cell therapies in the tongue intended to improve swallowing following treatment for head and neck cancer. Current treatments have not reliably improved swallow function in patients who have undergone partial and total glossectomy, which remain mainstay for treatment of cancer of the tongue. Post-surgical outcomes have revealed higher incidence of inadequate tongue control, inadequate chewing, delayed oral transit time, aspiration or penetration, residue within the vallecula and piriform recesses, and inadequate laryngeal elevation after surgery^[14], leading to varying degrees of dysphagia. The base of tongue is particularly critical for swallow function, with resection of only a quarter of the tongue base resulting in impaired ability to trigger the pharyngeal swallow^[15,16]. Current treatment consists of reconstructive options including myocutaneous, pedicled, and free flaps to restore bulk to the tissue, albeit typically without innervation. The field lacks clear guidelines and research into optimal reconstructive strategies, and long-term functional outcomes are poor. In a multicenter retrospective study comparing long-term functional outcomes of total glossectomy patients with or without laryngectomy, Lin *et al*^[17] report 55% gastrostomy tube dependence at last follow-up, similar to the 50% dependence found by Dziegielewski *et al*^[18] and 71% dependence by Rihani *et al*^[19]. Clearly, newer approaches are needed which can more closely imitate native, normal tissue.

Among the first to investigate the use of muscle stem cell tissue engineering for tongue defects was Kim *et al*^[20] in 2003, who described the use of a collagen-rich hydrogel populated with neonatal rat myoblasts for a partial glossectomy defect. Thirty rats underwent unilateral mucosal-sparing glossectomy, producing pockets which were then filled with either saline, collagen-rich hydrogel alone, or collagen-rich hydrogel with myoblasts. After six weeks, the group receiving the cell-containing

hydrogel demonstrated a statistically significant increase in tongue weight of the operated side compared with the control side. In contrast, the saline and hydrogel groups demonstrated loss of tongue weight. Histologically, this corresponded to islands of desmin-stain positive cells signaling presence and persistence of skeletal muscle with evidence of neovascularization and preliminary neurotization. Comparatively, the control group which received only isotonic sodium chloride demonstrated diffuse fibrosis and disorganized myofibril architecture, while the hydrogel group showed no evidence of new tissue formation.

Bunaprasert *et al.*^[21] in the same laboratory explored this hemiglossectomy-pocket approach further and reported similar findings. Sixty rats were separated into five groups: Hemiglossectomy alone, collagen gel implant alone, collagen gel implant with suspended myoblasts, myoblasts cultured for 7 d in a pre-molded collagen gel, and myoblasts cultured for 7 d in a collagen gel with 2% horse serum to promote muscle differentiation. All groups gained weight appropriately without statistically significant difference between them, up to 16 wk. However, those groups containing gel alone or scar alone resulted in significant scar formation and lack of new muscle formation, whereas myoblast-containing gel contained interdigitating new muscle fibers, as confirmed by desmin, and neuroma-like fibers as well. A semi-quantitative histology score was applied to rate scar tissue and muscle formation, with best results occurring for both the undifferentiated myoblast groups irrespective of collagen culture method. Differentiated myoblasts scored better than controls but worse than their undifferentiated counterparts, suggesting either a benefit to multipotency or a detriment of the differentiation medium containing horse serum.

The same laboratory then assessed the cellular persistence in the collagen-filled pockets by implanting myoblasts that were pre-labeled with membrane dyes^[22]. At six weeks, myoblasts were identified in all 12 rats studied. Cells primarily remained within their treatment pocket, with limited migration into normal tissue. Treatment group tongues showed significantly less scar contracture, increased muscle diameter, and similar architecture to normal tongue compared to control. Markedly increased desmin positivity was also observed within the treatment group as opposed to control, and microscopy revealed myoblast proliferation and fusion into viable myotubes. Note that cells alone were not tested in this series of reports.

More recently, human cells have been investigated in immune-deficient rodents, taking a step closer to human translation. Kuhn *et al.*^[23] demonstrated persistence of human MDSCs injections in immune deficient mice. MDSC survival was assessed using *in vivo* imaging to visualize luciferase-transduced MDSCs. At 12 wk, the human MDSC group exhibited greater bioluminescence than immediately following injection, and increased weight gain compared to mice receiving saline injections only. Separately, Vahabzadeh *et al.*^[24] performed partial glossectomy in 18 athymic rats. After two weeks for scar formation to mimic a tumor resection scenario, animals were treated with either low- or high-dose mesenchymal stem cell (MSC) or saline control. Three weeks post-injection, researchers found significantly reduced cross sectional scar burden and pathologic score for inflammation and fibrosis in the high-dose MSC group (250000 cells injected) relative to controls. Low-dose MSC (70000 cells injected) did not differ from controls. These recent studies support human stem cell persistence and efficacy in xenograft cell injection models within immunosuppressed animals, supporting the concept of autologous human stem cell injection to avoid immune rejection.

In addition to studies looking at structural improvement using stem cells, one study evaluated functional improvement in one animal. Plowman *et al.*^[25] utilized a partially denervated ovine tongue model to study tongue force following injury and treatment. Two animals were denervated and injected, but only one could undergo eventual tongue force testing. A very high dose of 500 million GFP-labelled autologous MDSCs were injected into the tongues one month after bilateral hypoglossal nerve crush; histology and tongue force recordings were collected 2 mo post injection. Researchers found GFP+ muscle fibers in both tongues, indicating MDSC survival at 2 mo. They also noted increased muscle fiber diameter in GFP+ fibers suggesting reduced atrophy and even increased diameter compared to pre-injury, suggesting new muscle growth. Regarding functional improvement, the authors reported a 27% increase in maximal tongue force and a 54% increase in base of tongue pressure compared to pre-injection in the one animal tested^[25]. Clearly, such a small sample size warrants further investigation to obtain more robust results. Nevertheless, this novel denervation model and functional analysis indicating not only anatomical but also improvement in force generation shows promise for further research. Whether reduced tongue atrophy and increased forced production translates into improved swallowing function, remains to be seen.

STEM CELL THERAPIES FOR XEROSTOMIA

Dysfunctional salivary glands prove to be another major etiology of dysphagia. Saliva plays an important role in swallowing, serving to solubilize food substance, form a solid bolus by mixing with food particles, add moisture, and facilitate lubrication of the mucosa during bolus propulsion, among its other vital functions^[26]. Patients with dry mouth, also known as xerostomia, due to insufficient saliva production, often report extreme difficulty in swallowing. Causes of dysfunctional salivary glands are numerous and include but are not limited to: Medications, radiation therapy for head and neck cancers, resection of salivary glands, Sjögren's syndrome, and other autoimmune disease. Regardless of cause, the symptom impacts many Americans, with a prevalence ranging from 5.5% to 46%^[27]. Current therapies consist of sialogogues such as pilocarpine or cevimeline which stimulate secretion of saliva *via* binding of muscarinic receptors, although these carry their respective side effect profiles and more importantly, depend on intact functional glandular tissue to be effective. Other remedies include intraoral electrostimulation and acupuncture. However, there has not been sufficient research to confirm these as viable treatment options^[27].

A number of groups have explored the use of stem cells for xerostomia, although these are still in early stages of investigation. Lombaert *et al*^[28] described an approach towards the restoration of salivary gland function by using salivary gland stem cells cultured *in vitro* then transplanted into irradiated glands. Cells isolated from murine submandibular glands and cultured *in vitro* were injected in low numbers into irradiated glands. Researchers found close to 20% more surface area of acinar cells per gland compared to the untreated irradiated group. Functionally, they observed a 42% increase in saliva production in the cell injection group compared to untreated irradiated glands^[28].

Likewise, Nanduri *et al*^[29] found improved saliva production (54.59% *vs* 21.5%) in intra-glandularly injected cells *vs* irradiated control in addition to improved tissue healing, as indicated by persistence of ductal stem cell markers and revascularization. These novel studies demonstrated much promise into the therapeutic potential of regenerative medicine for restoration of salivary gland function, but knowledge regarding salivary gland stem cell behavior and characteristics was still lacking. Notably, only general stem cell markers such Sca-1, c-Kit, and Musashi-1 were used to identify the cells of interest, but a specific salivary gland stem cell marker was unable to be identified, making it difficult to track activity and persistence over time^[30,31]. Furthermore, these studies were unable to maintain cells in prolonged culture, showing limited self-renewal capacity *in vitro* that serves as an additional barrier for further research.

To this end, Ikeura *et al*^[32] successfully cultured cells derived from wild type murine submandibular glands for over 80 passages while maintaining their proliferative ability and morphology. Cells were isolated and cultured in low calcium, serum-free growth media with the addition of cholera toxin and epithelial growth factor to inhibit fibroblast growth and stimulate an epithelial phenotype. Notably, at passages 20, 50 and even 80, their cells did not form aggregates and salivary spheres, implying lack of cellular transformation and maintenance of a basal ductal cell phenotype which expressed keratin 14, 18 and p63, markers for basal, ductal and basal duct cells respectively^[32]. This opens up exciting new avenues for research into stem cell regeneration of damaged salivary gland tissue, as researchers are now more capable of closely mimicking *in vivo* salivary gland cellular phenotypes for further study rather than relying on immortalized tumor-derived cell lines which may not behave similarly to normal cells.

Dai *et al*^[33] described a different approach, whereby they demonstrated the potential for adipose tissue-derived stem cells (ADSCs) to differentiate into acinar-like epithelium capable of secreting α -amylase and expressing AQP-5. ADSCs are multipotent and may provide the advantage of differentiation into different components of salivary gland epithelium, both secretory and ductal, in addition to providing local trophic effects to improve tissue healing response following injury^[34]. Platelet-rich fibrin was co-administered to promote transdifferentiating into an acinar-like phenotype and was found to increase levels of both α -amylase and AQP-5. Still, a unique and reliable marker for salivary gland stem cells remains to be identified and continues to be an active area of research.

Clinically, these promising initial results have been translated into a landmark randomized, placebo-controlled trial in Denmark (MESRIX trial). Grønhøj *et al*^[35] randomized 30 patients to receive either ultrasound-guided injection of autologous ADSCs or placebo in submandibular glands after radiation therapy for HPV-positive

squamous cell carcinoma of the oropharynx. Cell doses administered were not clearly noted, although a planned dose of 2.8 million cells per volumetric milliliter of the gland was stated; total cell numbers harvested were between 13 and 82 million cells. No adverse events were reported. At both one and four months, patients within the ADSC arm displayed significantly increased unstimulated salivary flow rates compared to placebo, with 33% improvement over baseline at one month and 50% improvement at four months. In the placebo arm, salivary flow rates decreased remained largely unchanged. Patient-centered questionnaires revealed markedly decreased symptom reports from the ADSC group compared to placebo, reporting less difficulty within the domains of thirst and eating solid foods. Biopsies revealed increases in serous gland tissue and decrease in fibrosis and fatty deposits within the ADSC arm compared to placebo^[35]. While long-term follow up is required and ongoing^[36], the findings of this initial trial are exciting. Meanwhile, a clinical trial of allogeneic mesenchymal stem cell transplantation, MESRIX-SAFE^[37], is currently recruiting participants.

STEM CELL TREATMENT FOR CRICOPHARYNGEAL DYSFUNCTION

Further along the alimentary canal, food must travel past the UES to enter the esophagus. As mentioned before, relaxation of the UES to allow food passage largely depends upon cricopharyngeus muscle (CP) relaxation. Several disorders impair this function, leading to oropharyngeal dysphagia and food trapped upstream. The pressure buildup may eventually lead to complications such as outpouching of the mucosa, known as Zenker's diverticulum. One common etiology of CP dysfunction includes stroke, one of the leading causes of dysphagia. A study by Yang *et al*^[38] utilizing videofluoroscopic imaging to assess swallowing function in patients suffering from dysphagia due to stroke found an incidence of CP dysfunction to be 5.7% among first-time ischemic stroke patients. This incidence increased to 14.3% among those with infratentorial lesions and decreased to 2.8% among those with supratentorial lesions, suggesting focal lesions, primarily to the dorsal motor nucleus of the vagus, to be the primary culprit^[38]. These lesions are typical of lateral medullary syndrome. Other causes include radiation for head and neck cancer, iatrogenic nerve injury, and oculopharyngeal muscular dystrophy (OPMD); many patients have idiopathic dysfunction. Current treatment consists of swallowing therapy, balloon dilatation, botulinum toxin injection, and surgical CP myotomy^[39,40]. However, although effective, these are often temporary measures and have high rates of recurrence.

Current literature surrounding the use of muscle stem cells to repair cricopharyngeal dysfunction is sparse. A study published in 2014 by Périé *et al*^[41] described a clinical pilot study, whereby 12 patients with OPMD and indication for CP myotomy were injected with a median of 178 million myoblasts at various sites of pharyngeal constrictors following CP myotomy. Pharyngeal propulsion, as measured by videoendoscopy and videofluoroscopy remained largely unchanged at both 12 mo and 24 mo. UES function, defined by quality of UES opening and closure and pooling within the hypopharynx, improved in 6/12 patients at 24 mo using videoendoscopy but only in 2/12 patients at 24 mo using the more sensitive videofluoroscopy. Of note, investigators did not elaborate on the discrepancy between endoscopy *vs* fluoroscopy results and specify scoring mechanisms for assessing function *via* these two visualization modalities. Swallowing function as assessed using the Salassa score and McHorney score improved at both time points. Finally, average time to swallow 80 mL of water decreased from 23.7 s to 10.2 s^[41]. It is important to highlight the lack of a control group within the study, since all 12 patients received myoblast injection following CP myotomy, making it difficult to compare to improvement had patients received CP myotomy alone. Furthermore, small scarifications were induced with a scalpel during surgery to induce muscle regeneration. The effects of these small injuries may or may not have affected the end outcomes of pharyngeal function. Lastly, the discrepancy between videoendoscopy and videofluoroscopy scores weaken the overall body of evidence. Further study with larger sample size would improve statistical power and warrants investigation following this proof of principle research.

STEM CELL THERAPIES FOR DYSPHAGIA IN THE SETTING OF STROKE

Post-stroke dysphagia is a very common morbidity affecting up to 50% of cerebrovascular accident patients at 6 mo after the initial insult^[42]. Etiology is multi-

factorial including deficits in mastication, oropharyngeal bolus propulsion due to muscle atrophy^[43], cricopharyngeal dysfunction, and perhaps most importantly, neurologic coordination of the precisely-timed swallow cascade. With the global neurologic function in mind, SC treatment for ischemic brain injury could have significant benefits on post-stroke swallowing. This is an active area of research and has primarily focused on neuron regeneration and structural improvement within the cortex. Multiple human clinical trials of SC transplantation have been conducted that provide evidence of safety, however the evidence of efficacy in these trials remains lacking^[44-48]. Stem cell transplantation methods include direct injection into infarcted brain parenchyma, infusion through intravenous and intra-arterial vasculature, and infusion into cerebrospinal fluid through lumbar puncture. Implanted neural stem cells migrate to ischemic cortex and impart benefits including stimulating endogenous neurogenesis^[49,50], differentiating into functional neurons and astrocytes, inhibiting inflammation and glial scar formation^[51,52], and becoming neuroprotective if injected during acute ischemic injury^[53]. Functional improvement has been limited to memory tests and improvement in skeletal muscle coordination within animals^[54] and NIH Stroke Scale in humans, neither of which directly test dysphagia outcomes following neural stem cell transplantation^[44-47]. While improvement of coordination is encouraging, extrapolation of gross movements of the extremities cannot be reliably transferred to improvements of fine deglutition muscle coordination and functional improvement.

STEM CELL TREATMENT FOR ESOPHAGEAL REPAIR

Esophageal disorders represent a large proportion of cases underlying dysphagia. Etiologies are numerous, ranging from obstructive lesions such as strictures, webs, and tumors, to gastroesophageal reflux disease (GERD), eosinophilic esophagitis, achalasia, autoimmune causes such as Sjögren's syndrome, systemic lupus erythematosus, and systemic sclerosis as part of the CREST syndrome, medications, and neurological diseases^[55,56]. As such, management is extremely varied based upon underlying pathophysiology and is beyond the scope of this review. It is worth noting the use of stem cells to manage esophageal dysphagia has not been studied extensively, perhaps due to difficulty in isolating targeted points of intervention given the broad range of conditions which can lead to esophageal dysfunction. In cases of autoimmune or neurologic etiologies for example, management of the primary disease likely represents a more effective strategy than stem cell-based therapies. For more primary causes of esophageal dysphagia, however, such as inherent dysmotility, achalasia, or even treatment refractory GERD, stem cell therapy may fill a niche yet to be occupied. Given the lack of literature surrounding this topic and the substantial decrease in quality of life for patients suffering from esophageal motility disorders, this may represent a highly beneficial avenue of study in the future.

CHALLENGES

It is important to realize that despite many of these recent advancements in stem cell therapy for treatment of dysphagia (Table 1), the overwhelming majority of research remains in the basic and translational stage. The behavior of multipotent cells following injection into native tissue continues to be a point of discussion for researchers studying regenerative medicine. Although many of the above studies correlate persistence of cells as evidence of successful engraftment, studies in other organ systems such as cardiac tissue have found benefit despite cell elimination. Davani *et al*^[57] and Iso *et al*^[58] both demonstrated *in vivo* improvements in cardiac function following MSC injection, even without long-term engraftment and differentiation. When compared to injection with pure cardiac progenitor cells (CPCs), combination CPCs with MSCs actually improved cardiac ejection fraction more than CPC injection alone^[59]. Particularly for the case of multipotent mesenchymal stem cells, it is thought apoptosis of these cells actually plays an important immunomodulatory role during tissue repair, exhibiting paracrine immunomodulation to promote tissue regeneration^[60]. Our lack of understanding regarding the direct mechanisms whereby stem cells promote tissue healing represents a significant roadblock towards widespread stem cell therapy in the near future.

Moreover, it is difficult to translate structural outcome measurements such as increased tongue mass and reinnervation into actual functional improvement in

Table 1 Recent advances in targeted stem cell therapy for oropharyngeal dysphagia

| Ref. | Sample, n | Main findings |
|---|-----------------|---|
| Tongue dysfunction | | |
| Kim <i>et al</i> ^[20] (2003) | 30 rats | Myoblast-containing collagen hydrogel group demonstrated statistically significant increase in tongue weight and desmin-positive cells at the surgery site |
| Bunaprasert <i>et al</i> ^[21] (2003) | 60 rats | Myoblast-containing gel group showed interdigitating new muscle and neuroma-like fibers, with less scar tissue formation |
| Luxameechanporn <i>et al</i> ^[22] (2006) | 12 rats | Six weeks post surgery, myoblasts persisted in all 12 rats, had limited migration, showed less scar contracture, and had increased muscle diameter |
| Kuhn <i>et al</i> ^[23] (2017) | 16 mice | Human MDSCs injected into a hemiglossectomy model survived to the endpoint demonstrating 132% bioluminescence compared to 15% in control groups, and exhibited the greatest weight gain among all groups |
| Vahabzadeh <i>et al</i> ^[24] (2018) | 18 athymic rats | Three weeks post MSC injection following partial glossectomy, rats which received MSC treatment were found to have reduced x-sectional scar burden and pathologic scores for inflammation and fibrosis |
| Plowman <i>et al</i> ^[25] (2014) | 1 ovine | MDSCs survived 2 mo following bilateral hypoglossal nerve crush, and demonstrated increased muscle fiber diameter, 27% increase in maximal tongue force, and 54% increase in base of tongue pressure compared to pre cell injection |
| Xerostomia | | |
| Lombaert <i>et al</i> ^[26] (2008) | 13 mice | Salivary glands cultured <i>in vitro</i> then injected into irradiated glands demonstrated increased surface area of acinar cells and 42% increase in saliva production compared to untreated irradiated group |
| Nanduri <i>et al</i> ^[29] (2013) | 15 mice | 54.59% increase in salivary gland function following intraglandular injection of salisphere-derived c-kit positive cells in irradiated mice, compared to 21.5% in untreated mice |
| Ikeura <i>et al</i> ^[32] (2016) | | Salivary gland basal and ductal cells isolated from submandibular glands were successfully cultured for over 80 passages while maintaining their proliferative ability and morphology |
| Dai <i>et al</i> ^[33] (2019) | | ADSCs demonstrated the ability to differentiate into acinar-like epithelium capable of secreting α -amylase and expressing AQP-5 |
| Grønhøj <i>et al</i> ^[35] (2018) | 30 patients | Patients who received ADSC injection in submandibular glands demonstrated 50% improved unstimulated salivary flow rates at four months, markedly decreased symptom reports, increase in serous glands, and decreased fibrosis and fatty deposit on biopsies |
| Cricopharyngeal dysfunction | | |
| Périé <i>et al</i> ^[41] (2014) | 12 patients | 6/12 patients by videoendoscopy but only 2/12 patients by videofluoroscopy demonstrated improved UES function following myoblast injection and CP myotomy. Swallowing function improved in all patients subjectively and mean swallowing time decreased in all patients from 23.7 s to 10.2 s |

MDSC: Muscle-derived stem cell; MSC: Mesenchymal stem cell; ADSC: Adipose tissue-derived stem cells; UES: Upper esophageal sphincter; CP: Cricopharyngeus muscle.

swallowing. The few studies that do attempt to assess functional measurements, such as videofluoroscopy analysis, are limited by small sample sizes. A large portion of this challenge stems from the incredible complexity and coordination needed for swallowing. The interplay between different components of a swallow may mean recovery of one structure does not translate into recovery of swallowing function as a whole. It is reasonable to infer, particularly in cases of denervation injury, that physical therapy will remain an essential component of therapy to relearn swallowing and achieve coordination between a regenerated tissue and native tissue.

CONCLUSION

Dysphagia is a highly prevalent yet challenging disorder to treat, particularly among patients who lack native, functional tissue upon which many conventional treatments exert their effects. In these patients, more novel therapies in the form of stem cell implantation may represent a new avenue to pursue to improve swallowing function. Initial research targeting different domains of swallowing have shown promise in restoring both structure and function. Large strides have been made in animal studies involving tongue dysfunction and xerostomia, with comparatively fewer studies about pharyngeal, esophageal, and neuromuscular etiologies of dysphagia. It is important to realize this field of research is still relatively young and far from becoming a part of standard clinical practice, with very few studies progressing into human clinical trials. Nevertheless, it represents an exciting new area of study with promising initial results

and is worth pursuing for its large potential to improve dysphagia in difficult to treat patients.

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Perspectives on mesenchymal stem/progenitor cells and their derivatives as potential therapies for lung damage caused by COVID-19

Aleksandra Klimczak

ORCID number: Aleksandra Klimczak 0000-0001-6590-4420.

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Aleksandra Klimczak, Laboratory of Biology of Stem and Neoplastic Cells, Hirsfeld Institute of Immunology and Experimental Therapy Polish Academy of Sciences, Wrocław 53-114, Poland

Corresponding author: Aleksandra Klimczak, PhD, DSc, Full Professor, Laboratory of Biology of Stem and Neoplastic Cells, Hirsfeld Institute of Immunology and Experimental Therapy Polish Academy of Sciences, Rudolfa Weigla 12, Wrocław 53-114, Poland.
aleksandra.klimczak@hirsfeld.pl

Abstract

The new coronavirus, severe acute respiratory syndrome coronavirus-2 (SARS-CoV-2), which emerged in December 2019 in Wuhan, China, has reached worldwide pandemic proportions, causing coronavirus disease 2019 (COVID-19). The clinical manifestations of COVID-19 vary from an asymptomatic disease course to clinical symptoms of acute respiratory distress syndrome and severe pneumonia. The lungs are the primary organ affected by SARS-CoV-2, with a very slow turnover for renewal. SARS-CoV-2 enters the lungs *via* angiotensin-converting enzyme 2 receptors and induces an immune response with the accumulation of immunocompetent cells, causing a cytokine storm, which leads to target organ injury and subsequent dysfunction. To date, there is no effective antiviral therapy for COVID-19 patients, and therapeutic strategies are based on experience treating previously recognized coronaviruses. In search of new treatment modalities of COVID-19, cell-based therapy with mesenchymal stem cells (MSCs) and/or their secretome, such as soluble bioactive factors and extracellular vesicles, is considered supportive therapy for critically ill patients. Multipotent MSCs are able to differentiate into different types of cells of mesenchymal origin, including alveolar epithelial cells, lung epithelial cells, and vascular endothelial cells, which are severely damaged in the course of COVID-19 disease. Moreover, MSCs secrete a variety of bioactive factors that can be applied for respiratory tract regeneration in COVID-19 patients thanks to their trophic, anti-inflammatory, immunomodulatory, anti-apoptotic, pro-regenerative, and proangiogenic properties.

Key Words: Mesenchymal stem cells; Stem/progenitor cells; Lung damage; Mesenchymal stem cell secretome; COVID-19 disease; COVID-19 pneumonia

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Core Tip: The new severe acute respiratory syndrome coronavirus-2 (SARS-CoV-2) has reached pandemic proportions, causing coronavirus disease (COVID-19), which leads to severe pneumonia. The lungs are the primary organ affected by SARS-CoV-2, with a very slow turnover for renewal. SARS-CoV-2 enters the lungs and induces immune response with cytokine storm and subsequent organ dysfunction. To date, there is no effective antiviral therapy for COVID-19. Cell-based therapy involving mesenchymal stem cells and/or their secretome is considered a supportive therapy for critically ill COVID-19 patients. Mesenchymal stem cells can regenerate severely injured respiratory tract cells through their trophic, anti-inflammatory, and immunomodulatory properties.

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INTRODUCTION

The new virus, which emerged in December 2019 in Wuhan, China, was initially named coronavirus 2019-nCoV, and based on its phylogeny and taxonomy, was later renamed severe acute respiratory syndrome coronavirus-2 (SARS-CoV-2). It has reached worldwide pandemic proportions, causing coronavirus disease 2019 (COVID-19)^[1,2]. As of 11 June 2020, the World Health Organization (WHO) Situation Report-143 states that COVID-19 has been confirmed globally in 7273958 patients and resulted in 413372 deaths (<https://www.who.int/emergencies/diseases/novel-coronavirus-2019/situation-reports>).

The clinical manifestations of COVID-19 vary and include an asymptomatic disease course, acute respiratory disease, and pneumonia with different stages of severity. The asymptomatic disease course, without fever or respiratory or gastrointestinal symptoms, does not protect the patients from SARS-CoV-2 transmission, which is transmitted from person-to-person by direct contact^[2,3]. Based on current observations, it is unknown whether asymptomatic patients recover without adverse organ damage, or if complications appear as the late effects of the disease in the future. Patients with clinical signs of acute respiratory disease have revealed fever and cough with no signs of pneumonia, and more than 30% of patients require oxygen therapy but not mechanical ventilation^[4]. Uncommon gastrointestinal symptoms such as vomiting, nausea, and diarrhea have also been observed. The most severe symptoms of COVID-19 including fever, cough, headache, dyspnea, and sputum production have been observed in patients who developed pneumonia. Most of them (> 70%) have needed oxygen therapy, and almost 30% require mechanical ventilation^[2,4]. Severely affected patients are usually older and have coexisting illnesses, including hypertension, chronic obstructive pulmonary disease, diabetes mellitus, and cardiovascular disease, which often lead to death^[4-6]. Most patients with SARS-CoV-2 infection have a good clinical outcome and prognosis; however, in elderly patients (aged > 65 years) with comorbidities, severe complications can occur including acute respiratory distress syndrome (ARDS), septic shock, metabolic acidosis, coagulation dysfunction, and multiple organ failure, causing an increased risk of death^[5-8].

The basis of the pathogenesis of SARS-CoV-2 virus is binding of the S protein, expressed on the surface of the coronavirus, to angiotensin-converting enzyme 2 (ACE2) receptors^[9-11], which are widely distributed on the surface of human cells, especially alveolar type II cells, and on the capillary endothelium of the lung^[12]. Moreover, cellular transmembrane protease, serine 2 (TMPRSS2), which is abundantly expressed on alveolar cells, is essential for SARS-CoV-2 entry into target cells and spreading^[13,14]. In addition, ACE2 receptors are present on the cells in different tissues and organs including the heart, liver, kidney, and gut. The SARS-CoV-2 virus uses the ACE2 receptor for entry and initiates fusion with the host cells, infecting them and inducing the immune response from the host's innate immune system^[9]. The virus-induced immune response leads to the accumulation of immunocompetent cells, which produce a large number of proinflammatory cytokines, leading to target organ

damage, and consequently, fatal organ dysfunction. One of the first studies with COVID-19 patients reported that severely affected patients with pneumonia, in the acute phase of the disease, had high levels of proinflammatory cytokines and chemokines including interleukin-1 β (IL-1 β), IL-1 receptor antagonist (IL-1Ra), IL-7, IL-8, IL-9, IL-10, basic fibroblast growth factor (bFGF), granulocyte-colony stimulating factor, granulocyte-macrophage colony-stimulating factor, interferon- γ (IFN- γ), IFN- γ -induced protein 10 kDa, macrophage inflammatory protein-1 (MIP-1 α), MIP-1 β , and tumor necrosis factor- α (TNF- α)^[6]. Activity of the innate immune response is necessary to contain and eliminate the virus infection; however, an out-of-control immune response leads to immunopathological changes.

Current therapies for COVID-19

To date, there are no effective therapies against COVID-19. To overcome this problem, global medical, scientific, pharma and funding groups have rapidly initiated more than 500 COVID-19 clinical trials based on currently available anti-viral drugs in various combinations^[15]. Current antiviral therapies are based on experience in treatment strategies against the previously recognized SARS-CoV and MERS-CoV^[16]. Remdesivir and chloroquine or hydroxychloroquine are commonly used to treat pneumonia in COVID-19 patients^[17-20]. Other currently available potent antiviral agents and their combinations repurposed for COVID-19 treatment are also widely used^[5,21,22]. New therapies include passive antibody transfer from the sera of convalescent patients^[23,24] and blocking the ACE2 receptor by the serine protease TMPRSS2 inhibitor (approved for clinical use)^[13].

The ACE2 receptor is not expressed in the bone marrow, lymph nodes, spleen, or on immune cells such as T and B lymphocytes and macrophages^[12]. This biological feature of these cells suggests that immunotherapy can be used to treat severely infected patients. In search of new treatment modalities for COVID-19, early studies on cell-based therapy with mesenchymal stem cells (MSCs) have been employed as supportive treatment for critically ill patients^[25]. Currently, a total of 28 trials exploring the potential of MSCs and their derivatives for the treatment of critically ill COVID-19 patients have been approved and registered at the WHO International Clinical Trials Registry Platform www.clinicaltrials.gov^[15], and more than 20 have been registered in the Chinese clinical trial registry (www.chictr.org.cn)^[26].

LUNG STEM/PROGENITOR CELLS AND TISSUE HOMEOSTASIS

Most human tissues and organs, including the pulmonary tract, contain stem/progenitor cells responsible for the maintenance of tissue homeostasis^[27]. The lung is a conditionally renewing organ, and in normal conditions, the turnover of airway epithelial cells is less than 1% per day, in contrast to other adult organs such as the skin, intestines, or bone marrow. However, severe damage increases the self-renewing capability of different types of endogenous epithelial stem/progenitor cells that reside in the lung and are important for regulation of the regeneration of damaged tissue^[28]. The lung contains various types of epithelial cells that reside in several regions along the pulmonary airways.

Endogenous epithelial stem and progenitor cells in the adult lung are organized specifically according to their regional decomposition and functional activity along the proximal-distal axis of the pulmonary tract. The proximal part of the respiratory tract encompasses the cartilaginous trachea, lined by columnar pseudostratified epithelial cells, and different types of stem/progenitor cells with distinct roles in lung regeneration, including basal, secretory, ciliated, and neuroendocrine cells. The regenerative processes in the pulmonary tract involve local stem/progenitor cells, which are characterized by high proliferative activity during the perinatal period and a slow turnover during adulthood. In response to injury, a population of basal cells, which represent the stem/progenitor cells of the bronchiolar epithelium, migrate from the bronchiolar niche into the damaged alveolar epithelium and proliferate in order to repair the lung alveolar cells^[28,29]. The distal part of the airways is lined by a columnar epithelium, and includes secretory club cells (also known as Clara cells) and populations of ciliated cells, goblet cells, and pulmonary neuroendocrine cells^[28,29]. To maintain epithelial homeostasis, club cells are capable of self-renewal and can generate ciliated cells, whereas ciliated cells do not have self-regeneration capacity^[29]. Another population of stem and progenitor cells residing in the distal airway, involved in epithelial homeostasis and regeneration, is a rare population of cells called the bronchioalveolar stem/progenitor cells with self-renewal potential. Their number

increases following bronchiolar damage, and these cells are able to differentiate into bronchiolar and alveolar colonies, thus contributing to tissue repair^[28]. The terminal part of the airway tree is composed of alveoli containing specific alveolar progenitor cells, which differentiate into surfactant-producing alveolar epithelial cells type II and squamous gas-exchanging alveolar epithelial cells type I, responsible for the maintenance and restoration of the gas exchange units of the distal part of the pulmonary tract^[28,29].

Mesenchymal stromal/stem cells residing in the lung constitute a key component supporting epithelial progenitor niches along the proximal-distal axis of the airway tree. The lung mesenchymal stromal/stem cells secrete a variety of bioactive factors, including FGF10, a critical trophic factor necessary for coordinating differentiation in the developing lung and supporting epithelial regeneration in steady-state conditions and after injury^[29]. Moreover, lung mesenchymal stromal/stem cells modulate the local microenvironment *via* a paracrine-mediated anti-inflammatory effect and support the proliferation and differentiation of lung epithelial progenitor cells.

The different populations of endogenous stem and progenitor cells residing in distinct niches of the pulmonary tract contribute to region-specific epithelial cell repair, and the balance between the immune regulation and promotion of tissue regeneration ensures homeostasis of the lung^[27].

BIOLOGICAL PROPERTIES OF MSCS IN TISSUE REGENERATION

MSCs are multipotent cells, which are able to differentiate into different types of cells of mesenchymal origin including alveolar epithelial cells, lung epithelial cells, and vascular endothelial cells^[30,31]. MSCs are extensively studied for their clinical application in regenerative medicine due to their trophic, anti-inflammatory, and immunomodulatory properties^[32,33]. The capability of MSCs to restore tissues is also accomplished through their ability to secrete a variety of bioactive proteins, including growth factors and chemokines, to induce the proliferation of tissue-resident progenitor cells and angiogenesis^[33]. In response to inflammatory cytokines, such as IL-1, IL-2, IL-12, TNF- α , and IFN- γ secreted by immunocompetent cells, MSCs secrete a variety of growth factors and anti-inflammatory proteins including prostaglandin 2 (PGE 2), transforming growth factor-1 β (TGF- β 1), stromal-derived factor-1 (SDF-1), IL-4, IL-6, IL-10, and IL-1Ra^[31]. Soluble factors secreted by the MSCs prevent the proliferation and function of many immunocompetent cells including T lymphocytes, B lymphocytes, natural killer cells, monocytes, macrophages, and dendritic cells. The immunomodulatory activity of MSCs involves decreasing the level of IFN- γ and increasing the level of IL-4 and IL-10, thus promoting a shift from T helper type 1 (Th1) to Th2 lymphocytes and a shift in macrophage balance from the M1 (proinflammatory) to M2 (anti-inflammatory) phenotype^[31,34,35].

The trophic properties of MSCs are associated with the secretion of growth factors and chemokines, such as TGF- α , TGF- β , hepatocyte growth factor (HGF), epithelial growth factor (EGF), insulin-like growth factor 1, bFGF, vascular endothelial growth factor (VEGF), angiopoietin-1 (Ang-1), and other bioactive factors involved in cell proliferation and angiogenesis, as confirmed by many studies^[31,36] including research conducted by the author of this article^[33,37,38].

The advantage of MSCs as a therapeutic option is the low or moderate expression of human leukocyte antigen (HLA) class I antigens and the lack of expression of HLA class II antigens, which makes MSCs “undetectable” by recipient immunocompetent cells in the allogeneic condition. However, a proinflammatory environment and IFN- γ production may increase the expression of their HLA class II antigens^[31]. The immunomodulatory activity of MSCs related to dendritic cells is associated with their capacity to produce anti-inflammatory factors (PGE 2 and TGF- β), which inhibit the activation and maturation of dendritic cells, impairing their function^[31].

MSCS AS SUPPORTIVE THERAPY IN COVID-19 PATIENTS

COVID-19 triggers a strong immune response with cytokine storm, especially in the lower airway, leading to lung damage^[5,6]. MSCs are the ideal candidate for respiratory tract regeneration because they not only contribute to structural tissue repair but also have immunomodulatory, anti-inflammatory, proangiogenic, and anti-fibrotic properties^[39,40]. This biological activity of MSCs may also affect tissue repair through modulation of the local microenvironment. The immunomodulatory properties of

MSCs can diminish the inflammatory response and ameliorate the cytokine storm, as documented in clinical trials conducted among patients with steroid-resistant graft-versus-host disease^[41] and among patients with an autoimmune disease^[42]. Cell-based therapies with allogeneic MSCs of bone marrow or adipose tissue origin have also been applied to patients with an acute lung injury and ARDS^[43-45]. In these studies, the administration of MSCs was safe and feasible; however, the clinical effect suggests that this strategy needs further optimization. ARDS is characterized by substantial damage to the capillary endothelium and alveolar epithelium, which leads to an increase in alveolar-capillary permeability, causing pulmonary edema and the formation and accumulation of inflammatory cells in the interstitial and alveolar space^[46]; extensive regeneration of the tissues is required to restore pulmonary function.

A clinical study that used MSCs to treat patients infected with influenza A (H7N9), who displayed symptoms similar to COVID-19 patients including cough, fever, shortness of breath, and dyspnea accompanied by ARDS and subsequent pneumonia, as well as corresponding multi-organ dysfunction, suggested that MSCs can be used as supportive therapy to treat SARS-CoV-2-infected patients^[47].

In the case of patients with COVID-19, MSCs may attenuate the cytokine storm by means of paracrine secretion of a variety of anti-inflammatory cytokines including TGF- β 1, SDF-1, IL-4, IL-6, IL-10, and IL-1Ra, which decrease the overactivation of immunocompetent cells, thus regulating the inflammatory response (Figure 1). A decreased immune response modifies the microenvironment of the damaged tissue and promotes tissue repair and regeneration. It is well known that MSCs transplanted intravenously are trapped by organs with a large capillary bed including the liver, spleen, and lung. MSCs accumulating in the lung may improve the pulmonary microenvironment, protect alveolar epithelial cells, prevent dysfunction of capillary endothelial cells, and prevent pulmonary fibrosis, thus helping to recover lung function^[25,48]. Moreover, systemic delivery of MSCs may ameliorate multi-organ dysfunction associated with SARS-CoV-2 infection including cardiovascular, renal, or hepatic damage^[25]. The therapeutic potential of MSCs for the treatment of patients in critical condition caused by COVID-19 pneumonia was proved in a pilot study on intravenous MSC transplantation^[25]. The delivery of MSCs significantly improved the functional outcome and pulmonary function of the patients within 2 d following transplantation. This effect was associated with the immunomodulatory properties of MSCs, which caused a shift in the immune response from Th1 towards Th2, resulting in a decreased level of the proinflammatory cytokine TNF- α and an increased level of the anti-inflammatory cytokine IL-10. The MSC therapy also resulted in a high production of the proangiogenic VEGF, which can help restore the function of capillary endothelial cells. A very important biological characteristic of MSCs, assessed by 10x scRNA-seq analysis, showed that MSCs transplanted to patients did not express the ACE2 receptor or TMPRSS2, thus providing resistance to COVID-19 infection^[25].

The progression of COVID-19 leads to the development of pulmonary diseases, such as idiopathic pulmonary fibrosis or ARDS, commonly associated with damage to alveolar epithelial cells, which in turn is related to a severe hypoxia of the alveolar cells, leading to a massive apoptosis, therefore, contributing to the pathophysiology of lung fibrosis^[49]. Experimental studies have indicated that not only MSCs but also their derivatives, such as a conditioned medium containing a variety of bioactive factors or extracellular vesicles (EVs) (microvesicles and exosomes) carrying various cytoplasmic components, including lipids, DNA fragments, and RNA (including mRNA and microRNA), contribute to the recovery of alveolar epithelial cells and endothelial cells and modify the function of inflammatory infiltrates in paracrine and endocrine manners^[50,51].

An experimental study on the lung alveolar cells of the rat showed that conditioned medium of human MSC culture had a paracrine anti-apoptotic effects on the hypoxia-induced apoptosis of the alveolar cells. The anti-apoptotic properties of MSCs involve the secretion of keratinocyte growth factor and HGF, which downregulate the proapoptotic signal caused by the hypoxia-inducible factor-1 α and reactive oxygen species^[49]. A similar study in a rat model using conditioned medium from a culture of MSCs of bone marrow or adipose tissue origin confirmed that MSC-derived bioactive factors protected alveolar epithelial cells from damage in hypoxic conditions by decreasing the secretion of proinflammatory cytokines, augmenting the production of IL-10, and delaying cell apoptosis^[52].

MSC-derived EVs, similarly to their parent cells, exhibit proregenerative, anti-inflammatory, anti-apoptotic, anti-oxidative, prometabolomic, and immunoregulatory properties with respect to the damaged tissue microenvironment. The effectiveness of treatment of lung damage using MSC-derived EVs is currently being tested *in vitro*

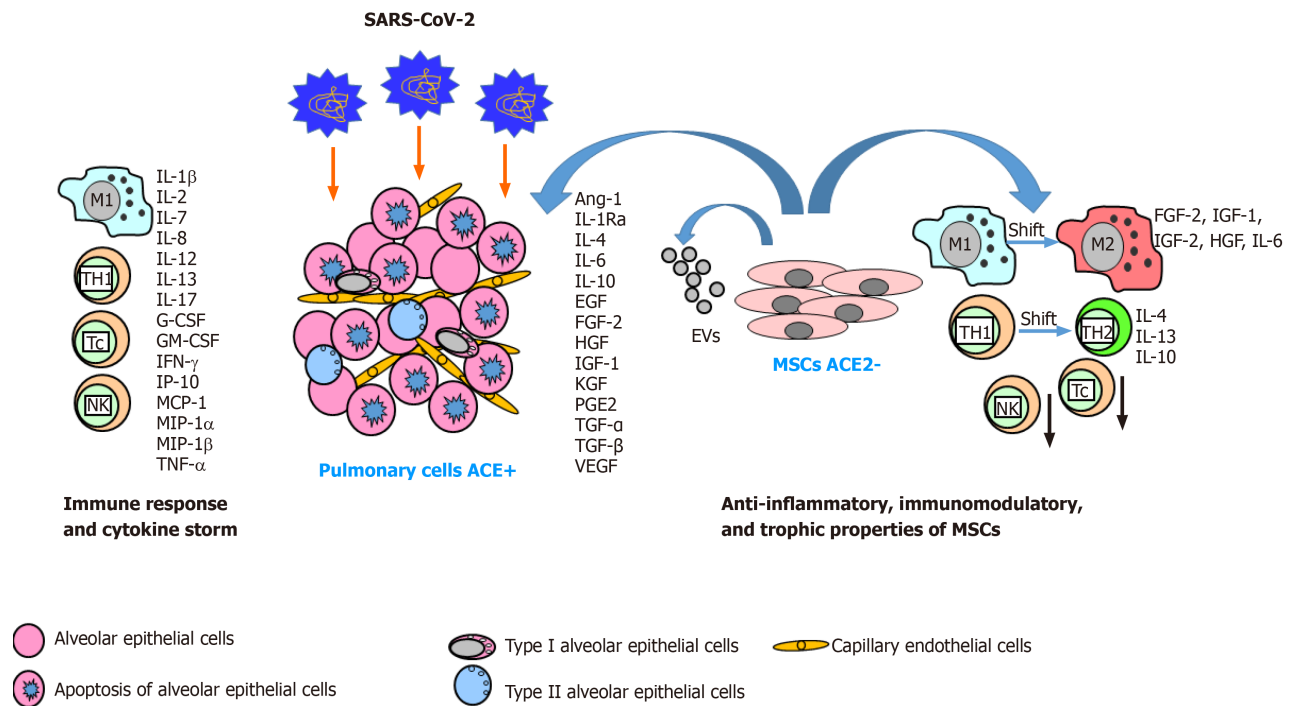


Figure 1 Immune response to severe acute respiratory syndrome coronavirus-2 infection and immunoregulatory activity of mesenchymal stem cells for treatment in patients with coronavirus disease 2019 pneumonia.

Upon entry into the alveolar epithelium, SARS-CoV-2 triggers a strong immune response with cytokine storm. Cytokines and trophic factors released by MSCs (ACE2 negative) and their derivate EVs modulate the inflammatory microenvironment within the damaged pulmonary cells and modulate immune response, promoting a shift from T helper type 1 to Th2 lymphocytes, and a shift in macrophage balance from the M1 (proinflammatory) to M2 (anti-inflammatory) phenotype, and decreasing the activity of cytotoxic T lymphocytes (Tc) and natural killer lymphocytes. ACE2: Angiotensin-converting enzyme 2; MSCs: Mesenchymal stem cells; Ang-1: Angiopoietin-1; SARS-CoV-2: Severe acute respiratory syndrome coronavirus-2; COVID-19: Coronavirus disease 2019; bFGF: Basic fibroblast growth factor; EGF: Epithelial growth factor; EVs: Extracellular vesicles; G-CSF: Granulocyte-colony stimulating factor; GM-CSF: Granulocyte-macrophage colony-stimulating factor; HGF: Hepatocyte growth factor; IFN- γ : Interferon- γ ; IGF-1: Insulin-like growth factor-1; IL-: Interleukin-; KGF: Keratinocyte growth factor; MIP-1 α : Macrophage inflammatory protein-1 α ; MIP-1 β : Macrophage inflammatory protein-1 β ; SDF-1: Stromal-derived factor-1; TGF- α : Transforming growth factor- α ; TGF- β : Transforming growth factor- β ; TNF- α : Tumor necrosis factor- α ; VEGF: Vascular endothelial growth factor; MCP-1: Monocyte chemoattractant protein-1; PGE2: Prostaglandin 2.

and in different preclinical experimental models^[51]. The beneficial effects of MSC-derived EVs have been demonstrated in influenza-induced acute lung injury in a pig model. Studies have shown that MSC-derived EVs, delivered 12 h after virus infection, result in reduced viral replication and shedding and a decreased level of proinflammatory cytokines^[53]. In addition to anti-inflammatory factors, MSC-derived EVs also contain Ang-1 mRNA, an angiogenic trophic factor that is essential in endothelial cell stabilization, and during injury, diminishes the interactions between leukocytes and vessel endothelial cells, and preserves vascular barrier integrity. The therapeutic effects of MSC-derived EVs in an experimental murine model of lipopolysaccharide-induced acute lung damage confirmed that a transfer of Ang-1 mRNA by EVs significantly contributed to the restoration of pulmonary capillary permeability^[54]. Moreover, MSC-derived EVs affected the immunomodulatory properties of the murine macrophage cell line by suppressing the expression of TNF- α and inducing the secretion of IL-10, thus attenuating inflammation. Transfer of Ang-1 mRNA to the injured endothelium restores partial protein permeability across the injured human lung microvascular endothelial cells through the internalization of MSC-derived EVs into the injured cells^[55]. A study in an experimental mouse model revealed that exosomes, isolated from MSCs derived from human Wharton's jelly and bone marrow, improved lung development, decreased lung fibrosis, and improved pulmonary vascular remodeling in a neonatal hyperoxia model of bronchopulmonary dysplasia. Exosomes originating from MSCs act as a paracrine anti-inflammatory mediator by modifying the pulmonary macrophage phenotype from M1 (proinflammatory) to M2 (anti-inflammatory) and suppressing lung inflammation and the immune response in favor of proper organ development^[34].

MSC-derived EVs, widely used in pre-clinical experimental models of pulmonary injury and disease, are a promising alternative to MSC-based therapy^[51]. However, many scientific and clinical questions regarding EV production, purification,

characterization, route of delivery (intravenous or inhalation), and bio-distribution need to be explored before clinical application. The first prospective non-randomized single-center clinical study using bone marrow-derived exosomes (ExoFlo™) was performed to address the safety and efficacy for the treatment of severely affected COVID-19 patients^[56]. Twenty-four patients with severe and moderate-to-severe symptoms of ARDS enrolled in this study received a single dose of ExoFlo™ administered intravenously, and no adverse effect was observed 72 h after exosome delivery. The survival rate was 83%, and the study demonstrated a profound reversal of hypoxia, downregulation of cytokine storm, and immune reconstitution. However, the biological characteristics of the delivered exosomes (ExoFlo™) were not presented. To determine the therapeutic potential of the applied therapy, future randomized controlled trials with a detailed characterization of the delivered exosomes are needed.

Extensive research on COVID-19 treatment have suggested that the MSC secretome should be employed as a supportive therapy in patients infected with SARS-CoV-2. Experimental pre-clinical studies on the biological activity of the MSC secretome, composed of both soluble bioactive factors (including cytokines, chemokines, and trophic factors) and EVs, suggest that the MSC secretome can be applied for cell-free therapy in severely affected COVID-19 patients^[57]. The bioactive proteins and EVs released by MSCs activate endogenous lung stem/progenitor cells, inducing their proliferation and differentiation, inhibit apoptosis, diminish inflammatory response, restore capillary barrier function, and reduce fibrosis and can also be used to treat acute and chronic lung injury, as they act similarly to parental MSCs^[50,57]. The advantages of cell-free therapy with the MSC secretome is its formulation as inhalable dosage forms or injectable dosage forms for potential clinical use^[58]. Both types of formulation are stored as freeze-dried powder and can be used to treat critically ill patients with COVID-19 pneumonia. The authors of the study introduced two Chinese clinical trials to investigate the inhaled secretome for the treatment of COVID-19 pneumonia (NCT04276987) and assess its tolerance in healthy volunteers (NCT04313647)^[57].

The current status of clinical investigations of cell-based therapy for COVID-19 patients has been reviewed very well by Khoury *et al*^[59] in the context of cell sources, doses, dosing strategies, and targeted patient populations. Khoury *et al*^[59] also highlighted the importance of upholding ethical standards to create a rational evidence-based platform for the potential therapeutic use of cell-based therapies in patients infected with SARS-CoV-2. A very recent editorial article, introduced by worldwide famous experts in the field of infectious diseases and MSCs therapies, discusses the rationale behind the use of MSCs in the treatment trials of patients with severe COVID-19 disease^[15]. The authors emphasized that the registered trials differ in design, sources of MSCs, doses and schedules of MSCs administration, and patient selection. All of these aspects indicate the need for standardizing protocols through a worldwide consortium network on cellular therapies for COVID-19 and other infectious diseases.

CONCLUSION

In summary, MSCs and their derivatives, such as the MSC secretome, may have a great curative potential for COVID-19 patients thanks to their trophic, paracrine, immunomodulatory, anti-inflammatory, anti-apoptotic, anti-oxidative, and prometabolomic activities. Moreover, the immunosuppressive properties of MSCs may decrease the alloreactivity of host immune cells in allogenic conditions. MSCs are attractive candidates for the supportive therapy of severely affected COVID-19 patients thanks to their high proliferative activity, multipotent ability to regenerate tissues *via* direct differentiation into the desired cells and tissues, and their immunomodulatory activity. MSCs are easily obtainable from different sources, such as bone marrow, adipose tissue, skin, or perinatal tissues, including the umbilical cord, cord blood, Warton's jelly, and amniotic fluid, and can be expanded into clinical grade and stored for potential clinical use. The most important biological characteristic of MSCs is that they do not express the ACE2 receptor or serine protease TMPRSS2, which makes them safe for the treatment of SARS-CoV-2 infection.

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Mass acquisition of human periodontal ligament stem cells

Hidefumi Maeda

ORCID number: Hidefumi Maeda
[0000-0002-1347-995x](https://orcid.org/0000-0002-1347-995x).

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Hidefumi Maeda, Department of Endodontology and Operative Dentistry, Division of Oral Rehabilitation, Faculty of Dental Science, Kyushu University, 3-1-1 Maidashi, Fukuoka 8128582, Japan

Corresponding author: Hidefumi Maeda, DDS, PhD, Chairman, Professor, Department of Endodontology and Operative Dentistry, Division of Oral Rehabilitation, Faculty of Dental Science, Kyushu University, 3-1-1 Maidashi, Higashi-ku, Fukuoka 8128582, Japan.
hide@dent.kyushu-u.ac.jp

Abstract

The periodontal ligament (PDL) is an essential fibrous tissue for tooth retention in the alveolar bone socket. PDL tissue further functions to cushion occlusal force, maintain alveolar bone height, allow orthodontic tooth movement, and connect tooth roots with bone. Severe periodontitis, deep caries, and trauma cause irreversible damage to this tissue, eventually leading to tooth loss through the destruction of tooth retention. Many patients suffer from these diseases worldwide, and its prevalence increases with age. To address this issue, regenerative medicine for damaged PDL tissue as well as the surrounding tissues has been extensively investigated regarding the potential and effectiveness of stem cells, scaffolds, and cytokines as well as their combined applications. In particular, PDL stem cells (PDLSCs) have been well studied. In this review, I discuss comprehensive studies on PDLSCs performed *in vivo* and contemporary reports focusing on the acquisition of large numbers of PDLSCs for therapeutic applications because of the very small number of PDLSCs available *in vivo*.

Key Words: Induced pluripotent stem cells; Mesoderm specific transcript; Periodontal ligament stem cells; Periodontal tissue; Regenerative medicine; Semaphorin 3A

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Core tip: For patients with severe periodontitis, deep caries, and trauma, which can lead to tooth loss, the development of highly effective regenerative therapies for severely damaged periodontal tissue is an urgent concern. As one possible method to address this issue, cell-based therapy using periodontal ligament stem cells (PDLSCs) shows great promise. However, the number of PDLSCs present *in vivo* is too small for implementation of this method, and PDLSC isolation requires patients to undergo invasive surgery. In this review, ways to acquire large numbers of PDLSCs and advances in periodontal regenerative therapy during the past two decades are summarized.

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HOW ARE REGENERATIVE TREATMENTS OF PERIODONTAL DEFECTS PERFORMED USING CELL-RELATED THERAPY?

Stem cell-based therapy (Figure 1)

In humans, autologous transplantation of cultured periosteum sheets^[1], periodontal ligament (PDL) progenitor cells^[2], PDL cell sheets^[3], dental pulp stem cells^[4,5], gingiva-derived cells^[6], and tissue-engineered bone constituted by bone marrow mesenchymal stem cells (BMMSCs)^[7] into patients with periodontal defects have been reported. All of the cited studies clinically verified the potency of stem cells for periodontal regeneration. In contrast, Chen *et al*^[8] transplanted PDL stem cell (PDLSC) sheets and found no significant improvement compared with the control group. However, these authors targeted very small periodontal defects and applied scaffolding materials as controls, possibly making it difficult to detect significant differences.

In animal periodontal defect models, Iwasaki *et al*^[9] reported no significant advantage of spheroid formation by human PDLSCs in rats, despite increased expression of genes related to angiogenesis and anti-inflammation^[9]. Nevertheless, a recent study demonstrated that coculture of human PDLSC spheroids with vascular endothelial cells promoted rat periodontal regeneration^[10]. In addition, a previous study revealed that pellets of cultured human PDLSCs showed periodontal regeneration capacity in mice^[11]. Meanwhile, application of other immature cells, including adipose-derived stem cells^[12], stem cells from human exfoliated deciduous teeth^[13], dental pulp stem cells^[14], dental follicle cells^[15], induced pluripotent stem (iPS) cells^[16], and iPS-derived mesenchymal stem cells (MSCs)^[17] was shown to induce periodontal regeneration *in vivo*. These reports suggest that the indicated cell sources may have potential for clinical use.

Gene/noncoding RNA modified cell therapy

No clinical studies on gene or noncoding RNA modified cell therapy for the treatment of patients with periodontal disease have been reported because of the associated safety issues. However, there have been some reports involving animal models with experimentally produced periodontal defects. *Osteoprotegerin* gene-transferred rabbit PDLSCs and *platelet-derived growth factor-BB*-transduced human PDLSCs exhibited increased bone formation in periodontal defects^[18,19].

The development and characterization of other tissue-derived cells with gene transduction have been reported. Specifically, *bone morphogenetic protein 2*-transfected canine BMMSCs^[20], *fibroblast growth factor 2*-transduced canine BMMSCs^[21], *hepatocyte growth factor*-transduced human dental pulp cells^[22], and *leptin*-transduced rat BMMSCs^[23] were able to restore periodontal defects *in vivo*.

Modification of PDLSCs using noncoding RNA, including microRNA, long noncoding RNA, and circular RNA have been reported to induce their osteogenic differentiation, suggesting the application of these cells to bone defective in periodontitis^[24].

Although the above studies indicated the potential of novel therapies for repair of severe periodontal defects, further basic studies are indispensable for future clinical trials.

Cell culture conditioned medium and exosomes

Conditioned medium from cultured cells and extracellular vesicles secreted from stem cells have various effects, including tissue regeneration, cell proliferation, chemotactic and metabolic activities, anti-inflammation, and cell-cell communication^[25]. Because these cells and vesicles possess great potential, researchers have examined their roles in periodontal regeneration studies, but related clinical trials have not been reported.

There have been some studies on the effects of conditioned medium or exosomes from PDLSCs as well as other tissue-derived stem cells in animal models. Recently, Nagata *et al*^[26] demonstrated periodontal regeneration activity of conditioned medium from cultured human PDLSCs injected into rat periodontal defects. Another study showed the capability of conditioned medium from human gingival stem cells as well

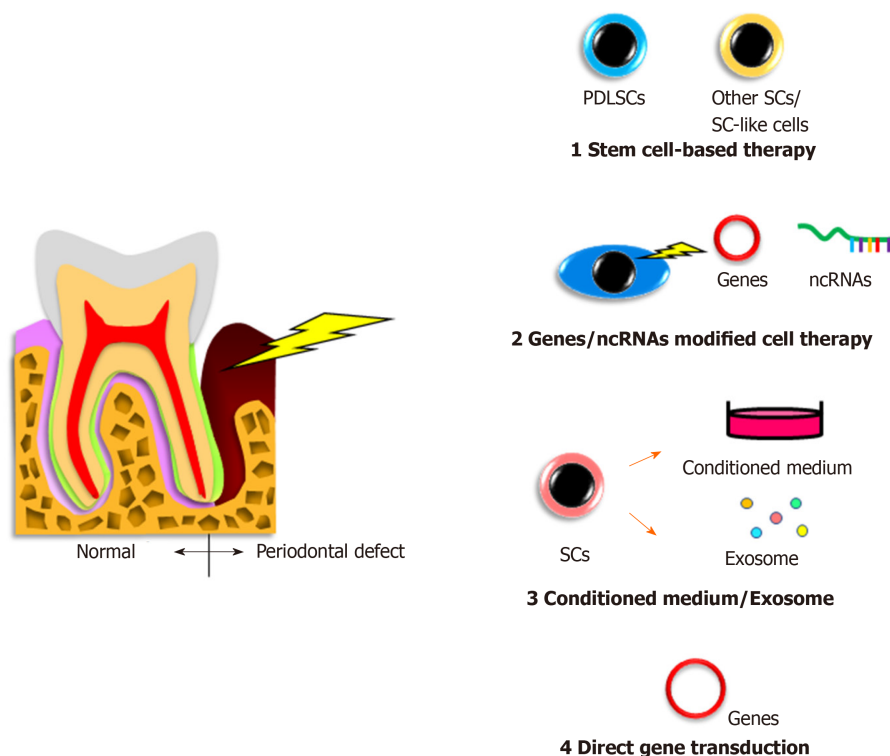


Figure 1 Cell-related therapies for periodontal regeneration. The regenerative treatments of periodontal defects performed using cell-related therapy are illustrated, which include the transplantation of stem cells, gene or noncoding RNA modified cells, application of conditioned medium or exosome from cell culture, and direct gene transfection to the lesion. PDLSC: Periodontal ligament stem cell; SC: Stem cell; ncRNA: noncoding RNA.

as human cultured human PDLSCs for periodontal regeneration^[27]. Furthermore, conditioned medium from human BMMSCs was clearly able to repair canine and rat periodontal defects^[28,29]. A recent report applying exosomes from human BMMSCs to rat periodontal defects showed induction of newly-formed bone and PDL tissue^[30].

Although the above effects do not reflect direct contributions of stem cells to treatment, these indirect effects of stem cells may deserve further consideration as treatment options.

Gene therapy

Direct *in vivo* gene transfer of the *bone morphogenetic protein 2/7*^[31] or *platelet-derived growth factor*^[32] genes to rat periodontal tissue promoted bone growth or bone regeneration and cementum formation, respectively. Meanwhile, another group directly transferred the *bone morphogenetic protein 4* gene to rat PDL tissue by electroporation but did not detect any obvious bone augmentation^[33]. Similarly, embedding of a *platelet-derived growth factor-B* plasmid with collagen gel into alveolar bone defects in rats had no significant effects^[34].

The gene therapy method has not been investigated in human patients, and its effectiveness needs to be fully verified before it can be used as a relatively easy therapeutic modality.

WHAT ARE PDLSCs?

Periodontal tissue (periodontium) is a complex tissue mainly composed of two hard tissues (alveolar bone and cementum coating tooth root surfaces) and two soft tissues (PDL tissue and gingival tissue)^[35]. In particular, PDL tissue has crucial roles in supporting the tooth and integrating the tissues.

PDLSCs are somatic stem cells localized in PDL tissue^[36] and derived from cranial neural crest cells^[37,38]. PDLSCs have similar features to BMMSCs and exhibit self-renewal capacity and multipotency^[39]. These cells have the potential to undergo triploblastic differentiation with the ability to differentiate into not only osteoblasts, adipocytes, chondrocytes, cementoblasts, and tendon/ligament fibroblasts^[40,41] but also myocytes^[42], neural cells^[43], retinal cells^[44], endothelial cells^[45], pancreatic islet cells^[46],

and hepatic cells^[47]. In addition, PDLSCs express cell surface markers such as STRO-1, CD146/MUC18^[36], CD44, and CD90 (markers associated with stromal cells), CD105 and CD166 (markers associated with stromal cells and endothelial cells)^[48], and CD10, CD26, CD29, CD73, and CD349/FZD9^[49] but do not express hematopoietic cell surface markers such as CD31 and CD45, similar to BMMSCs^[50].

PDLSCs also express embryonic stem cell-related transcription factors like NANOG and OCT-4 and embryonic stem cell antigens like stage-specific embryonic antigen-1 (SSEA-1)/CD15, SSEA-3, SSEA-4, TRA-1-60, TRA-1-81, alkaline phosphatase, and REX1/ZFP42^[49,51]. However, PDLSCs from aged people exhibit decreased capacities for proliferation, migration, and multiple differentiation with reduced SSEA-4 expression^[52].

Finally, PDLSCs possess immunomodulatory properties^[48], among which reactive oxygen species production may be interestingly regulated by dual mechanisms depending on the degree of inflammation^[53].

WHERE ARE PDLSCs REQUIRED?

Severe periodontitis, deep caries, and trauma cause irreversible damage to PDL tissue as well as the surrounding tissues such as alveolar bone, gingiva, and cementum, eventually resulting in tooth loss. The 8020 Promotion Foundation survey for causes of tooth loss in Japan (<https://www.8020zaidan.or.jp/english/>) performed in 2018 reported that periodontitis, caries, and tooth fracture accounted for 84.0% of all causes of tooth loss. The Global Burden of Disease 2015 study suggested that 7.4% of people worldwide suffered from severe periodontitis^[54]. Meanwhile, the National Survey of Dental Diseases in Japan performed in 2016 (<https://www.mhlw.go.jp/toukei/list/62-28.html>) reported that Japanese people with periodontal health (< 4 mm periodontal pocket depth) comprised less than 37.0% of people aged ≥ 50 years.

To date, transplantation of PDLSCs has led to successful periodontal regeneration in experimentally produced periodontal defects in dogs^[55,56], rats^[57], and pigs^[58]. Furthermore, Yan *et al*^[59] performed a systematic review and meta-analysis and decisively stated that cell-based therapy is an effective therapy for regeneration of lost periodontal tissue.

PDLSCs have been proposed as the most promising cells for regeneration of severely damaged PDL tissue, among other stem cells such as dental pulp stem cells, stem cells from human exfoliated deciduous, dental follicle stem cells, stem cells from apical papilla^[60], BMMSCs, and alveolar periosteal cells^[61].

Interestingly, the fate of transplanted PDLSCs was examined in a rat periodontal defect model^[62]. The findings revealed that PDLSCs contributed to periodontal repair but did not become markedly engrafted, suggesting a supportive role of PDLSCs for activating the regenerative capability in the damaged periodontium. Considering the critical role of PDLSCs in periodontal regenerative therapy, PDLSCs themselves may be difficult to engraft into defect sites, but the use of 2D or 3D construction methods combined with extracellular matrices may be effective.

WHY ARE LARGE AMOUNTS OF PDLSCs NEEDED?

In human PDL tissue, STRO1⁺/CD146⁺ cells, regarded as candidate PDLSCs^[36,63], were reported to comprise only about 0.07% of the total cells^[64]. Another study described that PDLSCs comprised 2.4% of the total cells^[63]. Regardless of the actual numbers, both studies indicated that very few PDLSCs are present in PDL tissue.

While the defect volumes in cases reported in human clinical studies have been very limited as described above, the defect areas in severe cases leading to tooth loss can vary across a wide range. Therefore, clinical application of PDLSCs to regenerative therapy of periodontal defects in humans will require the acquisition of large numbers of PDLSCs. Meanwhile, delivery of autologous PDLSCs to patients will necessitate the patients to undergo surgically invasive procedures. In addition, the subsequent expansion of small numbers of PDLSCs *in vitro* could lead to loss of their stemness. In this regard, it is of concern that large amounts of PDLSCs are needed for regenerative treatment. To address this issue, methods to acquire large numbers of PDLSCs have been explored.

HOW TO SOLVE THE INSUFFICIENCY OF PDLSCs?

Reprogrammed cells (Figure 2)

We have reported unique methods for conversion of PDL cells to PDLSCs by gene transduction^[65,66]. In a previous study, semaphorin 3A-transduced human PDL cells were converted into stem-like cells that showed multipotency and expressed both embryonic stem cell and MSC markers^[65]. Furthermore, we recently demonstrated that an unexplored gene, *mesoderm-specific transcript*, was expressed in PDLSCs and that human PDL cells transduced with the *mesoderm-specific transcript* gene acquired PDLSC properties similar to semaphorin 3A-transduced cells^[66]. In addition, the transduction changed the spindle shape of PDL cells to a stem cell-like round shape. Therefore, although the safety of these cells *in vivo* needs to be confirmed for clinical use, cell transformation with these genes is a potential method for mass acquisition of PDLSCs.

iPS cells

Our group was the first to report the development of PDLSC-like cells from human skin fibroblast-derived iPS cells^[67]. Our study indicated that iPS cells themselves were unable to directly differentiate into PDLSCs, whereas neural crest-like cells developed from iPS cells attained PDLSC properties when cultured on extracellular matrix secreted from human primary PDL cells. We believe that this method may have great potential to solve the issue of insufficient numbers of PDLSCs. In addition, a recent study produced human leukocyte antigen homozygous iPS cells by gene modification, which have immune compatibility^[68]. This development will enable the clinical use of iPS cell-derived PDLSCs benefiting many patients with severe periodontal defects. However, the issue of cost needs to be solved.

CONCLUSION

Many researchers have attempted to develop innovative and critical methods for periodontal therapy from various angles to support people's health and life and address the aging society. PDLSC-based therapy is one of these methods, and we believe that it has the potential to deliver sustainable oral health to people around the world.

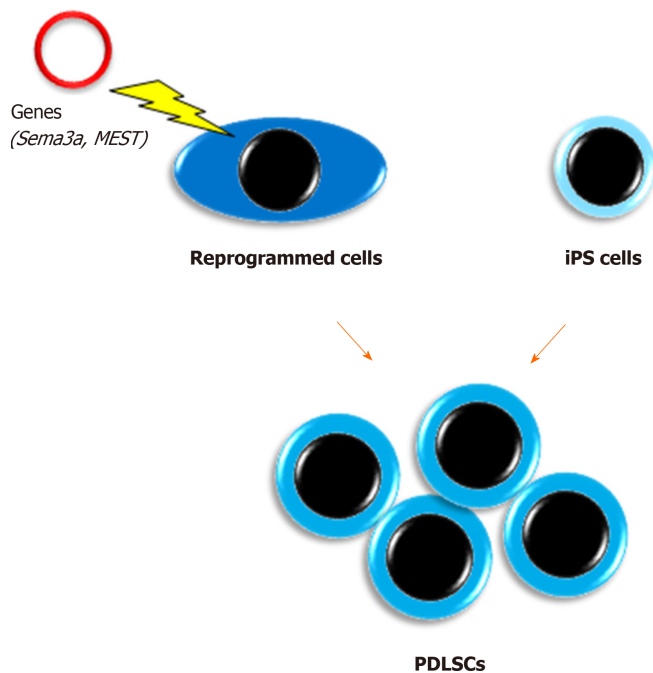


Figure 2 Acquisition of a large number of periodontal ligament stem cells. The illustration shows that the reprogramming of periodontal ligament cells with *semaphorin 3A* or *mesoderm-specific transcript*, or differentiation induction of induced pluripotent stem cells to human periodontal ligament stem cell lineage are promising to acquire a large number of periodontal ligament stem cells. iPS cells: Induced pluripotent stem cells; PDLSCs: Periodontal ligament stem cells. *Sema3a*: Semaphorin 3A; *MEST*: Mesoderm-specific transcript.

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Basic Study

Human mesenchymal stem cells derived from umbilical cord and bone marrow exert immunomodulatory effects in different mechanisms

Yunejin Song, Jung-Yeon Lim, Taekyu Lim, Keon-Il Im, Nayoun Kim, Young-Sun Nam, Young-Woo Jeon, Jong Chul Shin, Hyun Sun Ko, In Yang Park, Seok-Goo Cho

ORCID number: Yunejin Song 0000-0002-9379-422X; Jung-Yeon Lim 0000-0001-5903-8810; Taekyu Lim 0000-0002-3427-6705; Keon-Il Im 0000-0003-2811-9815; Nayoun Kim 0000-0001-8317-2921; Young-Sun Nam 0000-0002-9327-5745; Young-Woo Jeon 0000-0003-3362-8200; Jong Chul Shin 0000-0003-0360-2309; Hyun Sun Ko 0000-0001-6310-6206; In Yang Park 0000-0002-9458-2886; Seok-Goo Cho 0000-0002-5429-4839.

Author contributions: Song Y and Lim JY conceptualized the original idea, designed the experiments and wrote the manuscript; Song Y, Lim JY, Lim T, Im KI, Kim N, Nam YS and Jeon YW isolated the stem cells, performed the experiments and analyzed the data; Shin JC, Ko HS and Park IY provided human resources; All authors approved the final version of the article.

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Yunejin Song, Jung-Yeon Lim, Keon-Il Im, Nayoun Kim, Young-Sun Nam, Young-Woo Jeon, Seok-Goo Cho, Institute for Translational Research and Molecular Imaging, College of Medicine, The Catholic University of Korea, Seoul 06591, South Korea

Yunejin Song, Jung-Yeon Lim, Keon-Il Im, Nayoun Kim, Young-Sun Nam, Young-Woo Jeon, Seok-Goo Cho, Laboratory of Immune Regulation, Convergent Research Consortium for Immunologic Disease, College of Medicine, The Catholic University of Korea, Seoul 06591, South Korea

Yunejin Song, Department of Biomedicine and Health Sciences, College of Medicine, The Catholic University of Korea, Seoul 06591, South Korea

Jung-Yeon Lim, Precision Immunology Institute, Icahn School of Medicine at Mount Sinai, New York, NY 10029, United States

Taekyu Lim, Division of Hematology Oncology, Department of Internal Medicine, Veterans Health Service Medical Center, Seoul 05368, South Korea

Young-Woo Jeon, Seok-Goo Cho, Department of Hematology, Catholic Blood and Marrow Transplantation Center, Seoul St. Mary's Hospital, College of Medicine, The Catholic University of Korea, Seoul 06591, South Korea

Jong Chul Shin, Department of Obstetrics and Gynecology, CHA Bundang Medical Center, CHA University, Seongnam 13496, South Korea

Hyun Sun Ko, In Yang Park, Department of Obstetrics and Gynecology, College of Medicine, The Catholic University of Korea, Seoul 06591, South Korea

Seok-Goo Cho, Division of Hematology, Department of Internal Medicine, College of Medicine, The Catholic University of Korea, Seoul 06591, South Korea

Corresponding author: Seok-Goo Cho, MD, PhD, Professor, Division of Hematology, Department of Internal Medicine, College of Medicine, The Catholic University of Korea, Banpodaero 222, Seocho-Gu, Seoul 06591, South Korea. chosg@catholic.ac.kr

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Abstract**BACKGROUND**

Mesenchymal stem cells (MSCs) are an attractive tool to treat graft-versus-host disease because of their unique immunoregulatory properties. Although human bone marrow-derived MSCs (BM-MSCs) were the most widely used MSCs in cell therapy until recently, MSCs derived from human umbilical cords (UC-MSCs) have gained popularity as cell therapy material for their ethical and noninvasive collection.

AIM

To investigate the difference in mechanisms of the immunosuppressive effects of UC-MSCs and BM-MSCs.

METHODS

To analyze soluble factors expressed by MSCs, such as indolamine 2,3-dioxygenase, cyclooxygenase-2, prostaglandin E2 and interleukin (IL)-6, inflammatory environments *in vitro* were reconstituted with combinations of interferon-gamma (IFN- γ), tumor necrosis factor alpha and IL-1 β or with IFN- γ alone. Activated T cells were cocultured with MSCs treated with indomethacin and/or anti-IL-10. To assess the ability of MSCs to inhibit T helper 17 cells and induce regulatory T cells, induced T helper 17 cells were cocultured with MSCs treated with indomethacin or anti-IL-10. Xenogeneic graft-versus-host disease was induced in NOG mice (NOD/Shi-*scid*/IL-2R γ^{null}) and UC-MSCs or BM-MSCs were treated as cell therapies.

RESULTS

Our data demonstrated that BM-MSCs and UC-MSCs shared similar phenotypic characteristics and immunomodulation abilities. BM-MSCs expressed more indolamine 2,3-dioxygenase after cytokine stimulation with different combinations of IFN- γ , tumor necrosis factor alpha- α and IL-1 β or IFN- γ alone. UC-MSCs expressed more prostaglandin E2, IL-6, programmed death-ligand 1 and 2 in the *in vitro* inflammatory environment. Cyclooxygenase-2 and IL-10 were key factors in the immunomodulatory mechanisms of both MSCs. In addition, UC-MSCs inhibited more T helper 17 cells and induced more regulatory T cells than BM-MSCs. UC-MSCs and BM-MSCs exhibited similar effects on attenuating graft-versus-host disease.

CONCLUSION

UC-MSCs and BM-MSCs exert similar immunosuppressive effects with different mechanisms involved. These findings suggest that UC-MSCs have distinct immunoregulatory functions and may substitute BM-MBSCs in the field of cell therapy.

Key Words: Mesenchymal stem cells; Graft-versus-host disease; Umbilical cord; Cell therapy; Xenogeneic mouse model; Immunomodulation

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Core Tip: Mesenchymal stem cells (MSCs) are a therapeutic approach to treat graft-versus-host disease because of their unique immunomodulatory abilities. Here, we compared and analyzed the differences and similarities between umbilical cord-derived MSCs and bone marrow-derived MSCs due to the growing needs for new sources of MSCs. We suggest that umbilical cord-derived MSCs and bone marrow-derived MSCs exhibit similar immunosuppression by different mechanisms, and umbilical cord-derived MSCs have the potentials to substitute bone marrow-derived MSCs as cell therapy products.

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INTRODUCTION

Allogeneic hematopoietic cell transplantation (HSCT) is one of the most curative treatments for patients with hematological disorders, hematopoietic malignancies and immune diseases. Through HSCT, healthy hematopoietic donor cells can reconstruct the hematopoietic system of recipients. Despite the benefits of HSCT, there are risks of graft rejection, tissue toxicity, organ injury and leukemia relapse; among these risks, graft-versus-host disease (GVHD) is the major cause of death after transplantation^[1]. In GVHD, alloreactive donor T cells recognize histocompatibility antigens in host cells as foreign and activate to produce inflammatory cytokines, such as tumor necrosis factor alpha (TNF- α), interleukin (IL)-1, IL-2 and interferon-gamma (IFN- γ)^[2]. Although immunosuppressive drugs such as tacrolimus, cyclosporine and steroids are used in clinical therapy to lower GVHD mortality, a new therapeutic approach for GVHD following HSCT is needed.

Mesenchymal stem cells (MSCs) are multipotent stromal cells that have the ability to differentiate into different cell types, such as osteoblasts, chondrocytes and adipocytes^[3]. Recently, MSCs have been studied for cell therapy in the field of transplantation. A major characteristic of MSCs is that they express low major histocompatibility complex II, suppressing T cells independent from the major histocompatibility complex identity between the donor and recipient^[4]. Their immunosuppressive effects mainly occur through the production of soluble factors such as indolamine 2,3-dioxygenase (IDO), transforming growth factor- β , human leukocyte antigen (HLA)-G and hepatocyte growth factor^[5-8]. While soluble factors are the primary mechanism by which MSCs exert immunosuppressive effects, direct cell-to-cell contact is also a contributing factor^[9]. Cell-to-cell contact between CD3⁺ T cells and MSCs can induce CD4⁺CD25⁺ regulatory T cells^[10].

Traditionally, MSCs have been isolated from bone marrow, and bone marrow-derived MSCs (BM-MSCs) have been identified as a key candidate for cell therapy^[11]. However, their clinical application is restricted by the invasive procedures by which they are obtained, their decrease in proliferation and differentiation capacity with age and the difficulty of using them to treat patients with hereditary diseases^[12,13]. As a result, other adult and fetal tissues have been studied as alternative sources of stem cells, including adipose tissue, umbilical cord blood, umbilical cords, amniotic fluid and placental tissue^[14,15]. Although the major source of MSCs in clinical trials is bone marrow, recent studies have suggested that the allogenicity of MSCs has no significant adverse impact on the engraftment of MSCs in wound healing^[16]. It is better to use freshly isolated MSCs because the five major histocompatibility complex II molecules may increase during *in vitro* expansion^[17,18]. Additionally, the proliferative capacity of umbilical cord-derived MSCs (UC-MSCs) is higher than that of BM-MSCs. Several studies have emphasized the potential of UC-MSCs as an alternative to BM-MSCs; however, detailed comparisons of UC-MSCs and BM-MSCs are lacking.

Therefore, we compared the similarities and differences between UC-MSCs and BM-MSCs. In particular, we (1) investigated the *in vitro* immunoregulatory properties of UC-MSCs; (2) explored the mechanisms of immunosuppressive effects; and (3) analyzed the efficacy of UC-MSC and BM-MSC therapies to treat xenogeneic GVHD induced in severely immunodeficient NOG mice.

MATERIALS AND METHODS

Mice

Eight- to ten-week-old female NOG mice (NOD/Shi-*scid*/IL-2R γ^{null}) were purchased from the Central Institute for Experimental Animals (Kanagawa, Japan). Mice were maintained under pathogen-free conditions in an animal facility with controlled daylength (12L:12D), humidity (55% \pm 5%) and temperature (22 \pm 1 °C). The air in the facility passed through a HEPA filter system designed to exclude bacteria and viruses. Animals were fed mouse chow and tap water *ad libitum*.

Isolation and culturing of human MSCs

UCs were collected aseptically from full-term cesarean-section patients with informed consent. The UCs were transferred after collection, and the process was initiated within 24 h of delivery. The UC surface was rinsed with phosphate-buffered saline (Gibco-BRL) containing antibiotics and antifungal reagents (Antibiotic-Antimycotic, 100 ×; Gibco-BRL). In the explant method, the minced fragments were aligned and attached at regular intervals in 10-cm culture dishes. After the fragments were semi-dried and firmly attached to the bottom, culture medium was gently poured into the dishes. The cells were then washed with Alpha Minimum Essential Medium (Gibco) supplemented with 10% fetal bovine serum and seeded in 10-cm tissue culture dishes with culture medium as described above. The culture medium was refreshed once a week for 3-4 wk until fibroblast-like adherent cells reached 80%-90% confluence. The first-harvested master cells were defined as passage 0^[19]. BM-MSCs (passage 2-3) were purchased from Catholic MASTER Cells (Seoul, South Korea) and maintained in Dulbecco's modified Eagle's medium (Gibco) supplemented with 20% fetal bovine serum and 1% penicillin/streptomycin solution (Gibco).

Characterization of MSCs

Fluorescence-activated cell sorting flow cytometry analysis was performed using CD29 (TS2/16; eBioscience, San Diego, CA, United States), CD44 (IM7; eBioscience), CD105 (SN6; eBioscience), CD90 (5E10; eBioscience), CD73 (AD2; eBioscience), CD45 (2D1; eBioscience), CD31 (WM-59; eBioscience), CD34 (4H11; eBioscience), HLA-ABC (W6/32; eBioscience), HLA-DR (L243; eBioscience), C-C chemokine receptor type 1 (CCR1; 5F10B29; BioLegend, San Diego, CA, United States), CCR2 (K036C2; BioLegend), CCR7 (3D12; eBioscience), C-X-C chemokine receptor type 4 (CXCR4; 12G5; eBioscience) and CXCR5 (MU5UBEE; eBioscience) antibodies to confirm that the MSC phenotype was maintained after expansion in the culture. The samples were incubated with antibodies against each surface marker for 30 min, and this treatment was followed by fluorescence-activated cell sorting. Flow cytometry analysis was performed on a LSRFortessa (BD Pharmingen, San Diego, CA, United States).

Differentiation assay

One function of MSCs is to differentiate into osteoblasts, chondrocytes or adipocytes^[20]. For adipogenic differentiation assays, MSCs were seeded into 24-well plates at a density of 1×10^4 per well and induced to differentiate into adipocytes using the Human MSC Functional Identification Kit (R and D Systems, Minneapolis, MN, United States) following the manufacturer's protocol. The medium was changed three times a week for 14-21 d. Adipocytes were detected using goat anti-mouse FABP4 polyclonal antibody.

For osteogenic and chondrogenic differentiation assays, MSCs were seeded into 12-well plates at the manufacturer-recommended density and induced to differentiate into osteoblasts or chondrocytes using StemPro Chondrogenesis/Osteogenesis Differentiation Kits (Gibco, United States) following the manufacturer's protocols. The medium was changed three times a week for 21 d. Osteoblasts and chondrocytes were stained using Alizarin Red S and Alcian Blue, respectively.

Real-time reverse-transcription polymerase chain reaction

Total RNA was extracted using TRIzol LS reagent (Invitrogen). Isolated total RNA (2 µg) was reverse transcribed into complementary DNA at 50 °C for 2 min, followed by 60 °C for 30 min. Quantitative polymerase chain reaction was performed using the FastStart DNA Master SYBR Green I kit and a LightCycler 480 Detection system (Bio-Rad, CA, United States), as specified by the manufacturer. The crossing point was defined as the maximum of the second derivative from the fluorescence curve. Negative controls were included and contained all elements of the reaction mixture, except for template DNA. For quantification, we report relative mRNA expression levels of specific genes obtained using the $2^{-\Delta Ct}$ method. For normalization, *GAPDH*, a housekeeping gene, was used. The following gene-specific primers were used: *Klf4* (forward: 5'-CGAACCACACAGGTGAGAA-3'; reverse: 5'-GAGCGGGCGAATTTCCAT-3'), *OCT4* (forward: 5'-GGAGGAAGCTGACAACAATGAAA-3'; reverse: 5'-GGCCTGCACGAGGGTTT-3'), *Nanog* (forward: 5'-ACAACCTGGCCGAAGAATAGCA-3'; reverse: 5'-GGTTCCCAGTCGGGTTTAC-3'), and *GAPDH* (forward: 5'-TGCCAAATATGATGACATCA-3'; reverse: 5'-GGAGTGGGTGTCGCTGTTG-3').

Luminex multiplex cytokine assay

Different cytokines (IDO, IL-6) in human cell culture supernatants were assessed with a Luminex MAGPIX instrument (Luminex, Austin, TX, United States) using the ProcartaPlex Human 4-plex immunoassay kit (Affymetrix, Santa Clara, CA, United States) according to the manufacturer's instructions as described below. Briefly, samples were mixed with antibody-linked polystyrene beads in 96-well filter-bottom plates and incubated at room temperature for 2 h on an orbital shaker at 500-600 rpm. The plate was inserted into a magnetic plate washer and washed twice, then incubated with biotinylated detection antibody for 30 min at room temperature. Samples were washed twice as above and resuspended in streptavidin-PE. Two additional washes were performed as before with 30 min incubation at room temperature. After wash step, Reading Buffer was added to the sample. Each sample was measured in duplicate. Plates were read using a MAGPIX instrument with xPONENT 4.2 software (Luminex). Cytokine concentrations were calculated using ProcartaPlex Analyst 1.0 software (Affymetrix).

Western blot analysis

MSCs protein extractions were prepared from 1×10^5 cells by homogenization in lysis buffer with a protease/phosphatase inhibitor cocktail (Cell Signaling, Danvers, MA, United States) and centrifuged for 15 min at 14000 rpm. The protein concentration in the supernatant was measured following the Bradford method (Bio-Rad). Protein samples were separated using sodium dodecyl sulfate gel electrophoresis and transferred onto a nitrocellulose membrane (Amersham Pharmacia Biotech, Buckinghamshire, United Kingdom). Membranes were stained with primary antibodies specific to IDO, COX2, β -actin (Cell Signaling) or iNOS (R and D Systems). Then, horseradish peroxidase-conjugated secondary antibodies were added. Membranes were washed with Tris-buffered saline and Tween 20 solution, and the hybridized protein bands were detected using an enhanced chemiluminescence detection kit and Hyperfilm enhanced chemiluminescence reagents (Amersham Pharmacia Biotech).

Induction and treatment of xenogenic GVHD

Human peripheral blood was obtained from healthy volunteers with their consent, and peripheral blood mononuclear cells (PBMCs) were isolated with Ficoll-Hypaque (GE Healthcare +UK Ltd., United Kingdom) density centrifugation and washed in phosphate-buffered saline. Cells were resuspended in phosphate-buffered saline and injected through the tail vein into irradiated mice. The mice received a single dose of 200 cGy gamma irradiation from a linear accelerator before injection of human PBMCs on the same day. These animals were divided into three groups ($n = 12$ mice/group): GVHD, UC-MSC and BM-MSC. All animals were randomly allocated and coded. All animals were monitored for clinical symptoms of GVHD (weight loss, hunched posture, fur loss, reduced mobility, skin integrity) and mean serial weight measurements. The mice that showed severe inflammation in unintended body parts causing blindness and bowel obstruction, 20% weight loss compared to mice of same age, anorexia, quadriplegia and gait impairment were administered euthanasia by CO₂ exposure.

In vitro growth assay

MSCs at each passage were seeded at a density of 1×10^5 in 100 mm culture dishes. Culture dishes were incubated in 37 °C with 5% CO₂ until reaching 90% confluence and then counted.

In vitro proliferation assay

Human PBMCs (1×10^5 /well) from healthy adult donors were plated in 96-well flat-bottomed plates (200 μ L/well). Cells were then stimulated with 5 μ g/mL phytohemagglutinin (Sigma-Aldrich) and/or MSCs (5×10^3 , 1×10^4 , 5×10^4 , 1×10^5) for 72 h, followed by the incorporation of 1 μ Ci/mL [3H]-thymidine (GE Healthcare, Piscataway, NJ, United States) for the last 18 h of the indicated culture period. Radioactivity was measured using a Micro Beta instrument (Pharmacia Biotech, Piscataway, NJ, United States).

In other experiments, neutralizing antibodies for human IL-10 or transforming growth factor- β mAb (10 μ g/mL; R and D Systems) and chemical antagonists for COX2 (indomethacin, 20 μ M; Sigma-Aldrich), iNOS [N-nitro-L-arginine methyl ester (L-NAME), 1 mM; Sigma-Aldrich], heme oxygenase 1 inducer (hemin, 50 ng/mL; Sigma-Aldrich), selective A_{2B} adenosine receptor (alloxazine, 10 μ M; Sigma-Aldrich),

and CD73 (α , β -methylene ADP [APCP], 100 μ M; Sigma-Aldrich) were added into the coculture. All experiments were performed in quadruple and were repeated at least twice.

Flow cytometry analysis

PBMCs were immunostained using various combinations of the following fluorescence-conjugated antibodies: CD4 (RPA-T4; BioLegend), CD25 (BC96; eBioscience), Foxp3 (PCH101; eBioscience), IL-17 (eBio64DEC17; eBioscience) and IFN- γ (4S.B3; eBioscience). The cells were also intracellularly stained with the following antibodies: IL-17, IFN- γ and Foxp3. Before intracellular staining, cells were stimulated in culture medium containing 25 ng/mL phorbol myristate acetate (Sigma-Aldrich), 250 ng/mL ionomycin (Sigma-Aldrich) and 1 μ L/mL GolgiSTOP (BD Pharmingen) in an incubator with 5% CO₂ at 37 °C for 4 h. Intracellular staining was conducted using an intracellular staining kit (eBioscience) according to the manufacturer's protocol. Flow cytometric analysis was performed on a LSRFortessa (BD Pharmingen).

Statistical analysis

Statistical significance was determined using Student's two-tailed *t*-test. In all analyses, *P* values less than 0.05 were considered to indicate statistical significance.

Ethics

All procedures involving animals were performed in accordance with the Laboratory Animals Welfare Act, the Guide for the Care and Use of Laboratory Animals and the Guidelines and Policies for Rodent Experimentation provided by the Institutional Animal Care and Use Committee of the School of Medicine of the Catholic University of Korea (Seoul, South Korea). The protocols used in this study were approved by the institutional review board of The Catholic University of Korea (CUMC-2018-0270-01).

RESULTS

Characteristics of MSCs

We analyzed the expression of surface proteins for immunophenotypic characterization of culture-expanded UC-MSCs and BM-MSCs. All culture-expanded MSCs showed similar spindle-shaped morphologies (data not shown) and were uniformly positive for CD29, CD44, CD105, CD73, CD90 and HLA-ABC but negative for CD45, CD31, CD34 and HLA-DR (Figure 1A).

We used flow cytometry to examine the cell surface expression of chemokine receptors. Neither UC-MSCs nor BM-MSCs expressed CCR2. Both MSC types expressed CCR1, CCR7, CXCR4 and CXCR5 (Figure 1B).

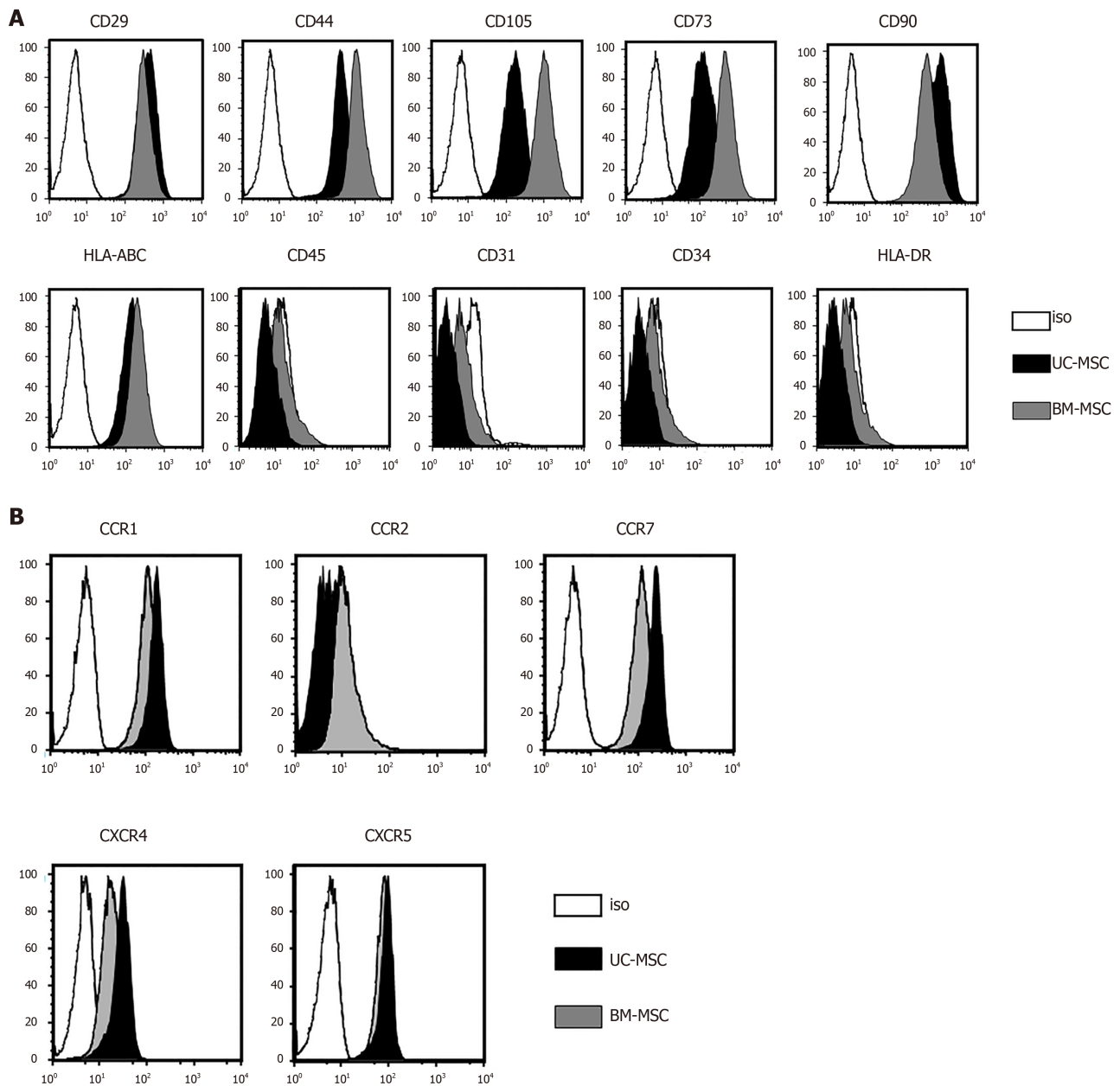
For adipogenic induction, BM-MSCs formed lipid vacuoles after 7 d and UC-MSCs after 14 d. After they changed morphology, adipocytes were detected by goat anti-mouse FABP4 polyclonal antibody under a fluorescence microscope. For osteogenic induction, both MSCs lost their spindle shape and became irregularly shaped. After 21 d, differentiated osteocytes were stained using Alizarin Red S. Chondrocytes were induced in the micromass cultures with chondrocyte differentiation medium for 21 d. Chondrogenic-induced cells were stained with Alcian Blue. These data showed that both UC-MSCs and BM-MSCs have the potential to differentiate into adipocytes, osteocytes and chondrocytes (Figure 1C). Previous reports have suggested that donor age affects the proliferation rate of bone marrow-derived MSCs; as donors get older, the proliferation rate tends to decline^[21]. We found that this trend also occurred with UC-MSCs (data not shown).

To compare the growth rates of each passage in UC-MSCs and BM-MSCs, we seeded 1×10^5 cells in 100-mm culture dishes and cultured until reaching 90% confluence. We compared the number of cells detached from the dish. The growth rate increased with passage number; however, UC-MSC growth increased more rapidly than that of BM-MSC (Figure 1D).

We then compared the expression levels of pluripotency transcription factors by quantitative real-time polymerase chain reaction. The expression levels of *Klf4* and *OCT4* were similar. The expression levels of *Nanog* in UC-MSCs and BM-MSCs were not statistically different (Figure 1E).

Immunomodulatory effects of MSCs with IFN- γ stimulation

The immunosuppressive effects of MSCs are enhanced when stimulated by pro-



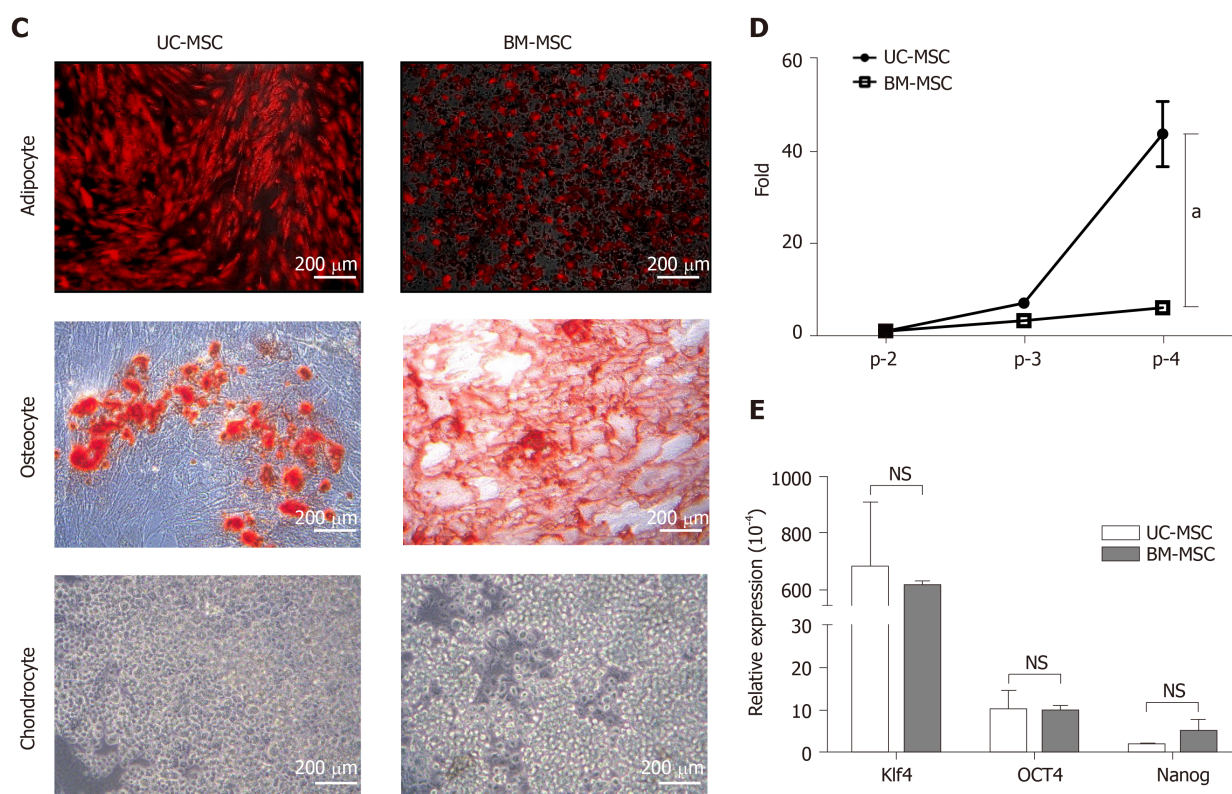


Figure 1 Characterization of umbilical cord-derived mesenchymal stem cells and bone marrow-derived mesenchymal stem cells. A: Surface protein expression was analyzed using flow cytometry. Mesenchymal stem cells (MSCs) were assessed at the fourth passage; B: Chemokine receptor expression was analyzed at passages 3–7 by flow cytometry; C: Representative images of umbilical cord-derived MSCs and bone marrow-derived MSCs differentiation into adipocytes (bone marrow-derived MSCs: day 7; umbilical cord-derived MSCs: day 21), chondrocytes (day 21) and osteocytes (day 14). Scale bars: 200 μ m. Adipocytes were detected by goat anti-mouse FABP4 polyclonal antibody under a fluorescence microscope. Osteoblasts and chondrocytes were stained with Alizarin Red S and Alcian Blue, respectively and observed under a light microscope; D: Growth rate of MSCs at different passages; and E: Pluripotency transcription factor expression levels of cultured MSCs measured by quantitative real-time polymerase chain reaction (target, *GAPDH*). D and E: Bone marrow-derived MSCs. Statistical analysis was performed by Student's *t*-tests, ^a*P* < 0.05 vs indicated group. iso: Isotype; Klf4: Kruppel-like factor 4; Nanog: Nanog homeobox; NS: No significance; OCT4: Octamer-binding transcription factor 4; UC-MSC: Umbilical cord-derived mesenchymal stem cells; BM-MSCs: Bone marrow-derived mesenchymal stem cells.

inflammatory cytokine IFN- γ ^[5]. Therefore, we created inflammatory conditions using different concentrations of IFN- γ and examined the expression levels of soluble factors representing the immunosuppressive capacity of MSCs. Stimulated MSCs were detached and lysed to analyze IDO by western blot. The IDO levels of both UC-MSCs and BM-MSCs increased in a dose-dependent manner with IFN- γ . However, BM-MSCs expressed more IDO than UC-MSCs (Figure 2A). We collected cultured medium to assess the IDO concentrations. The concentration of IFN- γ was positively correlated with IDO levels produced by both UC-MSCs and BM-MSCs; however, IDO in BM-MSC culture supernatant was significantly higher than that of UC-MSCs (Figure 2B).

Next, UC-MSCs and BM-MSCs were assessed for their expression of inflammatory mediators. When stimulated with IFN- γ , COX2 in UC-MSCs decreased in a dose-dependent manner, although BM-MSCs did not express COX2 with or without IFN- γ (Figure 2C). Also, IFN- γ stimulation did not affect expression of iNOS in both UC-MSCs and BM-MSCs (Figure 2C). According to recent studies, prostaglandin E2 (PGE2) is considered a major immunomodulatory factor of MSCs^[22]. Therefore, we measured the concentrations of PGE2 and IL-6, which is increased by PGE2 in cultured medium^[23]. PGE2 was notably secreted in UC-MSCs (Figure 2D). Interestingly, IL-6 levels were significantly high in UC-MSCs, and IFN- γ stimulation did not affect IL-6 levels (Figure 2E).

PD-L1 is known to maintain cancer cells as an immunosuppressive factor, which is necessary for cancer to evade the immune system^[24]. In contrast, PD-L1 may act as an immunomodulatory factor for MSCs, which are expected to suppress the immune system. PD-L1 is also needed for cell-to-cell contact between MSCs and T cells. We analyzed the expression of PD-L1 and PD-L2 in UC-MSCs and BM-MSCs with or without IFN- γ stimulation. Overall, UC-MSCs expressed higher levels of PD-L1 (Figure 2F) and PD-L2 (Figure 2G). We also found that PD-L2 expression increased

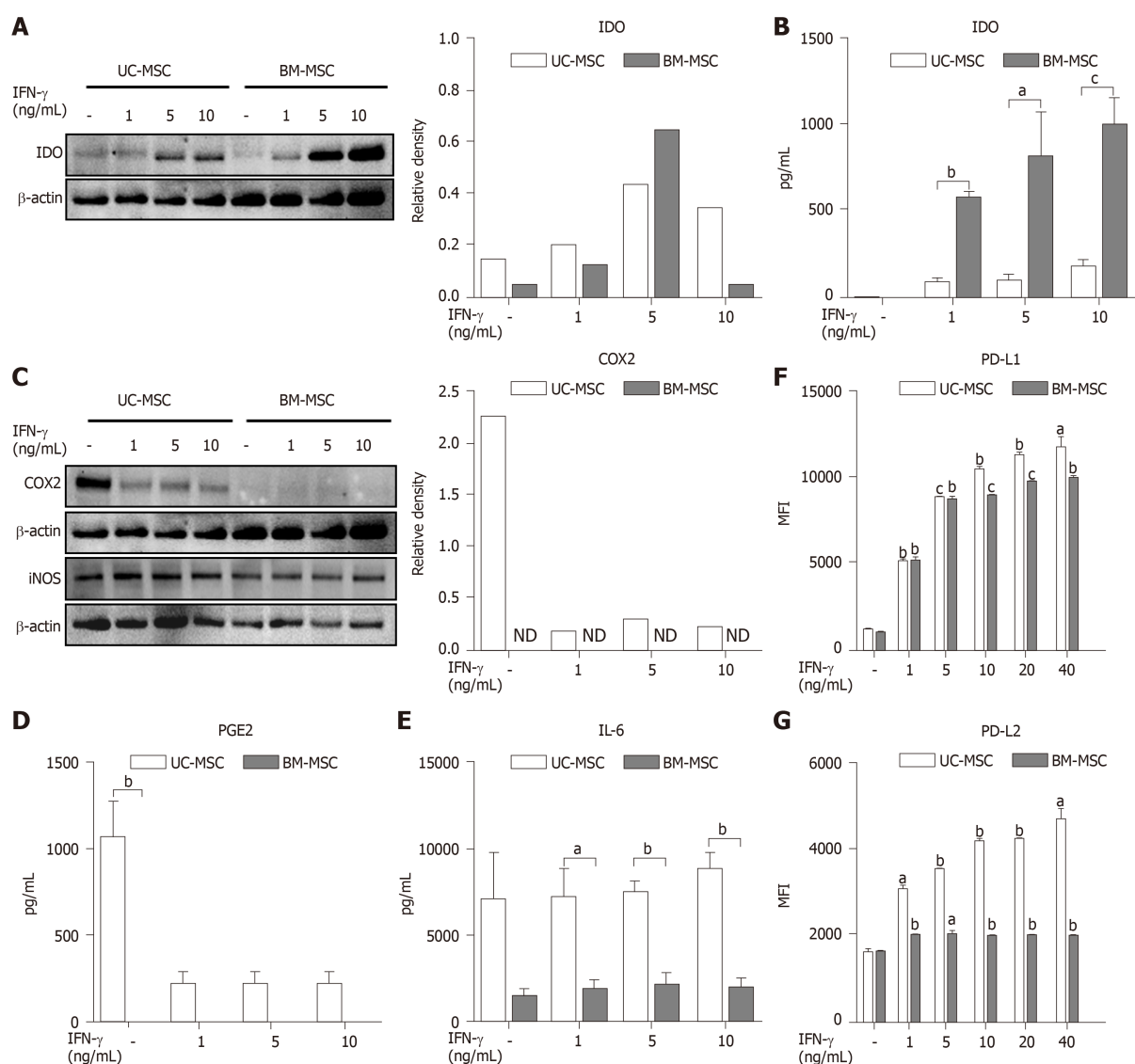


Figure 2 Immunomodulatory effects of interferon-gamma-stimulated mesenchymal stem cells. Umbilical cord-derived mesenchymal stem cells and bone marrow-derived mesenchymal stem cells were stimulated with 0, 1, 5 or 10 ng/mL of interferon-gamma in culture for 72 h. A and C: Expression of indoleamine 2,3-dioxygenase (A) and cyclooxygenase-2 (C) of interferon-gamma-stimulated mesenchymal stem cells measured by western blotting; B, D and E: Expression of indoleamine 2,3-dioxygenase (B), prostaglandin E2 (D), and interleukin-6 (E) in cultured medium measured by ELISA; F and G: Expression of PD-L1 (F) and PD-L2 (G) after interferon-gamma stimulation analyzed by flow cytometry. Statistical analysis was performed by Student's *t*-tests, ^a*P* < 0.05; ^b*P* < 0.01; ^c*P* < 0.0001 vs indicated group. B, D and E: ^a*P* < 0.05; ^b*P* < 0.01; ^c*P* < 0.0001 vs first bar of each group (F and G). BM-MSC: Bone marrow-derived mesenchymal stem cells; IDO: Indoleamine 2,3-dioxygenase; IFN-γ: Interferon-gamma; IL-6: Interleukin 6; iNOS: Inducible nitric oxide synthase; MFI: Mean fluorescence intensity; ND: Not detected; PGE2: Prostaglandin E2; UC-MSC: Umbilical cord-derived mesenchymal stem cells.

upon IFN-γ treatment in UC-MSCs but was consistent in BM-MSCs (Figure 2G).

Immunomodulatory effects of MSCs with combinations of diverse cytokines

To enhance their immunomodulatory capacity, we stimulated MSCs with multiple combinations of IFN-γ, TNF-α and IL-1β. We found that UC-MSCs and BM-MSCs responded differently to the combinations. Western blot revealed that combinations of IFN-γ, TNF-α and IL-1β elevated the expression level of both IDOs. IFN-γ treatment alone did not increase IDO and COX2, but stimulation with TNF-α and IL-1β did (Figure 3A). Conversely, the protein levels in UC-MSCs were not significantly affected by stimulation (Figure 3A). Next, we analyzed PGE2 and IL-6 in cultured medium with combination stimulations. Interestingly, BM-MSCs, which did not secrete detectable amounts of PGE2 with IFN-γ, secreted high levels of PGE2 and IL-6 with combinations of IFN-γ and TNF-α. Moreover, combinations of cytokines enhanced the secreted levels of PGE2 and IL-6 (Figure 3B and 3C).

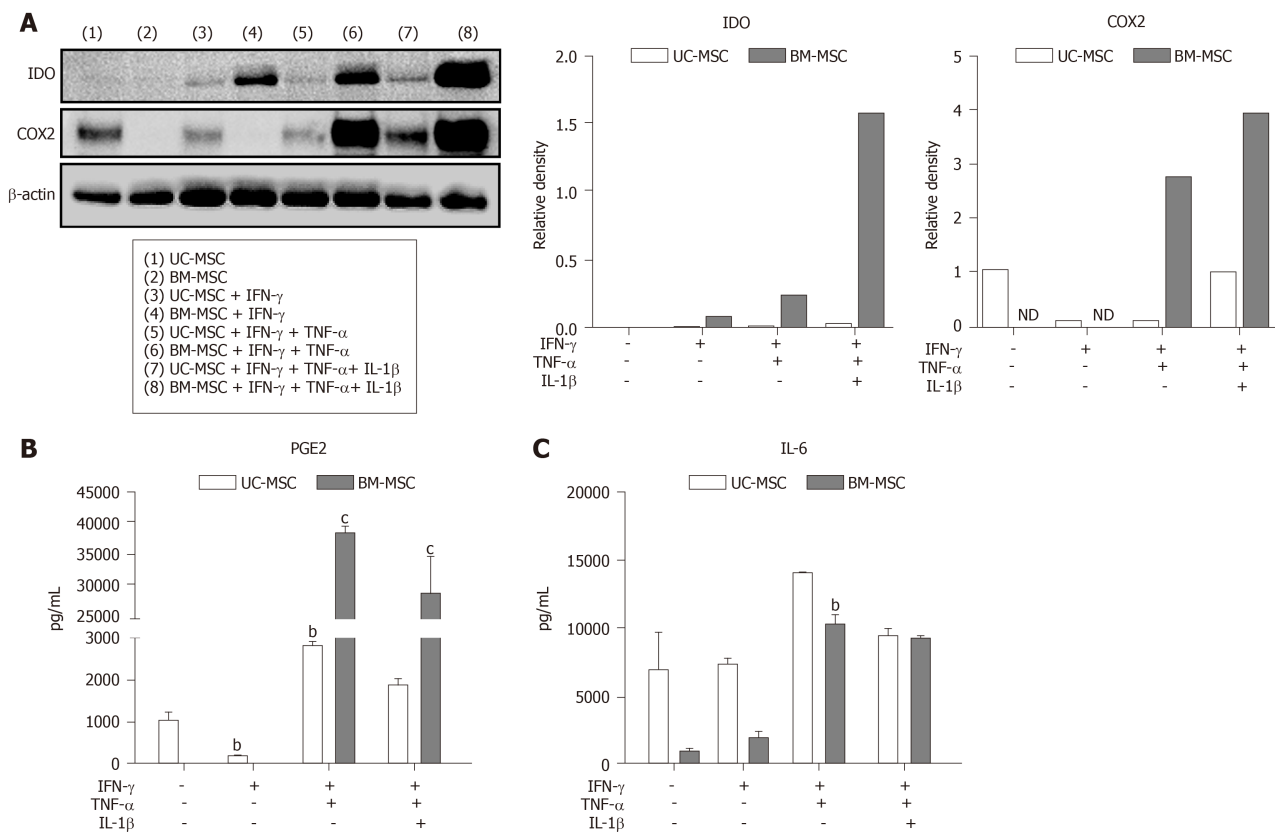


Figure 3 Immunomodulatory effects of mesenchymal stem cells treated with combinations of cytokines. Umbilical cord-derived mesenchymal stem cells and bone marrow-derived mesenchymal stem cells were stimulated with different combinations of interferon-gamma (5 ng/mL), tumor necrosis factor alpha (5 ng/mL), and/or IL-1 β (5 ng/mL) for 72 h. A: Expression levels of indoleamine 2,3-dioxygenase and cyclooxygenase-2 of cytokine-stimulated mesenchymal stem cells measured by western blotting; B and C: Expression levels of prostaglandin E2 (B) and interleukin-6 (C) in culture medium measured by ELISA. Statistical analysis was performed by Student's *t*-tests, ^a*P* < 0.05; ^b*P* < 0.01; ^c*P* < 0.0001 vs first bar of each group. (B and C) BM-MSC: Bone marrow-derived mesenchymal stem cells; IDO: Indoleamine 2,3-dioxygenase; IFN- γ : Interferon-gamma; IL-1 β : Interleukin 1 beta; IL-6: Interleukin 6; ND: Not detected; PGE2: Prostaglandin E2; TNF- α : Tumor necrosis factor alpha; UC-MSC: Umbilical cord-derived mesenchymal stem cells.

T cell inhibition

To test the immunosuppressive effects of the MSCs *in vitro*, we cultured phytohemagglutinin stimulated-human PBMCs in the presence of either UC-MSCs or BM-MSCs. When activated T cells were cocultured with MSCs, there was a decrease in T cell proliferation. Also, the immunosuppressive effects of UC-MSCs increased as the MSC-to-T cell ratio increased (Figure 4A). In the case of BM-MSCs, the immunosuppressive effects also tended to increase as MSC-to-T cell ratio increased; however, suppression effects of 20:1 and 10:1 were not significantly different (Figure 4A). Next, we inhibited various soluble factors with the respective inhibitors and assessed the effects on immunosuppressive activity. In both MSCs, the proliferation of T cells was recovered when cells were treated with indomethacin, which inhibits the COX2 pathway. This indicated that COX2 plays a critical role in the immunomodulation of MSCs. Another factor that restored T cell proliferation was anti-IL-10 (inhibitor of IL-10) in UC-MSCs and L-NAME (inhibitor of iNOS) in BM-MSCs. These findings suggested that UC-MSCs and BM-MSCs may regulate T cells through different pathways (Figure 4B).

Because IL-10 and PGE2 play important roles in the immunomodulatory effects of MSCs, we evaluated the effects of inhibiting PGE2 and/or IL-10 on the immunomodulatory functions of MSCs. Because PGE2 is produced *via* the COX2 pathway, we inhibited COX2 or/and IL-10 with indomethacin and anti-IL-10, respectively. In GVHD, the balance between T cell subpopulations, especially T helper cell 17 (Th17), Th1 and regulatory T cell (Treg) populations, is very important. Therefore, we investigated how the inhibition of these two factors affected MSCs to modulate Th17, Th1 and Treg populations. First, we cocultured phytohemagglutinin-activated T cells with MSCs and treated them with indomethacin and/or anti-IL-10 to assess the effects on IFN- γ -producing CD4⁺ T cells. Next, we induced Th17 and cocultured them with MSCs in the presence of each inhibitor to identify changes in

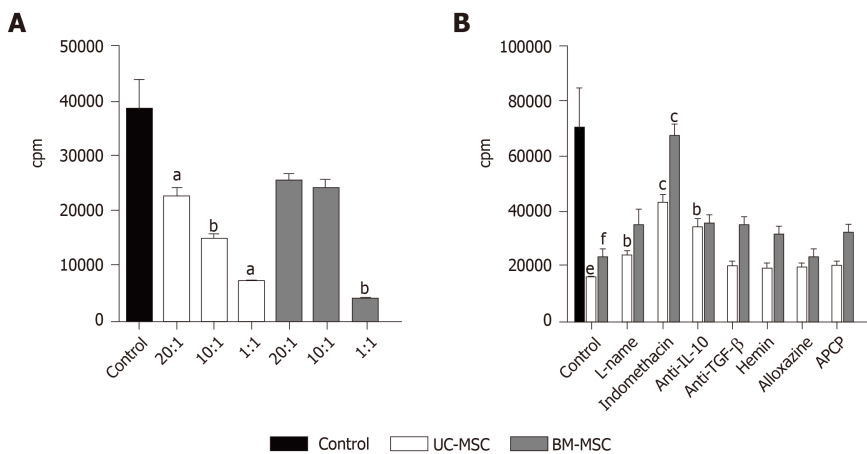


Figure 4 T cell inhibition by mesenchymal stem cells. T cell proliferation was inhibited by either umbilical cord-derived mesenchymal stem cells (MSCs) or bone marrow-derived MSCs in coculture. A: Human peripheral blood mononuclear cells (1×10^5 /well) from healthy adult donors were stimulated with phytohemagglutinin ($5 \mu\text{g/mL}$) with or without MSCs (5×10^3 , 1×10^4 , 5×10^4 , 1×10^5) for 72 h. In the final 18 h, ^3H -thymidine was added to the cultures, ^a $P < 0.05$; ^b $P < 0.01$; ^c $P < 0.0001$ vs control of each group, ^e $P < 0.01$; ^f $P < 0.0001$ vs control; and B: Human peripheral blood mononuclear cells were treated with L-NAME (iNOS inhibitor), indomethacin (cyclooxygenase-2 inhibitor), anti-IL-10, anti-transforming growth factor- β , hemin (heme oxygenase inducer), alloxazine (selective A_{2B} adenosine receptor antagonist), or adenosine 5'-(α,β -methylene)diphosphate (CD73 inhibitor) with or without MSCs for 72 h. In the final 18 h, ^3H -thymidine was added to the cultures. Statistical analysis was performed by Student's *t*-tests ^a $P < 0.05$; ^b $P < 0.01$; ^c $P < 0.0001$ vs control. Anti-IL-10: Anti-interleukin 10 antibody; Anti-TGF- β : Anti-transforming growth factor β antibody; APCP: Adenosine 5'-(α,β -methylene)diphosphate; BM-MSC: Bone marrow-derived mesenchymal stem cells; cpm: Count per minute; L-NAME: N-nitro-L-arginine methyl ester; UC-MSC: Umbilical cord-derived mesenchymal stem cells.

Th17 and Treg populations. In UC-MSCs, COX2 suppression increased the population of IFN- γ -producing CD4⁺ T cells and decreased the population of Treg cells. COX2 inhibition did not affect the population of IL-17-producing CD4⁺ T cells. In BM-MSCs, COX2 suppression increased the population of IFN- γ -producing and IL-17-producing CD4⁺ T cells. However, Treg cells were not affected. Through IL-10 inhibition, we concluded that IL-10 was more critical for UC-MSCs than BM-MSCs to suppress Th1 cells (Figure 5A and 5B).

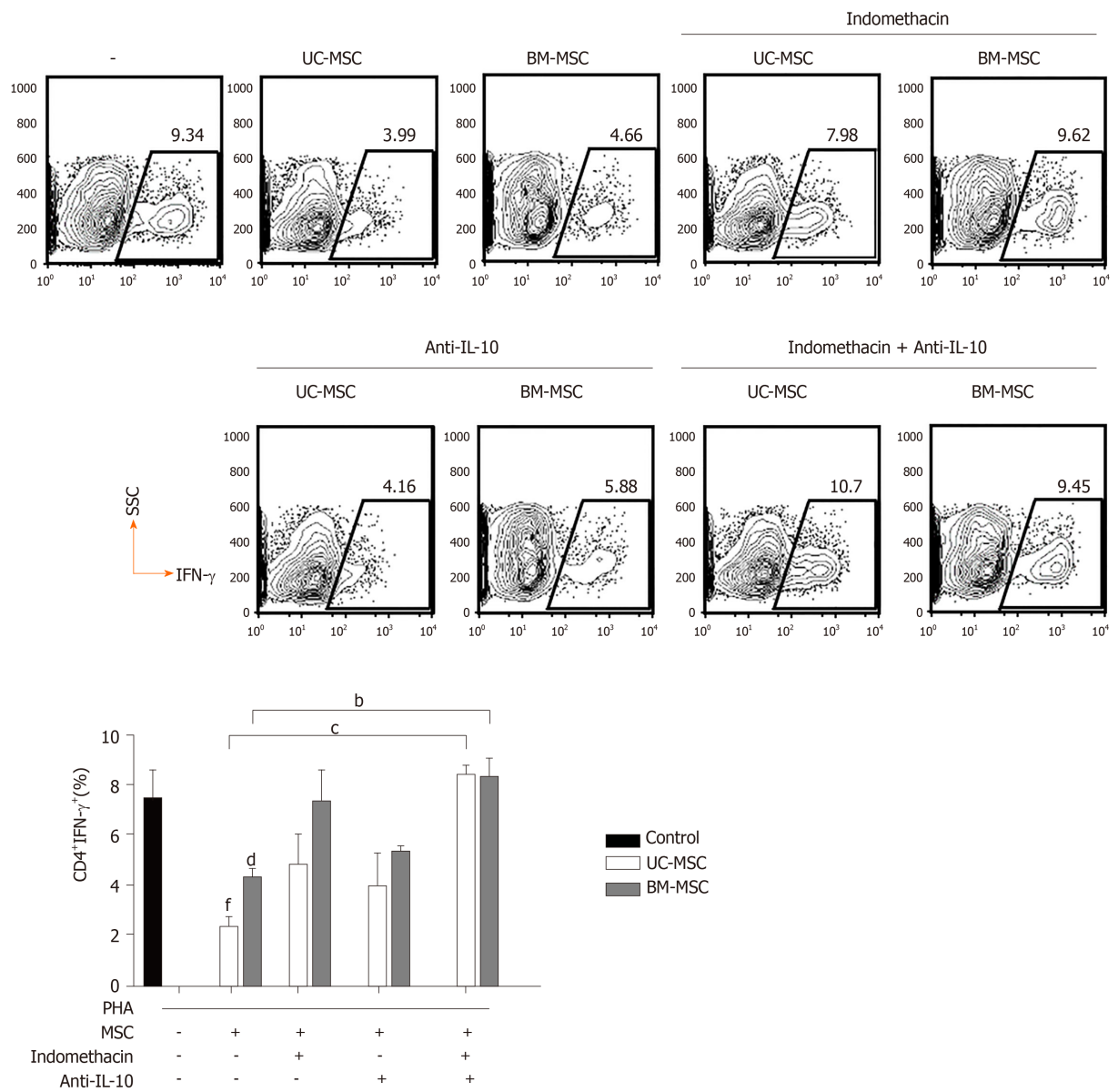
MSC therapy in a humanized GVHD mouse model

To assess the immunosuppressive activity of MSCs *in vivo*, we established a humanized GVHD mouse model in NOG mice that were exposed to a 200-cGy dose of radiation, and human PBMCs (2×10^7) were transferred intravenously to induce GVHD. At days 0, 7 and 14 after GVHD induction, mice were administered with UC-MSCs or BM-MSCs (1×10^5) for cell therapy. Mice were monitored at different time points after GVHD induction for survival, body weight and clinical GVHD scores. Figure 6 presents the combined results of two independent experiments under the same conditions. Most untreated GVHD-induced mice died between days 20 and 32. At 1 wk after the final death of untreated mice, survivors were treated with UC-MSCs (6/12) and BM-MSCs (8/12). MSC therapy significantly increased the survival rate (Figure 6A). Mice treated with MSCs also had less severe GVHD symptoms, such as declines in weight, activity, posture, fur texture and skin integrity (Figure 6B and 6C).

DISCUSSION

The use of MSCs to treat various diseases has been gaining popularity due to their immunosuppression abilities. Studies have shown that MSCs play a critical role in injury healing^[16,25], Crohn's disease^[26], systemic lupus erythematosus^[27] and rheumatoid arthritis^[28]. MSC therapy has been applied for many years to treat GVHD, which is a lethal disease occurring after allogeneic hematopoietic stem cell or organ transplantation. Several treatments, such as steroids with or without calcineurin inhibitors, are used to treat GVHD, but newer therapies are needed due to the poor prognosis of current methods. Since Le Blanc *et al*^[11] first reported that adult BM-MSCs were effective in treating severe treatment-resistant grade IV acute GVHD, many clinical trials have confirmed the potential of MSC therapy for GVHD. Given these promising results, MSCs have been derived from various sources, such as adipose tissue, molar cells, amniotic fluid and umbilical cords. However, it remains unclear which source is best, or how MSCs of different sources regulate other cells^[29]. Recently,

A



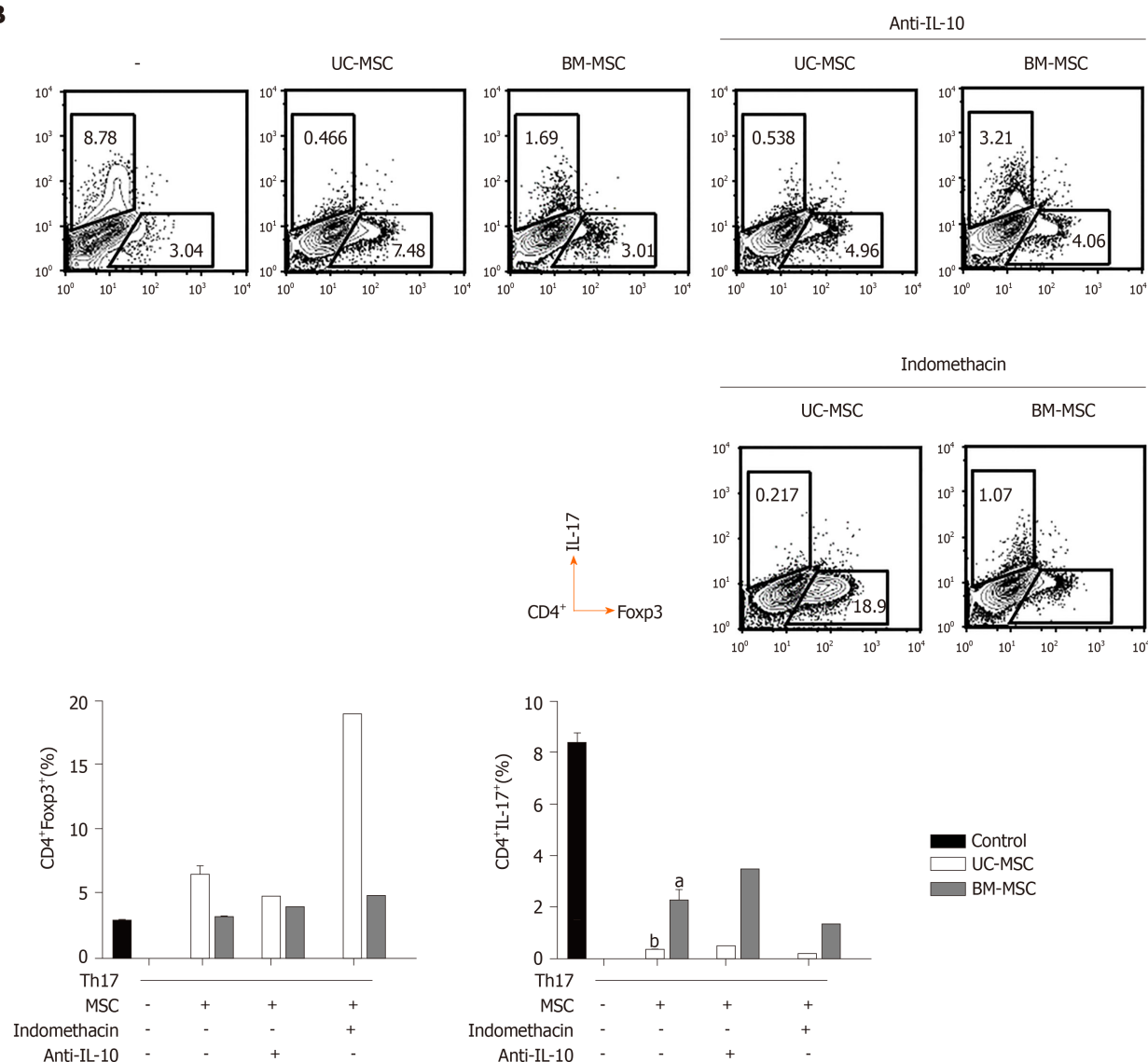
B

Figure 5 Roles of prostaglandin E2 and interleukin-10 in the immunomodulatory functions of mesenchymal stem cells. A: Human peripheral blood mononuclear cells were stimulated with phytohemagglutinin (10 μ g/mL) and cocultured with mesenchymal stem cells treated with indomethacin (20 μ M) and/or anti-interleukin (IL)-10 (5 μ g/mL). Then, interferon-gamma-producing CD4⁺ T cells were analyzed by flow cytometry, ^a $P < 0.05$; ^b $P < 0.01$ vs first bar; B: Human peripheral blood mononuclear cells were treated with anti-interferon-gamma (10 μ g/mL), anti-IL-4 (10 μ g/mL), IL-6 (10 ng/mL), IL-23 (5 ng/mL), IL-1 β (10 ng/mL), tumor necrosis factor alpha- α (5 ng/mL) and transforming growth factor- β (2 ng/mL) to induce T helper 17 cells. Induced T helper 17 cells were cocultured with mesenchymal stem cells treated with indomethacin (20 μ M) and/or anti-IL-10 (5 μ g/mL). Populations of CD4⁺Foxp3⁺ T cells and CD4⁺IL-17⁺ T cells were analyzed by flow cytometry. Statistical analysis was performed by Student's *t*-tests, ^a $P < 0.05$; ^b $P < 0.01$; ^c $P < 0.0001$ vs indicated group, ^d $P < 0.05$; ^e $P < 0.0001$ vs phytohemagglutinin control. Anti-IL-10: Anti-interleukin 10 antibody; BM-MSC: Bone marrow-derived mesenchymal stem cells; IFN- γ : Interferon-gamma; IL-17: Interleukin 17; MSC: Mesenchymal stem cells; PHA: Phytohemagglutinin; Th17: T helper 17; UC-MSC: Umbilical cord-derived mesenchymal stem cells.

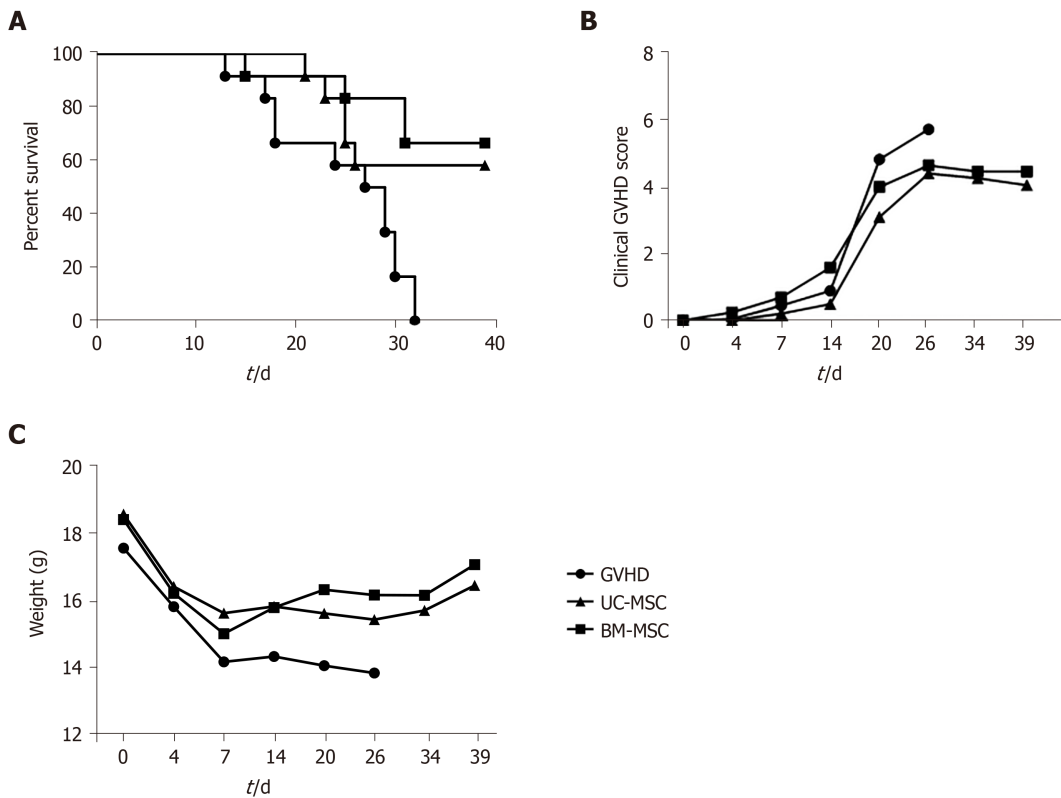


Figure 6 Inhibitory effects of mesenchymal stem cells therapy on graft-versus-host disease severity. A-C: NOG mice were administered 200 cGy of total body irradiation before transplantation of human peripheral blood mononuclear cells (2×10^7). At days 0, 7 and 14 after transplantation, mice were administered with umbilical cord-derived mesenchymal stem cells or bone marrow-derived mesenchymal stem cells (1×10^5). All NOG mice were monitored for survival (A), clinical signs of graft-versus-host disease (B) and weight (C). BM-MSC: Bone marrow-derived mesenchymal stem cells; GVHD: Graft-versus-host disease; UC-MSC: Umbilical cord-derived mesenchymal stem cells.

UC-MSCs have gained attention for their ease of collection from a young source.

In this study, we compared UC-MSCs and BM-MSCs not only to find the difference in degree of immunoregulation but also to discover the difference in factors affecting immunoregulation. Specifically, we compared the phenotypic and functional features of human UC-MSCs and human BM-MSCs. Our findings demonstrated that UC-MSCs and BM-MSCs share similar phenotypic characteristics and immunomodulation capacities. Furthermore, we suggest that UC-MSCs and BM-MSCs may suppress activated immune systems *via* different pathways.

Early studies emphasized the critical roles of chemokines and their receptors in the migration of MSCs to sites of injury. For example, interactions between stromal cell-derived factor-1 and CXCR4 and between monocyte chemoattractant protein-1 and CCR2 regulate the migration of MSCs *in vitro*^[30,31]. In this study, our data showed that UC-MSCs and BM-MSCs share similar immunophenotypic characteristics and chemokine receptors. In addition, they possess similar abilities to differentiate into adipocytes, osteocytes and chondrocytes. Moreover, the expression levels of pluripotency transcription factors such as *Klf4*, *OCT4* and *Nanog* are similar between UC-MSCs and BM-MSCs. Our results provide evidence that UC-MSCs and BM-MSCs share similar phenotypic characteristics.

MSCs have enhanced immunosuppressive effects under acute inflammatory conditions, especially in the presence of the pro-inflammatory cytokine IFN- γ ^[5]. As expected, exposure to IFN- γ increased the expressions of IDO in both UC-MSCs and BM-MSCs. However, BM-MSCs produced more IDO than UC-MSCs with stimulation by IFN- γ .

Previous studies have claimed that combinations of cytokines upregulate IDO and COX2 levels in MSCs. For instance, upregulated IDO activity of TNF- α - and IFN- γ -activated MSCs differentiated monocytes into IL-10-secreting M2 immunosuppressive macrophages, which suppress T cell proliferation^[32]. Another study observed that the induction of IDO in MSCs was regulated by IFN- β and IFN- γ ^[33]. Finally, IL-1 β has also been shown to induce COX2^[34]. In this study, we treated MSCs with diverse combinations of cytokines and assessed factors representing the immunosuppressive activity of MSCs. BM-MSCs expressed more upregulated IDO and COX2. However, UC-MSCs secreted high levels of IL-6 compared to BM-MSCs. UC-MSCs expressed low levels of IL-6 even without stimulation and high levels with cytokine stimulation. Paradoxically, while IL-6 is mostly known as a pro-inflammatory cytokine, it is also an anti-inflammatory cytokine in terms of maintaining the immunosuppressive capacity of MSCs^[35]. When MSCs are differentiated, IL-6 is downregulated, which leads to loss of immune privilege in MSCs^[36]. At the same time, IL-6 is claimed as a critical factor for maintaining the stemness of MSCs. Thus, the role of IL-6 in MSCs is to enhance MSC proliferation, protect MSCs from apoptosis and inhibit differentiation^[37]. Based on our findings, we speculate that high levels of IL-6 in UC-MSCs are involved in suppressive effects.

Li *et al*^[38] suggested that overexpression of IL-6 in tumor tissue enhanced PD-L1 expression, suggesting that the high levels of IL-6 in UC-MSCs might be related to the higher levels of PD-L1 and PD-L2 in UC-MSCs than BM-MSCs. In tumor tissue, PD-L1 acts as a ligand of PD-1 expressed in T cells, inhibiting anti-tumor effects^[39]. Therefore, much like PD-L1 in tumor tissue suppresses T cells *via* PD-1, UC-MSCs may inhibit T cell proliferation through the PD-1/PD-L1 pathway.

Although the Th1-mediated response is considered a main contributor to the induction of GVHD, Th17 cells are also capable of developing lethal GVHD^[40]. Also, it is well known that imbalances between Th17 and Treg cells affect the severity of GVHD^[41]. In this study, we demonstrated that UC-MSCs and BM-MSCs effectively suppressed Th1 and Th17 cells and induced Treg cells.

In conclusion, we have demonstrated that UC-MSCs and BM-MSCs share similar phenotypic characteristics and immunomodulation abilities. Moreover, cytokine stimulation enhances the immunomodulation of both MSCs, although UC-MSCs and BM-MSCs exhibit different tendencies toward expression of IDO, COX2, PGE2, IL-6, PD-L1 and PD-L2. These findings suggested that UC-MSCs and BM-MSCs may induce immunosuppression *via* different pathways. High expression of IDO and COX2 in BM-MSCs suggests that these two factors are involved in T cell suppression. Meanwhile, high expression of IL-6, PD-L1 and PD-L2 in UC-MSCs suggests that UC-MSCs inhibited T cell proliferation through cell-to-cell contact *via* the PD-1/PD-L1 pathway. Finally, we demonstrated that treating a GVHD mouse model with MSCs improved the clinical score, survival and weight loss of irradiated mice. Interestingly, the mechanisms by which UC-MSCs and BM-MSCs alleviated GVHD seemed to differ, but their ability to attenuate GVHD in a mouse model was overall similar. Taken together, these findings underscore the need for future studies to identify the

mechanisms of immunosuppression of different types of MSCs and further studies in mechanisms of MSCs may allow advanced MSC therapy in clinical use.

ARTICLE HIGHLIGHTS

Research background

Mesenchymal stem cells (MSCs) are a promising therapeutic approach to treat graft-versus-host disease (GVHD) because of their immunoregulatory properties. Until recently, human bone marrow-derived MSCs (BM-MSCs) were used widely as cell therapy sources. However, the needs for new source of MSCs are growing due to the invasive collection method and decrease in donors. Among many other adult and fetal tissues, human umbilical cord has emerged as a promising source of MSCs because of their ethical and noninvasive collection.

Research motivation

Although several studies have pointed out the potential of human umbilical cord-derived MSCs (UC-MSCs), the difference in immunomodulatory effects and mechanisms of BM-MSCs and UC-MSCs should be examined in greater detail.

Research objectives

In this study, we aim to investigate the difference in mechanisms of the immunosuppressive effects of UC-MSCs and BM-MSCs.

Research methods

Western blot, quantitative real-time polymerase chain reaction and luminex multiplex cytokine assay were employed to examine the expression of soluble factors after MSCs were primed with different combinations of interferon-gamma, tumor necrosis factor alpha and interleukin (IL)-1 β , or interferon-gamma alone. Human peripheral blood mononuclear cells stimulated with phytohemagglutinin were cocultured with MSCs to examine the immunosuppressive effects of the MSCs *in vitro*. Several inhibitors of soluble factors were used to identify which soluble factors played critical roles in the immunomodulation of MSCs. Lastly, xenogeneic GVHD was induced in NOG mice (NOD/Shi-scid/IL-2R γ null) and UC-MSCs or BM-MSCs were used as cell therapies.

Research results

BM-MSCs and UC-MSCs shared similar phenotypic characteristics and immunosuppressive effects. COX2 and IL-10 were key factors in the immunomodulatory mechanisms of both MSCs. However, upon *in vitro* cytokine stimulation, BM-MSCs expressed more indoleamine 2,3-dioxygenase, and UC-MSCs expressed more prostaglandin E2, IL-6, PD-L1 and PD-L2. UC-MSCs and BM-MSCs established different T cell subpopulations when cultured with stimulated T cells. UC-MSCs inhibited more T helper 17 cells and induced more regulatory T cells than BM-MSCs. In a humanized GVHD mouse model, UC-MSCs and BM-MSCs showed comparable effects in attenuating GVHD.

Research conclusions

Our data provides a deeper understanding in similarities and differences between UC-MSCs and BM-MSCs. This study demonstrated that UC-MSCs and BM-MSCs exhibited similar immunosuppression in different mechanisms. Also, this study introduced that UC-MSCs have the potential to substitute for BM-MSCs as cell therapy products.

Research perspectives

In summary, we have demonstrated that UC-MSCs and BM-MSCs exhibit different tendencies toward expression of proteins known to contribute to immunosuppression although they share similar phenotypic characteristics and immunomodulation abilities. Our data also suggest that UC-MSCs and BM-MSCs induced immunosuppression through different pathways underscoring the need for future studies to identify detailed mechanisms of MSCs derived from different sources.

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